



Diastolic Activation Dynamics in the Phase Plane

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APS March Meeting

Indianapolis, IN

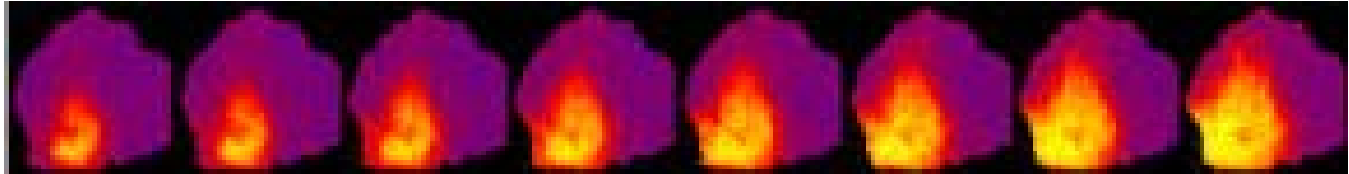
March 18-22, 2002



Temporal Response of Cardiac Tissue to Point S1 and Field S2

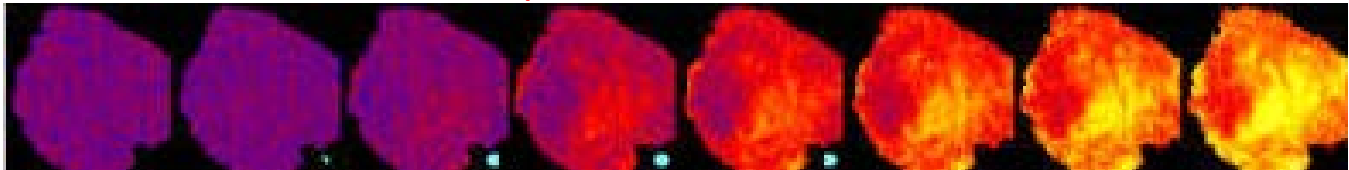
Normal, propagated activation

Point S1



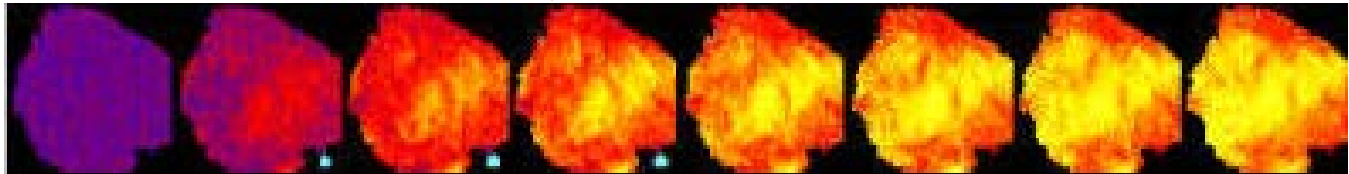
Prompt, distributed activation

10V/cm S2



Faster, distributed activation

40V/cm S2



Question: How best to quantify the differences in the three responses?



Statement of the Problem

- The response of cardiac tissue to strong electrical stimulation is critical to understanding the defibrillation process.
- Theory predicts that tissue heterogeneities will produce localized regions of depolarization and hyperpolarization (**virtual cathodes** and **virtual anodes**).
- In studying the response of resting cardiac tissue to field stimulation, we observed multiple **VC**s but neither **VA**s nor the expected **VC-VA** pairs, and we saw distributed heterogeneous activation that was faster for stronger shocks.



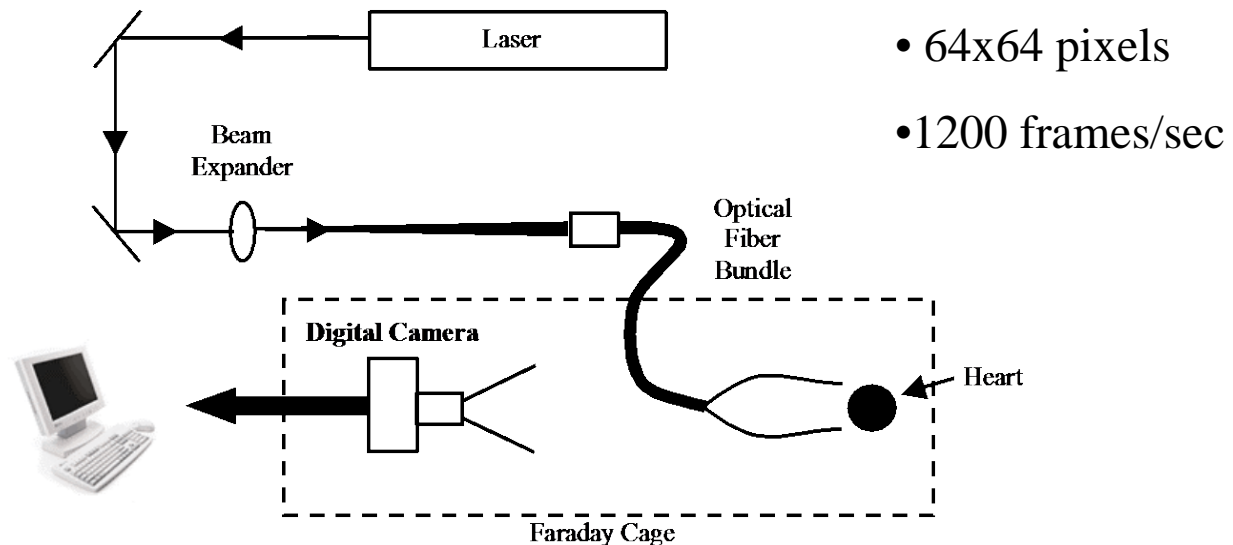
Statement of the Problem

- Optical fluorescence data are typically viewed in the spatio-temporal plane.
- Phase-plane techniques are useful in studies of the dynamics of cardiac reentry and fibrillation.
 - Gray, R. A., Pertsov, A. M., and Jalife, J., "Spatial and temporal organization during cardiac fibrillation," *Nature*, **392**: 75-78, 1998.
 - Bray, M.-A., Lin, S.-F., Aliev, R. R., Roth, B. J., and Wikswo, J. P., Jr., "Experimental and theoretical analysis of phase singularity dynamics in cardiac tissue," *Journal of Cardiovascular Electrophysiology*, **12**: 716-722, 2001.
- In this presentation, we describe phase-space imaging techniques that highlight key differences between **VC** and **VA** response during strong stimuli.



Methods

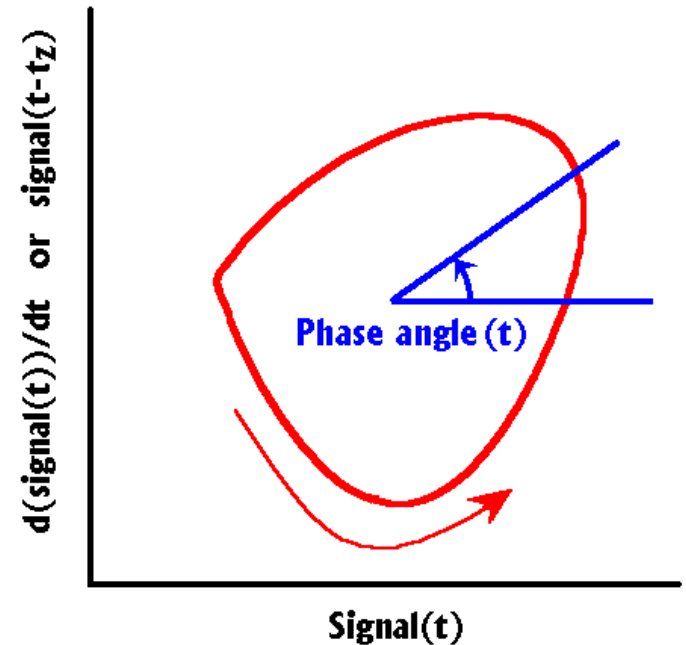
- Dye fluorescence imaging of transmembrane potential allows characterization of shock-tissue interaction.
- Isolated rabbit hearts are Langendorff-perfused and stained with the fluorescent dye, di-4-ANEPPS.
- Illumination is achieved by a diode-pumped solid state laser.
- Images are acquired with a 12-bit Dalsa CCD camera.





Data Pre-Processing for Phase Space

- The data are spatially filtered using a 3x3 Gaussian filter with a standard deviation of one.
- No temporal filtering is utilized.
- The data are then normalized pixel-by-pixel by dividing by the pixel maximum response to S1.
- Phase space plots are developed by plotting the data against a time delayed version of itself. Unless otherwise noted, a time delay of 8 frames (6.66 ms) is used.



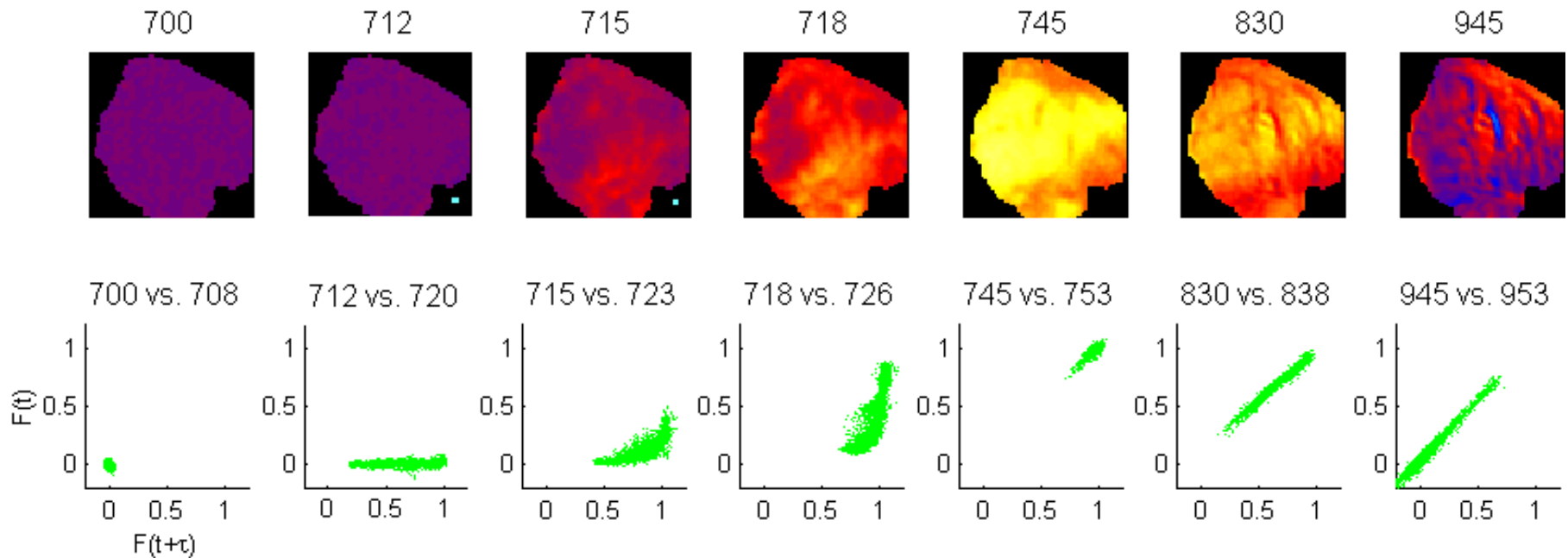


Voltage and Phase Plane Movies

Endocardial isolated right ventricle data

S2 = 5 V/cm field shock

0.83 ms/frame

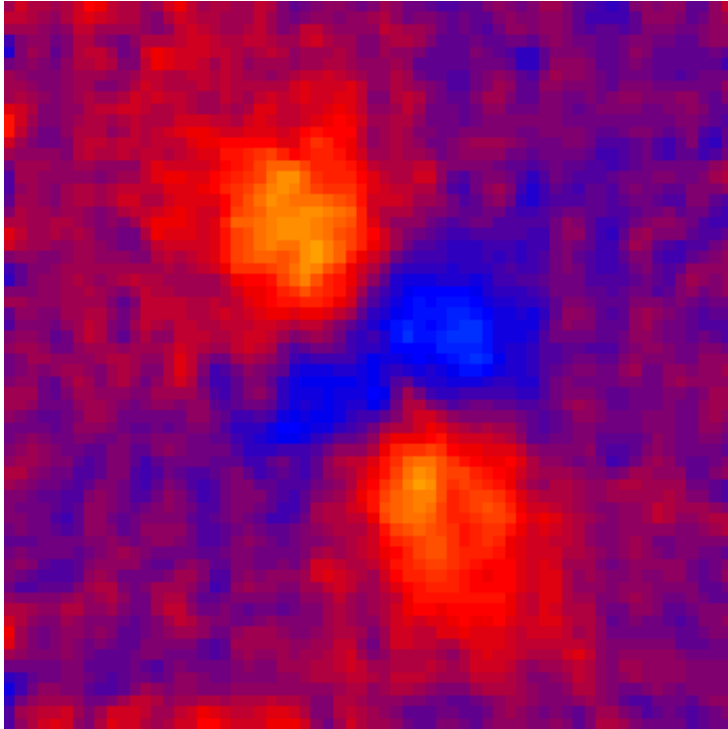


rv_5Vcm_swarm.mov



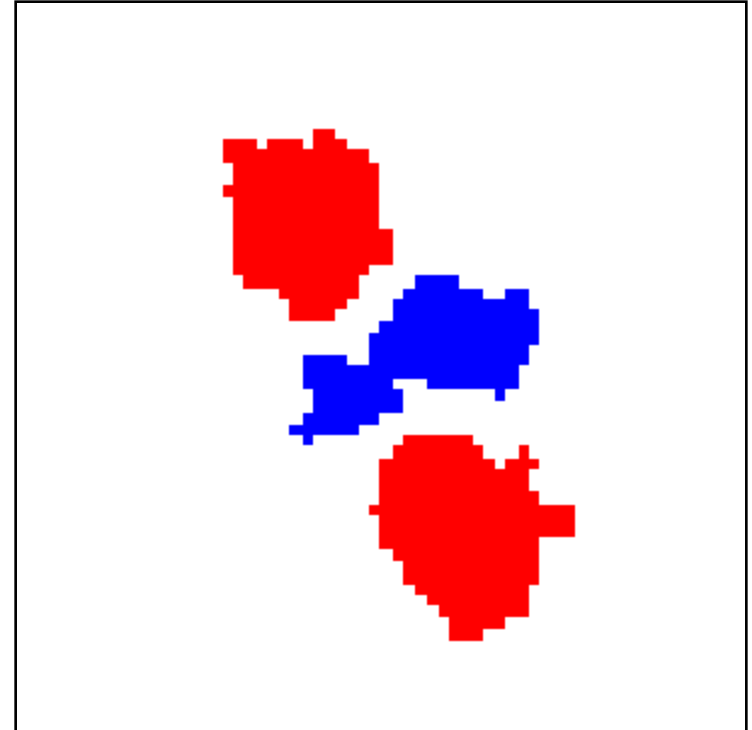


Virtual Electrode: Proof of Concept



Anodal Diastolic Point Stimulation

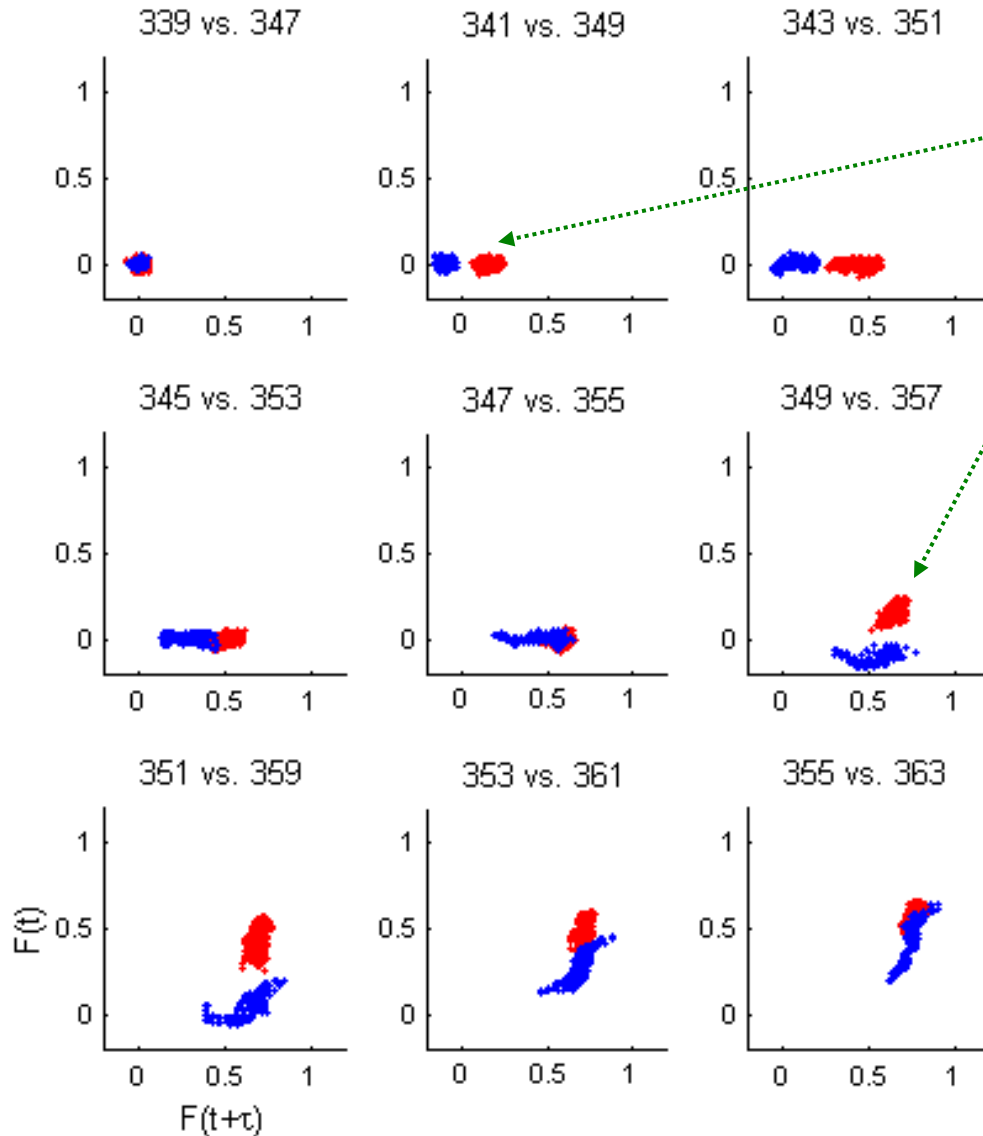
- 4 ms duration
- 20 mA
- S1-S2 coupling interval 330 ms



Threshold normalized
voltage to demarcate
Virtual Cathodes and
Virtual Anodes



Virtual Electrode Phase Plane Movie



Hyperpolarization denoted by blue movement to the left and downward

Red – cathode pixels

Blue – anode pixels

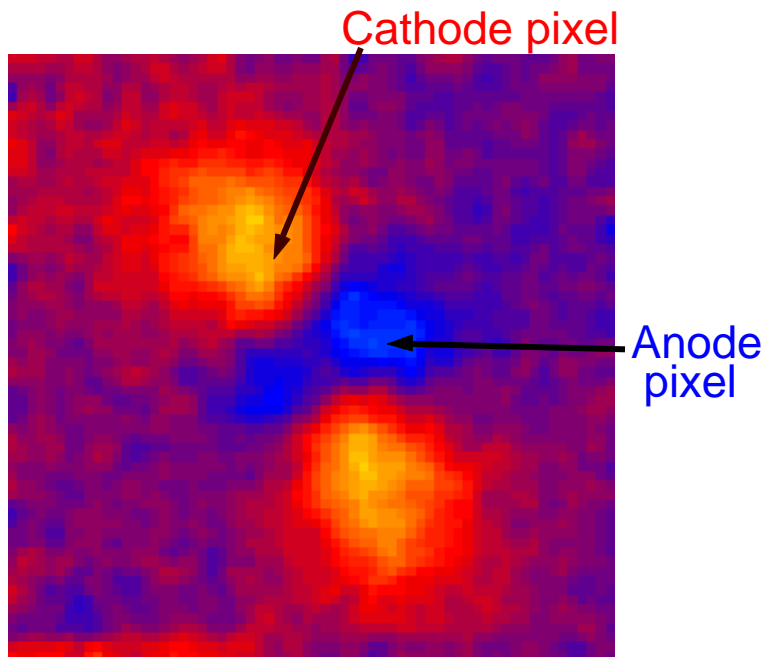


anode_cathode_multiplepixels_lag8.mov

Visualization in phase space clearly delineates **VC** and **VA** responses

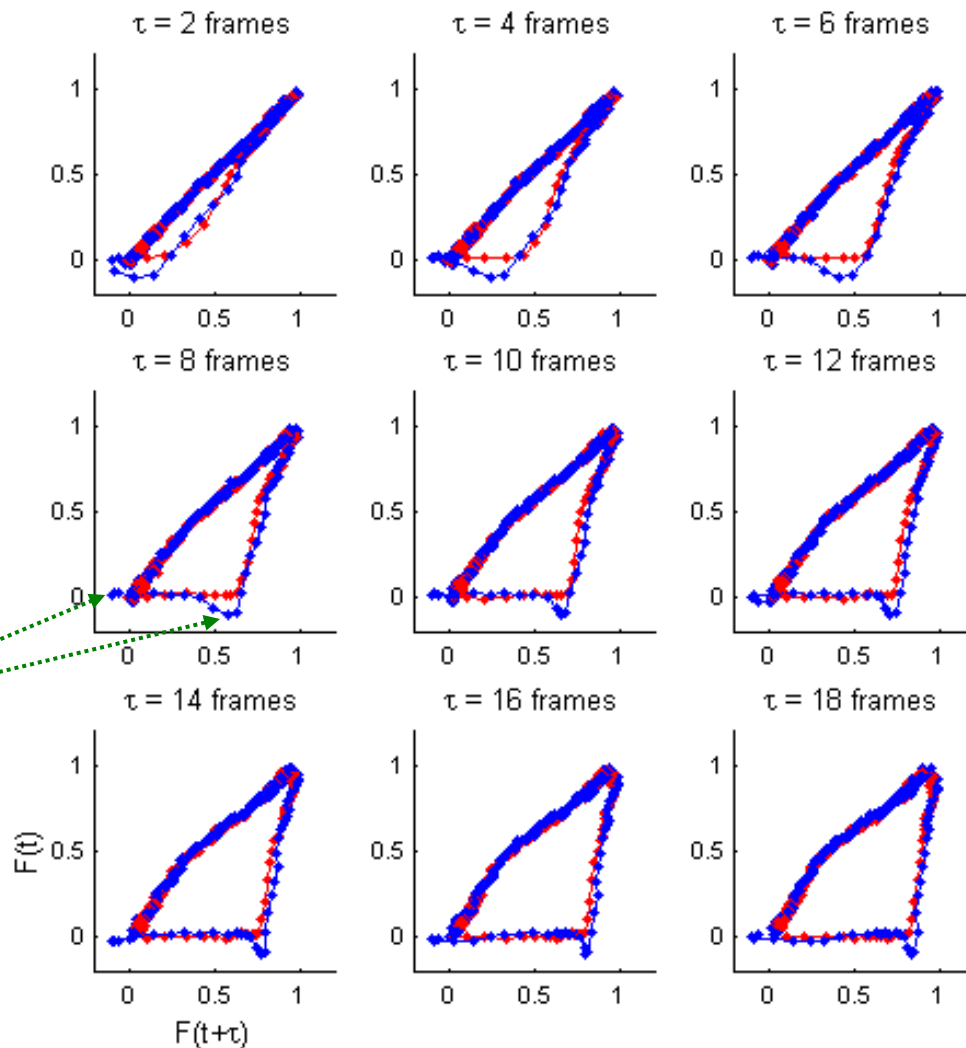


Dependence upon Lag



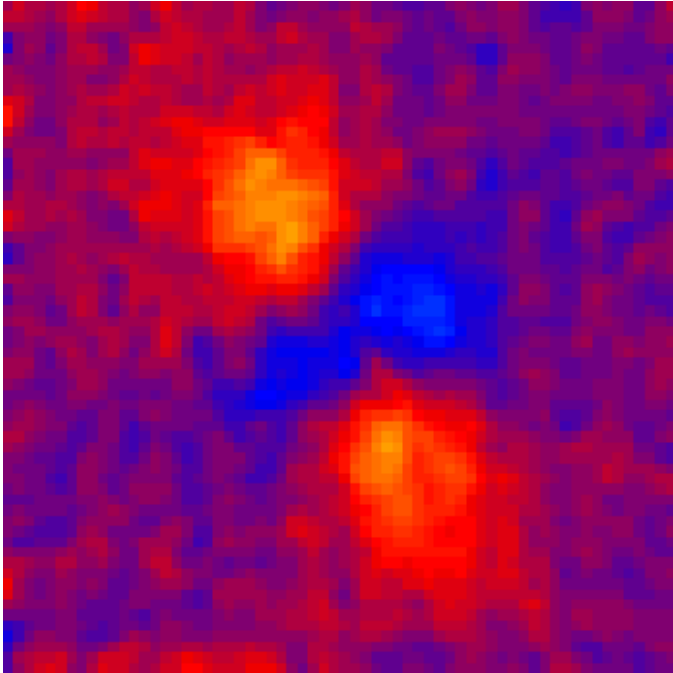
- Blue movement left and downward reveals hyperpolarization

- Within limits, trajectory topology is not sensitive to lag choice



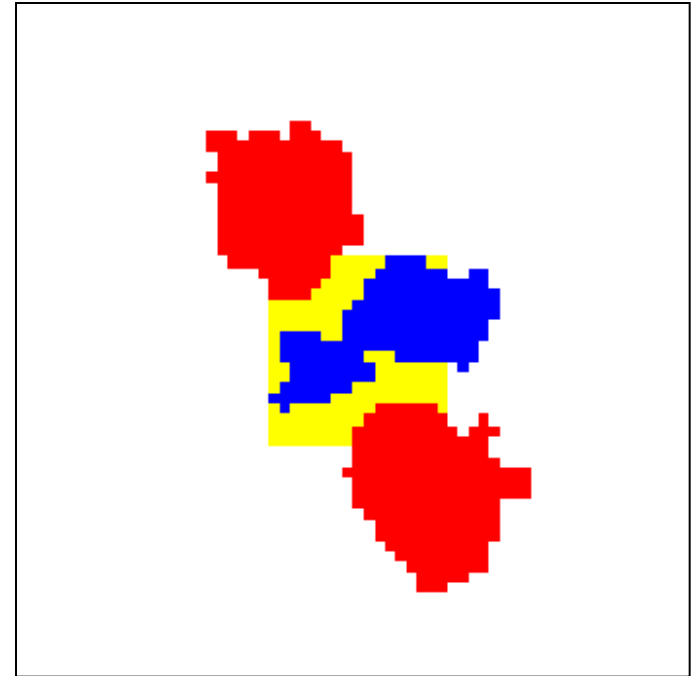


Virtual Electrode and Border Region



Anodal Diastolic Point Stimulation

- 4ms duration
- 20mA
- S1-S2 coupling interval 330ms



Threshold normalized voltage to demarcate **Virtual Cathodes** and **Virtual Anodes** and identify **Border Regions**



Virtual Electrode Phase Plane Movie

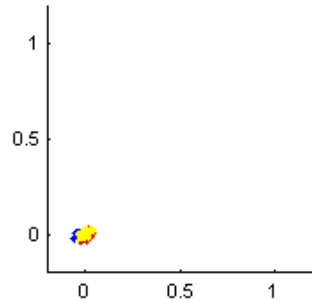
Red – cathode pixels

Blue – anode pixels

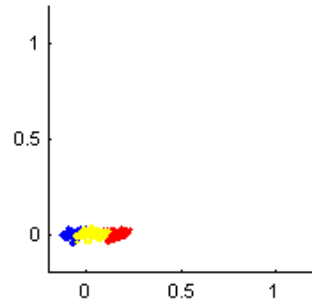
Yellow – border pixels

Phase plane characteristics of border regions are intermediate between those of VC and VA.

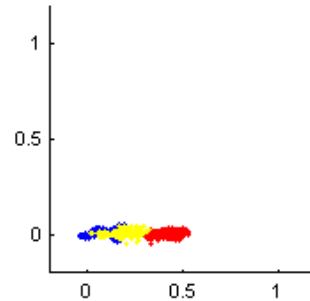
339 vs. 347



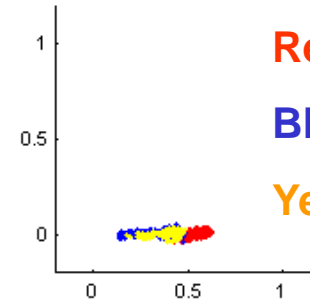
341 vs. 349



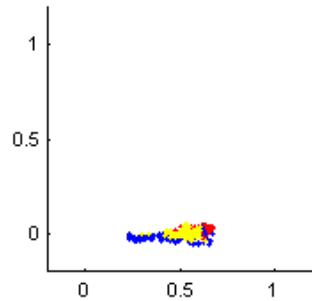
343 vs. 351



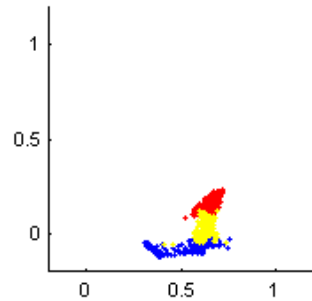
345 vs. 353



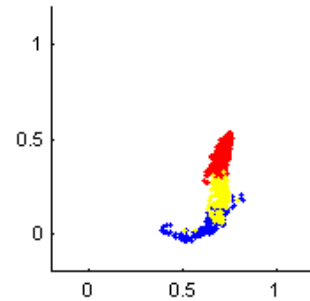
347 vs. 355



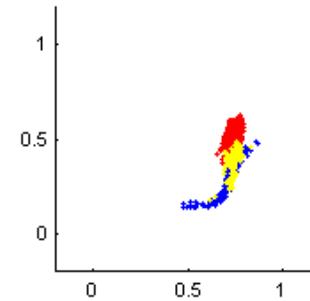
349 vs. 357



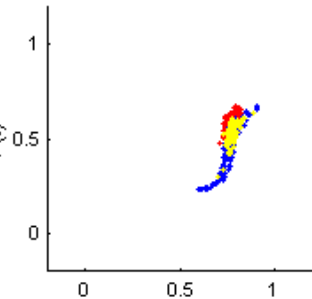
351 vs. 359



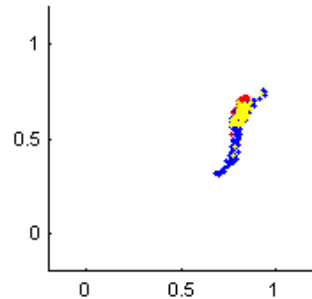
353 vs. 361



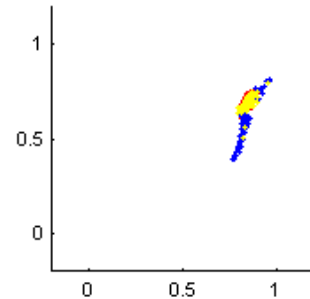
355 vs. 363



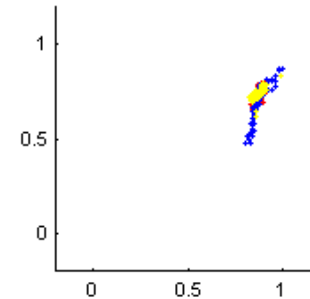
357 vs. 365



359 vs. 367



361 vs. 369



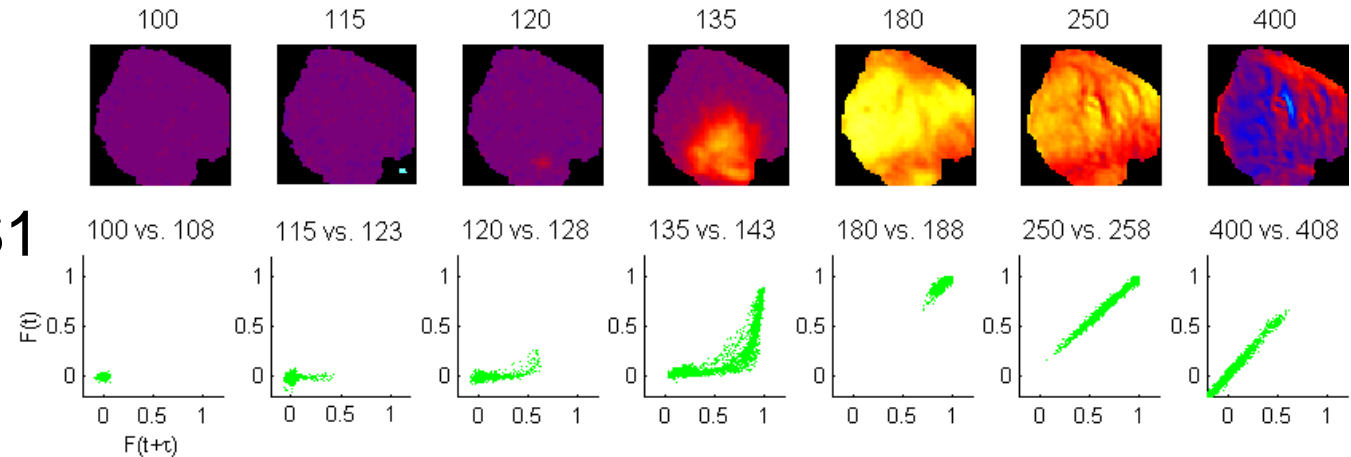
$F(t)$



Point S1-Field S2

Voltage and Phase Plane Movies

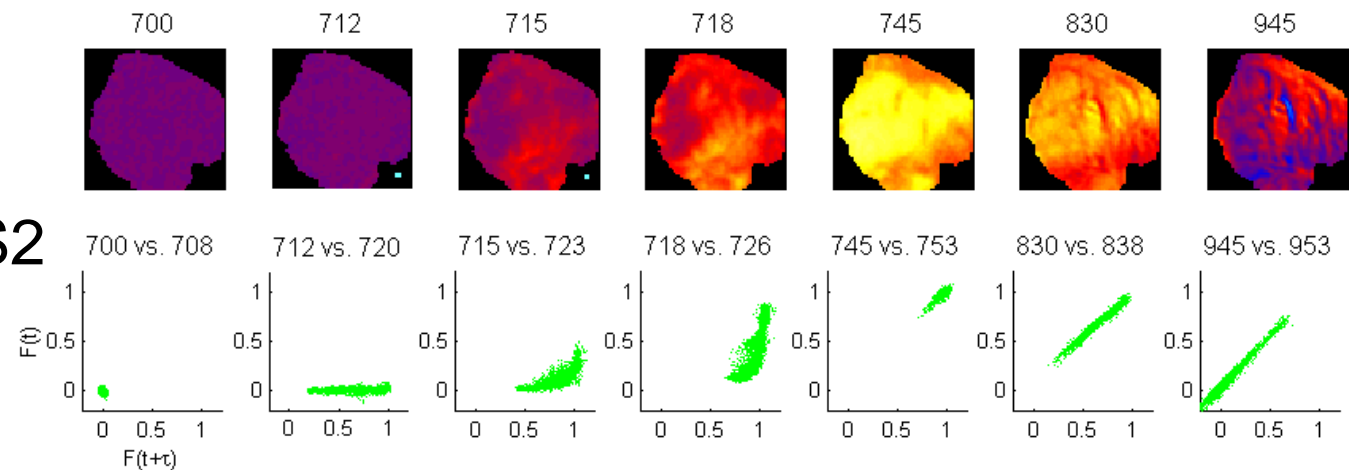
Point S1



Endocardial isolated
right ventricle data

0.83 ms/frame

5 V/cm S2



rv_5Vcm_swarm.mov





Point S1-Field S2

Activation Dynamics in Phase Space

Single Endocardial Pixel Dynamics

$S2 = 40 \text{ V/cm}$

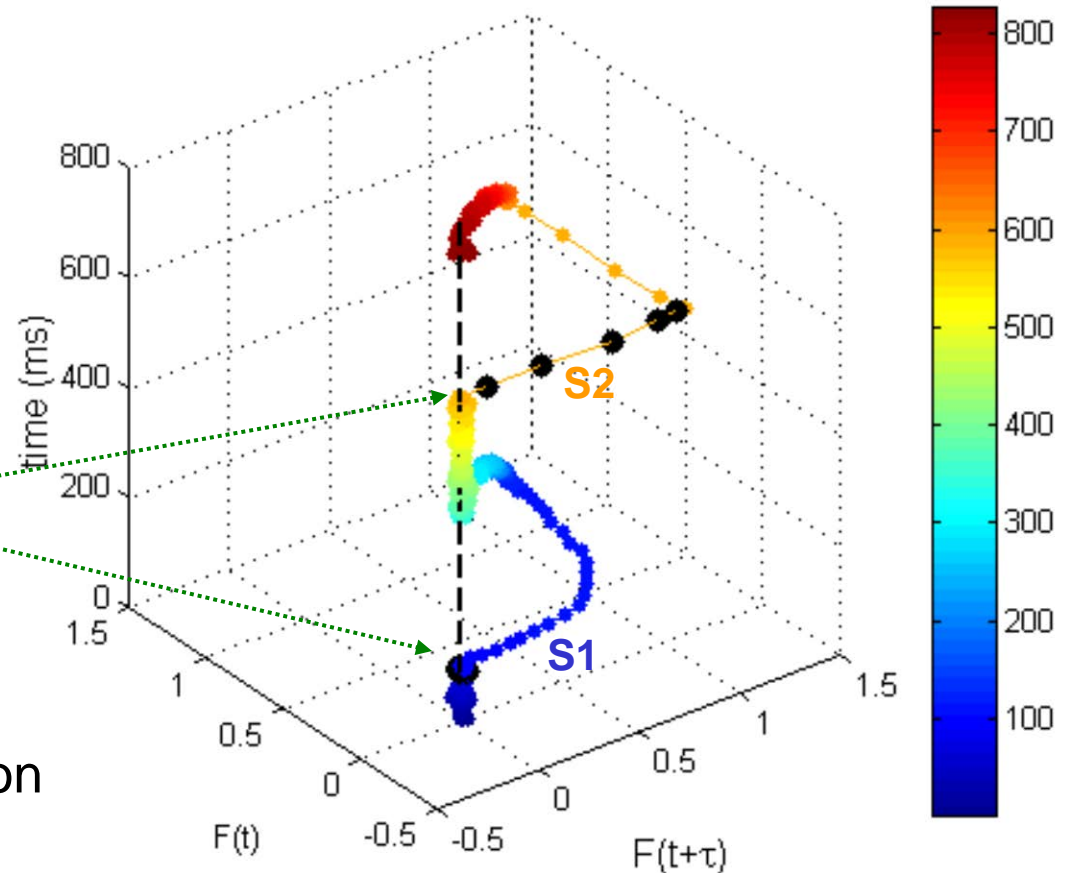
$\tau = 8 \text{ frames}$

- Isolated right ventricle preparation

- 2 ms S1 point stimulation
- 2 ms S2 field stimulation
- S1-S2 coupling interval 500 ms

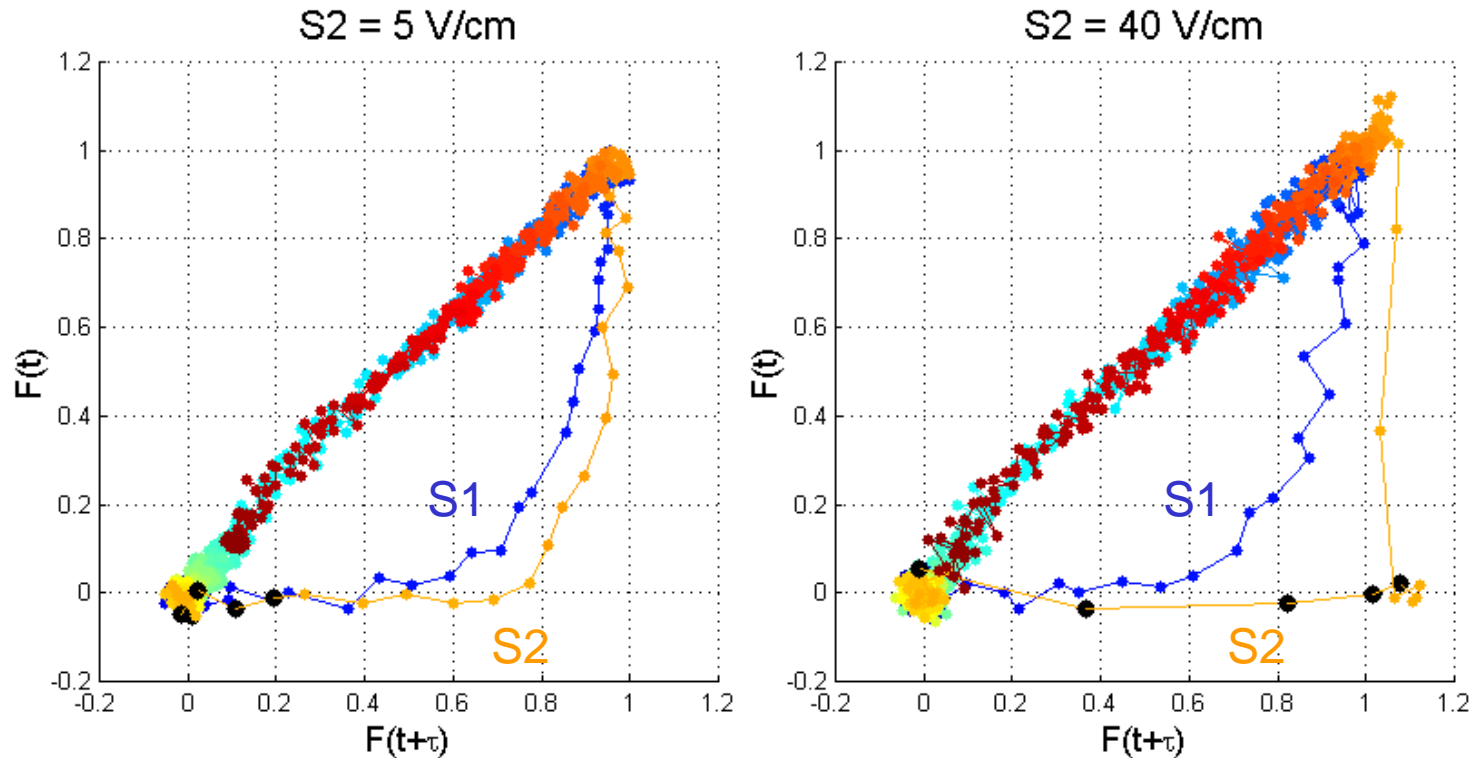
Larger black pixels ● indicate stimuli timing.

Strong field S2 reveals much more rapid change in comparison with point S1.

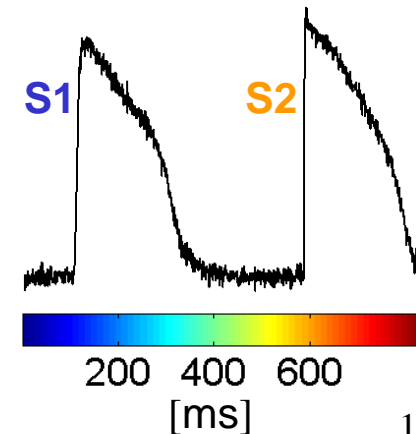




Endocardial Activation Dynamics



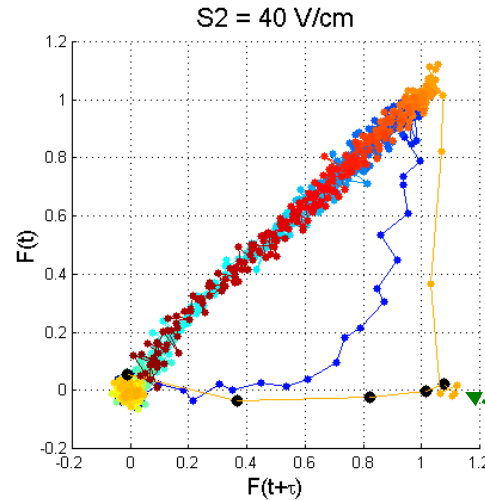
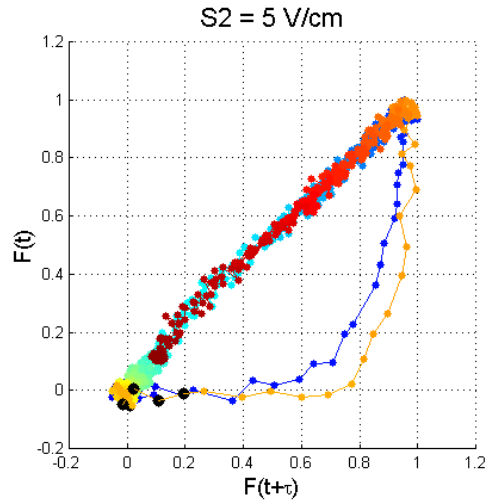
- Faster activation with stronger S2 shock strength
- S1 trajectory lies within S2 trajectory
- S1 and S2 repolarization trajectories are the same



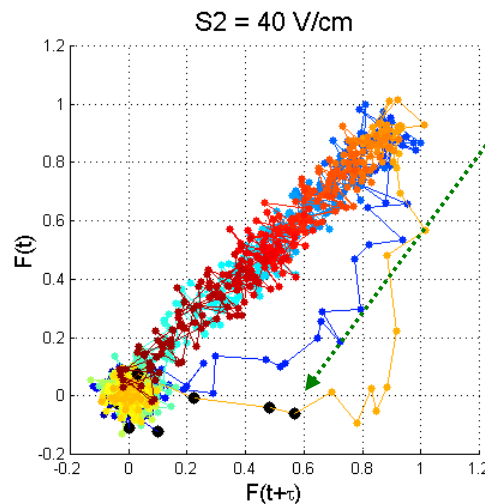
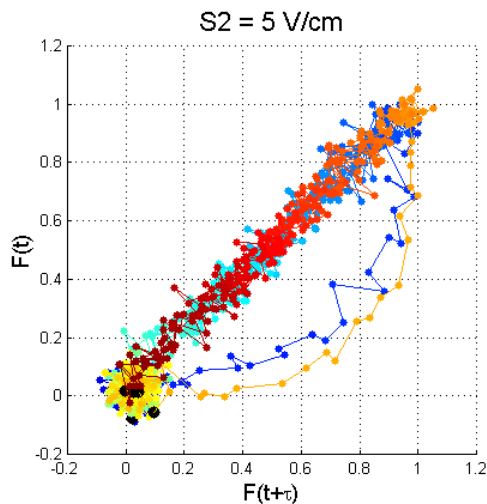


Endocardial and Epicardial Activation Dynamics

Endocardium



Epicardium



Endocardium
activates faster
than epicardium.



Observations

- Activation and repolarization stages are clearly delineated in phase space.
- **Virtual cathodes**, **virtual anodes**, and **border regions** are uniquely characterized in phase space.
- Faster response due to stronger field shock is obvious in phase space plots.
- Repolarization after point and field stimulation follows the same path in phase space.
- Point stimulation trajectories lie within field stimulation trajectories in phase space plots.



Conclusions

- We originally developed this approach to search through large amounts of point-S1/field-S2 right ventricle data to identify any small, localized regions of hyperpolarization that we did not detect with conventional spatio-temporal imaging.
- We have not yet observed any hyperpolarization in phase space from diastolic field shocks.
- We recognize that this approach is useful for comparing cardiac response to different shocks.
 - Krinsky, VI and Pumir, A. “Models of Defibrillation of Cardiac Tissue,” *Chaos*, **8**: 188-203, 1998.



Future Work

- We have shown *qualitatively* that the details of diastolic activation dynamics are highlighted in phase space. However there is also great potential to extend this approach to *quantitative* phase space measurement:
 - Rise time calculation as the slope of the upstroke in phase space
 - Measurement of phase space trajectory area as a function of shock strength
 - Maximum dV_m/dt can be determined by computing the maximum Euclidean distance traveled in one time step in phase space
- In the virtual electrode phase space movies, we showed that the **virtual anode**, **virtual cathode**, and **border regions** have different phase space characteristics. Thus the dynamics in phase space can be used to back-project into physical space to delineate between regions of different activation dynamics.
- We will explore the use of the phase plane to predict shock response.

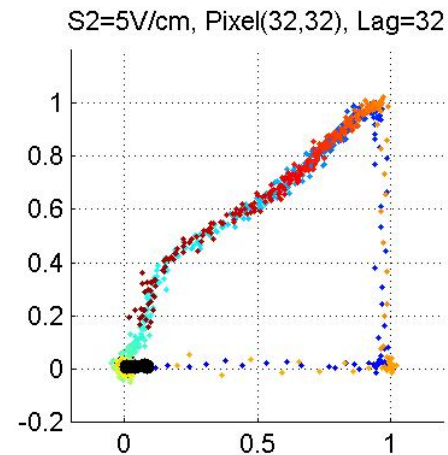
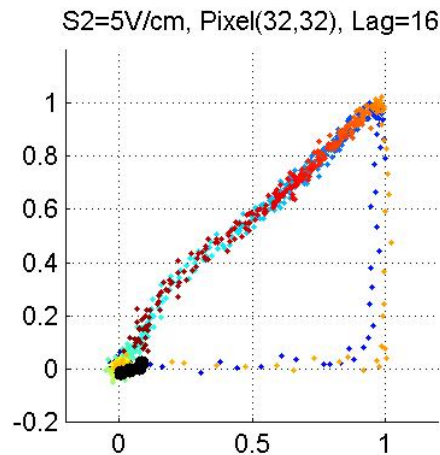
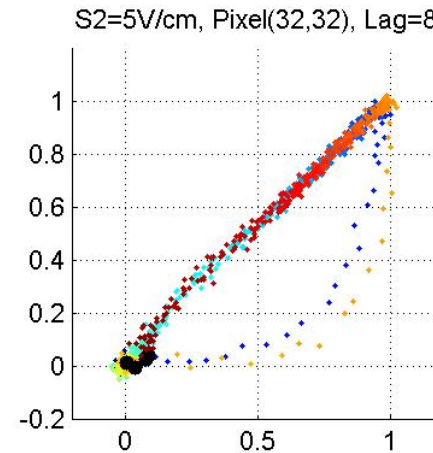
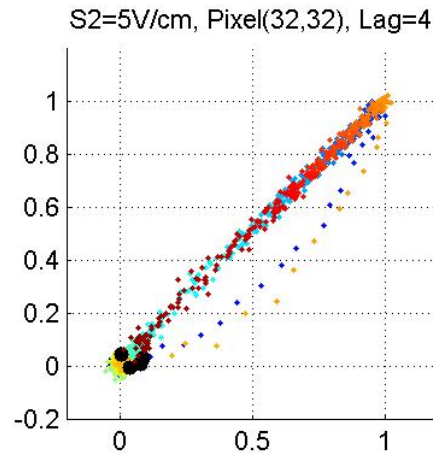


Acknowledgments

- This research was supported in part by
 - NIH grant R01-HL68241
 - NIH 5 T32 HL07411Cardiovascular Mechanisms Training Grant



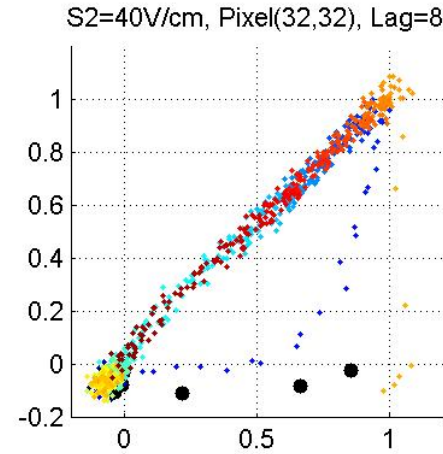
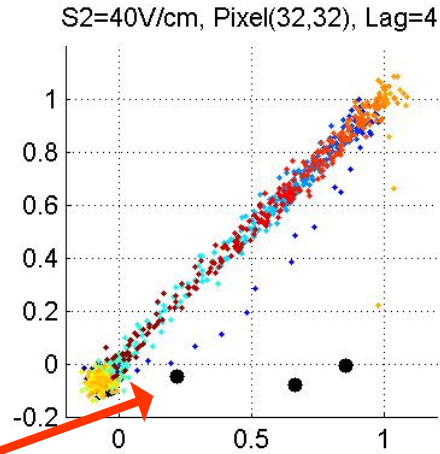
Endocardium: Dependence of Lag



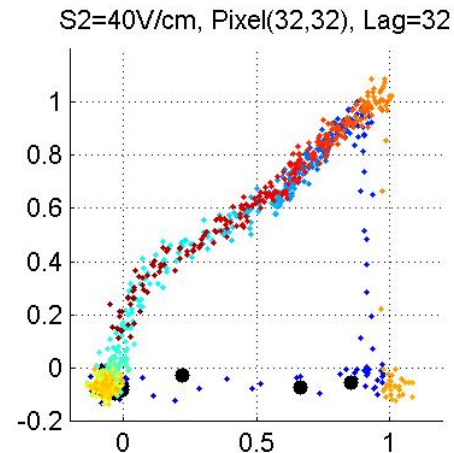
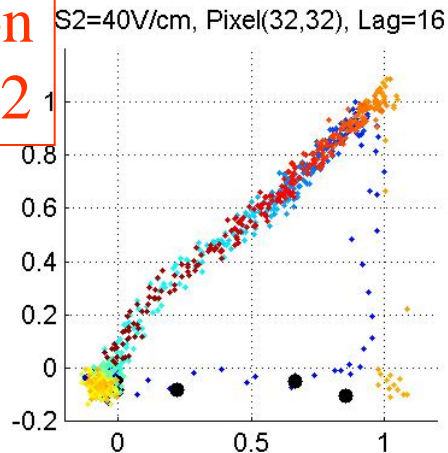
If lag is too long, the difference between S1 and S2 is lost.



Endocardium: Dependence of Lag

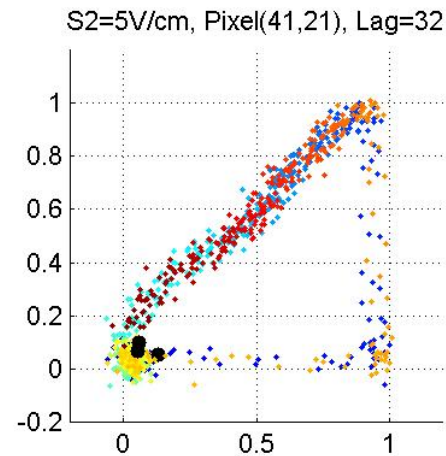
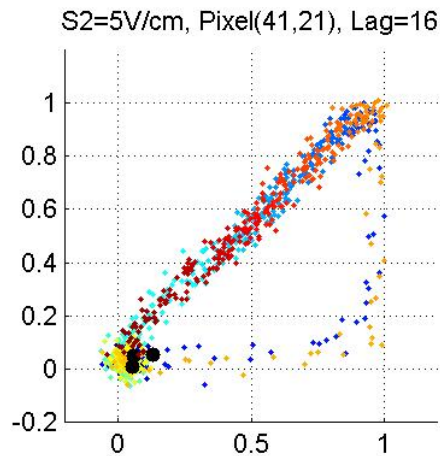
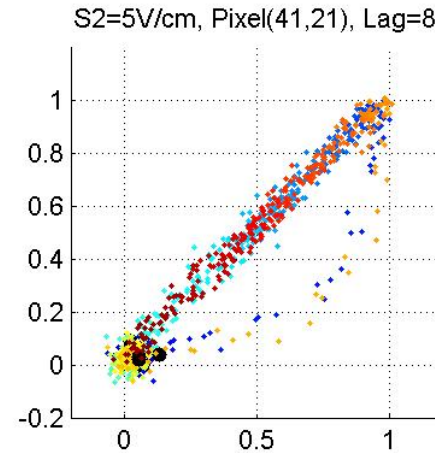
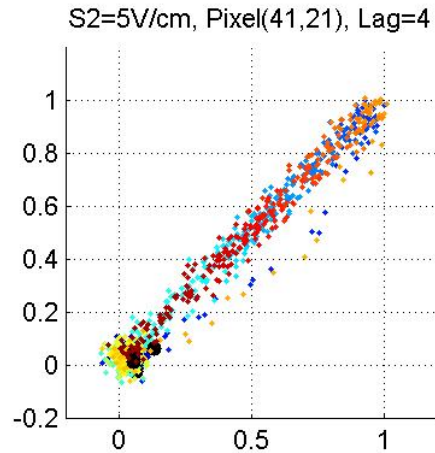


Faster activation
with stronger S2



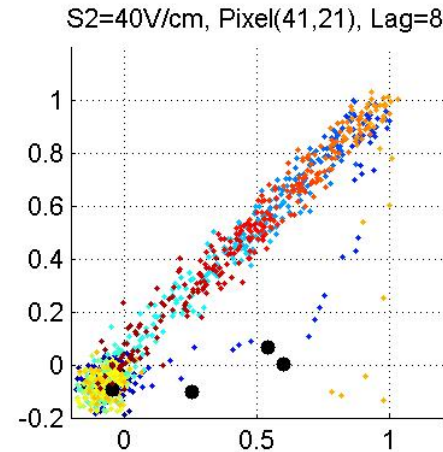
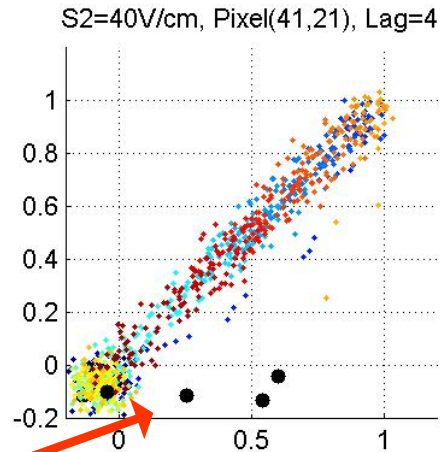


Epicardium: Dependence of Lag





Epicardium: Dependence of Lag



Faster activation
with stronger S2

