



LIVING STATE PHYSICS GROUP  
DEPARTMENT OF PHYSICS AND ASTRONOMY, VANDERBILT UNIVERSITY

# The Magnetocardiogram, Tissue Anisotropy, and the Cardiac Bidomain

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1 meter

# The First Clinical VMCG Machine

Vector  
Magnetocardiography  
Stanford  
~1974





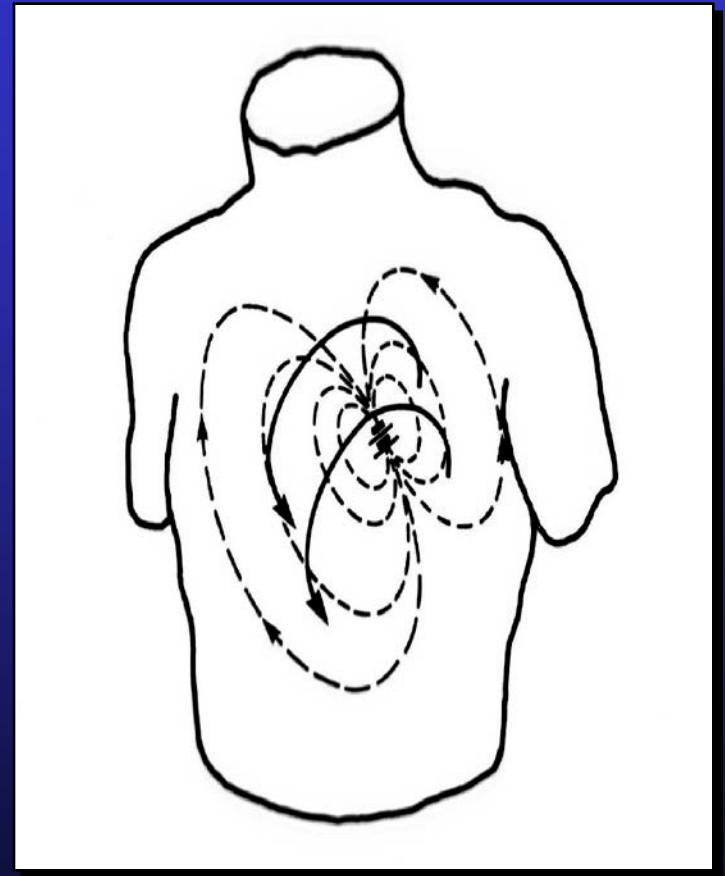
# Questions Regarding the MCG

## Information Content?

- Does the MCG contain information not present in the ECG?

## The Inverse Problem

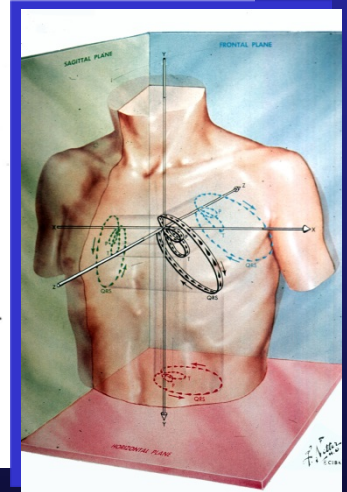
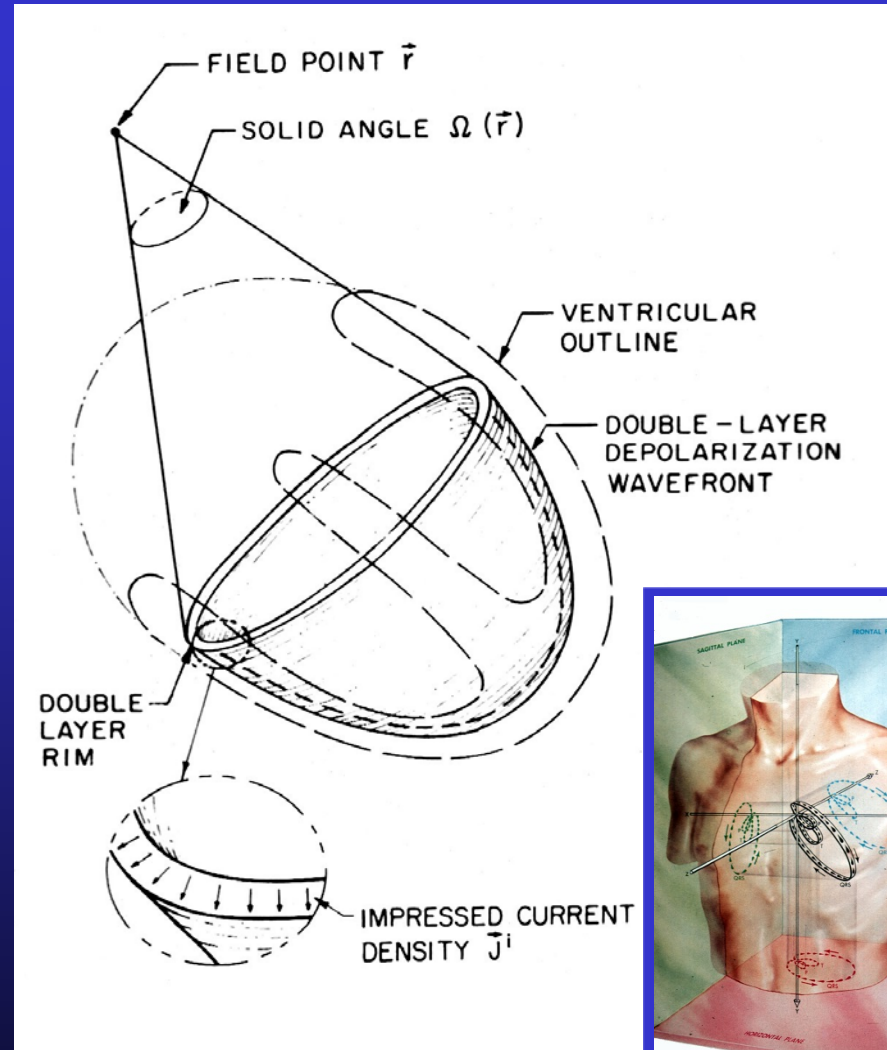
- There is no unique solution to the ECG, MCG, or ECG-MCG inverse problem. What role do Silent Sources play?





## The uniform double-layer model

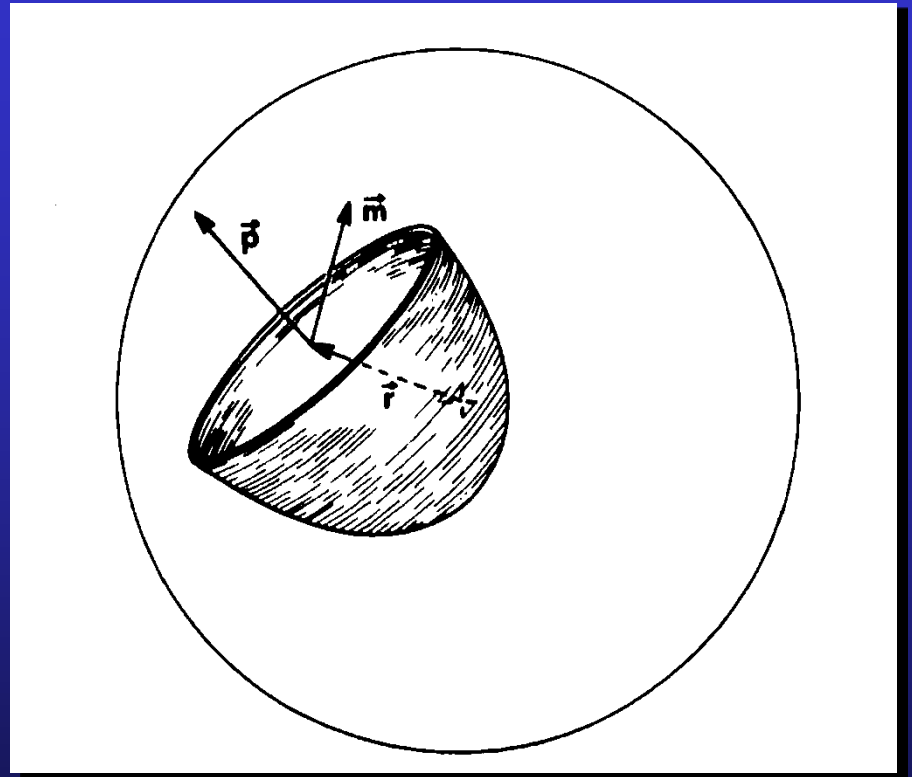
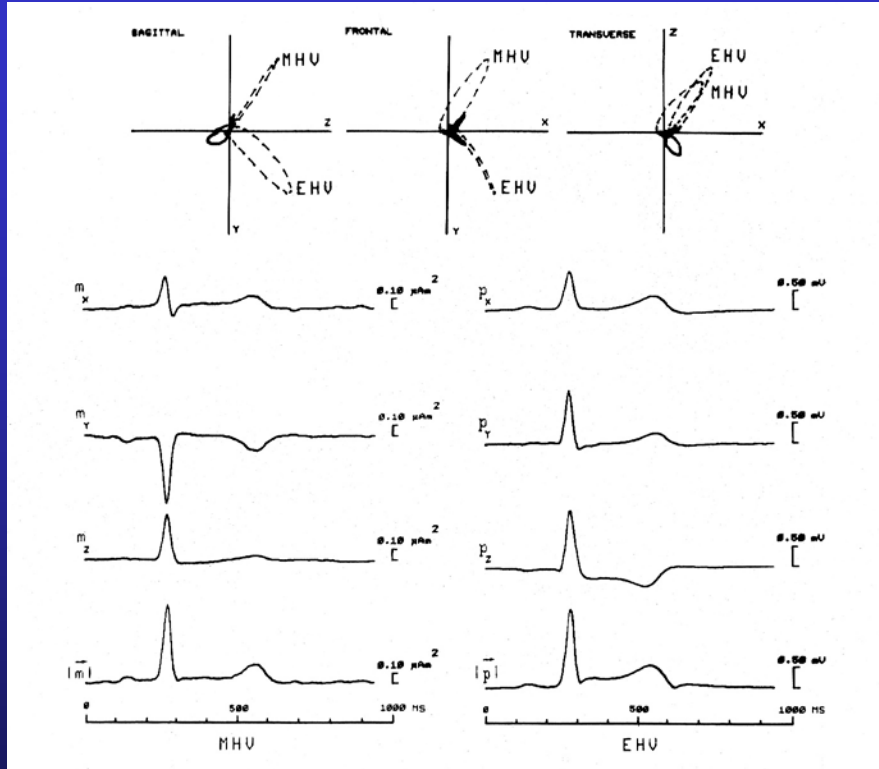
- Assumes
  - Uniform thickness
  - Uniform strength
  - Current perpendicular to the wave front
- **Dipole moment** and potential  $V(r)$  are determined by the solid angle subtended by the double-layer rim



Heart vector or dipole moment versus time



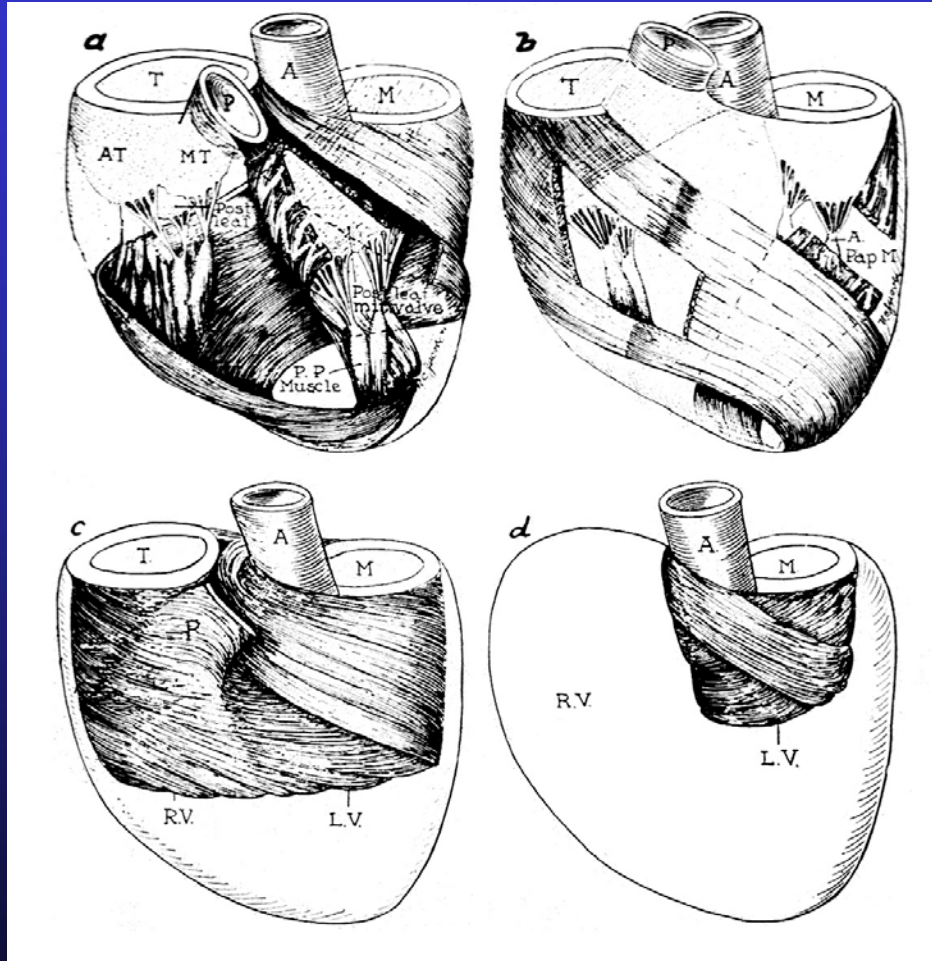
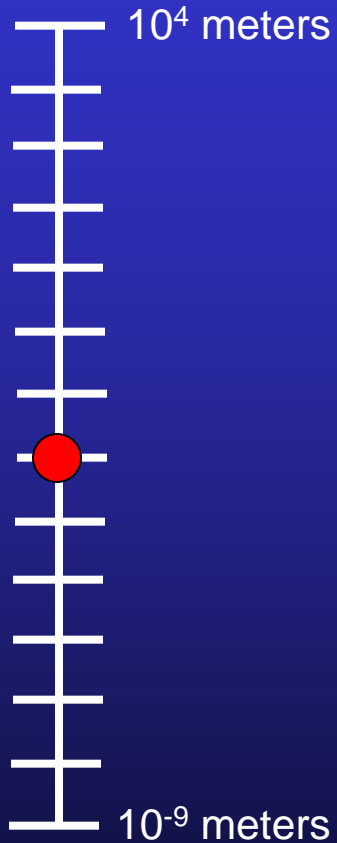
# The electric and magnetic heart vectors



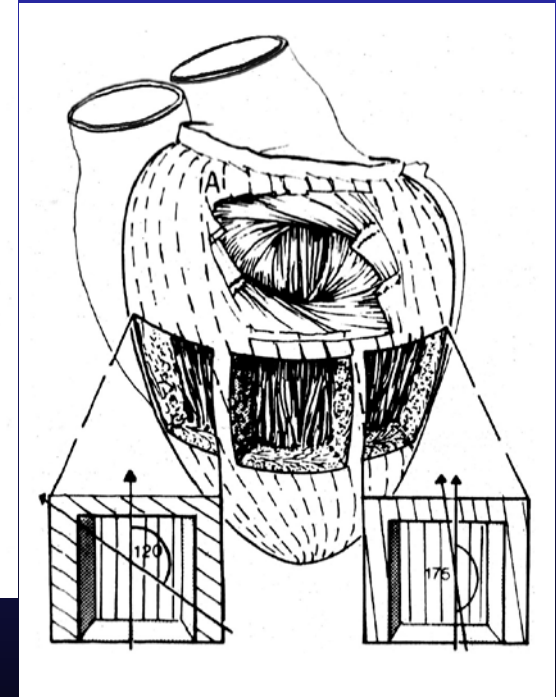
- $m = \frac{1}{2} r \times p$  explains relation of electric and magnetic vectors
- Double-layer rim determines both  $m$  and  $p$
- Little significant new information in the MCG...?



# 1 millimeter: Cardiac fiber sheets



s00397

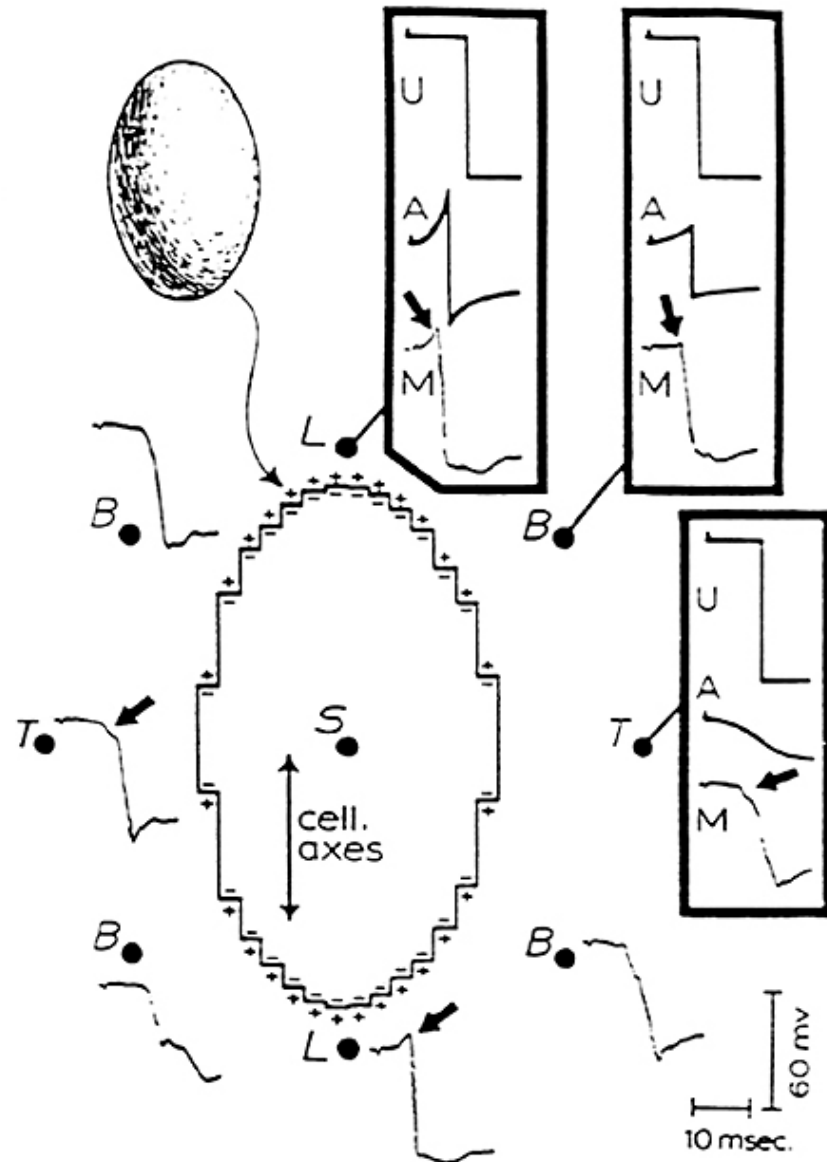
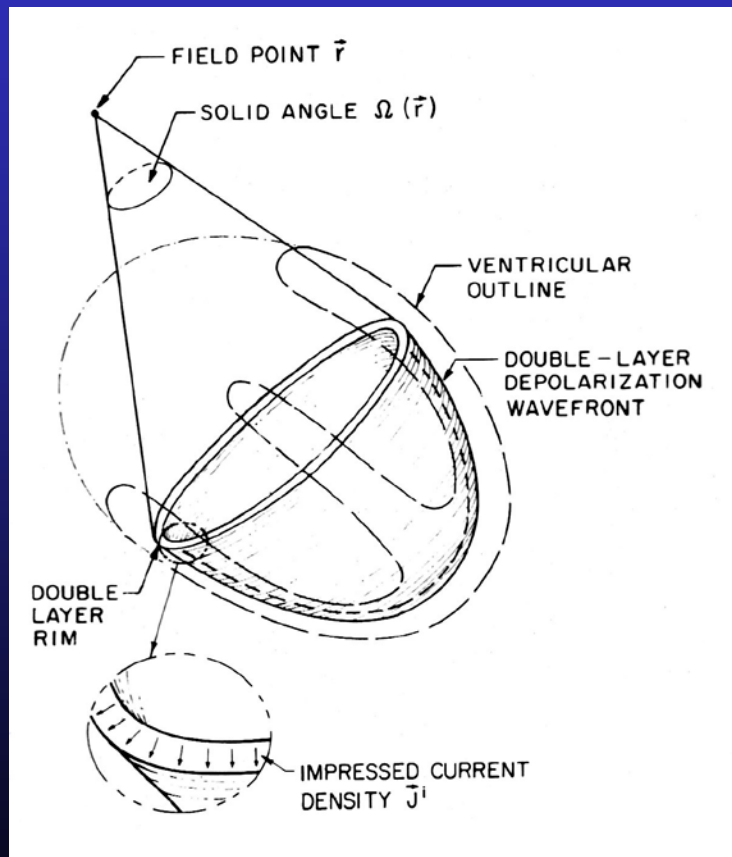


S00703



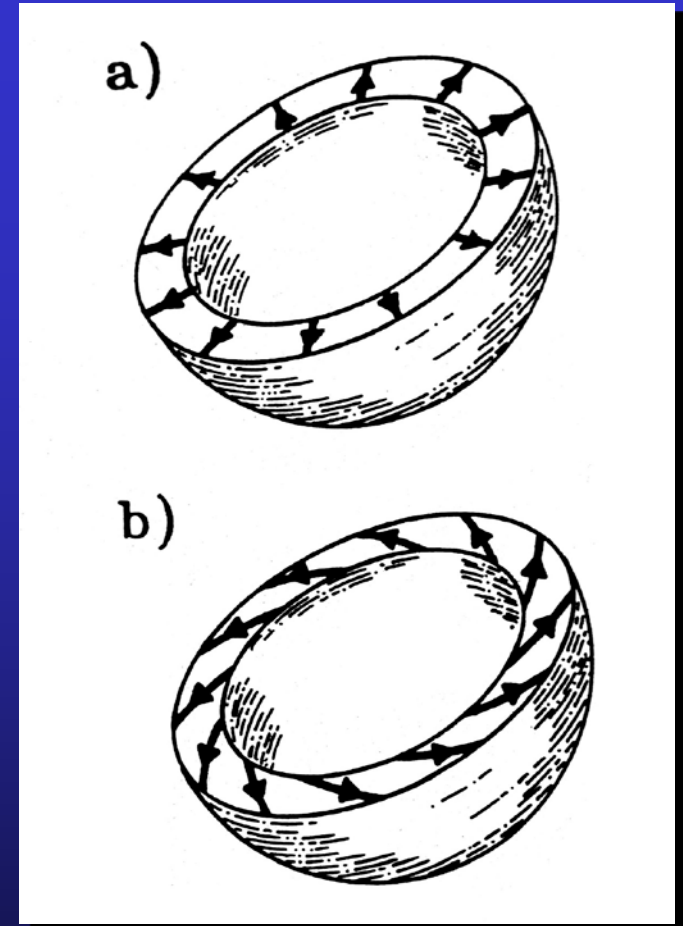
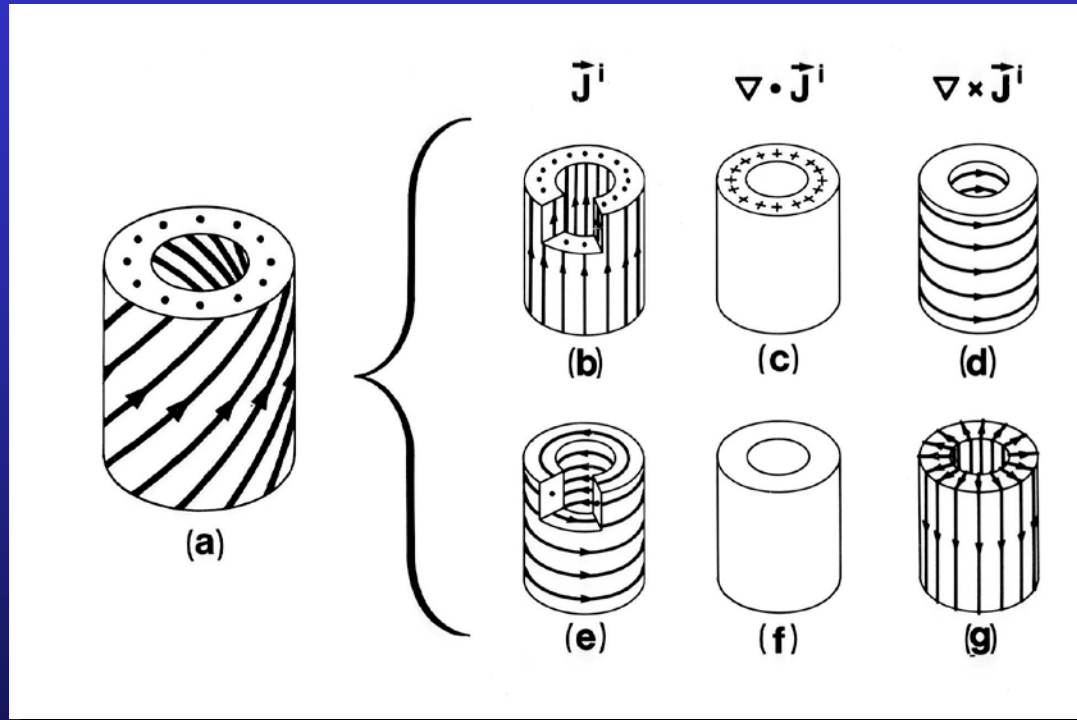


# It's the anisotropy...





## Cardiac fiber orientation is the source of the new information

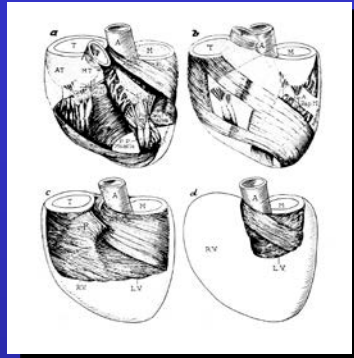


- Circulating current components are electrically silent
- Only magnetic fields can distinguish between two possible models

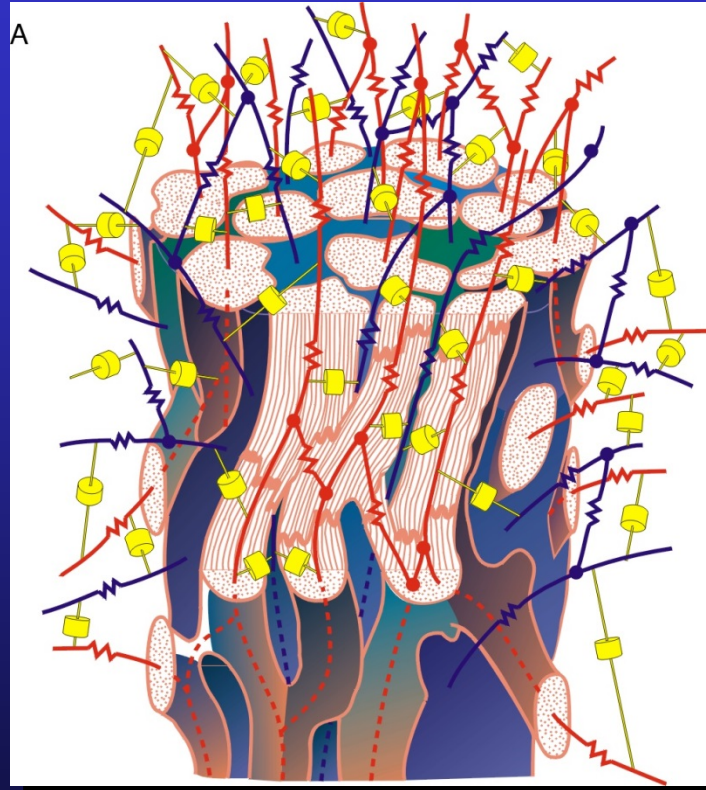
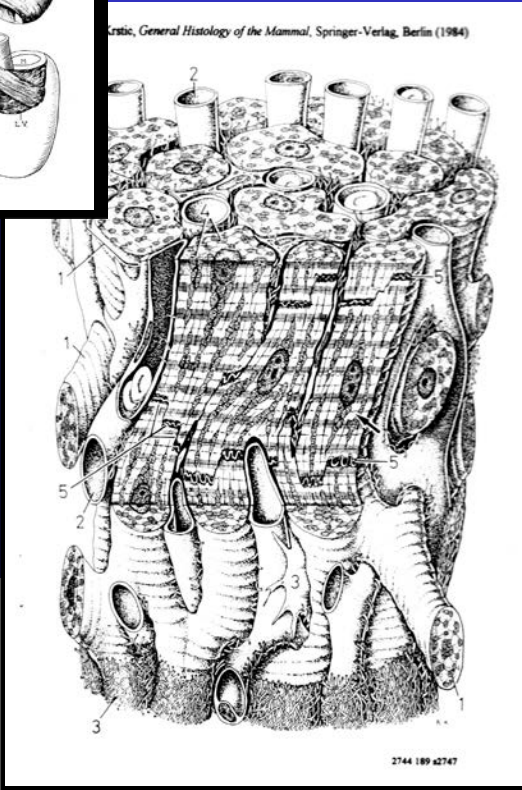




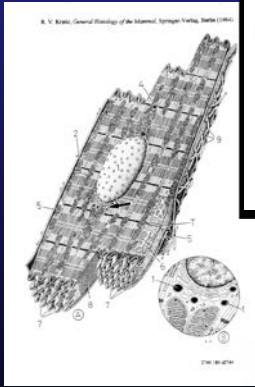
# The cardiac syncytium: A three-dimensional non-linear anisotropic bidomain



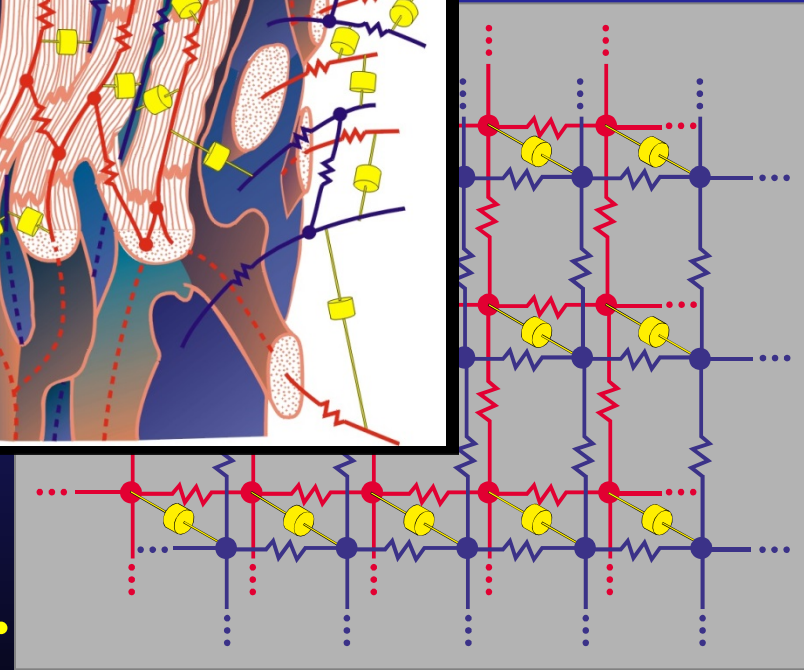
Artis, General Histology of the Mammal, Springer-Verlag, Berlin (1984)



3-D  
VS.  
2-D



It's the anisotropy....





## 2-D Bidomain Equations

- Homogenized
- Coupled  $V_m$  &  $V_e$
- Nonlinear reaction-diffusion equation
- Boundary value equation

$$C_m \frac{\partial V_m}{\partial t} = -J_{ion} - \frac{1}{\beta} \nabla \cdot \tilde{g}_e \nabla V_e ,$$

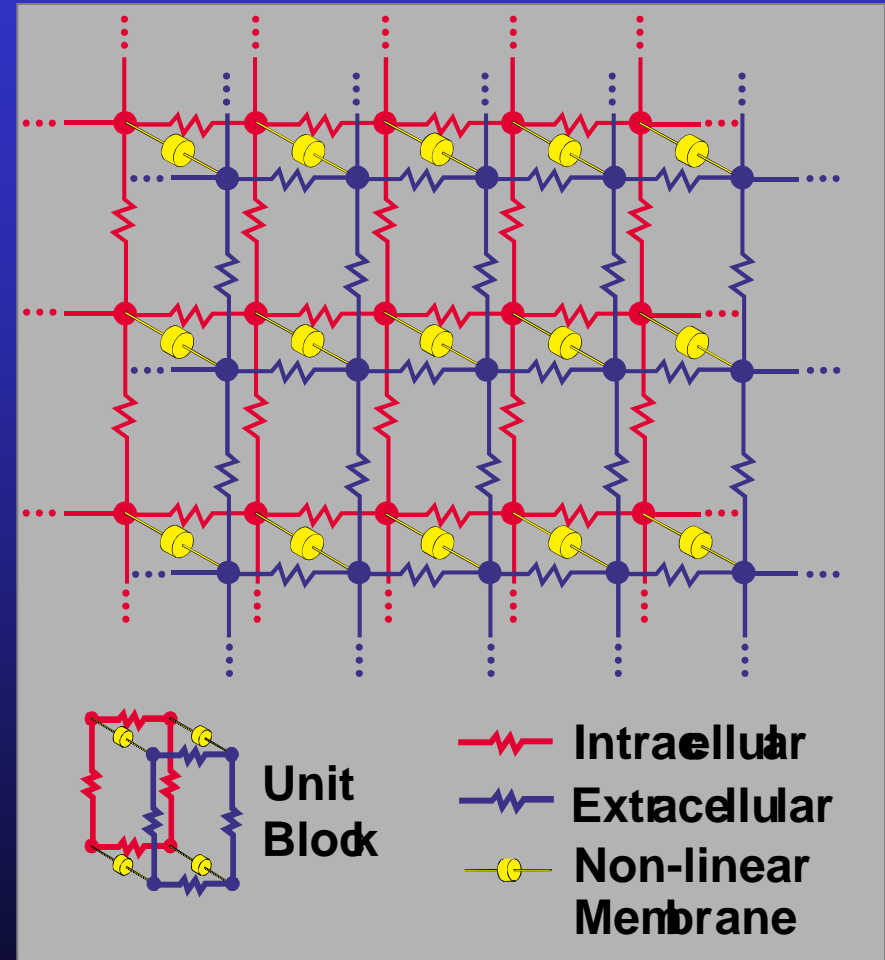
$$\nabla \cdot (\tilde{g}_i + \tilde{g}_e) \nabla V_e = - \nabla \cdot \tilde{g}_i \nabla V_m ,$$

where  $\tilde{g}_i$  and  $\tilde{g}_e$  are the intracellular and extracellular conductivity tensors;  $\beta$  is the ratio of membrane surface area to tissue volume ( $0.3 \mu\text{m}^{-1}$ );  $C_m$  is the membrane capacitance per unit area ( $0.01 \text{ F/m}^2$ ); and  $J_{ion}$  is the membrane current per unit area



# The Cardiac Bidomain

- Intra- and extracellular spaces have unequal anisotropies in their electrical conductivities.  
Really?
  - Magnetic fields
  - Virtual electrodes
  - Quatrefoil reentry
  - Defibrillation?





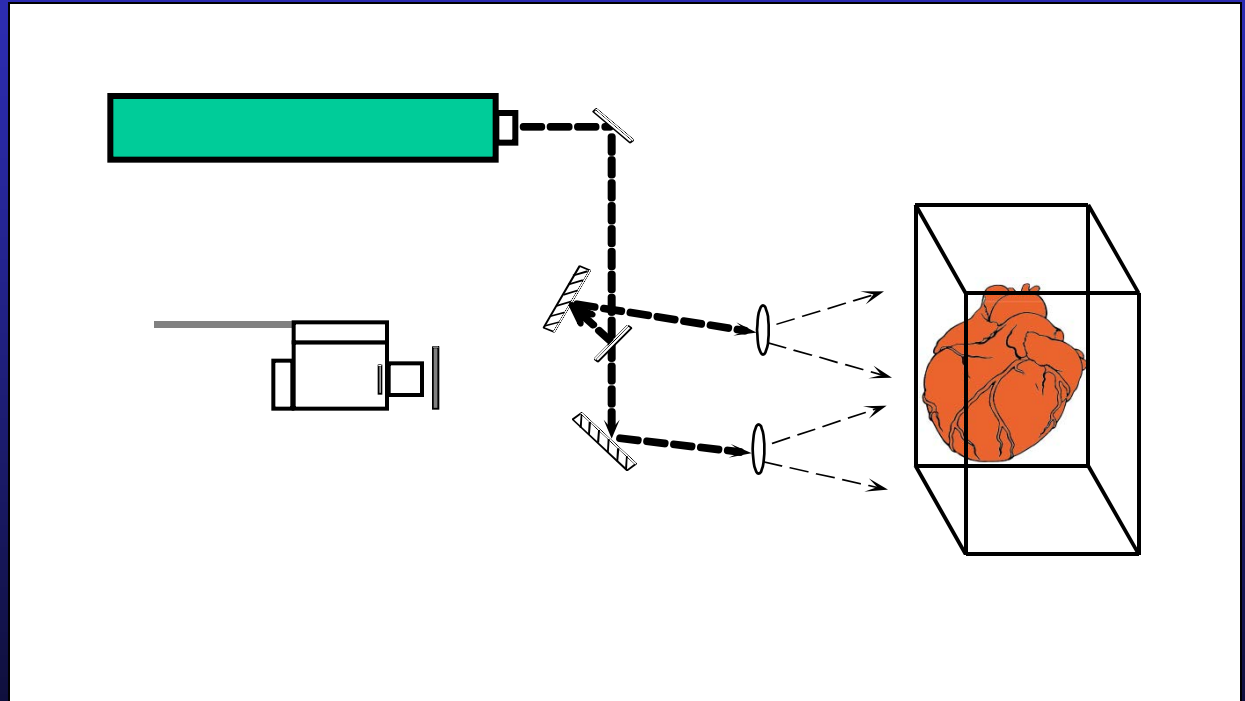
# Recording from the Bidomain

- Extracellular potential
  - Extracellular electrode arrays (  $\leq 1250$  )
- Intracellular potential
  - Intracellular microelectrodes (  $\leq 2$  )
- Membrane potential
  - **Voltage-sensitive fluorescent dyes ( 256 – 10,000 )**
- Net action currents
  - Scanning SQUID microscope ( 1 )



# Optical Imaging of the Transmembrane Action Potential During Stimulation, Reentry, Fibrillation, and Defibrillation

- Langendorff-perfused rabbit heart
- Voltage-sensitive dye in membrane measures  $V_m$
- Laser illumination
- High-speed charge-coupled-device (CCD) camera

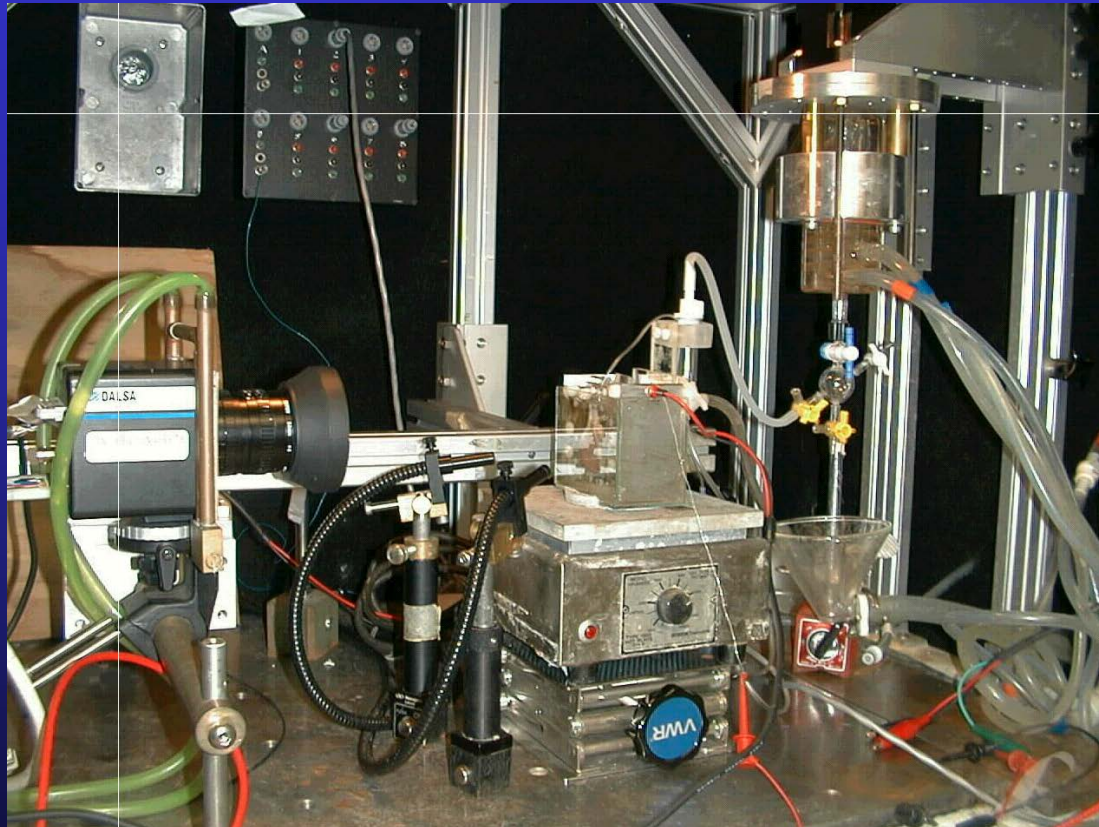






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# Vanderbilt cardiac imaging system



Verdi diode-pumped solid-state laser

Di-4-ANEPPS voltage dye

Light delivered by bundles of optical fibers

Dalsa CCD camera:

12 bit

64x64 pixels

**1200 frames/sec**

10 x 5 x 7.5 cm<sup>3</sup> bath

37 °C Tyrode's solution

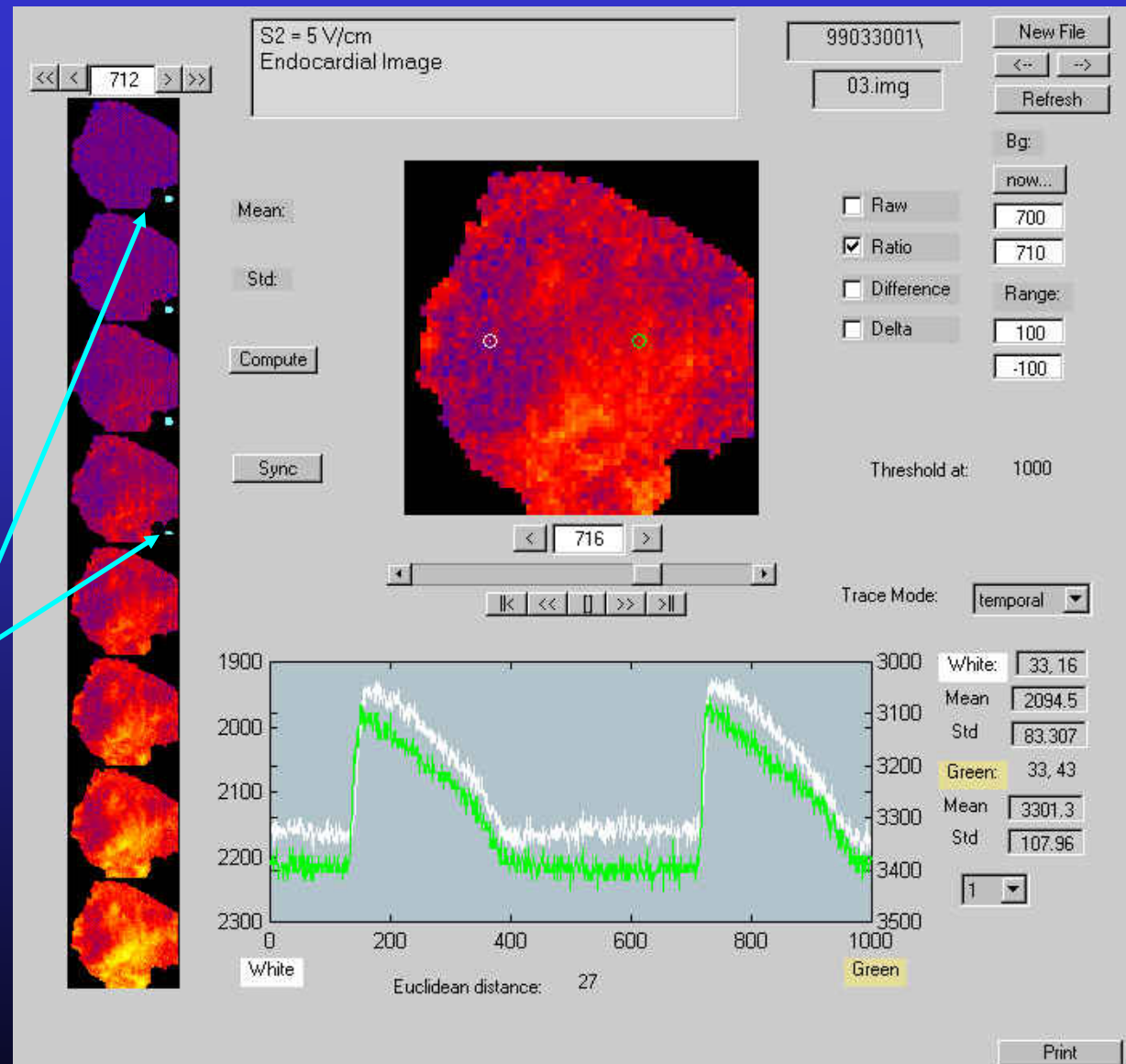




# Gus2: MATLAB Data Viewing Program

Four S2 frames  
indicated by LED

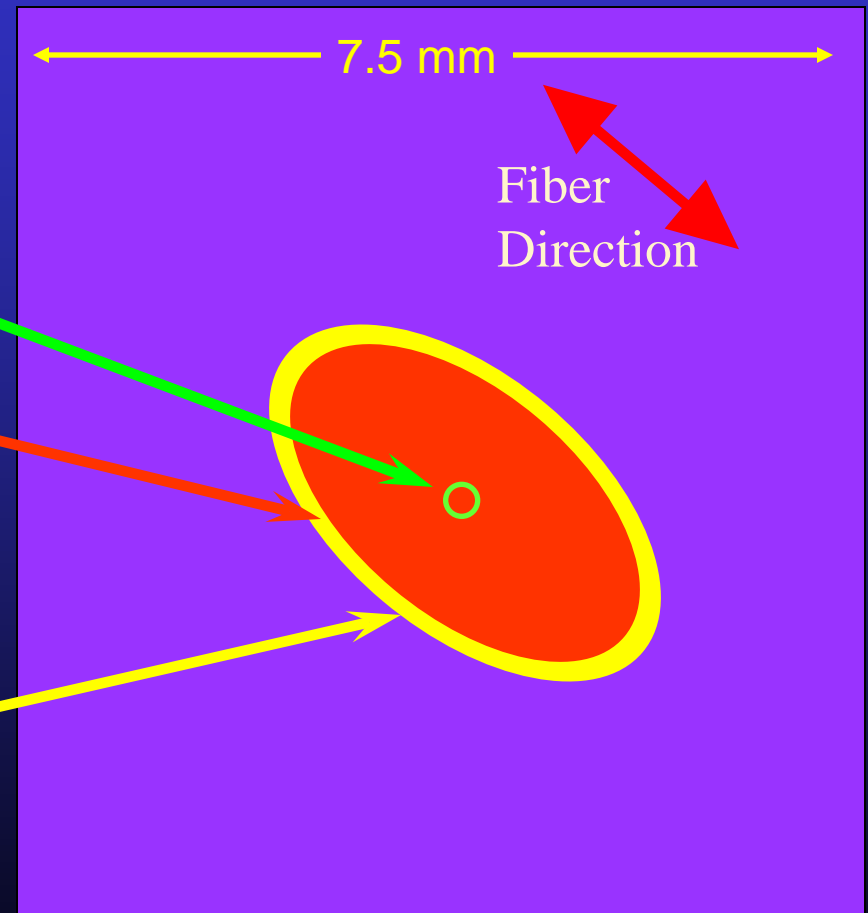
Written by  
Gustavo Rohde





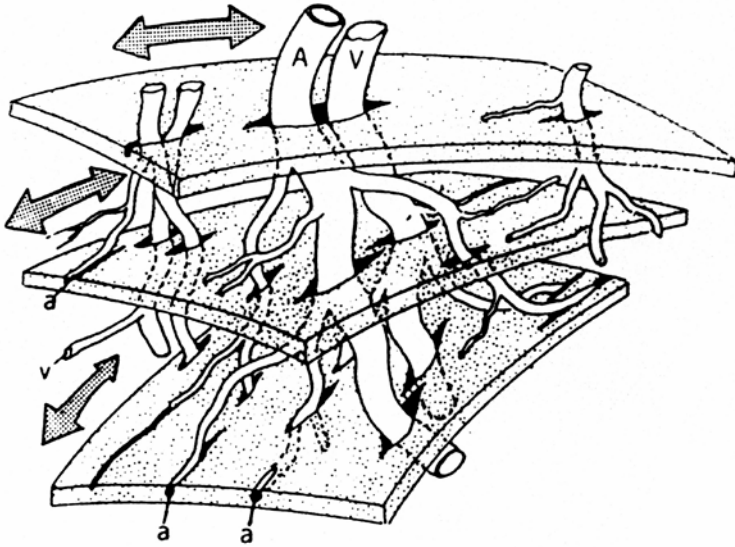
# Injecting -20 mA into Equal-Anisotropy Cardiac Tissue

- Point cathodal stimulation
- Virtual cathode depolarizes (red)
- Wave front propagates from the edge of the virtual cathode (yellow)





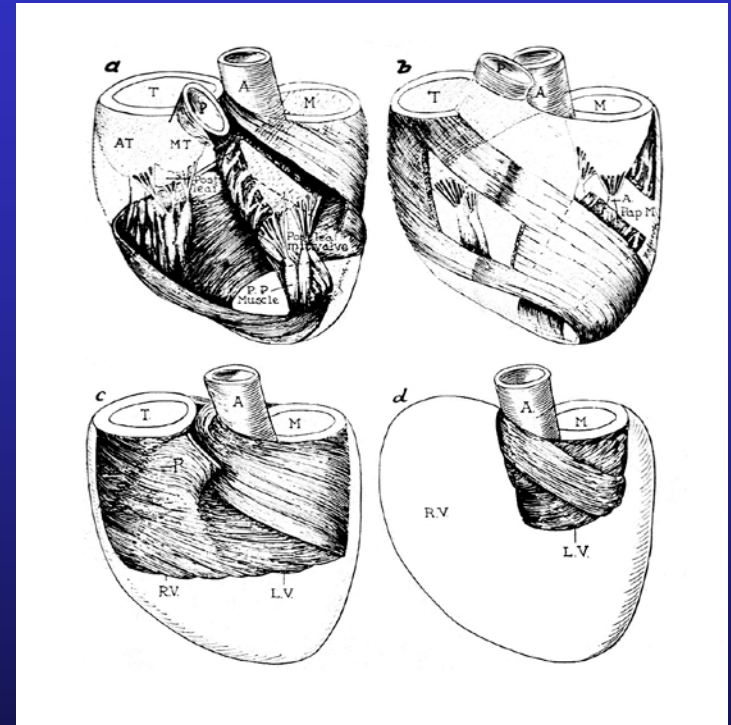
# Bidomain Anisotropy



$$\begin{array}{ll} \sigma_{ix} & 0.2 \text{ S/m} \\ \sigma_{iy} & 0.02 \text{ S/m} \\ \sigma_{ex} & 0.8 \text{ S/m} \\ \sigma_{ey} & 0.2 \text{ S/m} \end{array}$$

$$\sigma_{ix} / \sigma_{iy} = 10$$

$$\sigma_{ex} / \sigma_{ey} = 4$$

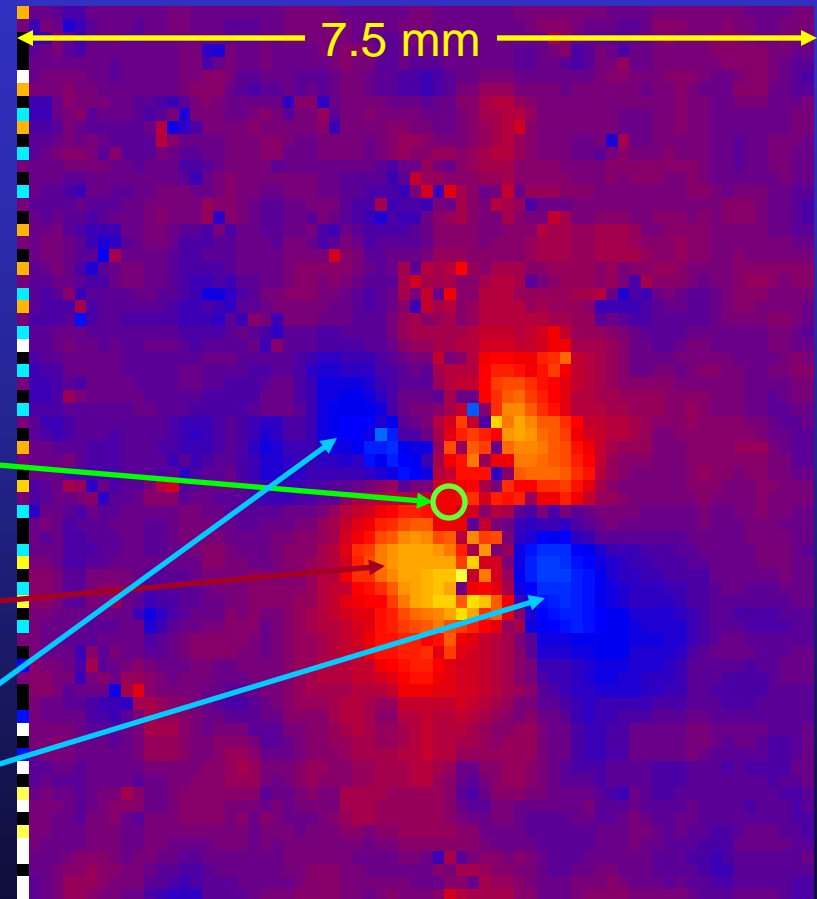


There is no single coordinate system in which the tensor conductivity is everywhere diagonal!



# Virtual electrodes in cardiac tissue

- As a result of unequal electrical anisotropies in intracellular and extracellular spaces:
- Point cathodal stimulation
- Virtual cathode depolarizes (red)
- Virtual anodes hyperpolarize (blue)



Wikswa, Lin and Abbas. *Biophys. J.* 69:2195-2210, 1995



# Puzzle

## Four modes of stimulating cardiac tissue

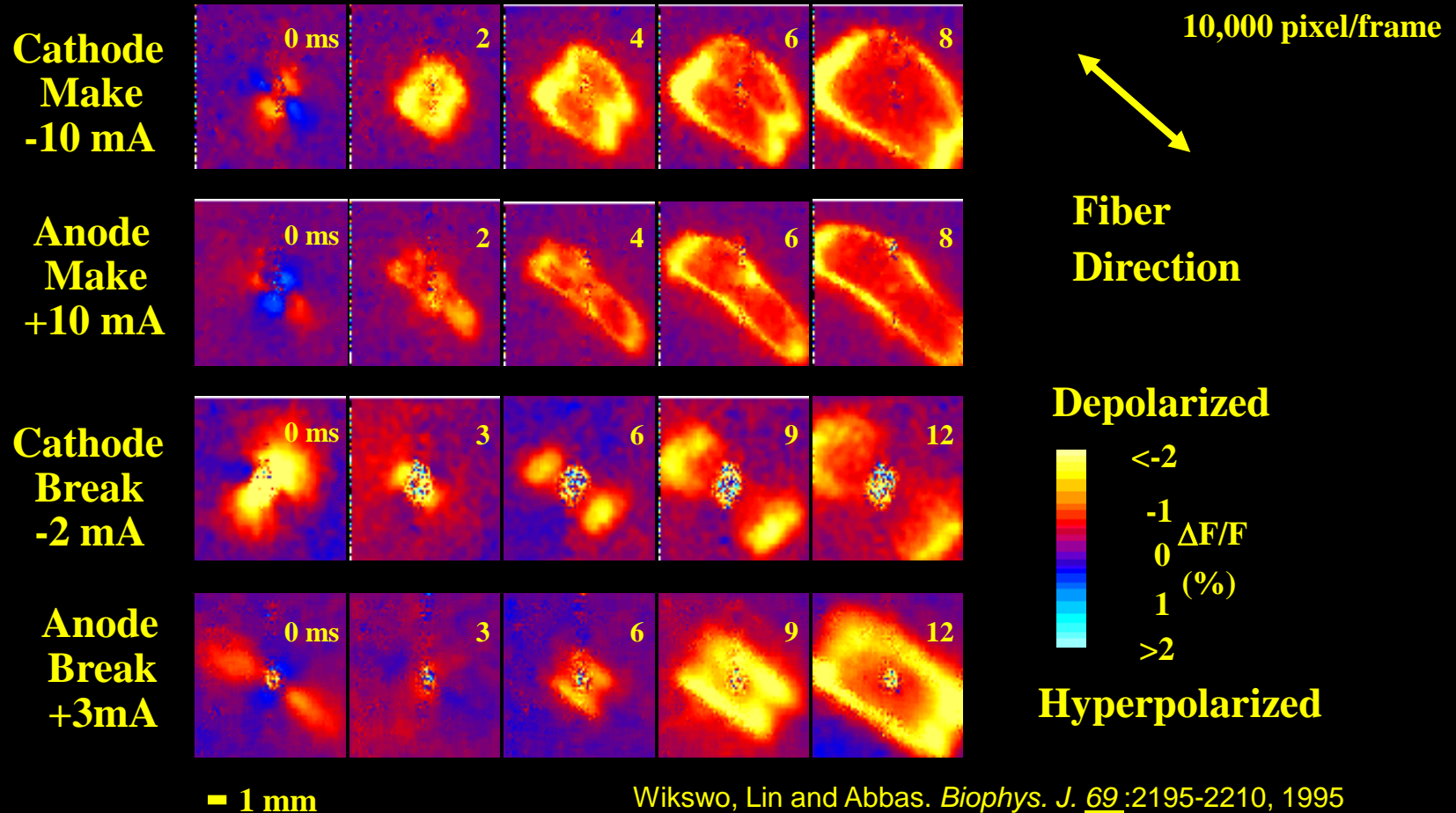
- **Cathode make** (turn on negative current)
- **Anode make** (turn on positive current)
- **Cathode break** (turn off long negative current)
- **Anode break** (turn off long positive current)

Dekker, E. "Direct current make and break thresholds for pacemaker electrodes on the canine ventricle." *Circ Res*, 27:811, 1970



# Synchronous Imaging of Point Activation Patterns

## --- Virtual Electrodes ---



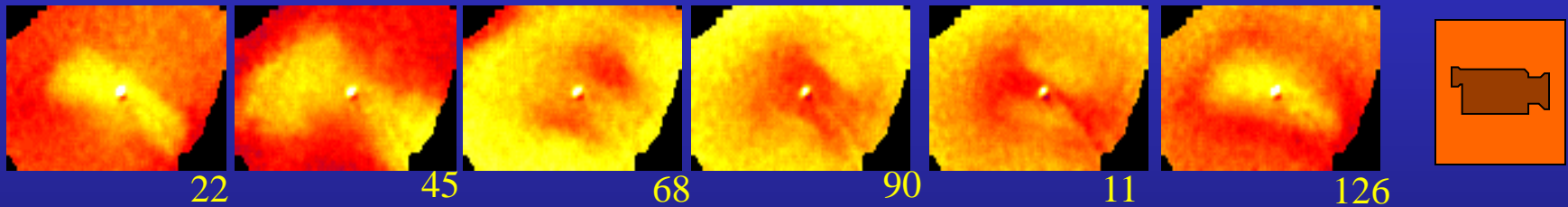




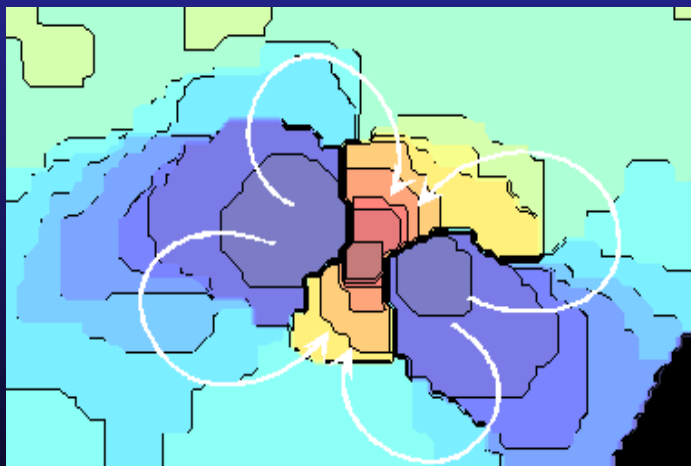
# Optical imaging of quatrefoil reentry

Transmembrane potential distributions from selected frames of a movie for cathodal-break stimulation

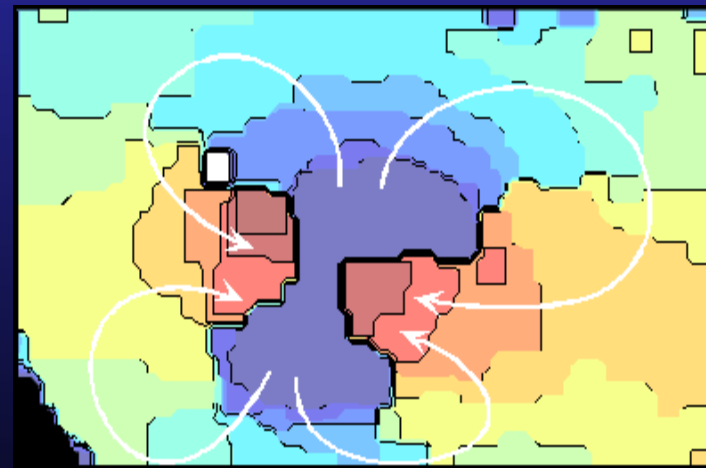
Vm\_expt.mpg



*Cathodal-Break Isochrones*



*Anodal-Break Isochrones*

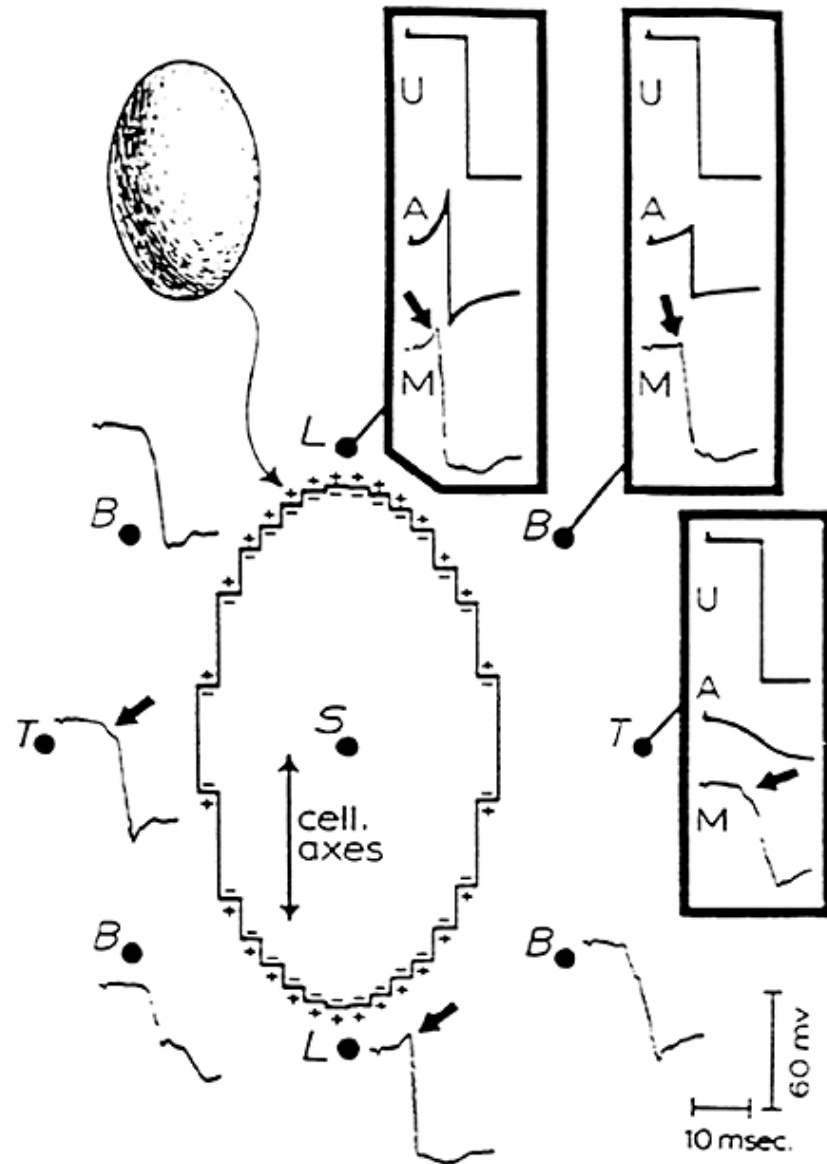
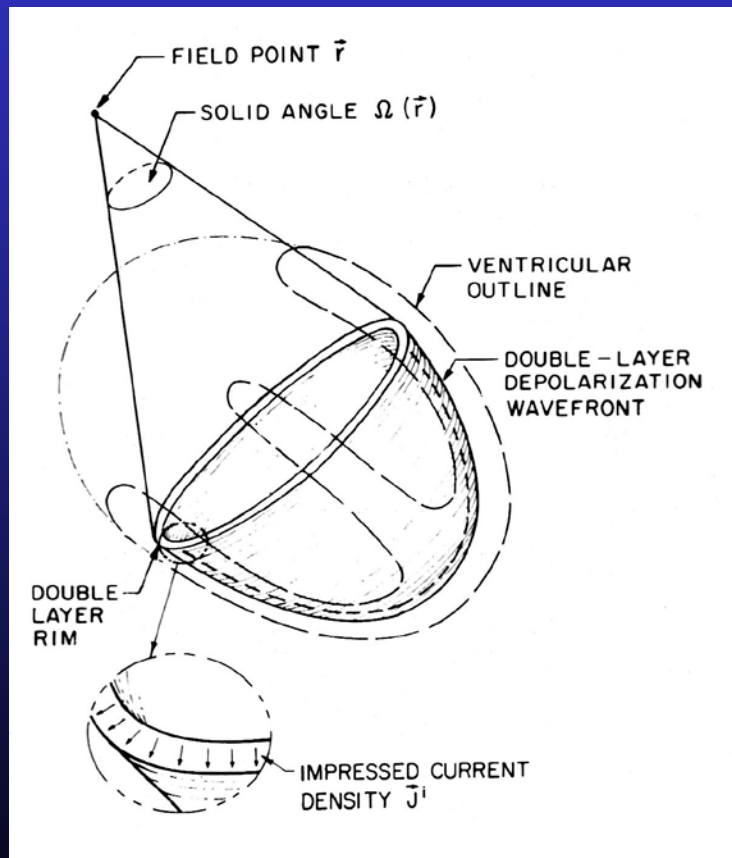


Courtesy of Marc Lin

Lin, Roth, and Wikswo, *J. Cardiovasc. Electrophysiol.*, **10**: 574-586 (1999)



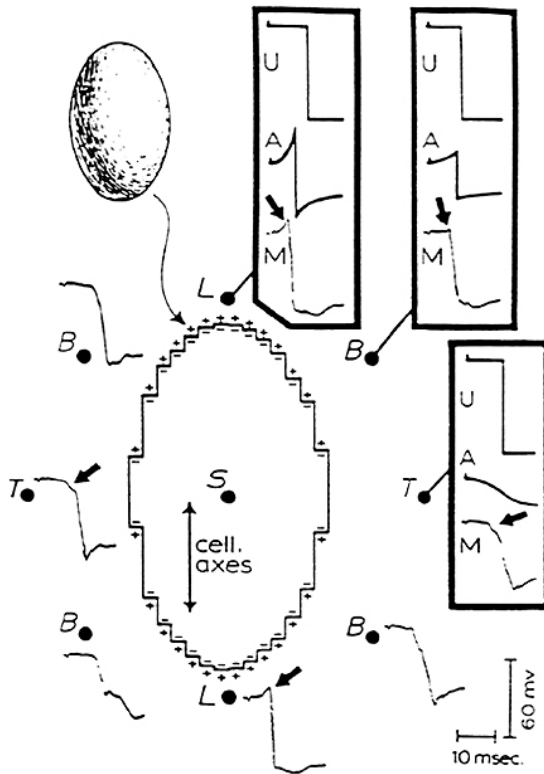
# It's the anisotropy...



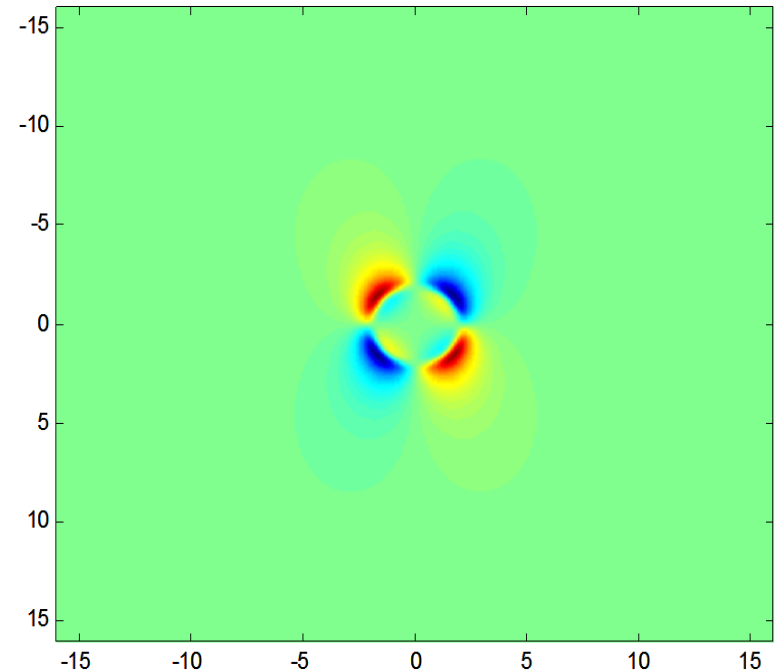
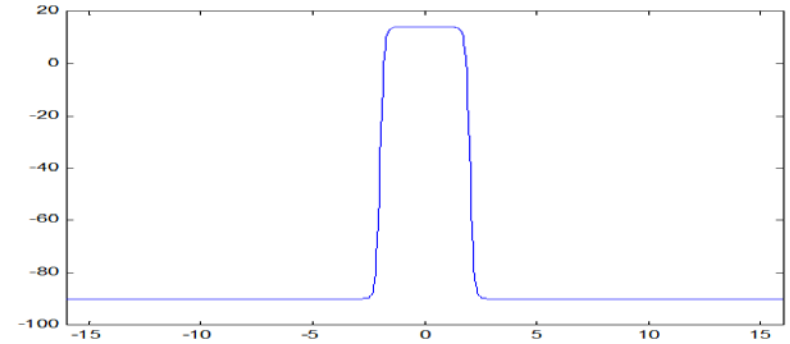


# Magnetic Field From a Circular Action LV Free Wall Action Potential:

L.V. Corbin II and A.M. Scher, *Circulation Res.* 41: 58-67 (1977)



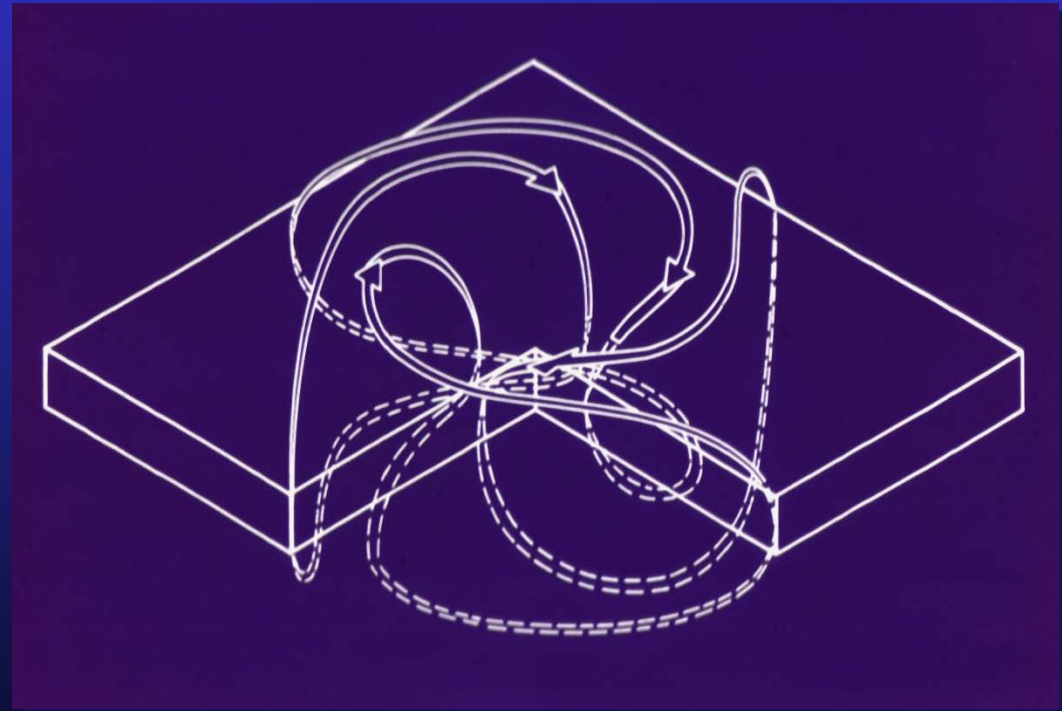
2660 188 s2663



$$V_m(x, y) = 52.0 \cdot \tanh \left[ 5.4 \cdot \left( R - \sqrt{x^2 + y^2} \right) \right] - 38$$



# The Apex Will Have a Complicated B Field





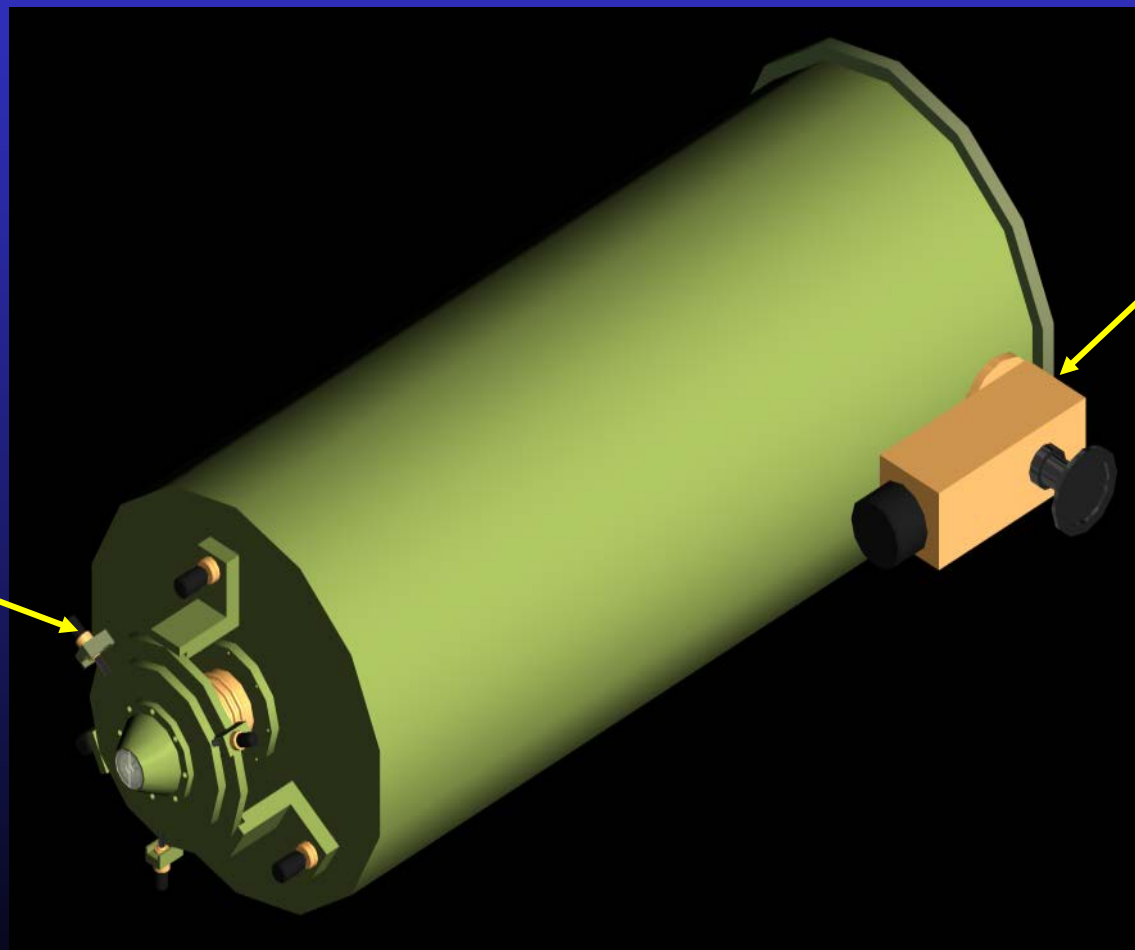
# SQUID Magnetometers

- Superconducting
  - QUantum
  - Interference
  - Device
- 
- Bandwidth: DC-10 kHz
  - Image net action current in x-y plane
  - Big, smaller, smallest...



# NanoSQUID: Cooled with liquid N<sub>2</sub> and liquid He .....

Bellows  
Mechanism

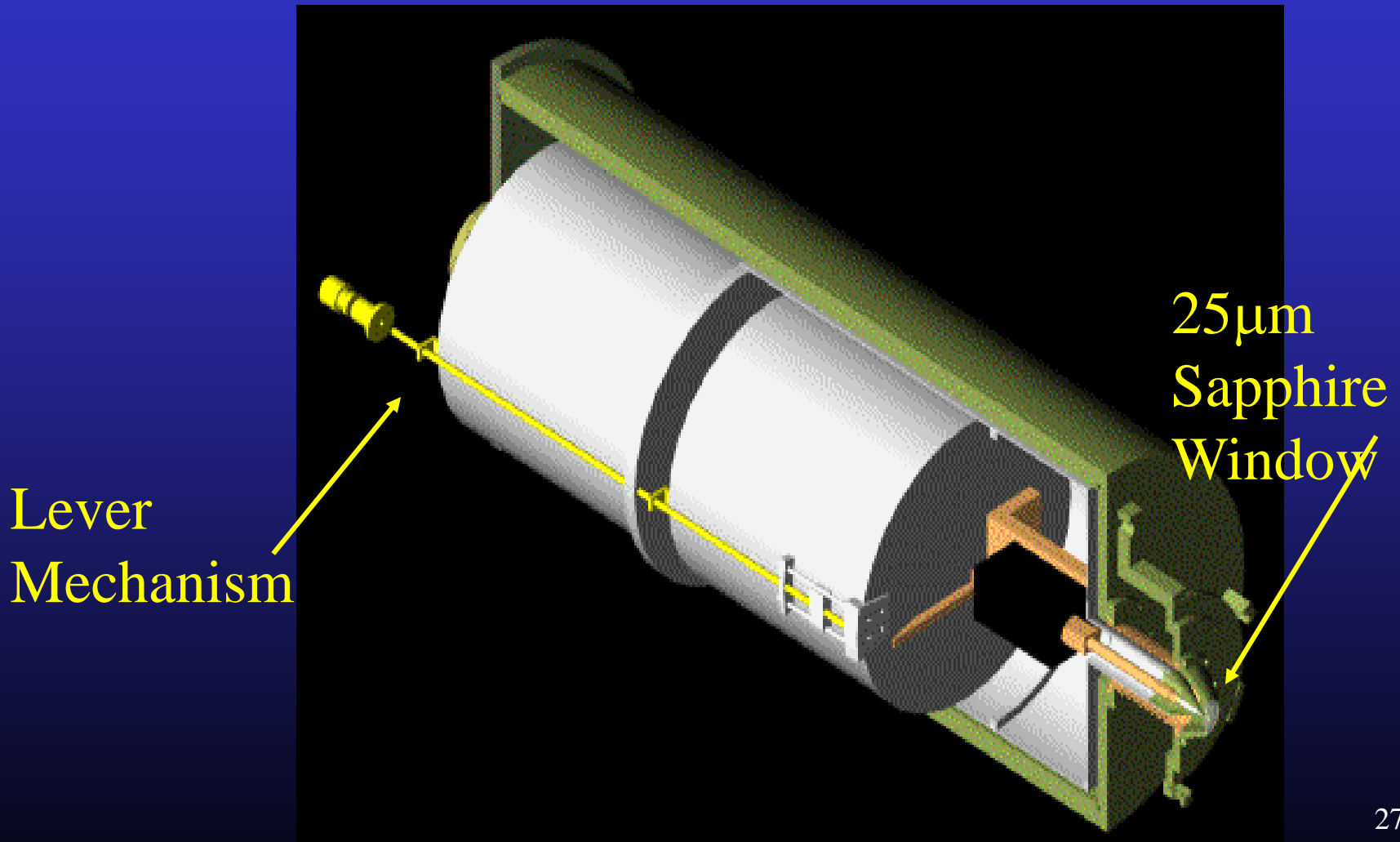


Vacuum  
Port



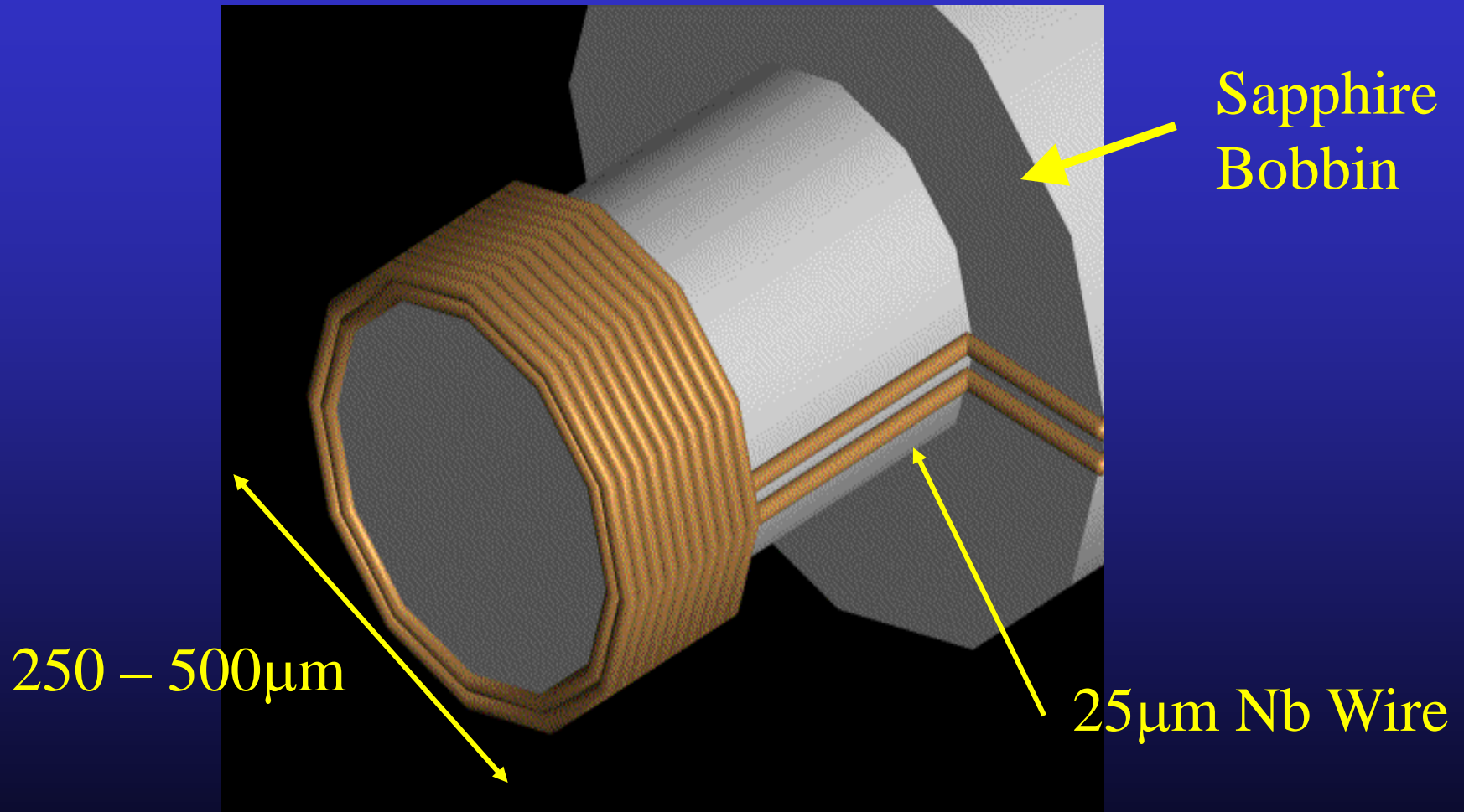


# The SQUID lives in the vacuum space ...





# Wind a Pickup Coil ....





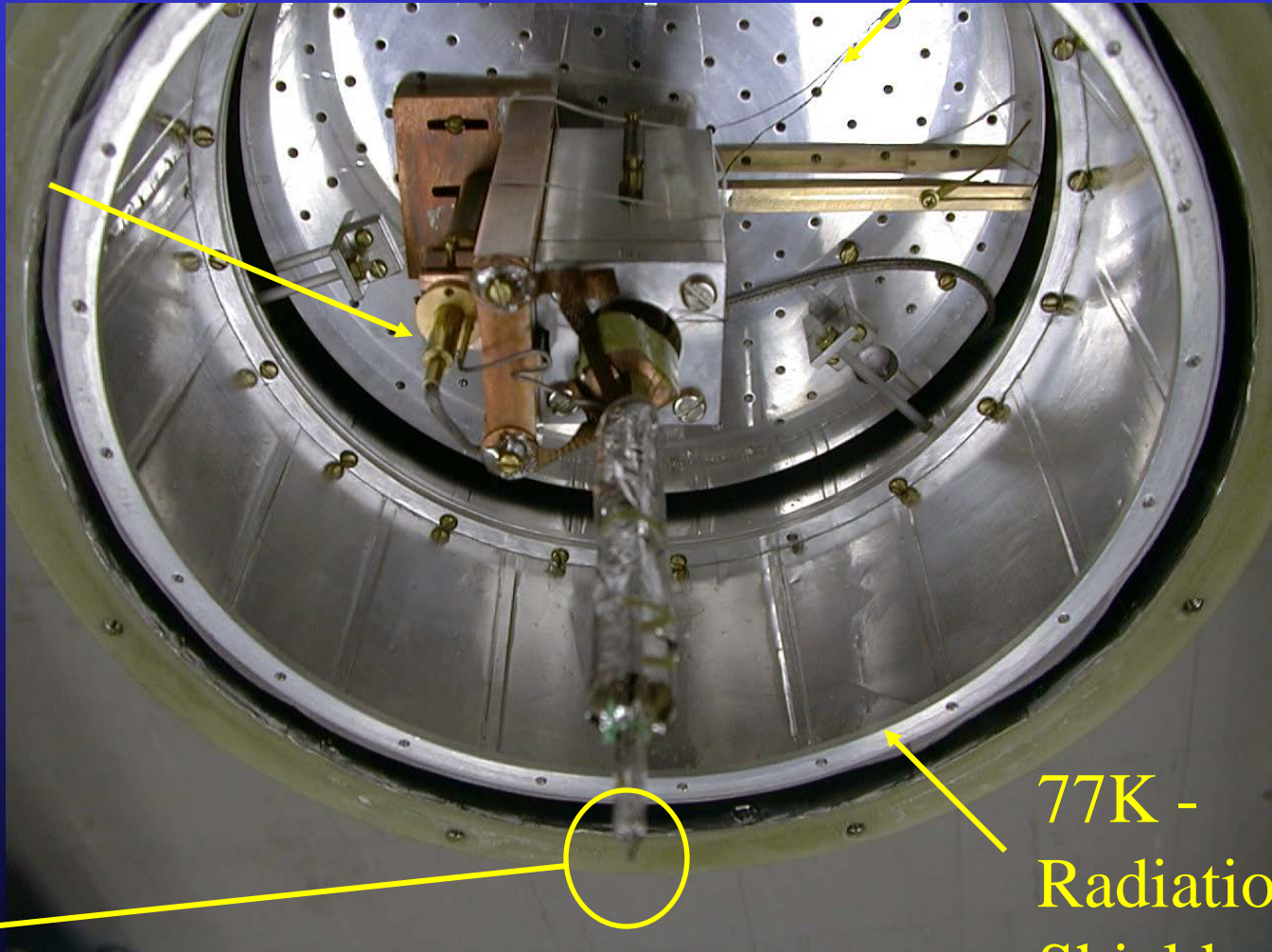
# In Reality ..

SQUID

He-  
Reservoir

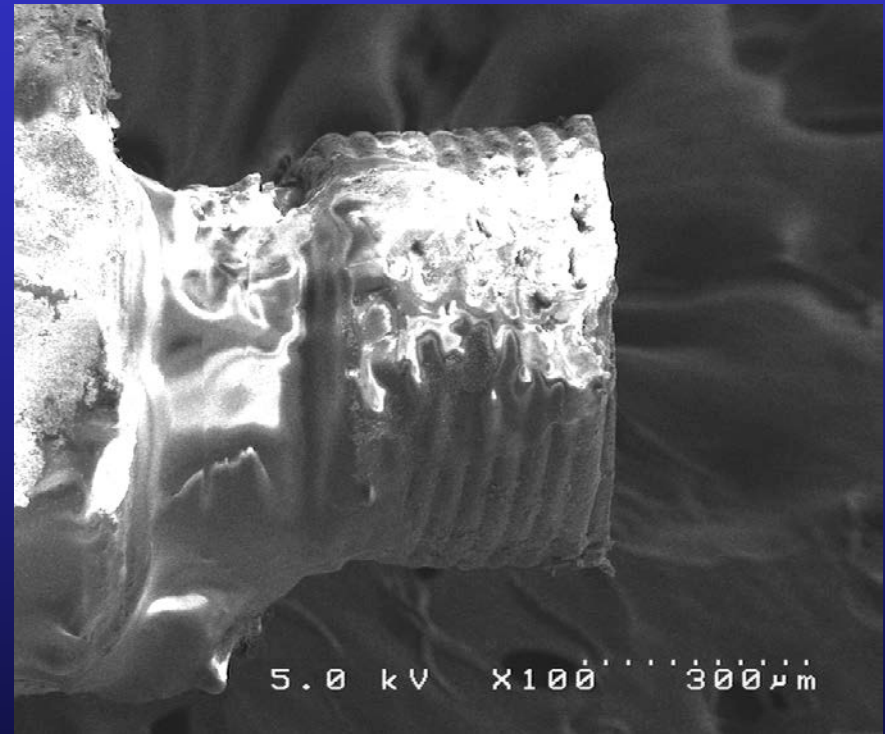
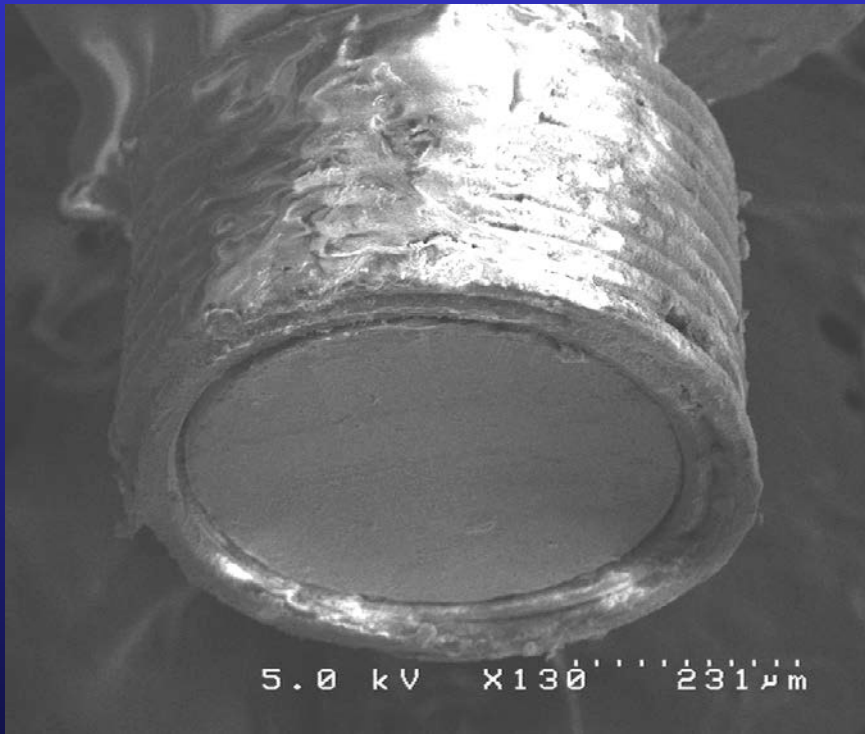
Pickup  
Coil

77K -  
Radiation  
Shield





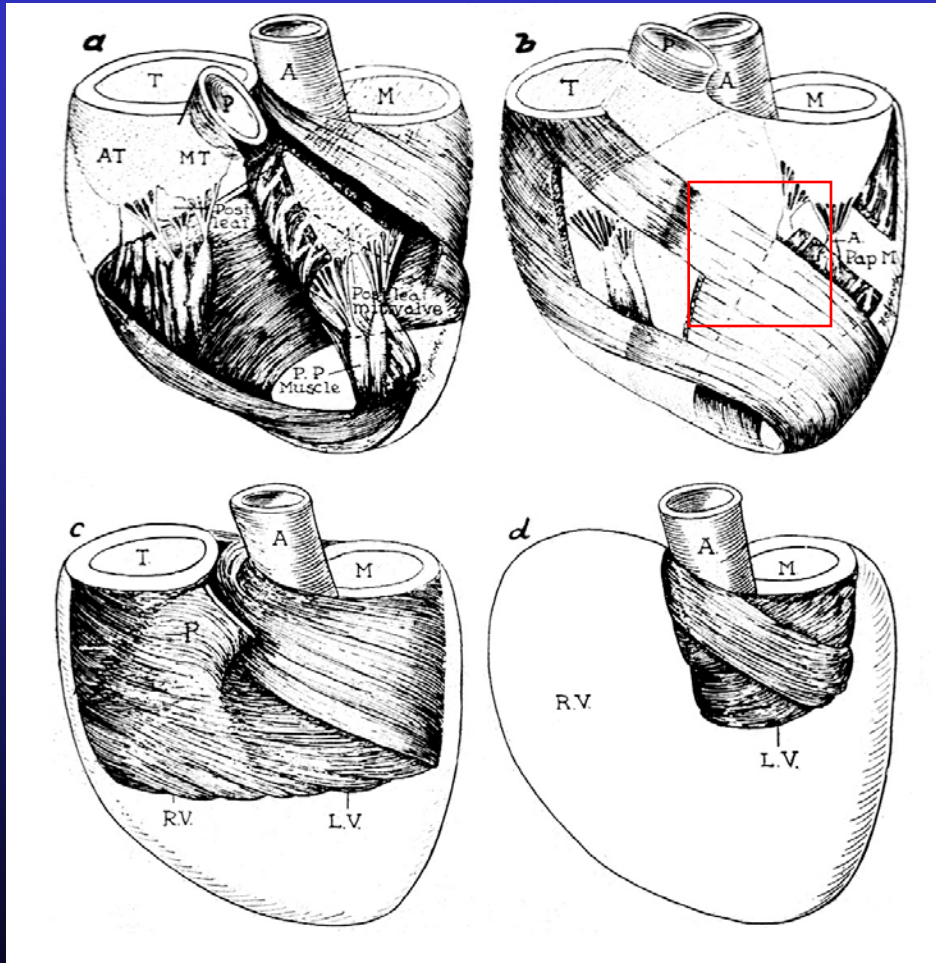
# Pickup Coil







# Image the LV Free Wall ...



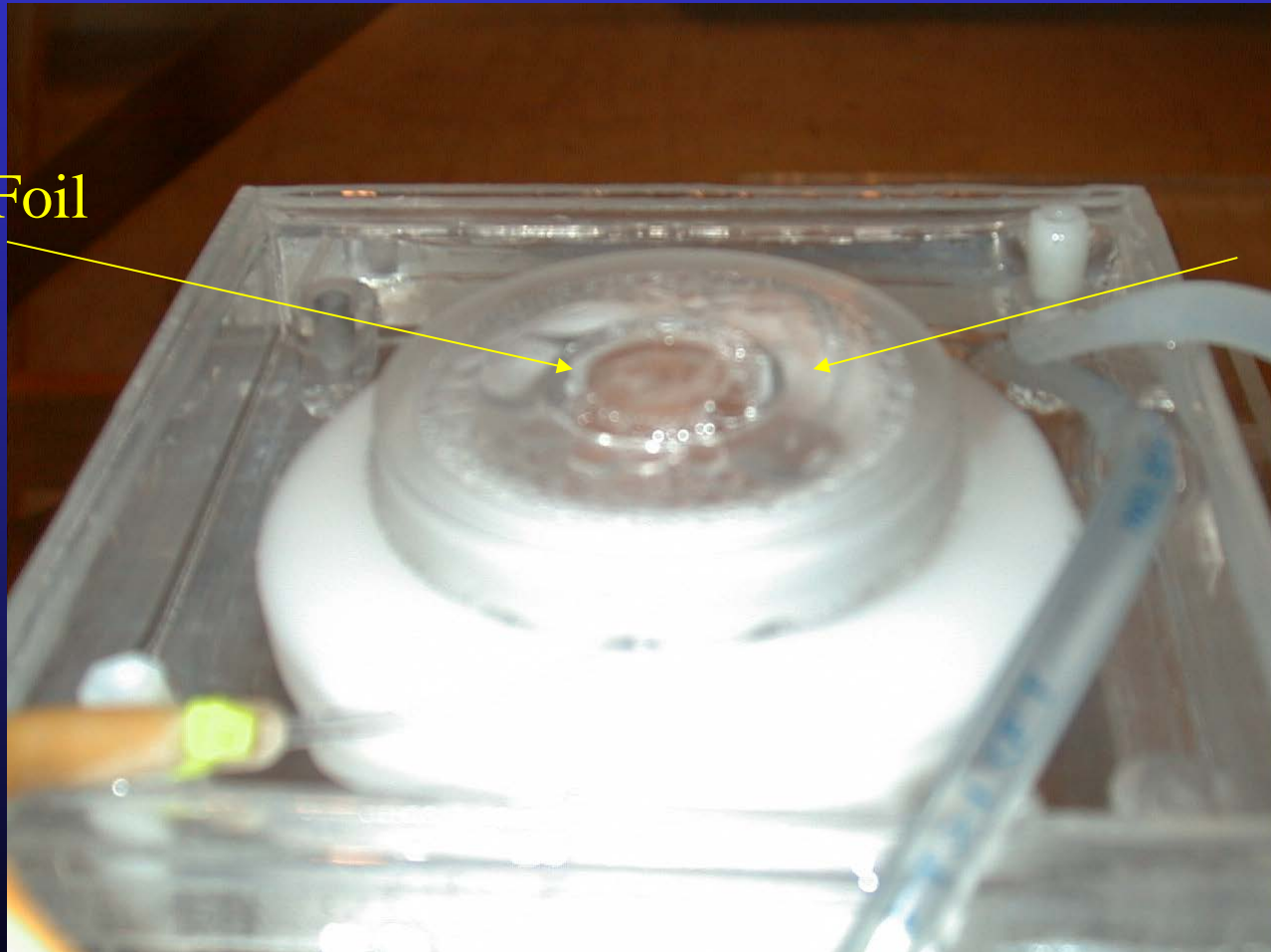
- Scanning SQUID microscope
- Isolated rabbit heart
- Point stimulation
- Anisotropy should produce a quatrefoil current pattern



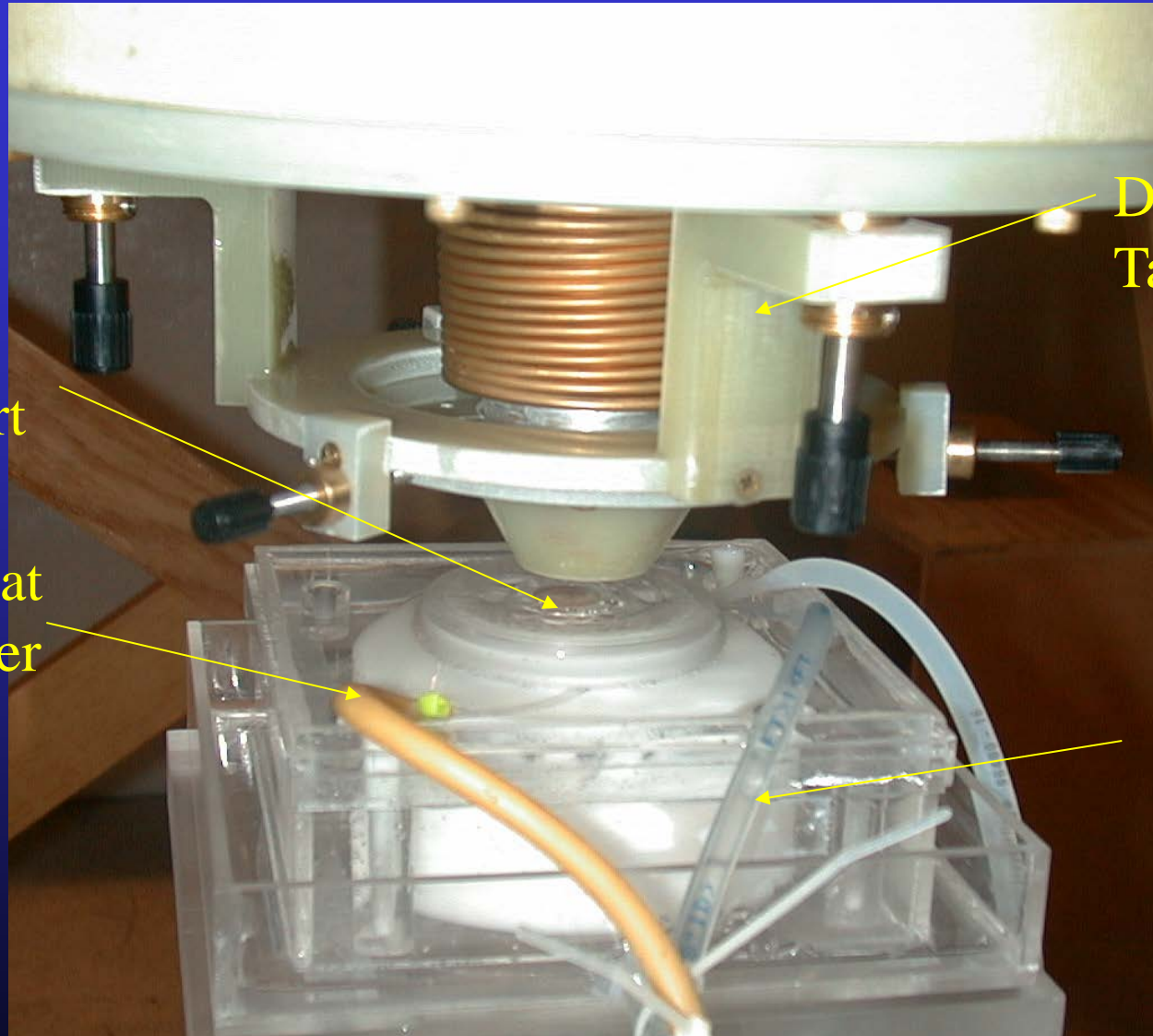
# Langendorff-Perfused Isolated Rabbit Heart

15 $\mu$ m Mylar-Foil

Bath







Isolated  
Rabbit Heart

From Heat  
Exchanger

Dewar  
Tail

To Heat  
Exchanger



# MCG From the LV Free Wall

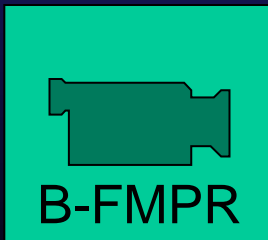
Scan Area

16  
mm

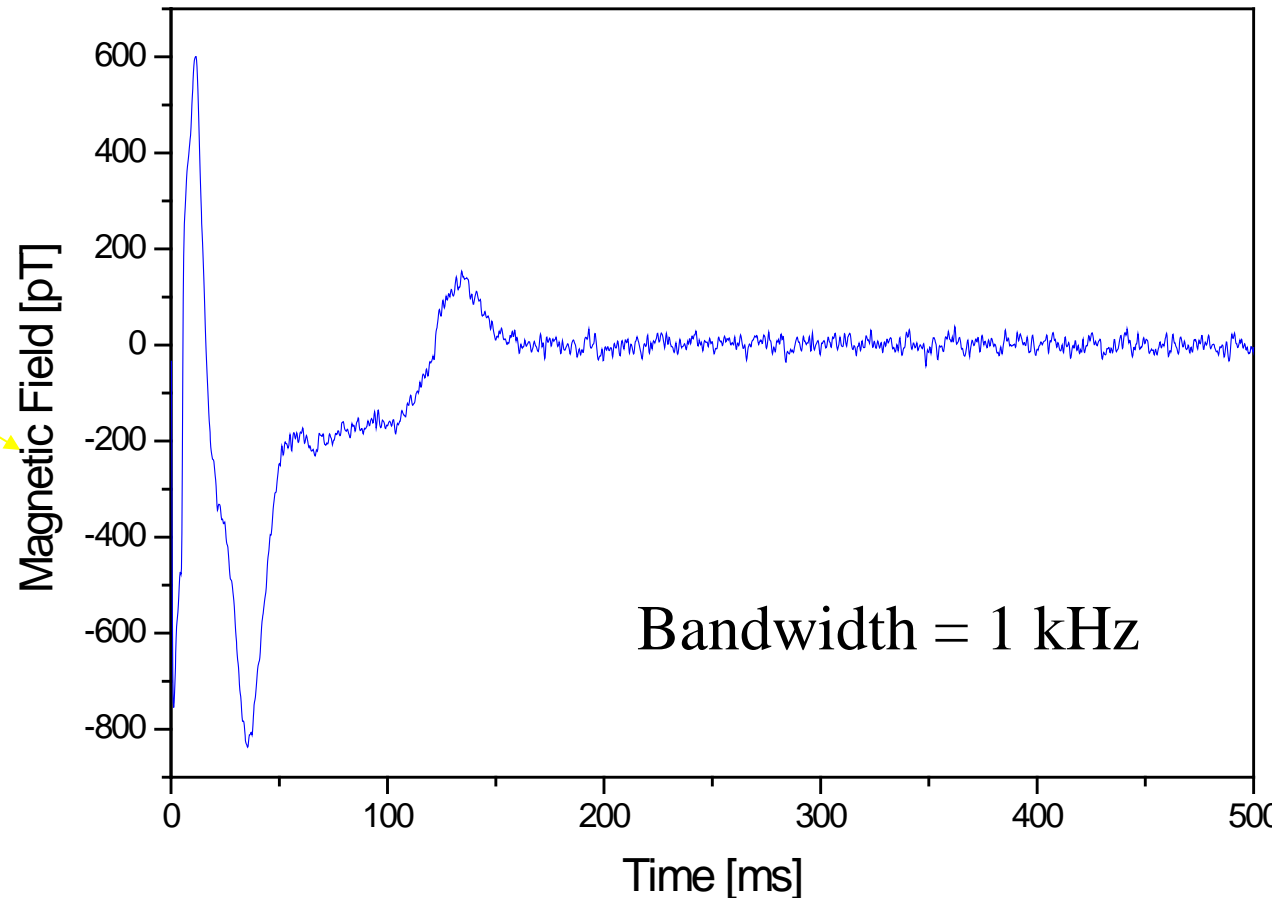


16  
mm

Pixel size 0.16  
mm<sup>2</sup>



B-FMPR



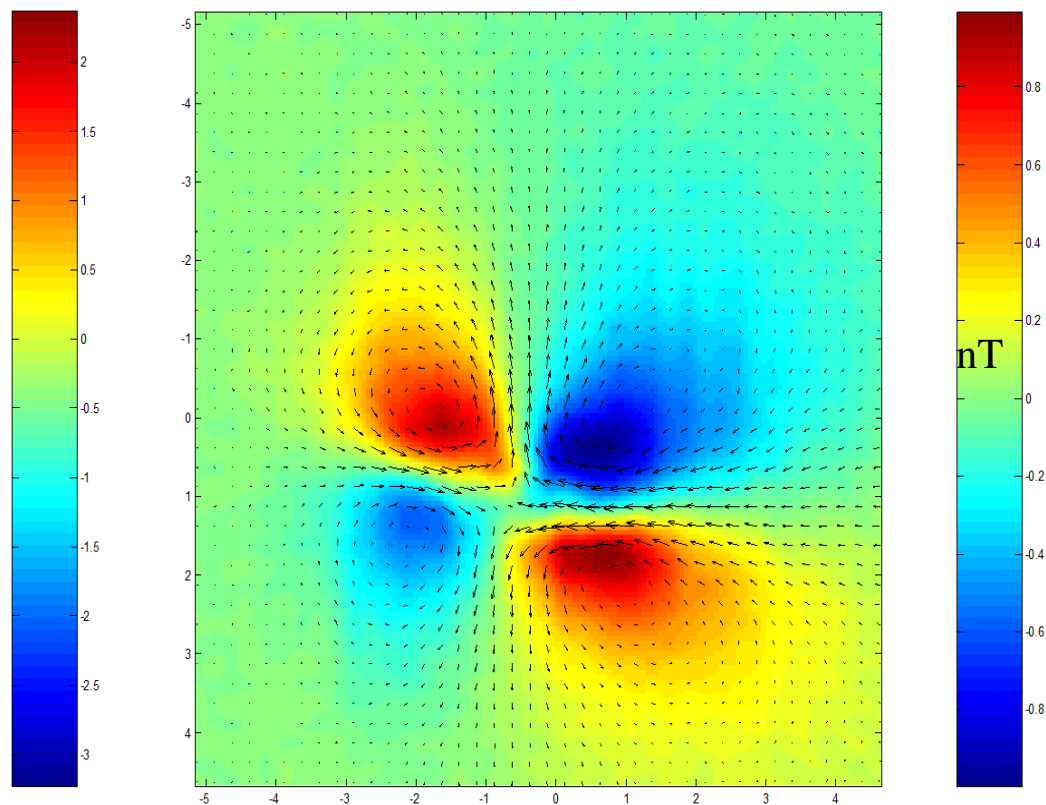
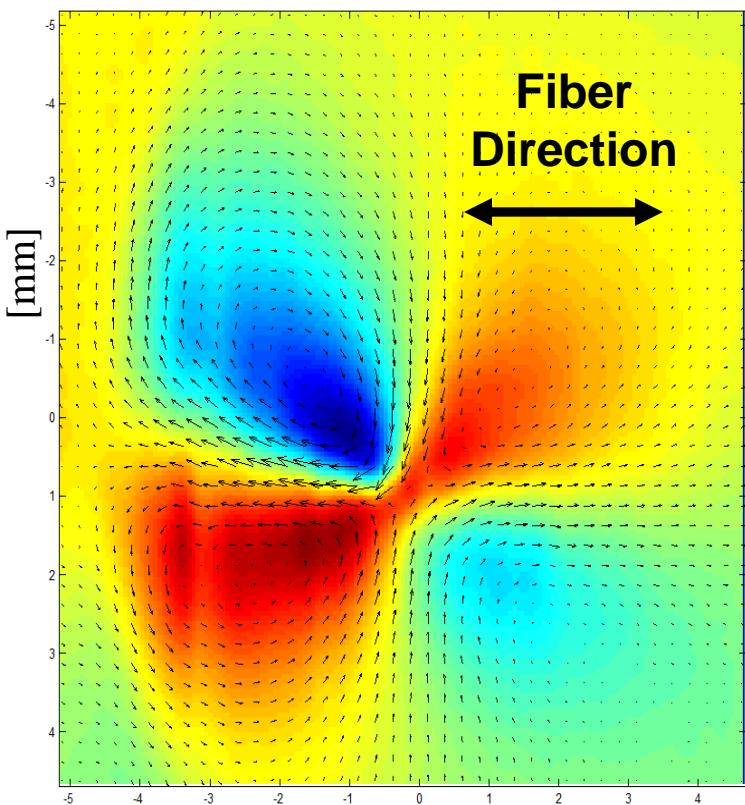
$$1 \text{ pT} \sim B_{\text{earth}} / 100,000,000$$



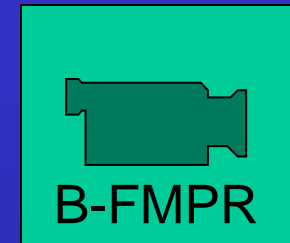
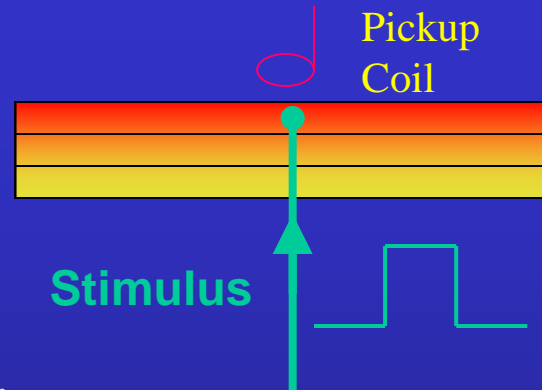
# Cathodal Current Injection Followed by Initiation of Action Currents

Stimulus: 5 ms, 1.5 mA

1 ms after Stimulus



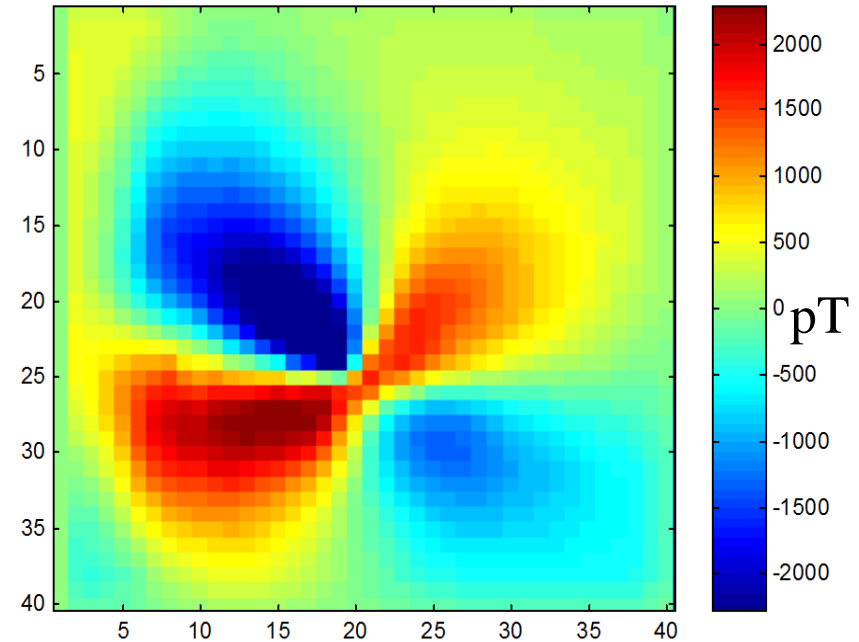
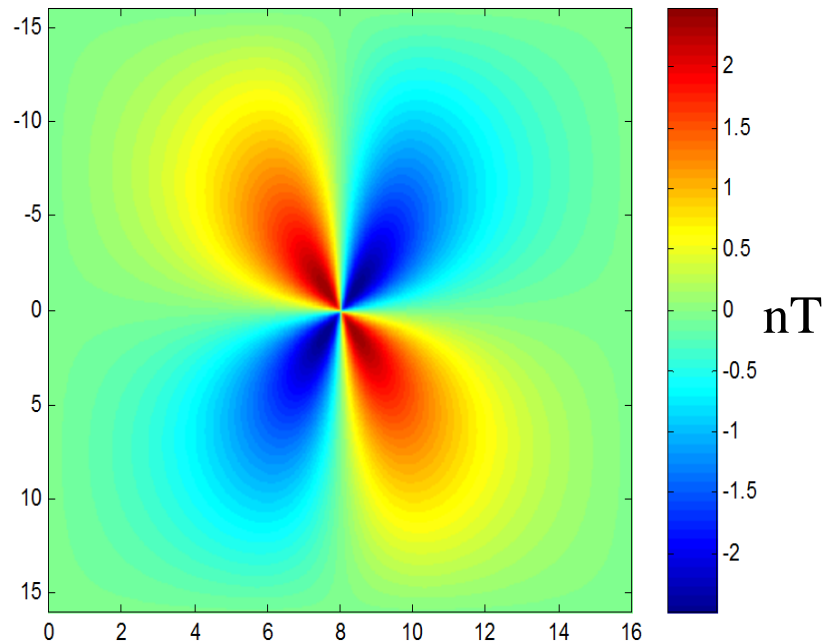
1 cm



## Layered Bidomain

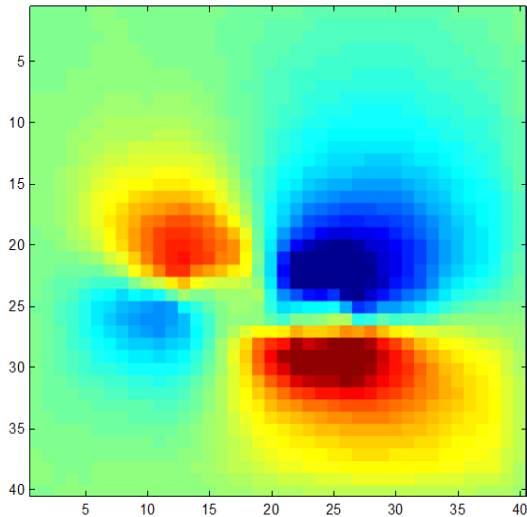
## Experiment

Total Bi-domain Field of 3mm cardiac slice during current injection of 1.5mA  $z=0.1\text{mm}$

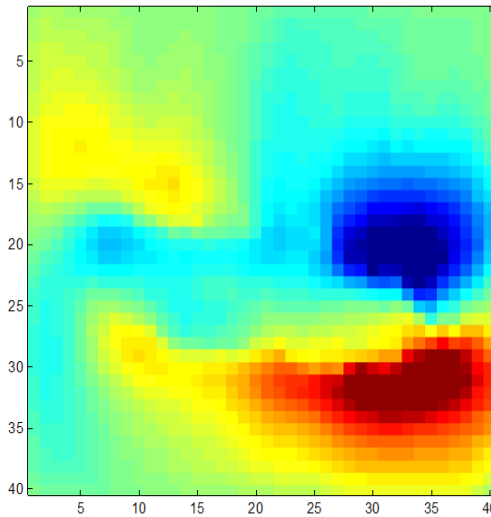




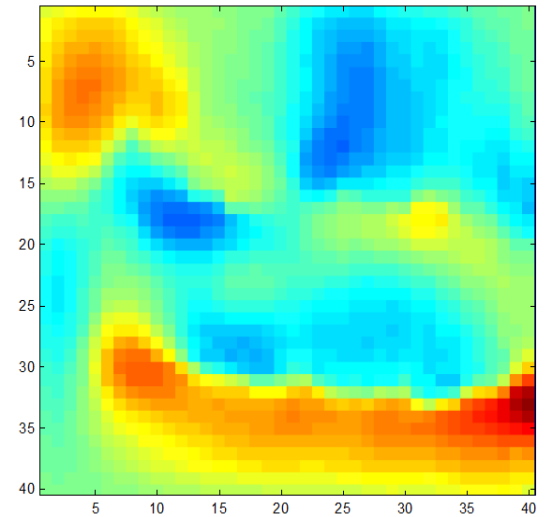
# Propagation of Action Currents



4 ms



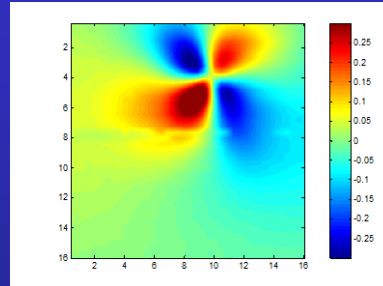
10 ms



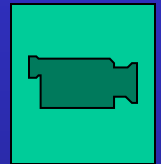
16 ms



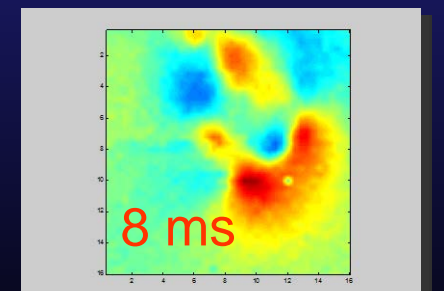
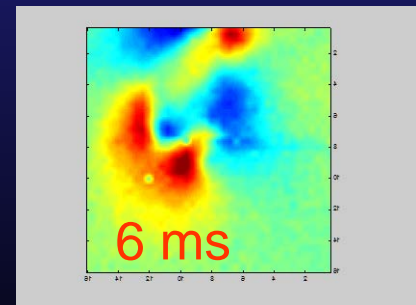
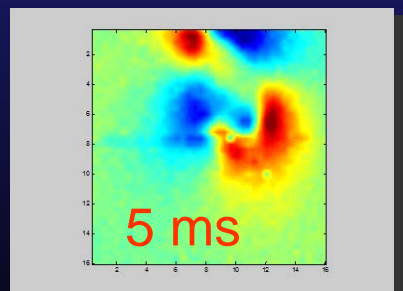
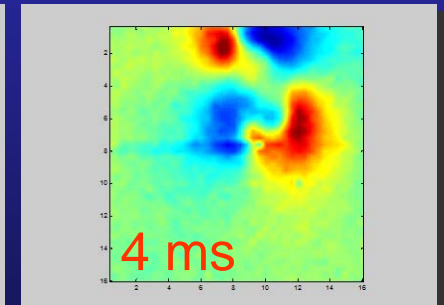
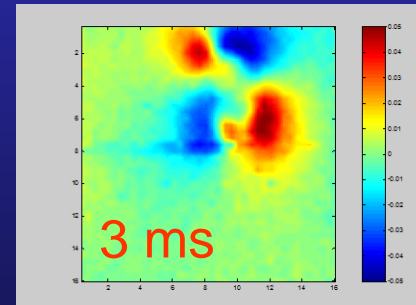
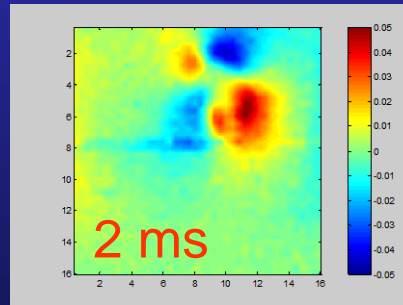
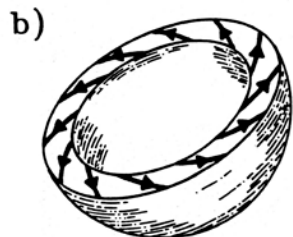
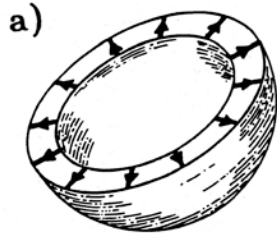
# The Magnetic Field From Action Currents in Isolated Cardiac Tissue – The Apex



Stimulus  
0.6 mA 5 ms



Near\_apex.mpg





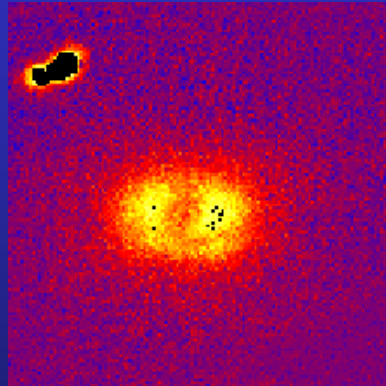
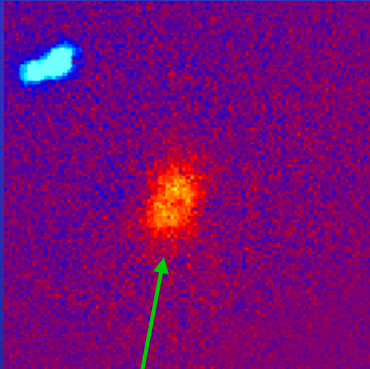


# Forthcoming...

- Measured magnetic field gives current
- Measured  $V_m$  gives the voltage
- Model of both requires the bidomain conductivities (Eason and Trayanova)
- Obtain the doubly anisotropic bidomain conductivities by fitting the model to the data



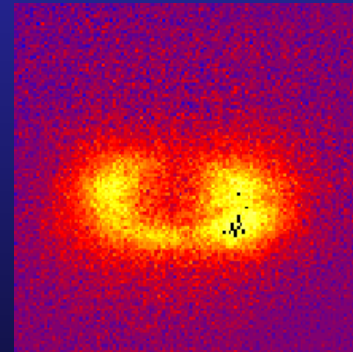
# S2- Point Stimulation



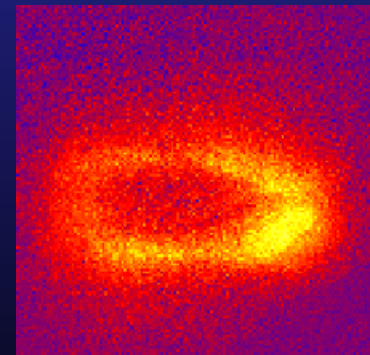
6 ms

Point Electrode

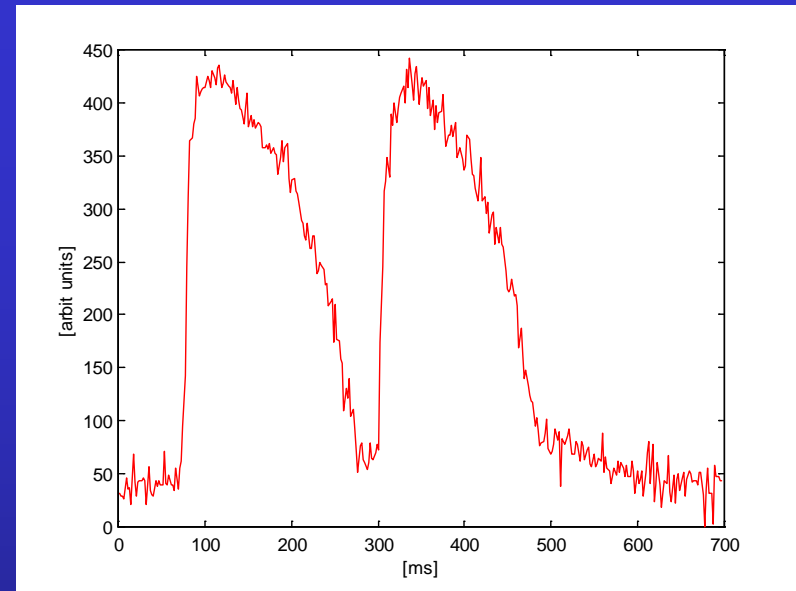
$$S = 6 * \text{Threshold}$$



12 ms



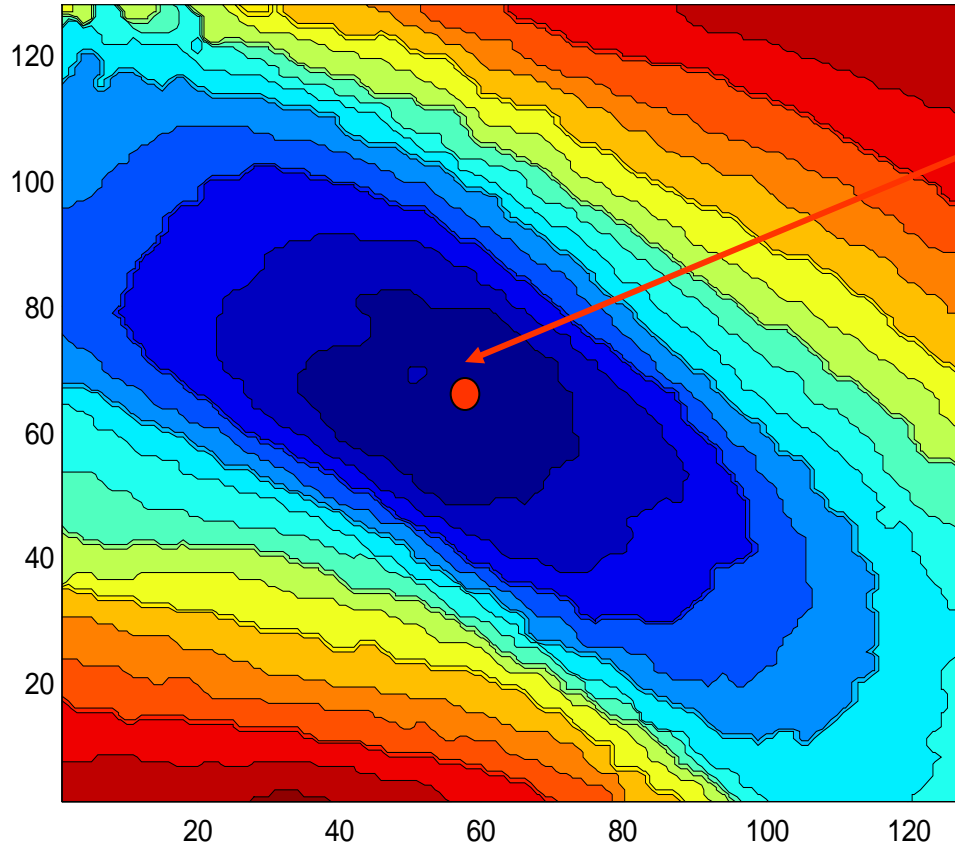
18 ms 40



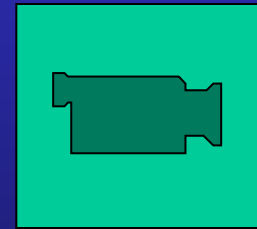
S2-S1=240 ms



# $V_m$ Isochrones – LV Free Wall



Point Stimulation

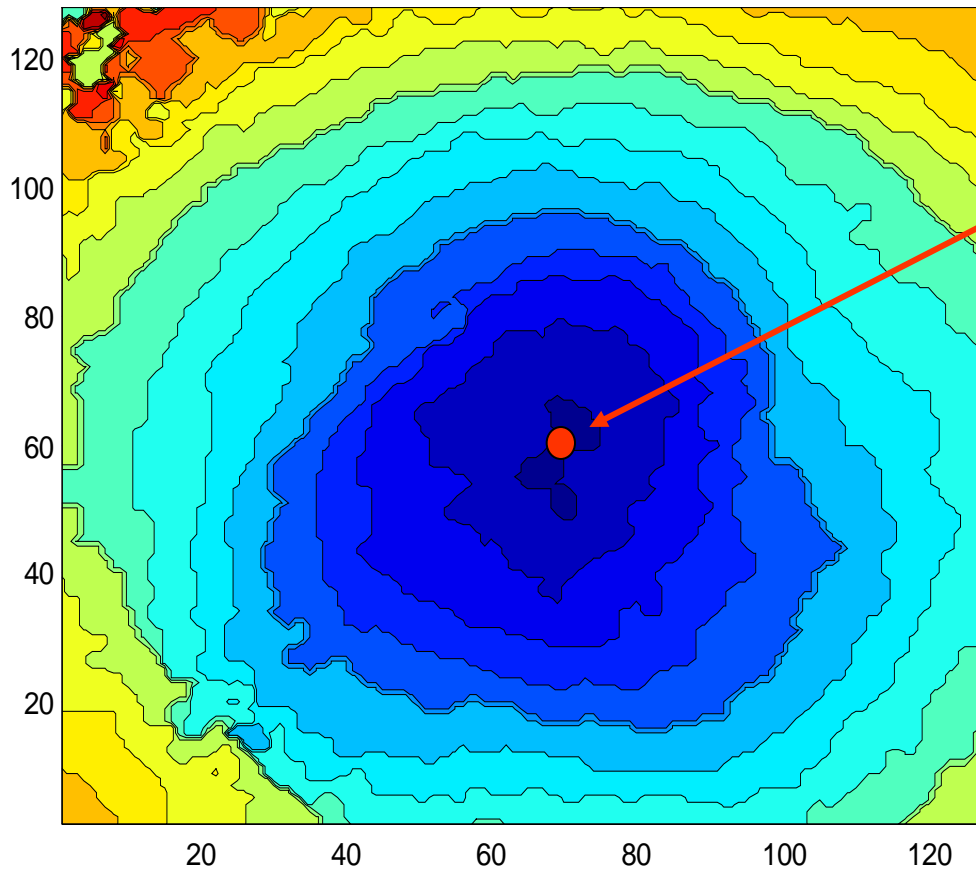


ventricle\_propagation.mpg

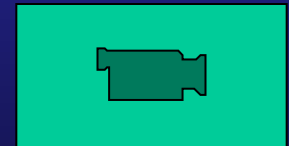
Fiber  
Orientation



# $V_m$ Isochrones - Apex



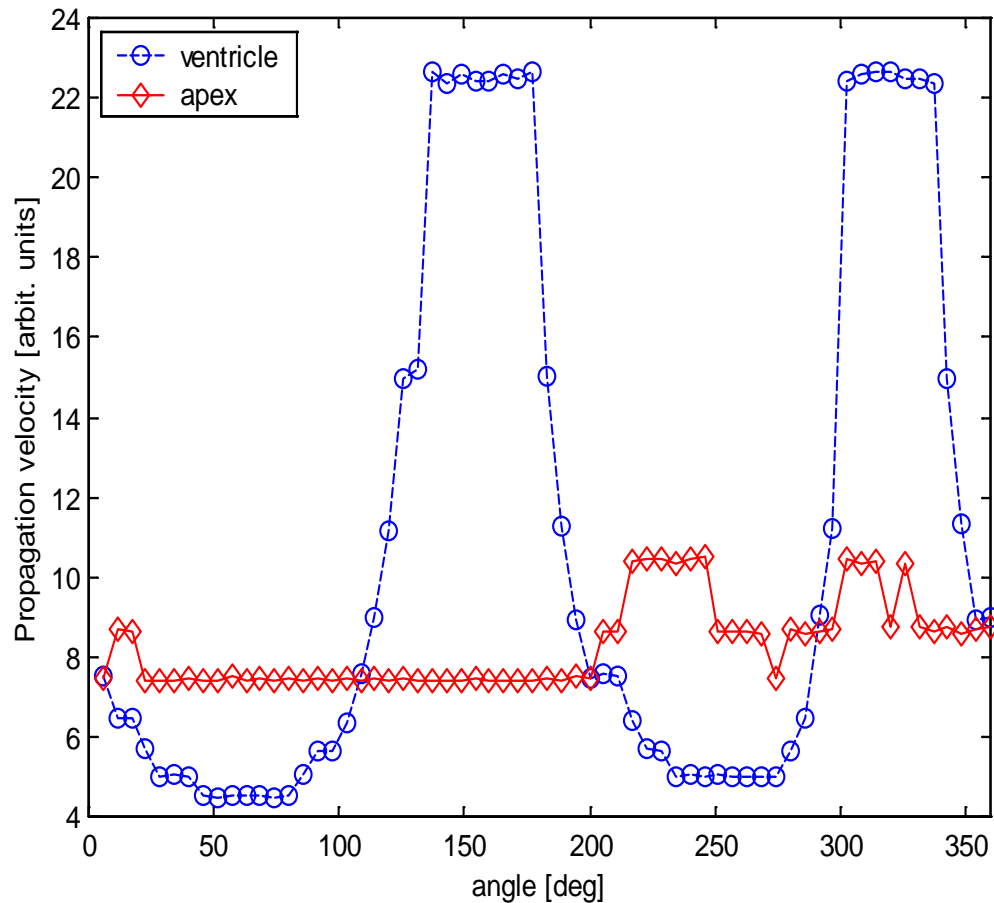
Point Stimulation



apex\_propagation.mpg



# Velocities as a function of direction

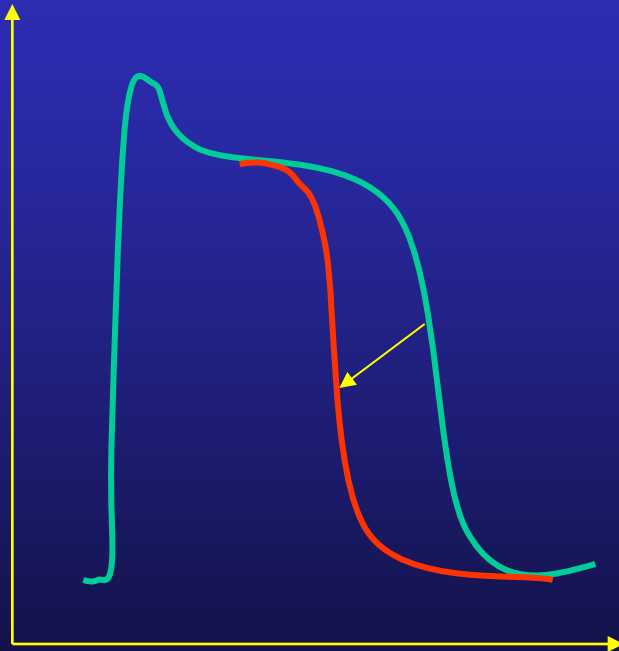




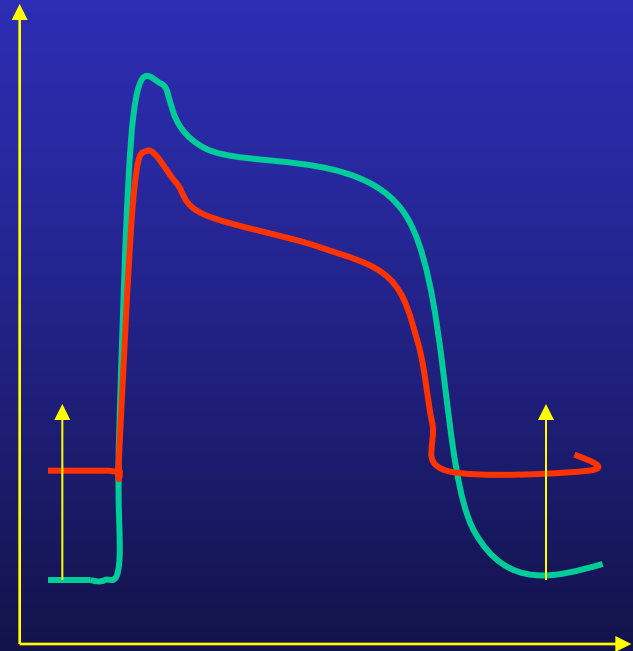


# SQUID Senses Spatial $V_m$ Gradients

Repolarization

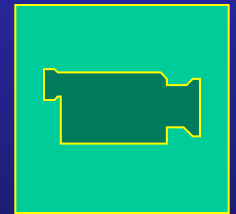
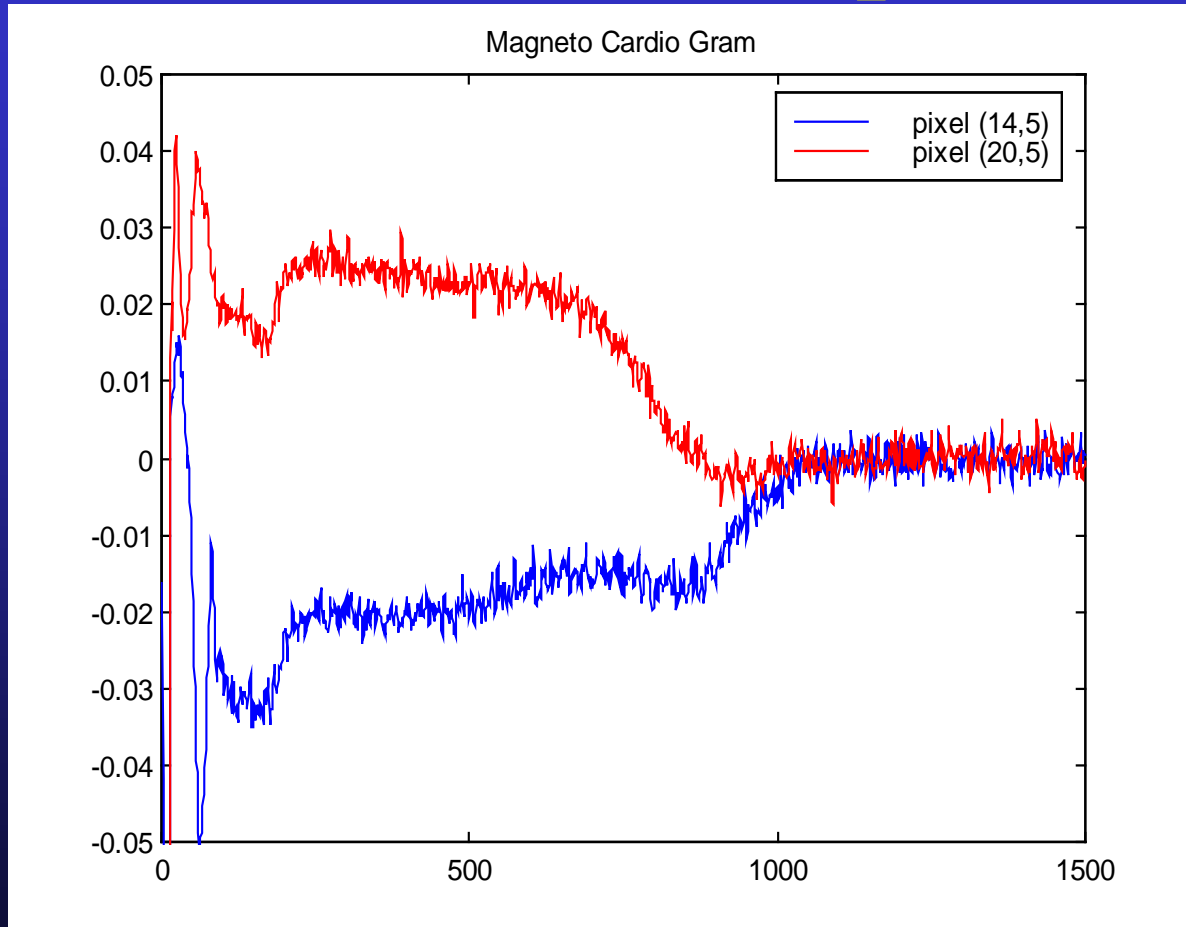


Injury Currents





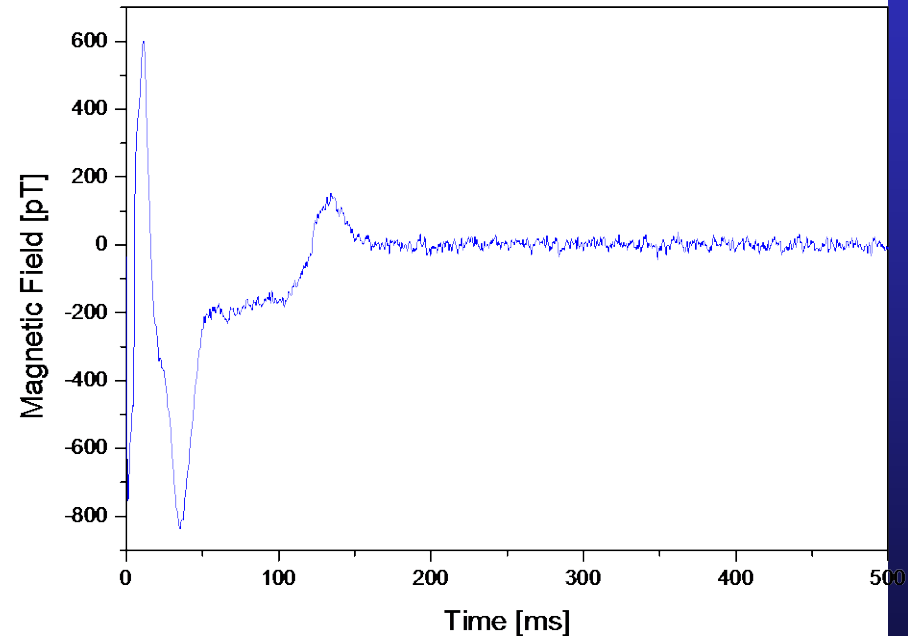
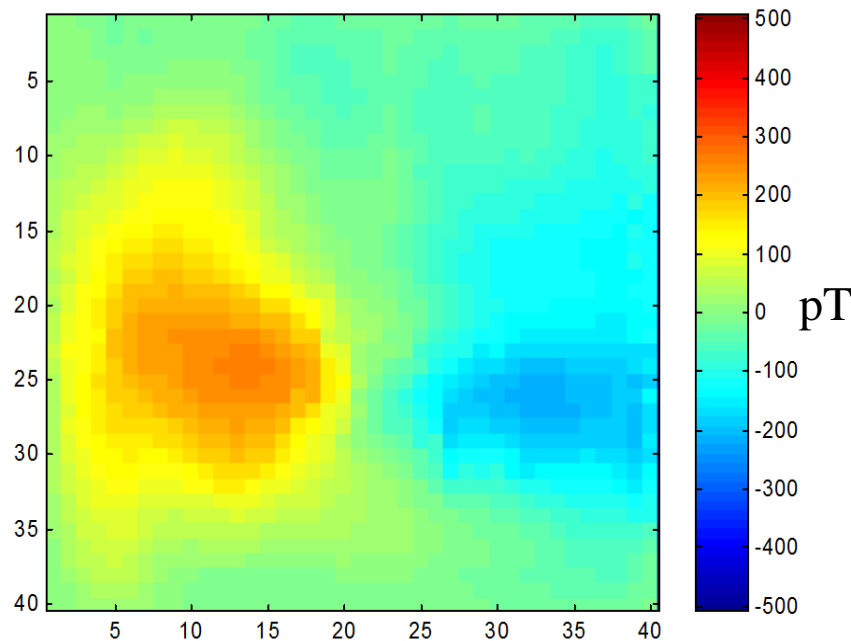
# Gradients in Repolarization



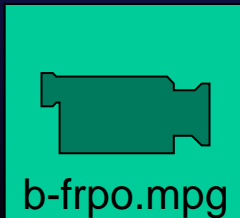
repolarization.mpg



# Dipole Signature in ST-segment



71 ms





# Information Content of the MCG

- Evidence that electrically silent sources exist.
- Magnetic mapping can provide images of net action current in cardiac tissue.
- Combined electric and magnetic measurements can provide the anisotropic conductivities and the non-linear membrane properties.
- A dimensional biodomain model combined with a realistic fiber architecture may provide a better understanding of the MCG.
- MCG allows probing of gradients in repolarization and resting potentials (injury currents).



# Acknowledgements

Rashi Abbas

Petra Baudenbacher

J. J. Koola

Joe Kirschvink

Jenny Holzer

Luis Fong

Marc Lin

Nick Peters

Scott Renkes

Brad Roth

Zvonko Trontelj

Ben Weiss



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