

The Challenges of Spatial Scales in Modeling and Understanding Cardiac Fibrillation

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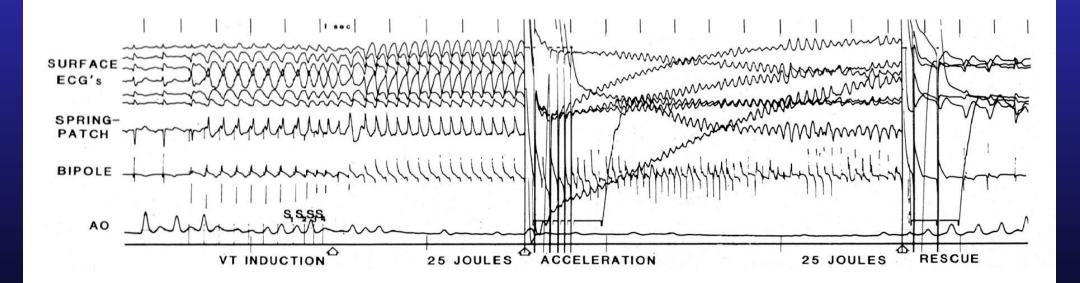
Theme

- The abrupt termination of the Cardiac Arrhythmia Suppression Trial (CAST) was the result of fatal drug effects that were not anticipated by model or experiment
- There is a rapidly growing knowledge base on the structure and function of membrane ion channels
- What is involved in providing a stronger numerical connection between the ion channel and the electrophysiology of the entire heart?
- Models of the electrical activity of the heart during cardiac fibrillation provide serve as a valuable example of just how hard this might be.



Will a particular antiarrhythmic drug alter either the fibrillation or defibrillation thresholds?

• Or... Why I use rabbit hearts as analog computers.





The <u>Ultimate</u> Forward Problem:

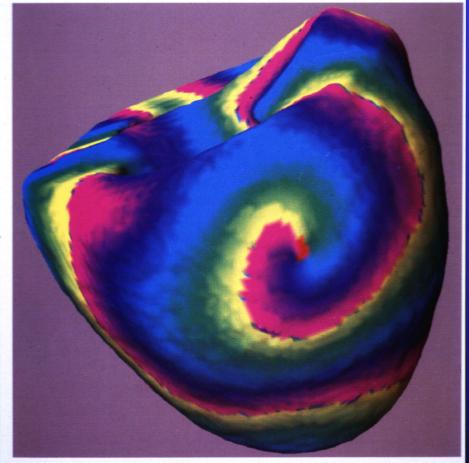
How can we use knowledge of the protein sequence for voltage-gated ion channels to predict numerically the electrocardiogram during a long episode of fibrillation?



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The characteristics of cardiac fibrillation are set by the spatial scale of the <u>entire</u> heart





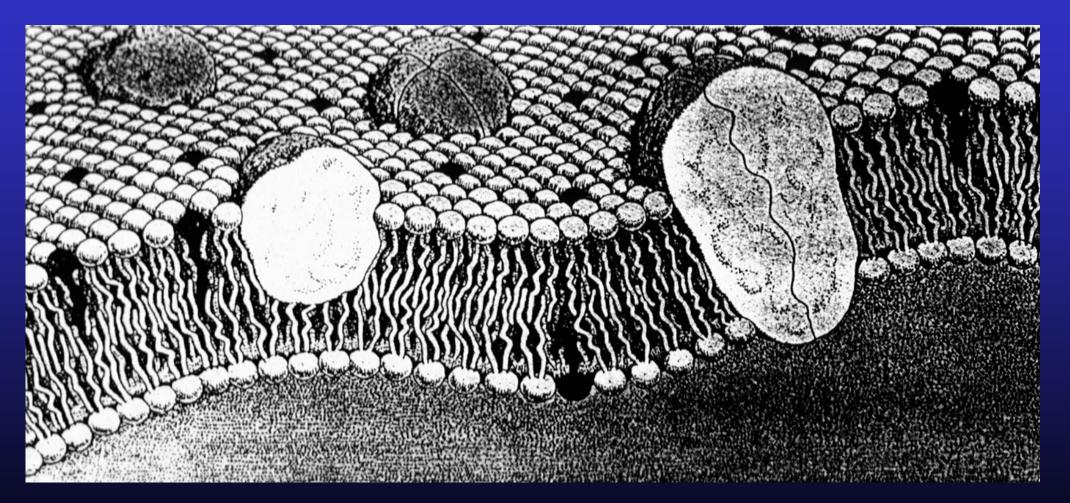
DYNAMICS OF CARDIAC ARRHYTHMIAS

Leon Glass

10 nanometers: Ion channels are in control

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nanometer: Pore in a gated ion channel

The <u>Ultimate</u> Device

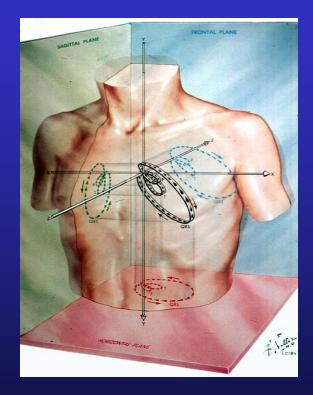
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10⁴ meters pore Lipid neurotransmitter outside bilayer binding pocket Voltage Ð sensor Cytoplasmic Extracellular ĕ Θ side side closed inside Aqueous pore Narrow Gate selectivity filter Sugar Channel Ð residues. protein ACh P 10⁻⁹ meters LOC Anchor protein 0 1 2 3 open nm

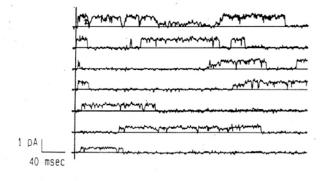


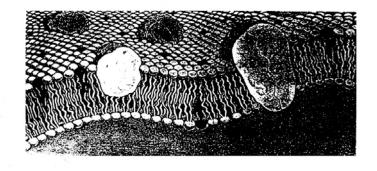
Two extremes: Models of cardiac activity



Einthoven triangle and the cardiac dipole moment 1 m, 10 sec

Channel kinetics from patch clamp 10 nm, 1-10 nsec







The problem of scales: The characteristic lengths and times in biological systems span MANY orders of magnitude.

- An ion channel: $10 \text{ nm} \sim 1 \text{ channel/mm}^2$
- Cardiac cell: 150 mm x 15 mm x 15 mm 500 to 30,000 channels per cell depending upon cell type
- The heart: 10 cm
 - 4×10^9 cells
 - 2×10^{14} channels
- The body: 1 m
- Ratio of spatial scales: 10⁸ in distance, 10²⁴ in volume
- Channels change in 1 10 ns, fibrillation time scale ~10 s
- Ratio of temporal scales: 10⁹ in time



The <u>Ultimate</u> Forward Problem:

- •Assume gated ion-channel protein sequence: **1 nm**
- •Assume that you can compute
 - Protein structure: 1 10 nm
 - Protein kinetics: 1 ns 100 ms
 - Channel response to antiarrhythmic drugs: 10 nm, 1 ns 100 ms
 - Cellular, tissue and cardiac electrodynamics: **10 mm, 10 ms**
 - Electrocardiogram: 1 m, 10 s
 - Fibrillation and defibrillation thresholds: **1 m, 10 s**
- •What will this involve?

Start with the DNA sequence for a potassium channel...

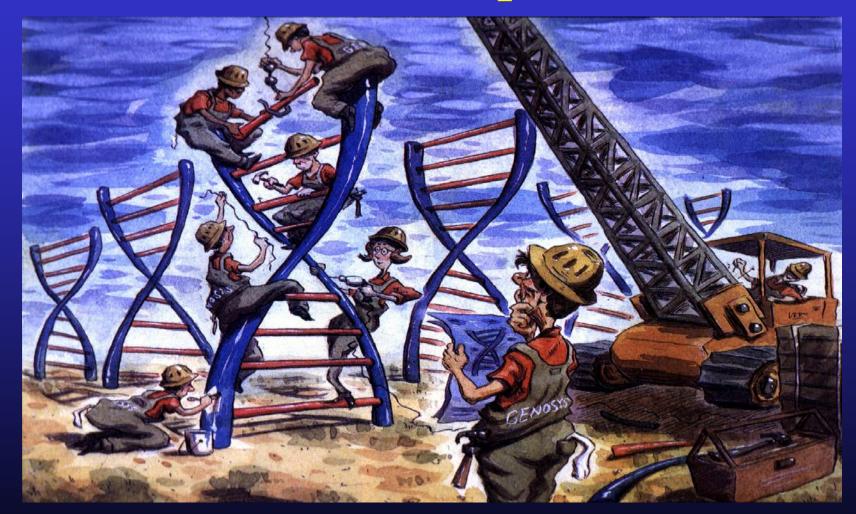
human Kv1.5

GCGGCCGCGCGCGCTTTTTGACGTCAGGGCCAAGCGAGGGGATCGCGCCAGCAACCCCAGCTCTCCCCCAGAGAGGGGCCGG CCGACCGCTGGAGCGGAGCCTGACGCCAGGCGCCCGCGGAGCGTGAGTAGGGGGGCGCGGGAGCCGGTCAGCTGGGGCGCG GCATGCCCTCTGCTCCCGCGCCATGGAGATCGCCCTGGTGCCCCTGGAGAACGGCGGTGCCATGACCGTCAGAGGAGGCG AAGGAGCCGGCGCAAAGGGGCGCGCGCGCAGAGAGACGCGGACTCGGGAGTGCGGCCCTTGCCTCCGCTGCCGGACCCGGG ATCCCGGCCTGGGCACGGTGGAGGACCAGGCTCTGGGCACGGCGTCCCTGCACCACCAGCGCGTCCACATCAACATCTCC GGGCTGCGCTTTGAGACGCAGCTGGGCACCCTGGCGCAGTTCCCCAACACACTCCTGGGGGGACCCCGCCAAGCGCCTGCC **GTACTTCGACCCCCTGAGGAACGAGTACTTCTTCGACCGCAACCGGCCCAGCTTCGACGGTATCCTCTACTACTACCAGT** CCGGGGGCCGCCTGCGAGGGGTCAACGTCTCCCTGGACGTGTTCGCGGACGAGATACGCTTCTACCAGCTGGGGGGACGAG GCCATGGAGCGCTTCCGCGAGGATGAGGGCTTCATTAAAGAAGAGGAGAAGCCCCTGCCCCGCAACGAGTTCCAGCGCCA TCTCCATCATCACCTTCTGCTTGGAGACCCTGCCTGAGTTCAGGGATGAACGTGAGCTGCTCCGCCACCCTCCGGCGCCC CACCAGCCTCCCGCGCCCCCGGGGCCAACGGCAGCGGGGTCATGGCCCCCGCCTCTGGCCCTACGGTGGCACCGCT GCTTCTTCGCCTGCCCCAGCAAGGCAGGGTTCTCCCCGGAACATCATGAACATCATCGATGTGGTGGCCATCTTCCCCTAC CCTGGCCATCCTCCGAGTCATCCGCCTGGTCCGGGTGTTCCGCATCTTCAAGCTCTCCCGCCACTCCAAGGGGGCTGCAGA TCCTGGGCAAGACCTTGCAGGCCTCCATGAGGGAGCTGGGGCTGCTCATCTTCTTCCTCTCATCGGGGTCATCCTCTTC TCCAGTGCCGTCTACTTCGCAGAGGCTGACAACCAGGGAACCCATTTCTCTAGCATCCCTGACGCCTTCTGGTGGGCAGT GGTCACCATGACCACTGTGGGGCTACGGGGGACATGAGGCCCCATCACTGTTGGGGGGCAAGATCGTGGGGCTCGCTGTGTGCCA TCGCCGGGGTCCTCACCATTGCCCTGCCTGTCCCGTCATCGTCTCCAACTTCAACTACTTCTACCACCGGGAAACGGAT CACGAGGAGCCGGCAGTCCTTAAGGAAGAGCAGGGCACTCAGAGCCAGGGGCCGGGGCTGGACAGAGGAGTCCAGCGGAA GGTCAGCGGGAGCAGGGGATCCTTCTGCAAGGCTGGGGGGGACCCTGGAGAATGCAGACAGTGCCCGAAGGGGCAG CCCTAGAGAAGTGTAACGTCAAGGCCAAGAGCAACGTGGACTTGCGGAGGTCCCTTTATGCCCTCTGCCTGGACACCAGC CGGGAAACAGATTTGTGAAAGGAGATTCAGGCAGACTGGTGGCAGTGGGAGTAGGGAATGGGAGGCTTCTGAACATGGATA TCTACATTATCCGCAGAGTATTTGACTCACTCCTCT

Courtesy of Dirk Schneiders



Assemble the proteins

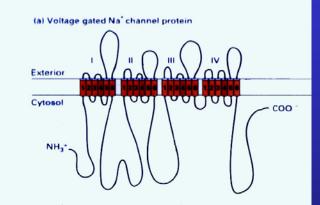




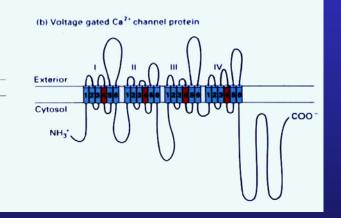
And we solve the protein folding problem...



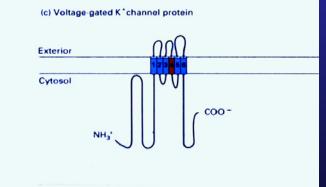
Insert the folded proteins into the membrane



Voltage-gated Na⁺ channel



Voltage-gated Ca++ channel



Voltage-gated K⁺ channel

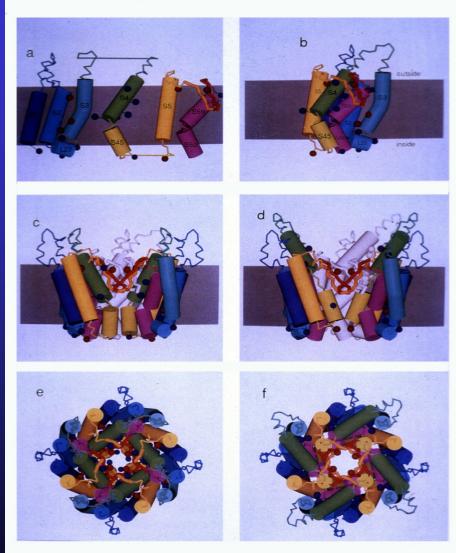
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Compute how the protein conformation depends upon voltage or ligand binding

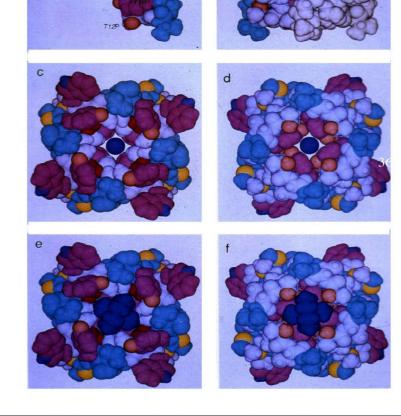
S.R. Durrell and H.R. Guy, Biophysical Journal, 62: Discussions 1992 238-250 (1992)





See which drugs block the channel

S.R. Durrell and H.R. Guy, Biophysical Journal, 62: Discussions 1992 238-250 (1992)





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Compute the channel kinetics to determine the switching behavior

Courtesy of Dirk Schneiders

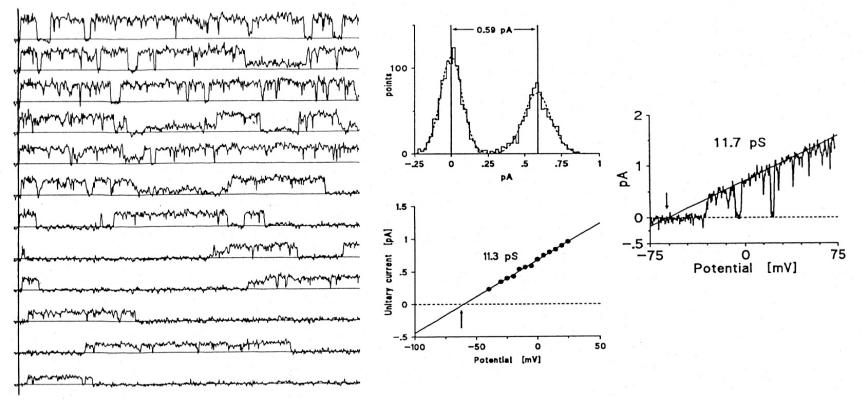
 $D_4 \stackrel{4\alpha}{\longrightarrow} D_3 A \stackrel{3\alpha}{\longrightarrow} D_2 A_2 \stackrel{2\alpha}{\longrightarrow} DA_3 \stackrel{\alpha}{\longrightarrow} A_4 = 0$ 47 8 37 8 37 8 T 8 $D \Longrightarrow D \Longrightarrow A$ $D_3I \xrightarrow{3\alpha}{A} D_2AI \xrightarrow{2\alpha}{A} DA_2I \xrightarrow{\alpha}{A} A_3I$ $D \Rightarrow D \Rightarrow A$ $D \Rightarrow D \Rightarrow A$ $D_4 \stackrel{*}{\longleftarrow} D_5 A \stackrel{*}{\longrightarrow} D_2 A_2 \stackrel{*}{\longrightarrow} DA_3 \stackrel{*}{\longleftarrow} A_4$ $D \rightleftharpoons D \rightleftharpoons A \rightleftharpoons I$ k i 2k 1 4 3k 1 3g 4k 1 2 $D_3O \xrightarrow{34} D_2AO \xrightarrow{24} DA_2O \xrightarrow{8} A_3O$ $D \stackrel{*}{\longrightarrow} A \stackrel{*}{\rightarrow} 0$ k 21 2k 21 1 3k, 21 34 $D \stackrel{*}{\underset{\scriptscriptstyle B}{\longrightarrow}} A \stackrel{*}{\underset{\scriptscriptstyle P}{\longleftarrow}} 0$ $D_2O_2 \xrightarrow{21}{\beta} DAO_2 \xrightarrow{2}{\beta} A_2O_2$ $D \stackrel{\alpha}{\longrightarrow} A \stackrel{A}{\longrightarrow} 0$ k 31 24 31 -1 $D_n \xrightarrow{n \propto} A_m A_m D_{03} \xrightarrow{q} A_{03}$ $D \stackrel{\circ}{=} A \stackrel{\circ}{=} 0$ m.k. p.L k 41



1 pA

40

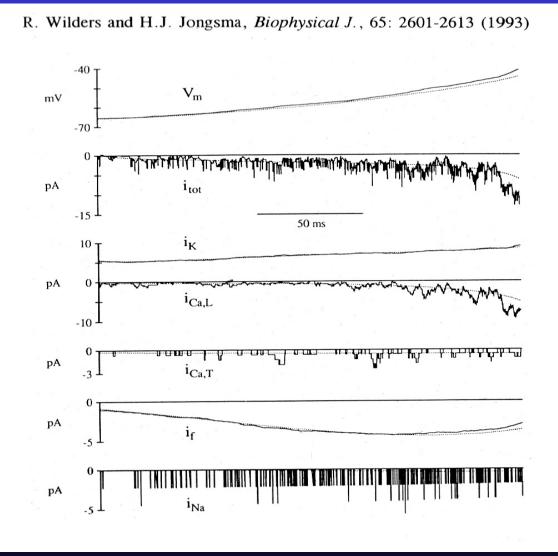
Compute the time-dependent channel conductance



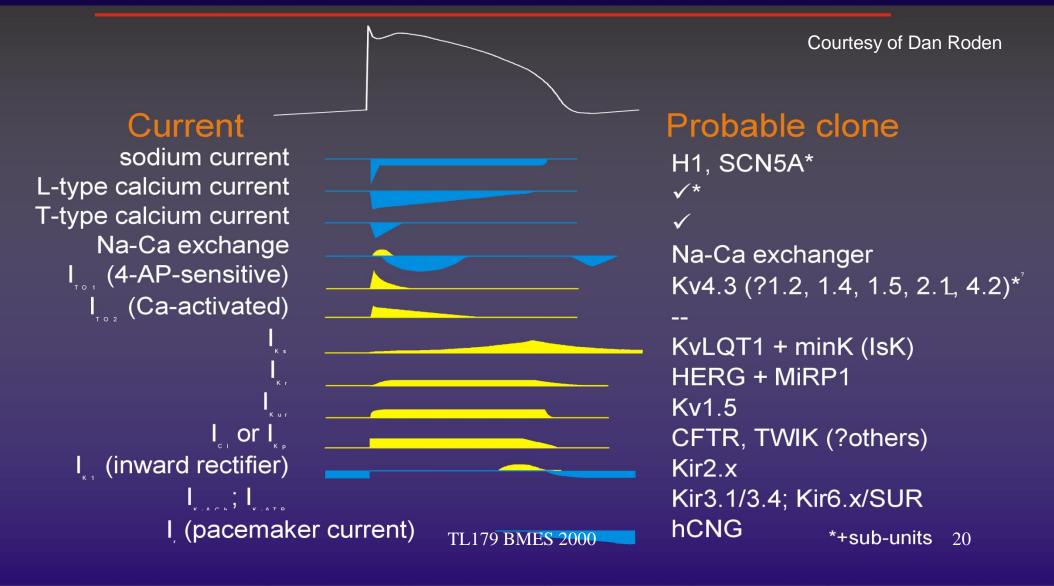
Wilders and Jongsma, Biophys. J., 65: 2601-2613 (1993)

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Stochastically activate the channels

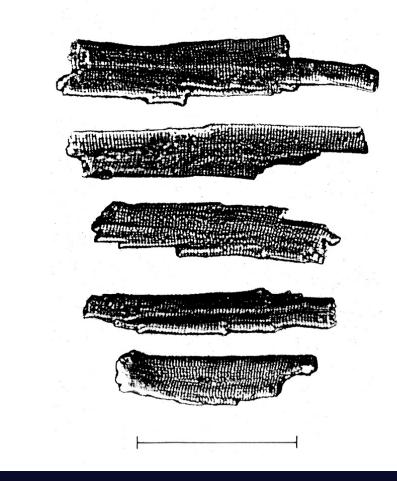


Describe the channel currents in terms of a Hodgkin-Huxley-like model such as Luo-Rudy I or II



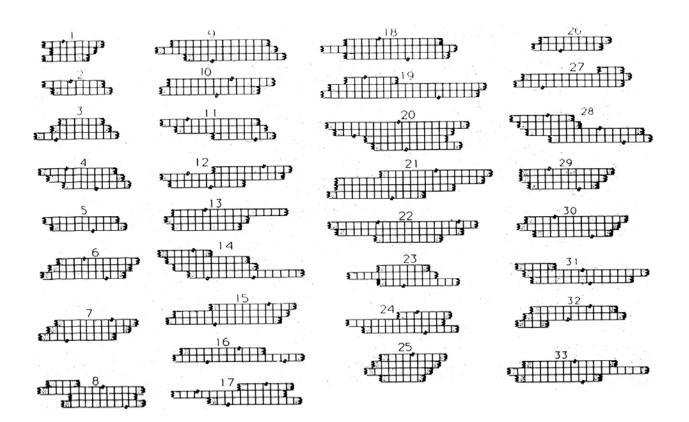


Sprinkle the channels and their currents onto a family of virtual cardiac cells M.S. Spach and J.F. Heidlage, in *High Performance Computing in Biomedical Research*, T.C. Pilkington *et al.*, Eds., (CRC, Boca Raton, 1993) pp 289-317



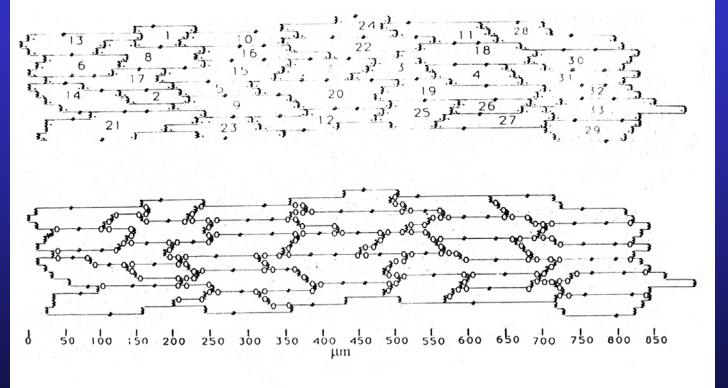


Divide each cell into a numerically stable subunit M.S. Spach and J.F. Heidlage, in High Performance Computing in Biomedical Research, T.C. Pilkington et al., Eds., (CRC, Boca Raton, 1993) pp 289-317

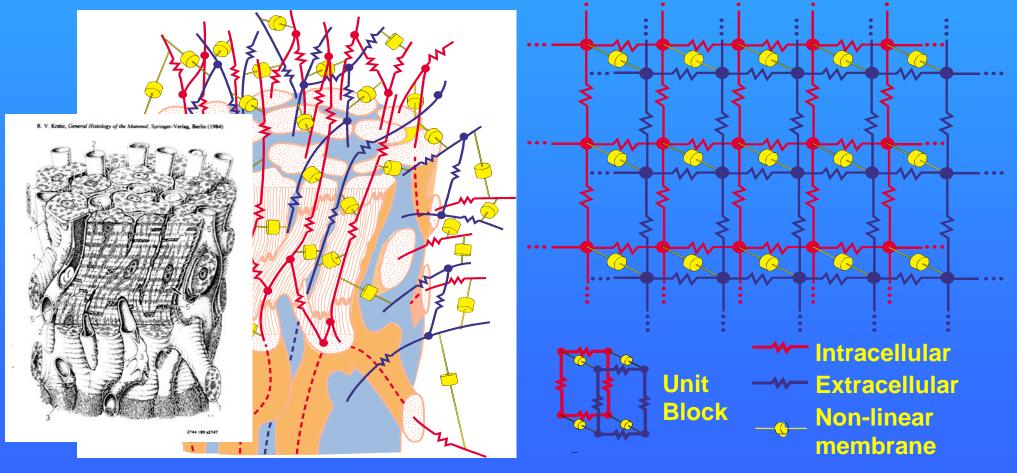




Assemble the cells into small regions of cardiac tissue M.S. Spach and J.F. Heidlage, in High Performance Computing in Biomedical Research, T.C. Pilkington et al., Eds., (CRC, Boca Raton, 1993) pp 289-317



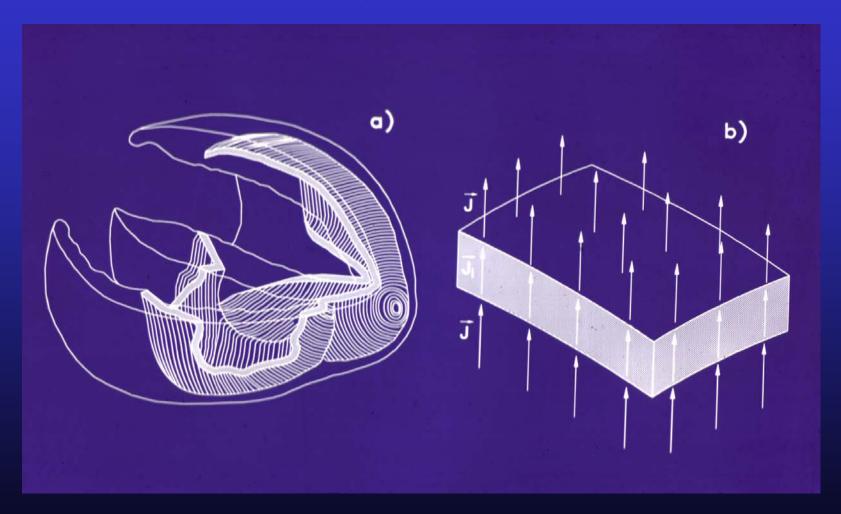
Include the three-dimensional cable properties of the anisotropic cardiac syncytium





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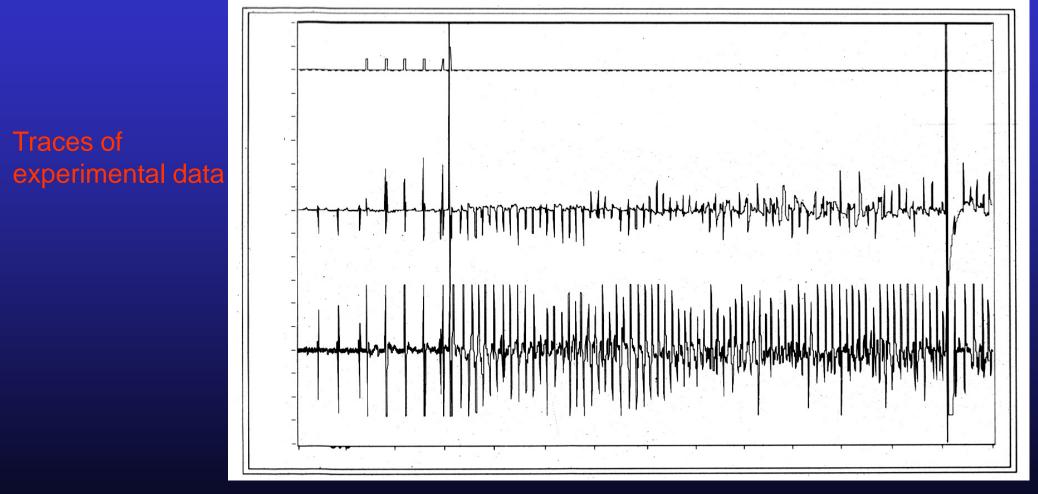
Assemble the regions into a whole heart





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Compute 10 seconds of fibrillation ...



Courtesy of Debra Echt

The computer runs forever.... Look at the model

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81 free parameters for each volume element in the model

Potentials	(2)
V _i , V _e	
Anisotropy tensors	$(3 \times 6 = 18)$
conductivity, stress, strain	
Volume fractions	(3)
vol_e/vol_i , vol_{sr}/vol_i , $area_m/vol_i$.	
Concentrations	(12)
$[Na^+]_i$, $[Na^+]_e$, $[K^+]_i$, $[K^+]_e$, $[K^+]_e$] _{cleft} ,
[Cl ⁻] _i , [Cl ⁻] _e , [Ca ⁺²] _i , [Ca ⁺²] _e , [Ca ⁺	⁻²] _{sr} ,
$[ATP]_{i}, [ACh]_{e}, [H^{+}]_{i}, [H^{+}]_{e}$	
Currents with activation and inactivation	$(6 \times 3 = 18)$
$I_{Na}, I_{Ca}, I_{Ca,Na}, I_{Ca,K}, I_{rel}, I_{Cl,Ca}$	
Currents with activation	$(7 \times 2 = 14)$
I_{K1} , I_{Kp} , I_{K} , $I_{ns,Na}$, $I_{ns,K}$, I_{tr} , $I_{stretch}$	
Steady-state currents	(7)
$I_{Ca,b}, I_{Na,b}, I_{leak}, I_{k,ATP}, I_{k,ACh}, I_{k,PC}, I_{h}$	k,AA
Pumps	(7)
$I_{NaK}, I_{p(Ca)}, I_{up}, I_{NaCa}, I_{ATPCa}, I_{HK}, I_{HC}$	1
Total	81
	701 199 -0704
2.	791 188 s2794

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The Problem of Scale: Numerical Models

- Divide each cardiac cell into 10 segments:
 - 4×10^{10} segments/heart
- At least 50 currents and other variables/segment
 - 2×10^{12} variables/heart
- 5 μ s/timestep: 2 x 10⁶ timesteps/10s of fibrillation
- 4×10^{18} equations to solve ... micromoles
- 46,000 years on a 25 MFLOP workstation
- 10 years on 1200 100 MFLOP workstations
- 1 year on a 1 TFLOP workstation
- At 100 bytes/segment, 4 Tbytes of memory or disk to store the model

Cherry, Greenside, Henriquez PRL 2/7/00: Whole-heart, minimal adaptive mesh LR1 estimated 10⁻⁵ real time with a 533 MHz DEC **a**; 70x increase with a 100-parallel computer.



Discussion

- Whole-heart cardiac models involve brute-force solution of partial differential equations, using either HH-type models (LR, etc), or eikonal equations
- At present, there are few if any numerical, theoretical, or analytic connections between the molecular description of the channel and either HH-type or eikonal models



Solutions to the Ultimate Forward Problem

- Develop efficient multiscale/mesoscale models to span the full range of space and time
 - Molecular dynamics vs. statistical mechanics vs. thermodynamics
 - Eikonal equations for the wave front properties
 - Direct physiological determination of eikonal equation parameters
- An isolated rabbit heart: a self-assembling, multivarible, multistate, massively parallel, nonlinear analog computer
 - Solves ~ 10^{17} equations/second at \$30/hour
 - Requires improved programming techniques
 - Requires improved readout of the answer



Characterizing the Cardiac State What do you do with all the data?

- <u>Ontological failure</u>: "The phenomena you are interested in requires elements or laws outside of the set you have been given."
- <u>Epistimological Failure</u>: "You have enough elements and the laws do apply, but you yourself cannot understand the explanation that they provide."

D Bray, TIBS 22, pp 325-326 (1997)



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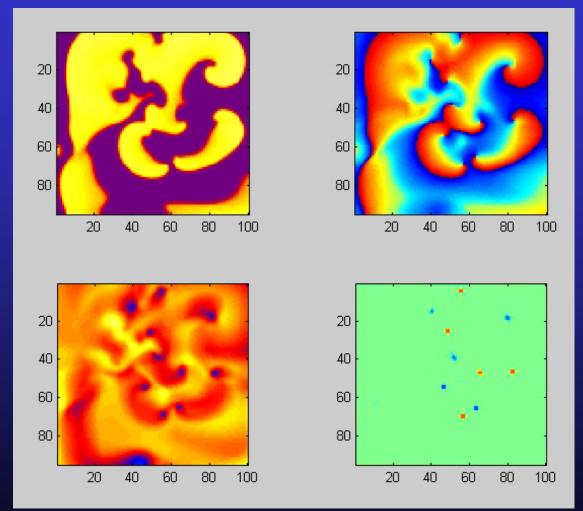
Visualizing Fibrillation

V_m Phase

Variance Curl

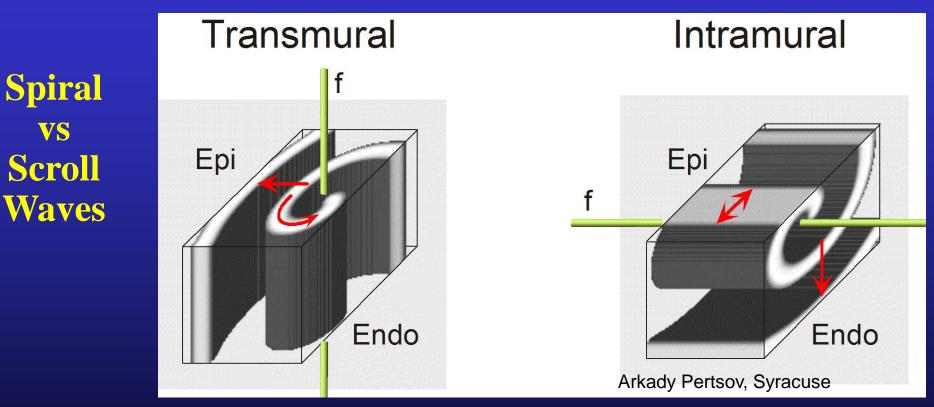


Vm_Var_Phase_Curl.mp4





And the Third Dimension...

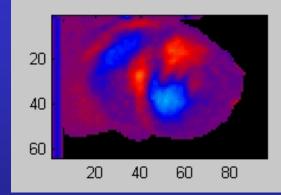


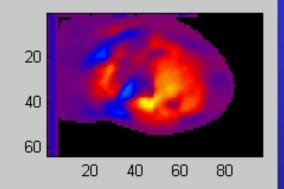
- Transmural waves can exist in 2-D (thin) or 3-D (thick)
- Intramural waves require ~1 cm wall thickness

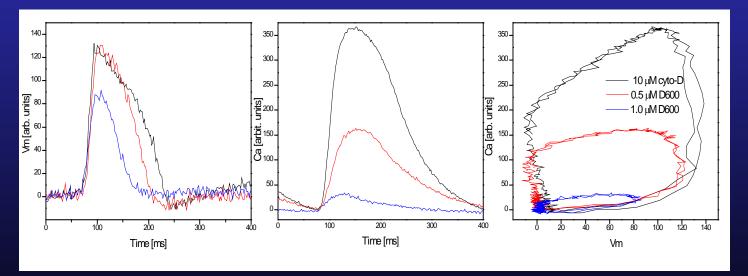


Understanding Cardiac Dynamics

V_m & Ca⁺⁺ vs. Methoxyverapamil (D-600)









Vm_Ca.mp4



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