



VANDERBILT
UNIVERSITY

Synthesis and Characterization of a New Class of Shape Memory Polymers for Development of “Smart” Vascular Constructs

James Taylor, Timothy Boire, Joshua Stewart, Mukesh K. Gupta Ph.D., and Hak-Joon Sung, Ph.D.

Department of Biomedical Engineering, Vanderbilt University, Nashville, TN

UMBC

AN HONORS
UNIVERSITY
IN MARYLAND

Introduction - Shape Memory Polymers

- Shape memory polymers (SMPs) are materials that can be molded into different shapes but will also return to their original shape with a specific stimulus
- Our aim is to create an injectable thermal responsive SMP based on poly(caprolactone) (PCL)-derived copolymers that can be used for implantable vascular patches
- PCL's biodegradability and biocompatibility make it a promising base for SMPs

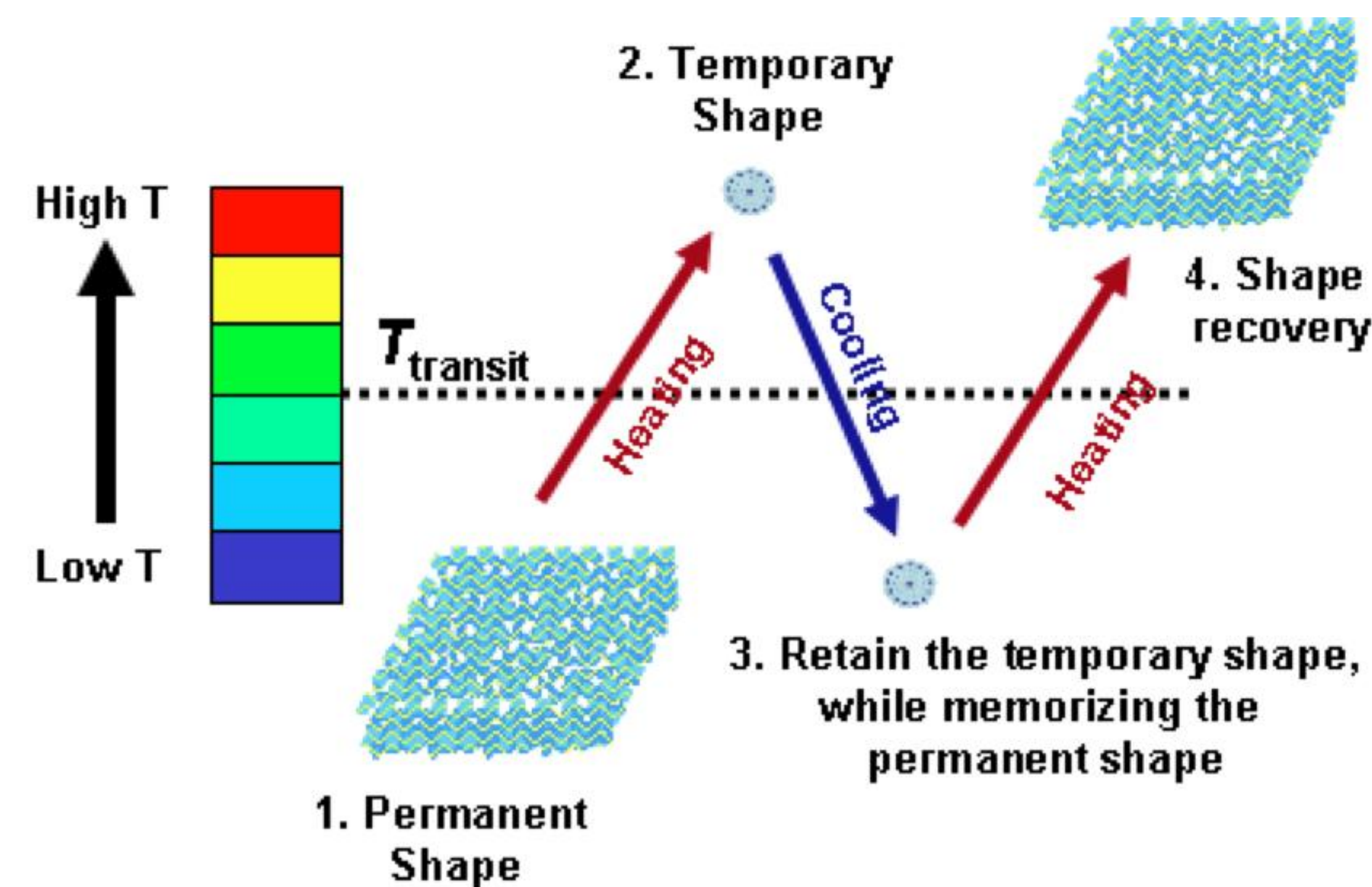


Figure 1: Typical thermal response shape memory cycle. The polymer is heated past a transition temperature and if it is cooled past that temperature under strain, it keeps that temporary shape until it is reheated. Diagram Courtesy of Dr. Hak-Joon Sung

Characterization of Shape Memory Polymer

Differential Scanning Calorimetry (DSC)

- DSC measures heat flow associated with phase changes as a function of temperature.
- We use it to determine the melting (transition) and crystallization temperatures as well as the glass transition point.

Dynamic Mechanical Analysis (DMA)

- In DMA, the polymer is characterized as it is subjected against different forces, deformations, and temperatures.

Contact Angle Characterization

- Water is dropped on the polymer film and the contact angle is recorded using a goniometer
- The way the water wets across the surface gives us an idea of the film's hydrophilicity

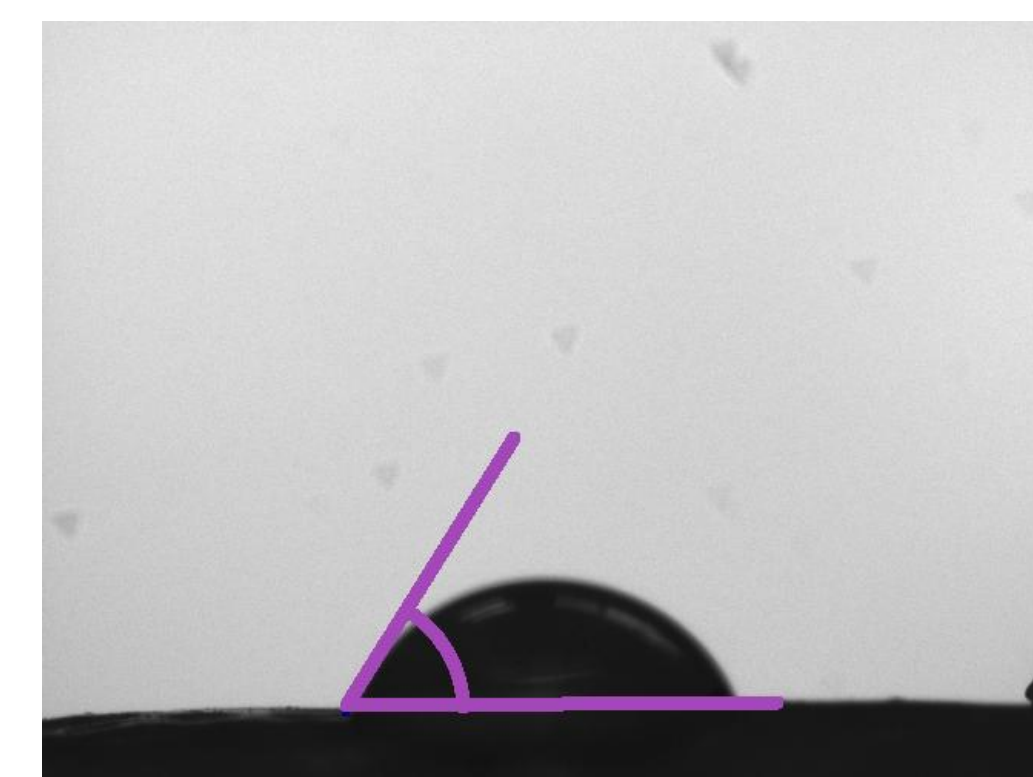


Figure 3 (Left): A picture of a 26%ACPCL-74%PCL film on the goniometer. The goniometer measures the angle at which a drop of water lays on the film. Picture courtesy of Joshua Stewart

Figure 4 (Right): A typical DSC graph after the thermal history has been removed. The exothermic peaks (pointing upward) represent crystallization peaks and the endothermic peaks (pointing downward) represent transition peaks. The curve at ~-50 represents a glass transition state

Preliminary Results

- Our synthesis is capable of producing polymer films that have transition temperatures around body temperature (~29-41) and have molecular weights of 10 kDa although the weights are not consistent
- The polymer films yield under 1 N of force applied
- The films exhibit slightly different thermal properties once their thermal histories have been destroyed. Prior to this, most exhibited multiple transition and crystallization peaks due to heterogeneity.

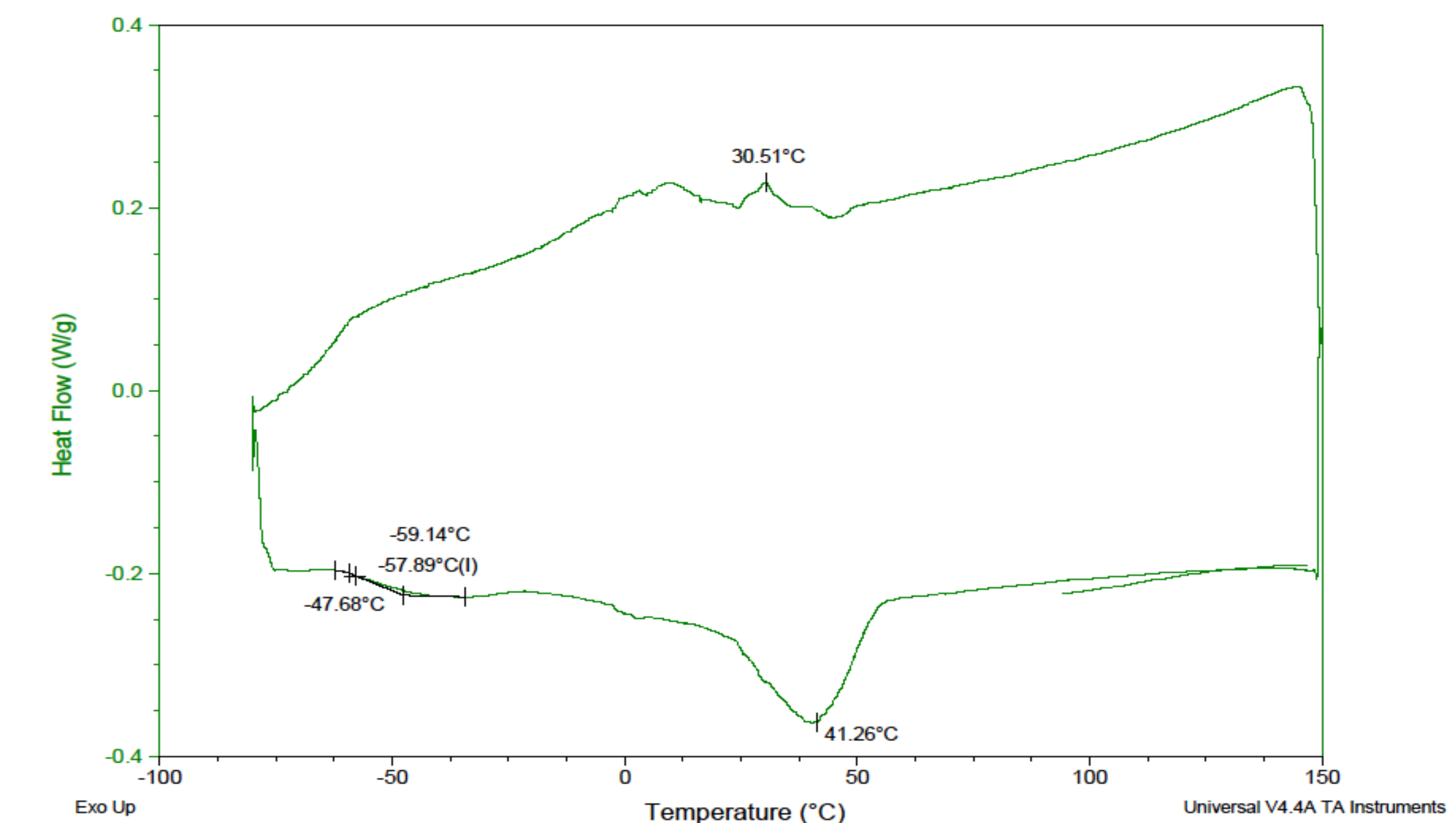


Figure 5 (Bottom): A DMA plot of a 100% PCL during a thermomechanical cycle experiment. The stress and strain are measured as the temperature and force are cycled between 10-60°C and 0.005-0.5N.

Table 1 (Right): Preliminary data for two films. We see that hydrophilicity, transition temperature, and crystallinity decrease as the amount of PCL decreases

	DSC Data				Goniometer Data				
	Glass Transition Point (°C)	Crystallization Point (°C)	Melting (Transition) Point (°C)	Enthalpy of Crystallization (J/g)	Enthalpy of Fusion (J/g)	Right Contact Angle (°)	Left Contact Angle (°)	Width of Droplet (mm)	Height of Droplet (mm)
100% PCL	N/A	26.44	49.11	37.22	38.08	46.8	48.4	3.675	0.627
26%ACPCL-74%PCL	-58.91	29.90	38.65	1.36	17.78	71.8	70.7	2.654	0.801

Polymer Synthesis

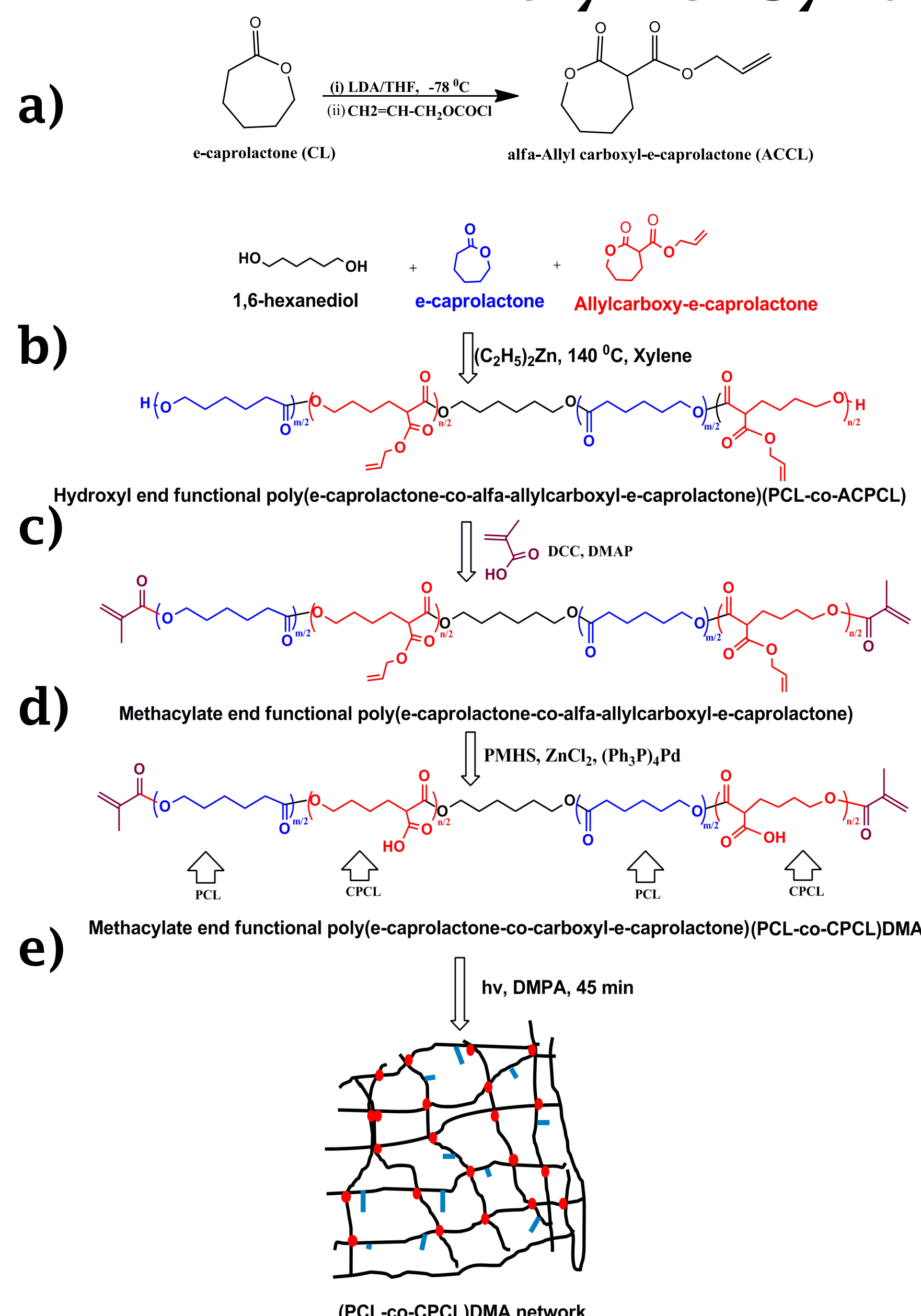


Figure 2: Our synthesis scheme. a), α-(allyloxycarbonyl)-ε-caprolactone (ACCL) is synthesized to be used as a monomer. **b)** We polymerize 1,6-hexanediol with ε-caprolactone and ACCL with diethyl zinc as a catalyst to get PCL-ACPCL. **c)** The polymer ends are functionalized with methacrylate groups which allow the polymer to crosslink. **d)** The carboxyl groups inside the chain are deprotected by removing the allyl groups. These carboxyl groups are to be used for peptide linkage in the future. **e)** We crosslink the polymer under ultraviolet radiation in a solution of methylene chloride by using 2,2-dimethoxy-2-phenylacetophenone (DMPA) as a photoinitiator.

Acknowledgements

I would like to acknowledge the VINSE REU through the NSF grant DMR-1005203 and Program Staff and the Biomaterials Group at Vanderbilt for all their help and support, as well as Alex Short and Elizabeth Adolph for help with instrumentation. This investigation was sponsored in part by NIH/NIGMS MARC U*STAR T34 08663 National Research Service Award to UMBC and the NSF Career CBET 1056046 Award

Conclusions and Future Work

- We have seen that we can make polymer films that transition at the appropriate temperature
- Testing has shown that most of the films we've made cannot withstand much force (<1 N)
- Run Gel Permeation Chromatography (GPC) to estimate the molecular weight and degradation time of the polymers based on their elution times compared to standards.
- Enhancing the reproducibility of the synthesis & crosslinking to get consistent molecular weight, thermal properties, and mechanical properties.
- Tune the molar concentrations of PCL & ACPCL in order to create a film with an appropriate transition temperature as well as one that can withstand appropriate force
- Continue thermomechanical cycle experiments to calculate and optimize shape fixity and strain recovery rate.