

(12) **United States Patent**
Reiserer et al.

(10) **Patent No.:** **US 11,745,180 B2**
(45) **Date of Patent:** **Sep. 5, 2023**

(54) **MICROFLUIDIC SYSTEMS, PUMPS, VALVES, FLUIDIC CHIPS THEREOF, AND APPLICATIONS OF SAME**

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(*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 0 days.

(21) Appl. No.: **18/084,634**

(22) Filed: **Dec. 20, 2022**

(65) **Prior Publication Data**
US 2023/0122594 A1 Apr. 20, 2023

Related U.S. Application Data
(63) Continuation of application No. 17/623,350, filed as application No. PCT/US2020/040061 on Jun. 29, (Continued)

(51) **Int. Cl.**
B01L 3/00 (2006.01)
F04B 43/12 (2006.01)
F16K 11/16 (2006.01)

(52) **U.S. Cl.**
CPC . **B01L 3/502738** (2013.01); **B01L 2300/0627** (2013.01); **B01L 2300/123** (2013.01);
(Continued)

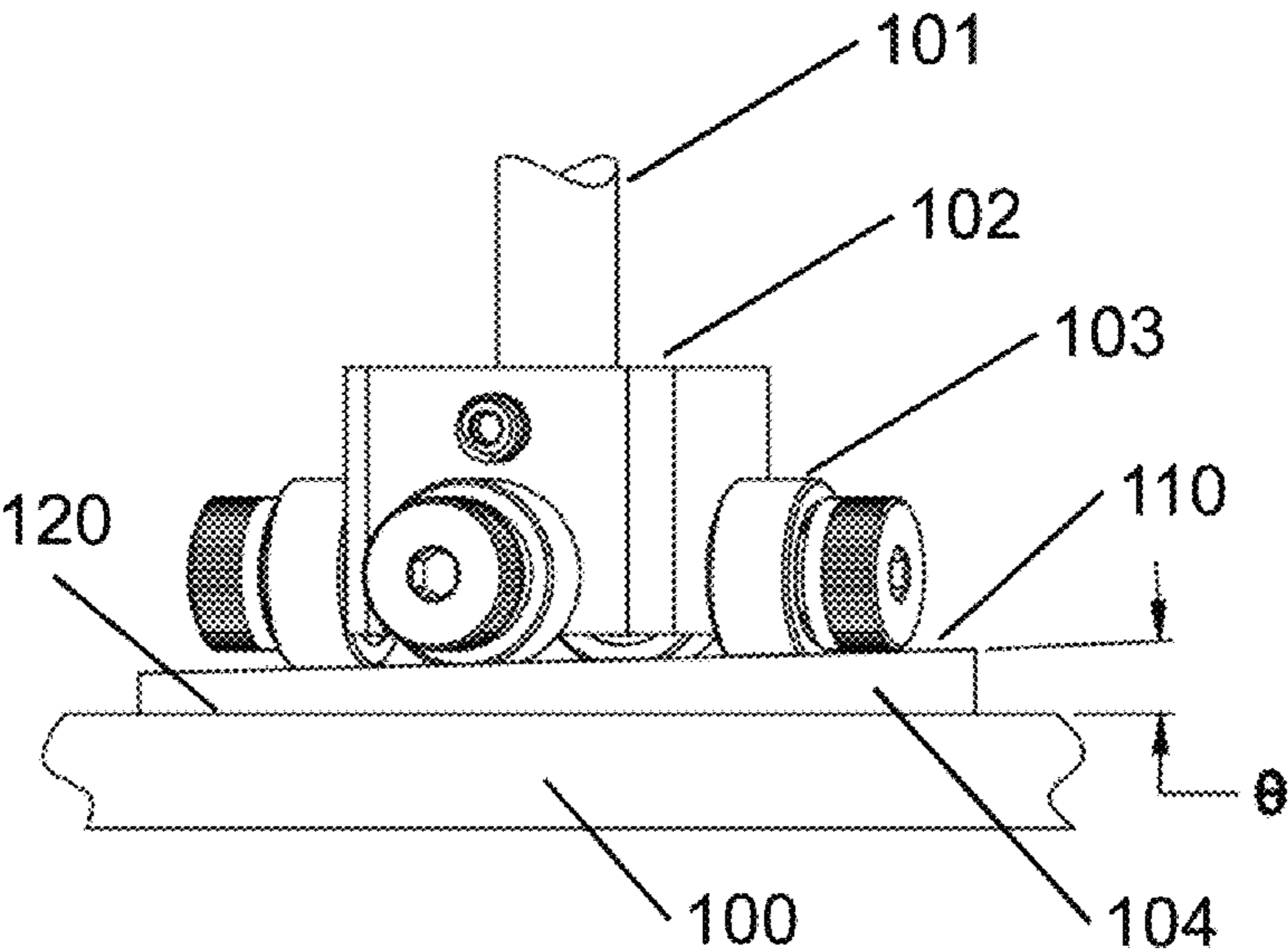
(58) **Field of Classification Search**
CPC **B01L 3/502738**; **B01L 2300/0627**; **B01L 2300/123**; **B01L 2400/0644**; **F04B 43/1261**; **F16K 11/163**
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(57) **ABSTRACT**
Microfluidic systems, pumps, valves and applications of the same are provided. The microfluidic system may be a pump or a valve having a fluidic chip and an actuator controlling the opening and closing of the fluidic channel in the fluidic chip. The actuator may be disposed to tilt from the fluidic chip, forming a tilted-rotor peristaltic pump. Alternatively, the actuator may be a rolling ball actuator, and different fluidic chips may be used in different applications. For example, the fluidic chip may be a spiral pump chip having spiral channels, a rotary peristaltic pump chip having multiple output channels, or a multi-port valve chip having one port interconnected with multiple different ports. An analytical valve chip may switchably interconnect bioreactor and rinse/calibration input channels to sensor and waste output channels. The actuator of a random-access valve can move from one valve position to another without opening or closing intermediate ones.

11 Claims, 9 Drawing Sheets



- Related U.S. Application Data**

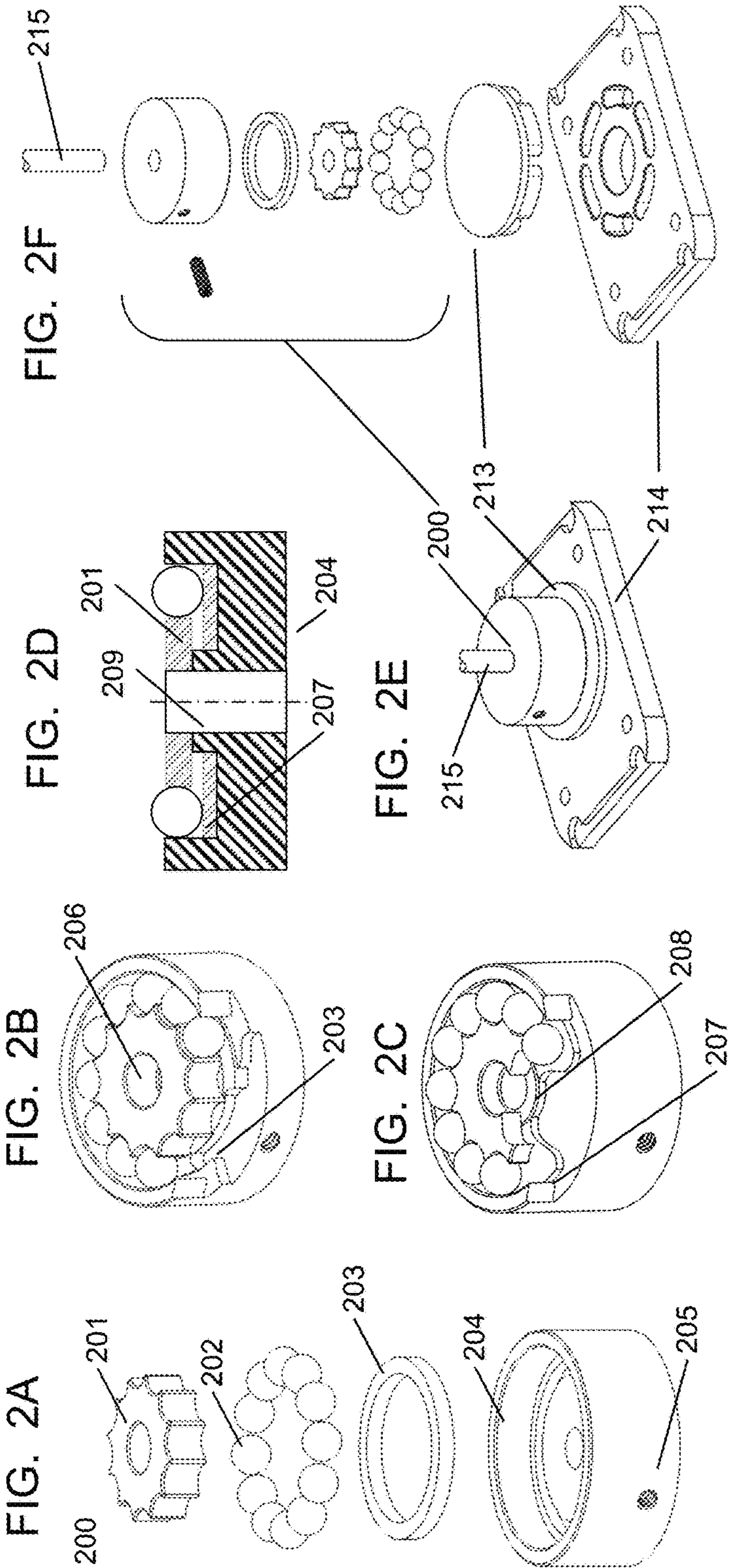
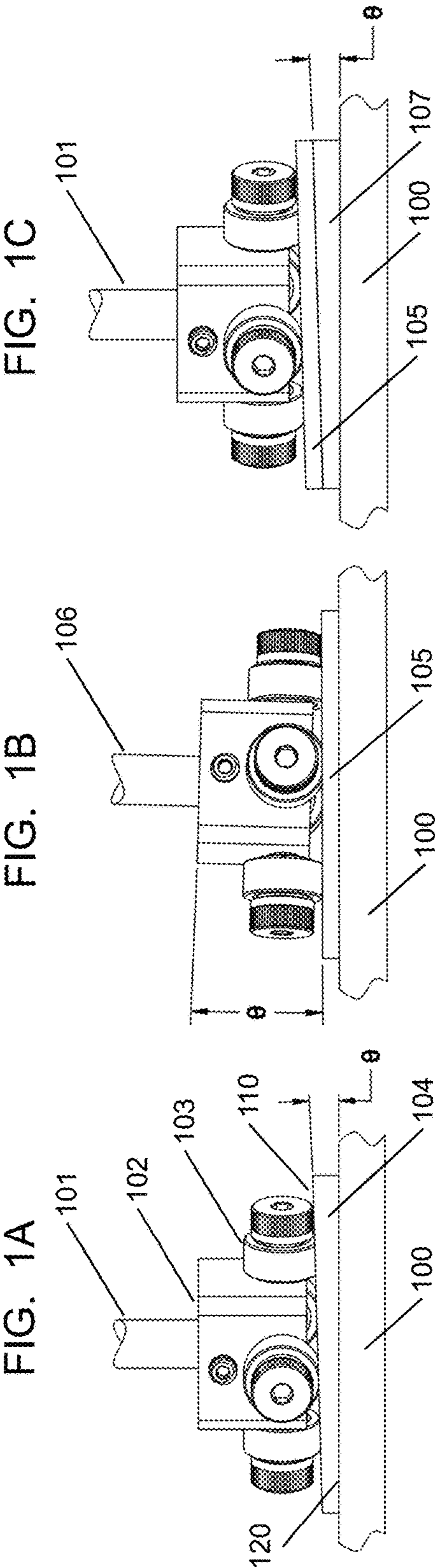
2020, now Pat. No. 11,565,256, which is a continuation-in-part of application No. PCT/US2019/047324, filed on Aug. 20, 2019, and a continuation-in-part of application No. PCT/US2019/047307, filed on Aug. 20, 2019, and a continuation-in-part of application No. PCT/US2019/047190, filed on Aug. 20, 2019.
- (60) Provisional application No. 62/868,303, filed on Jun. 28, 2019.
- (52) **U.S. Cl.**
CPC ... *B01L 2400/0644* (2013.01); *F04B 43/1261* (2013.01); *F16K 11/163* (2013.01)
- (58) **Field of Classification Search**
USPC 137/3, 625.15, 625.17, 883, 887, 616.7, 137/827, 828; 422/602, 64, 72, 505, 542
See application file for complete search history.
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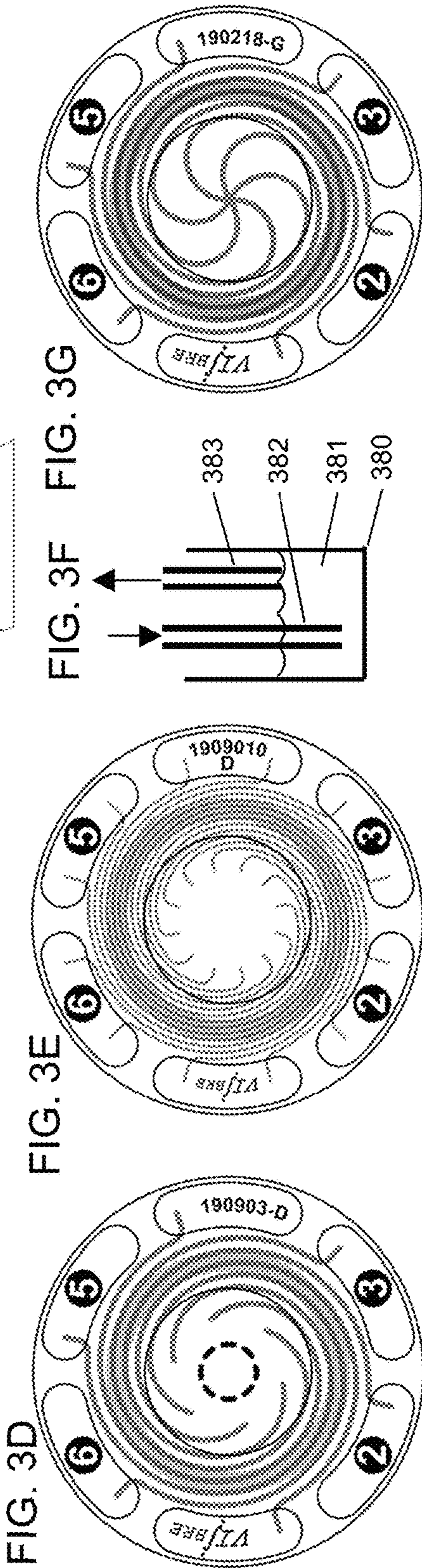
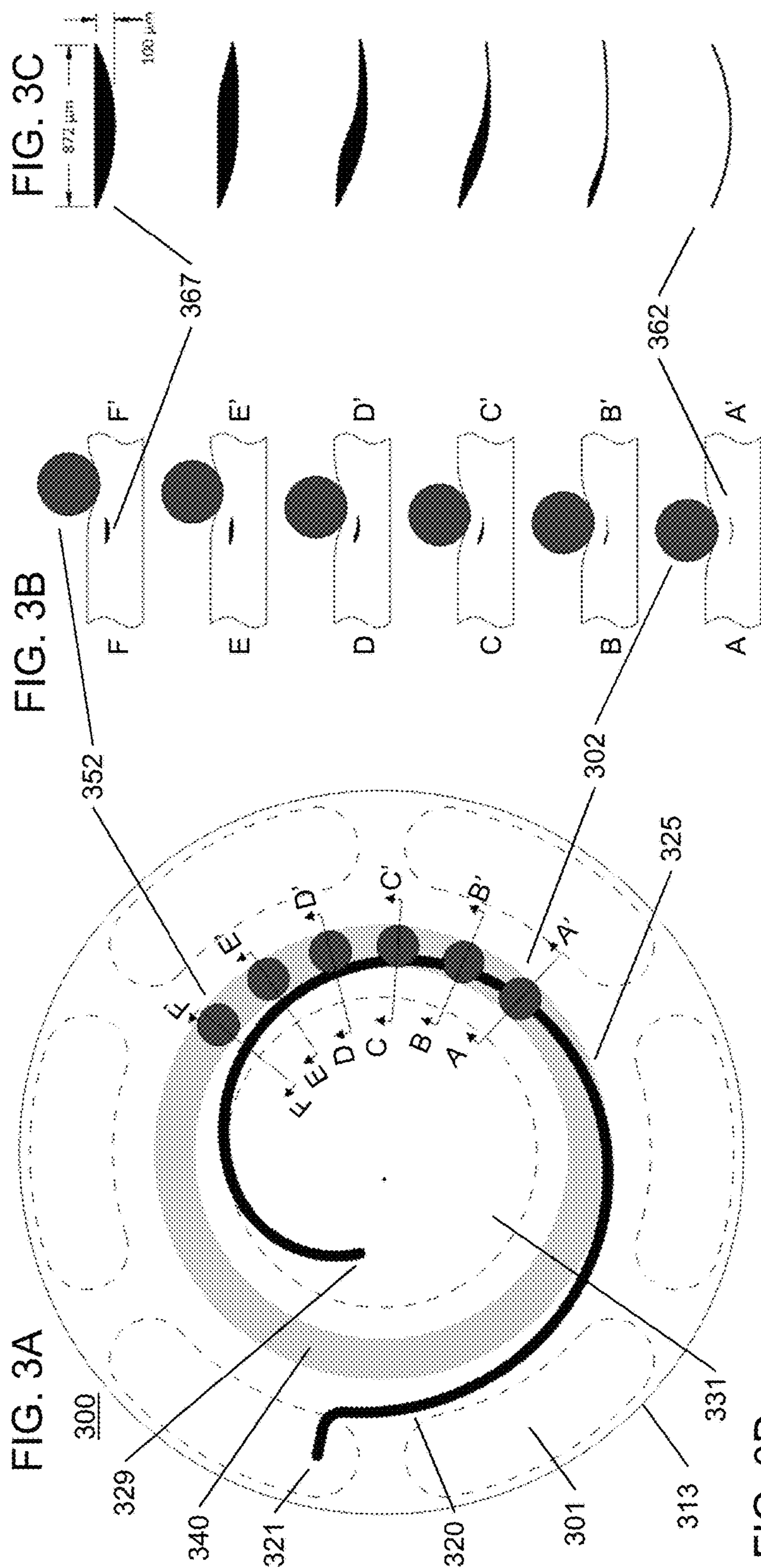


FIG. 4

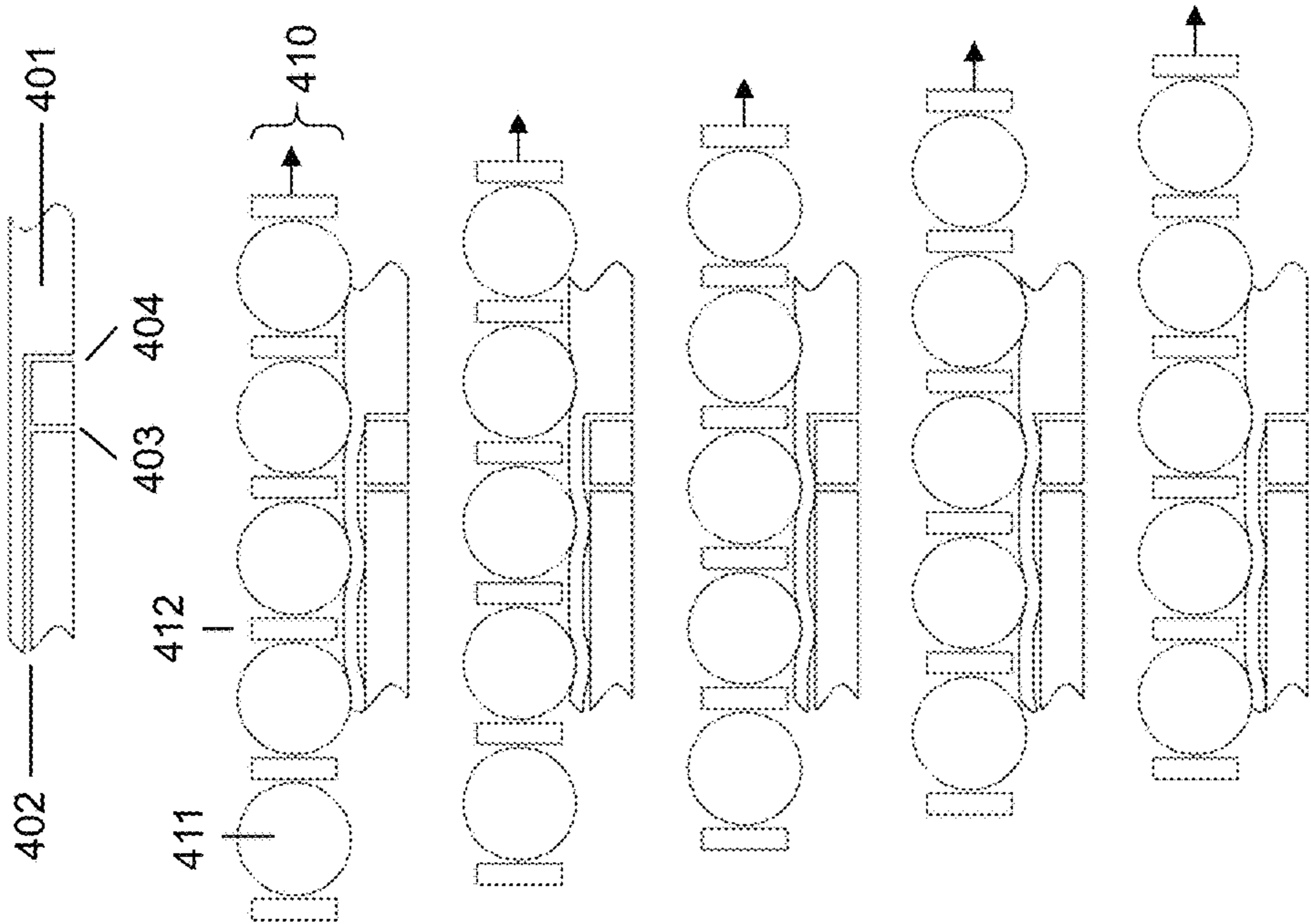


FIG. 5A

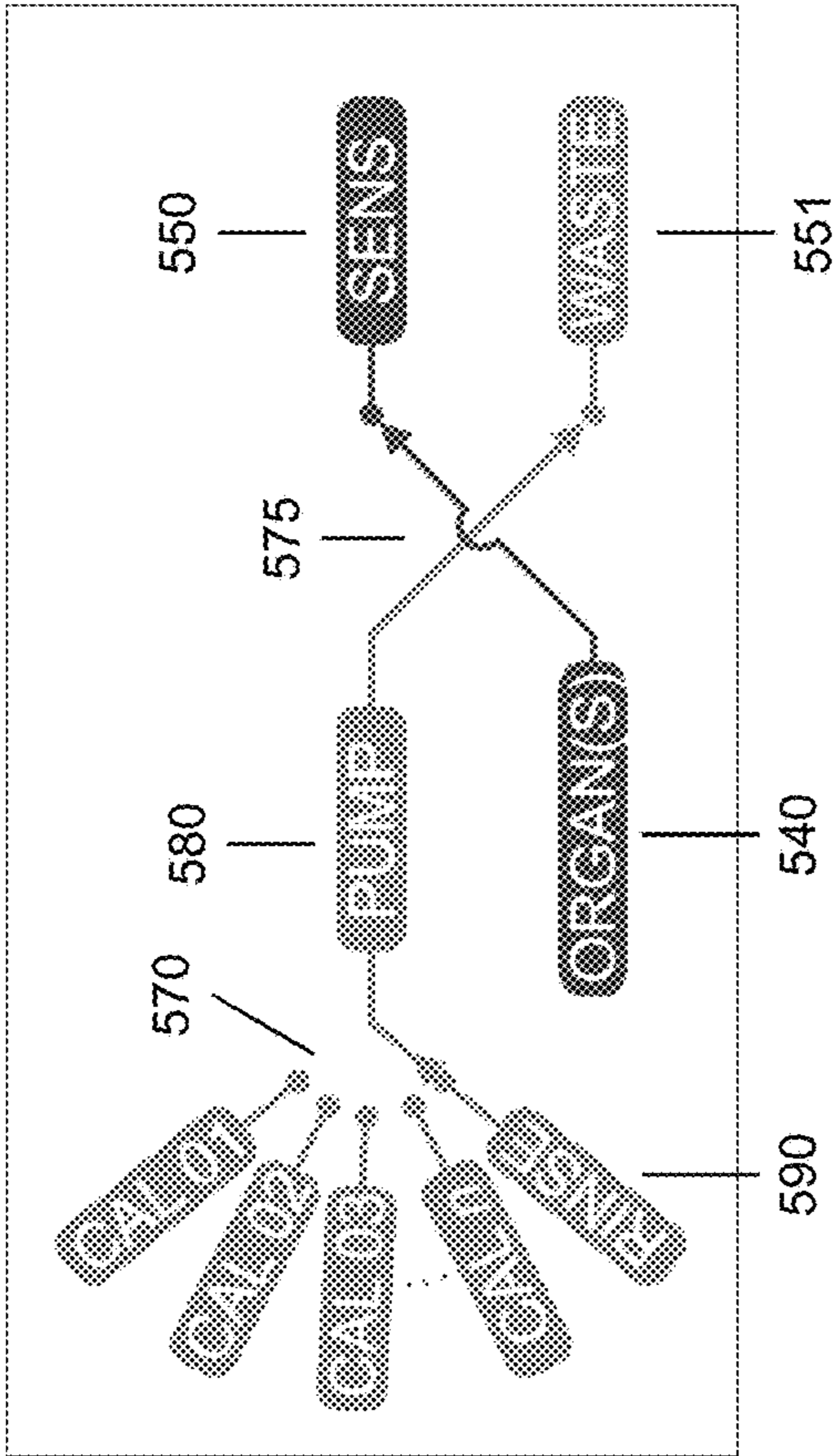


FIG. 5B

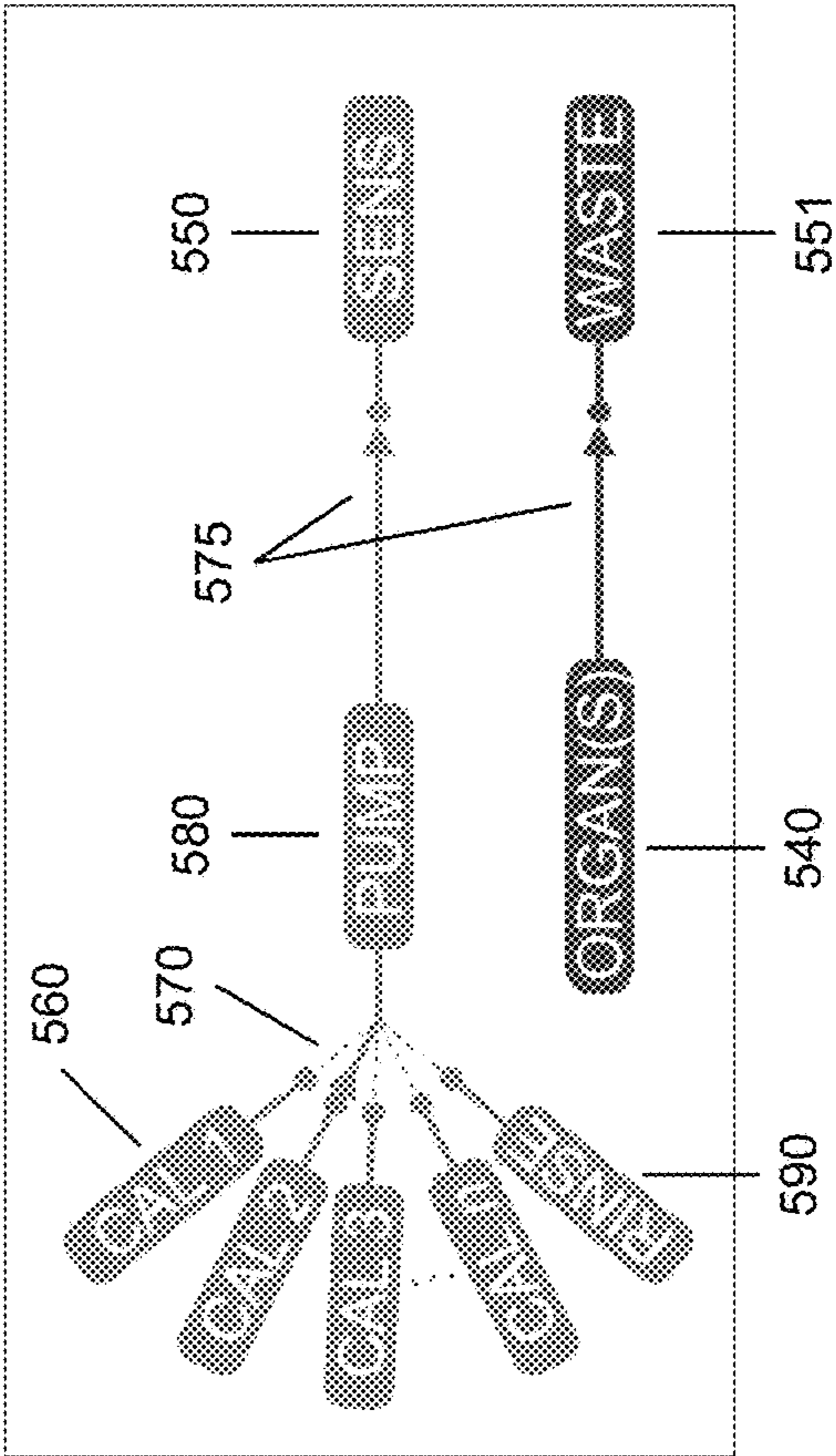


FIG. 5C

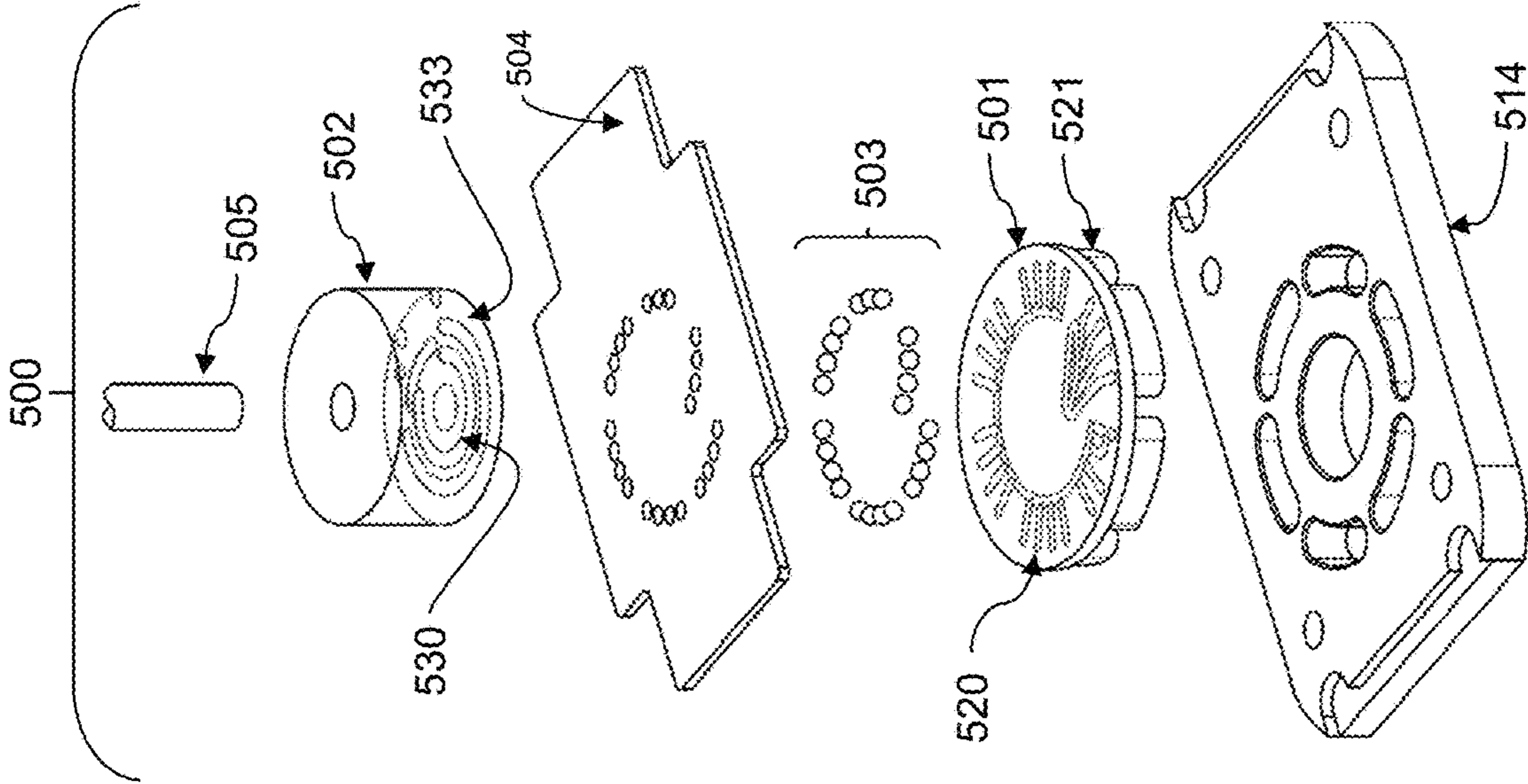


FIG. 5D

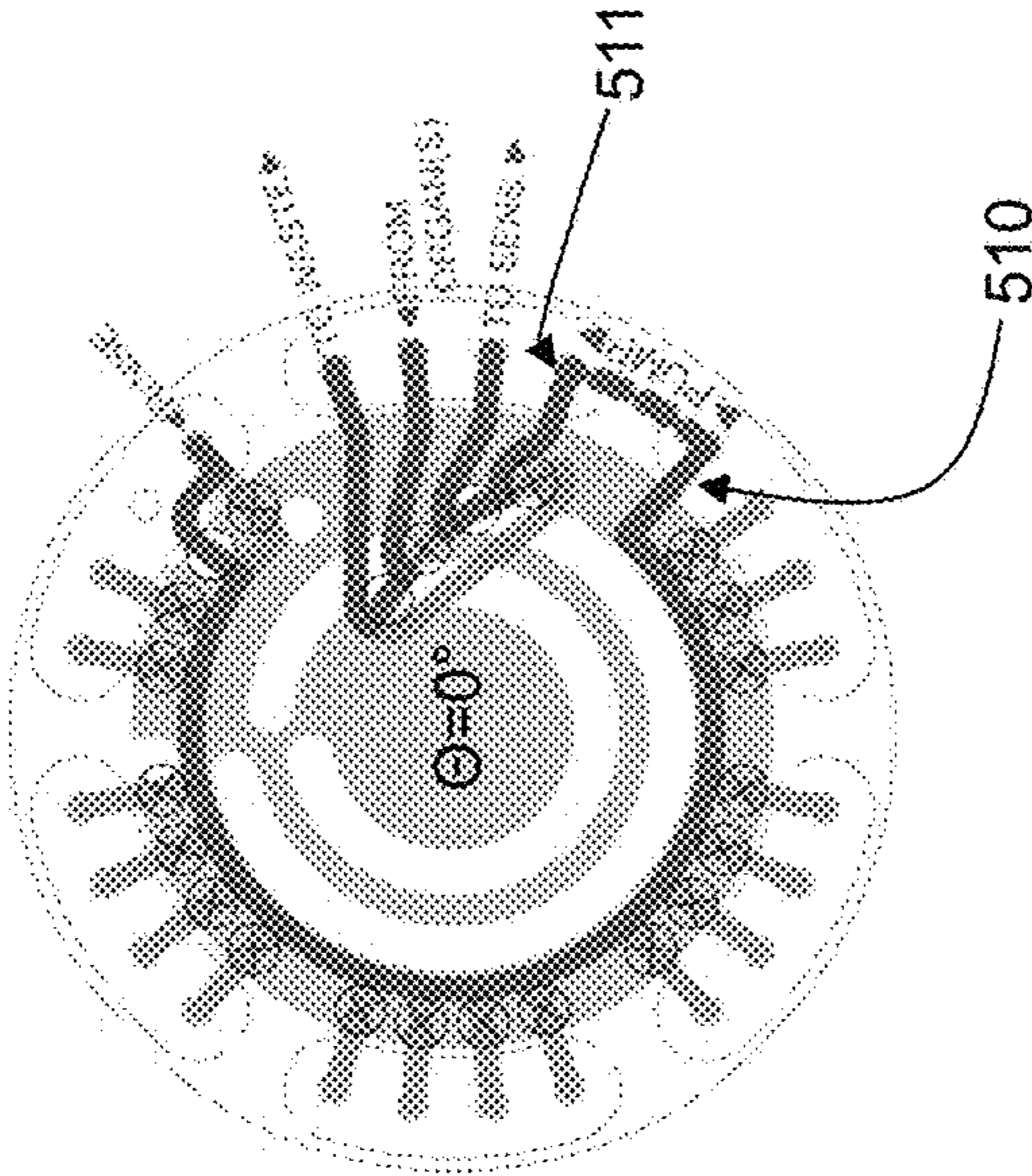


FIG. 5E

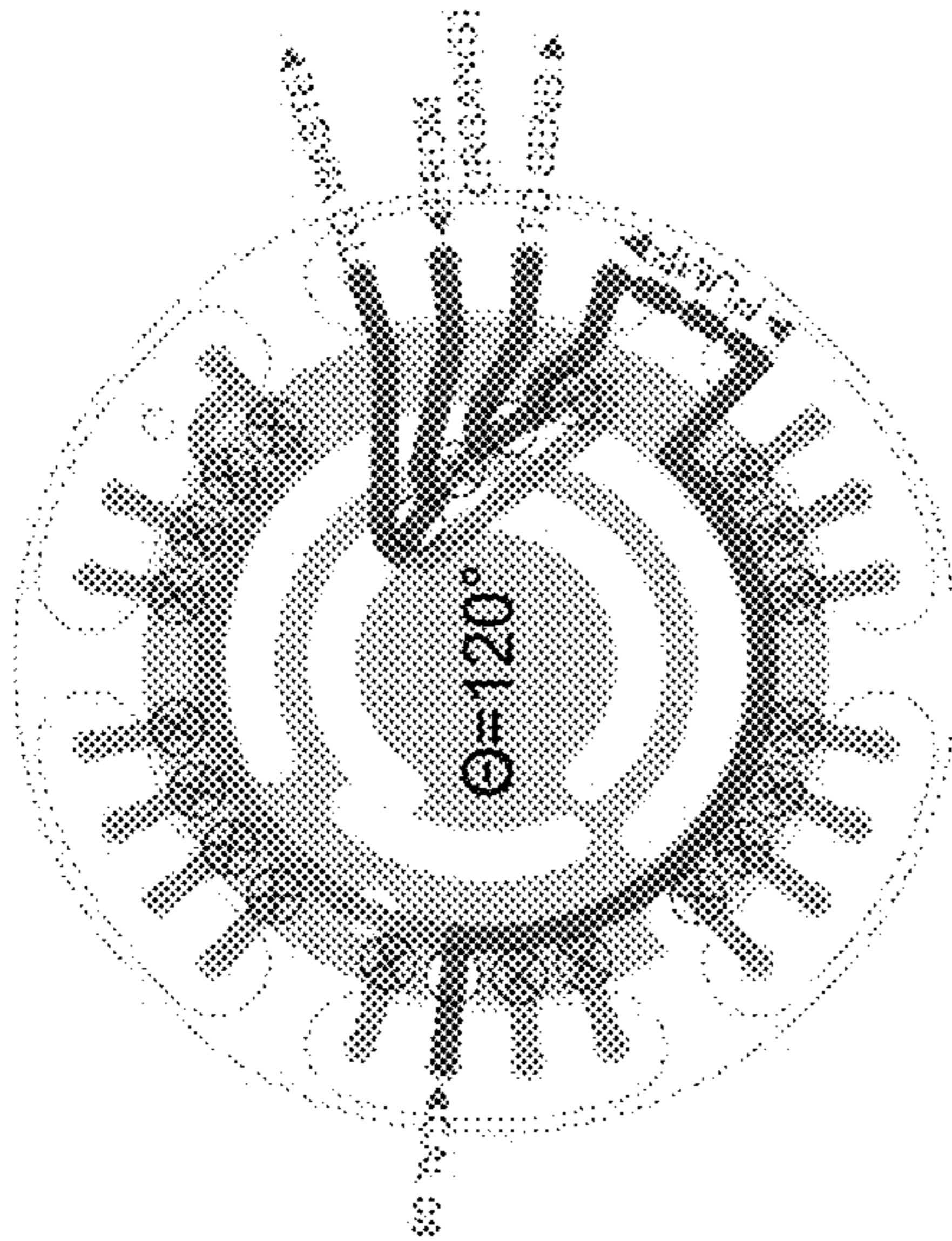


FIG. 5F

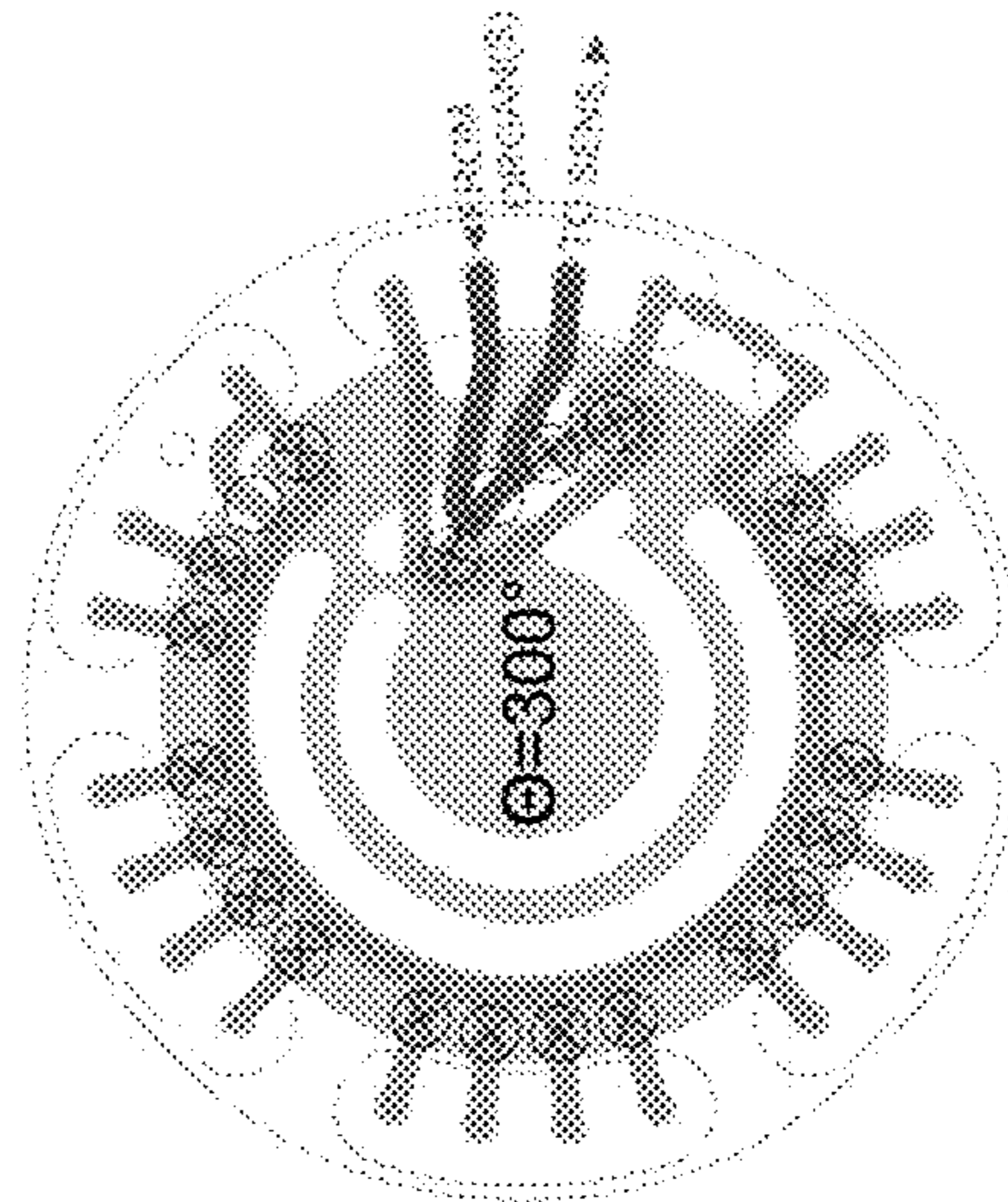
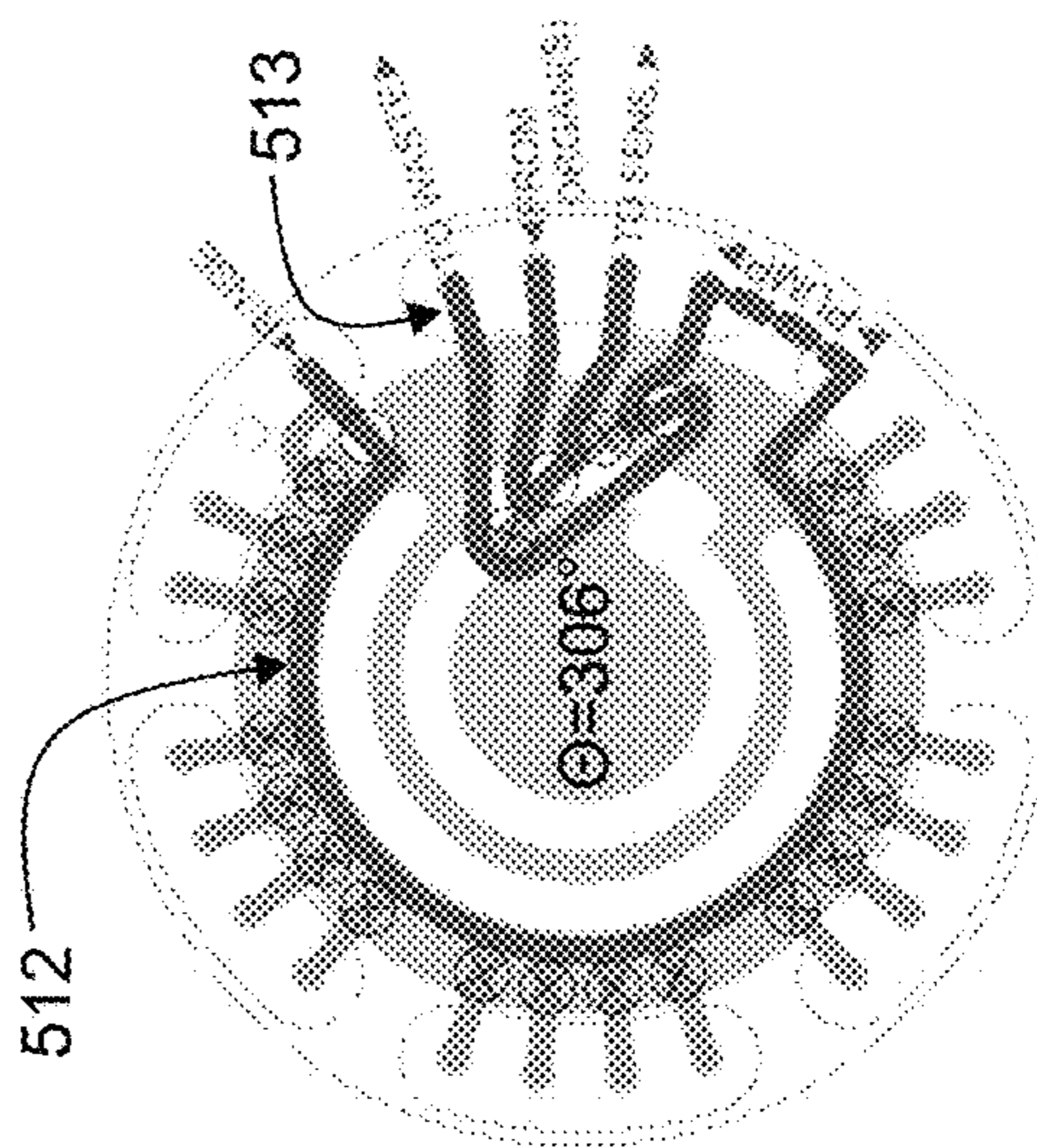
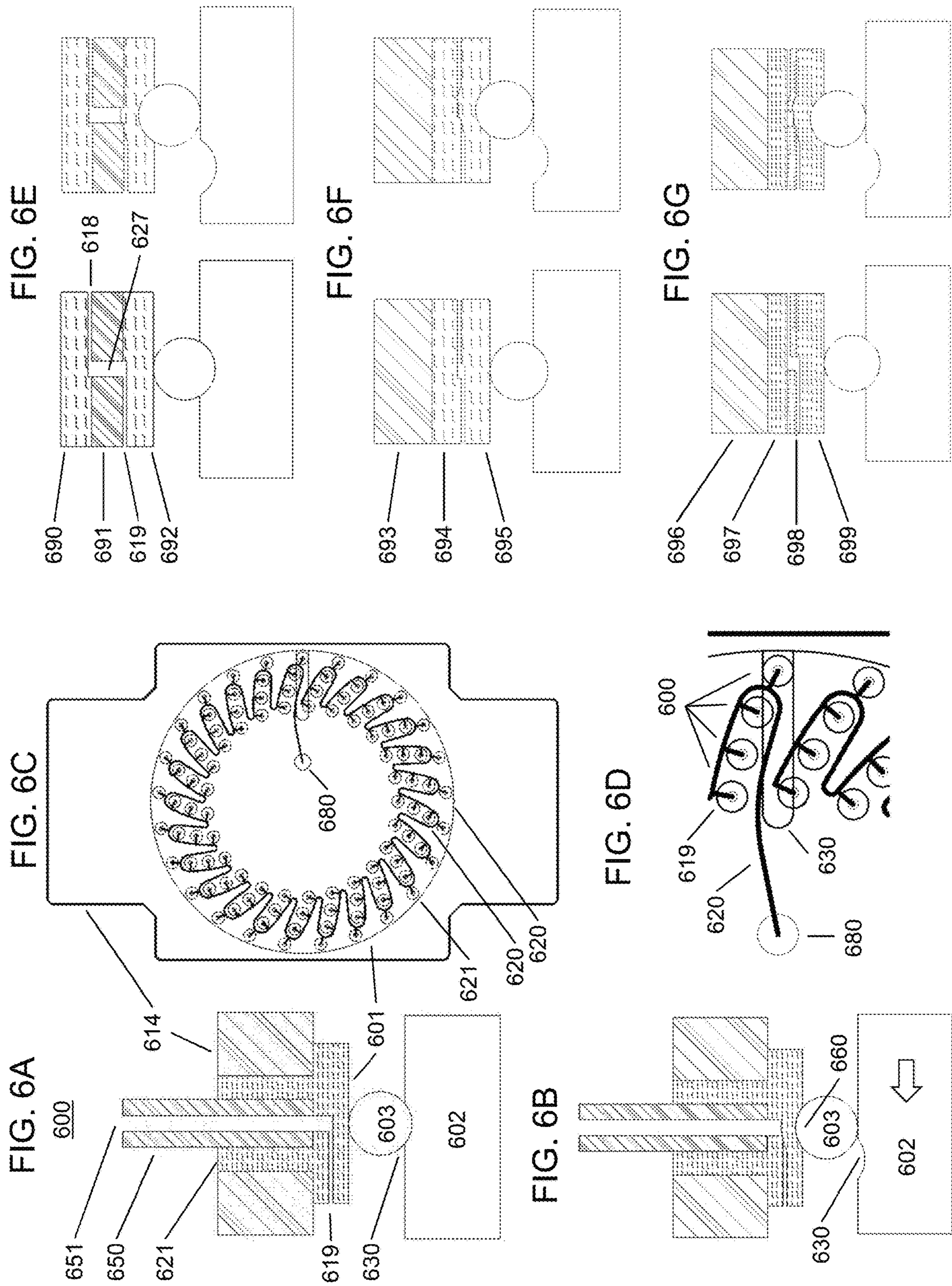
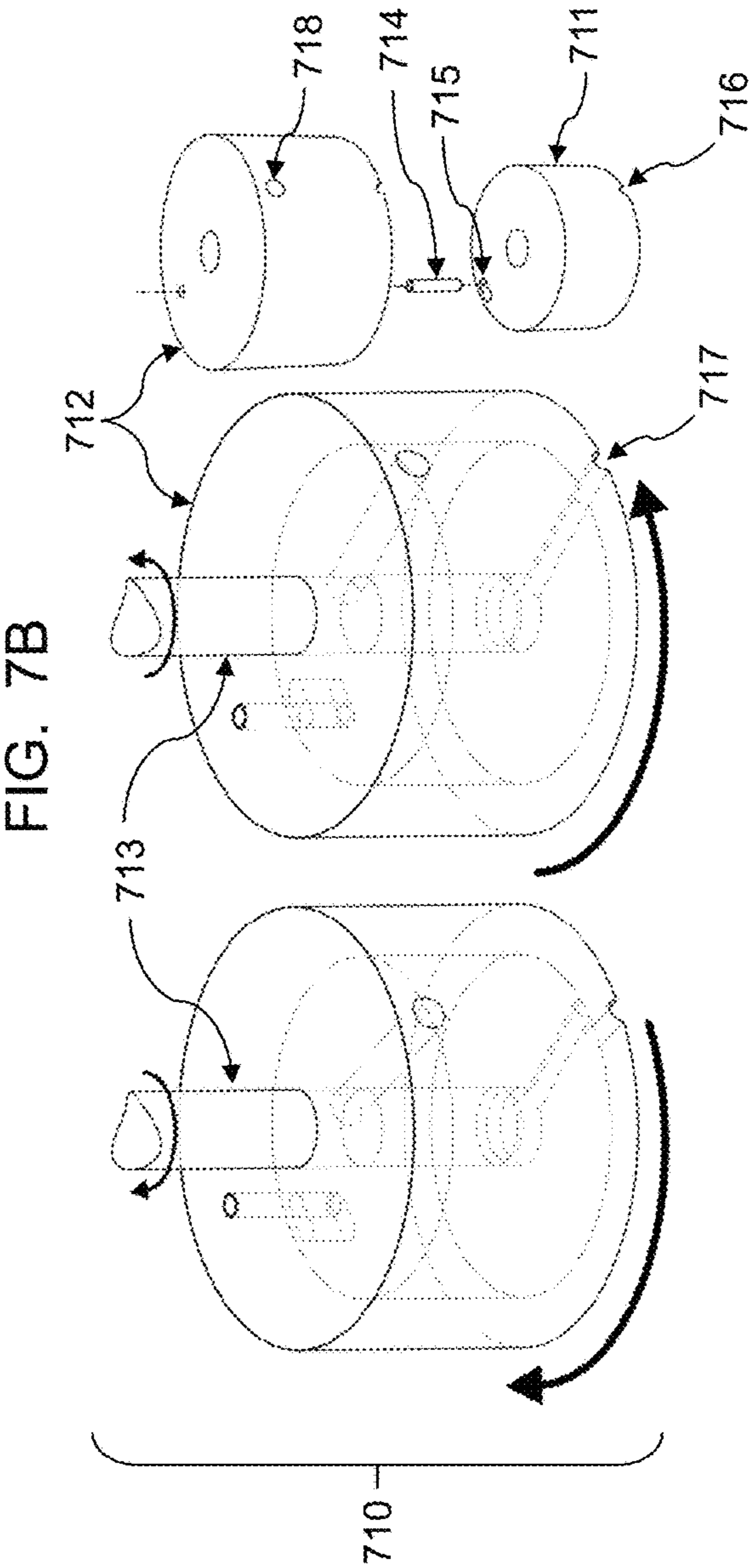
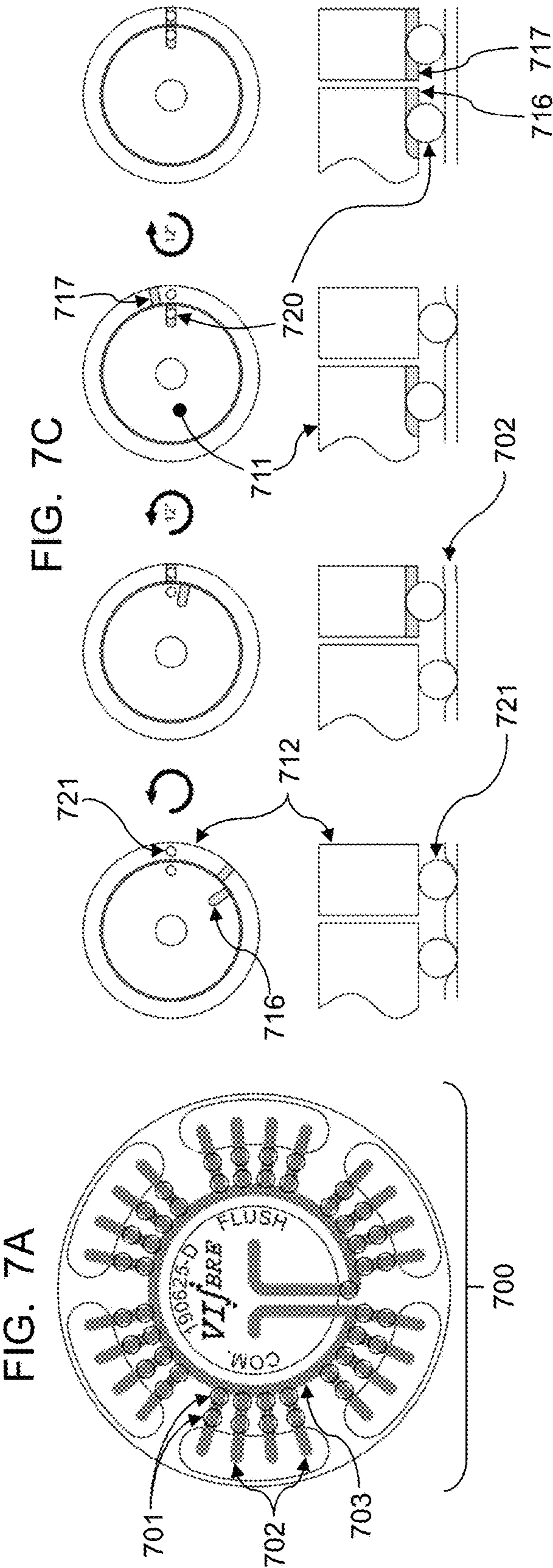


FIG. 5G







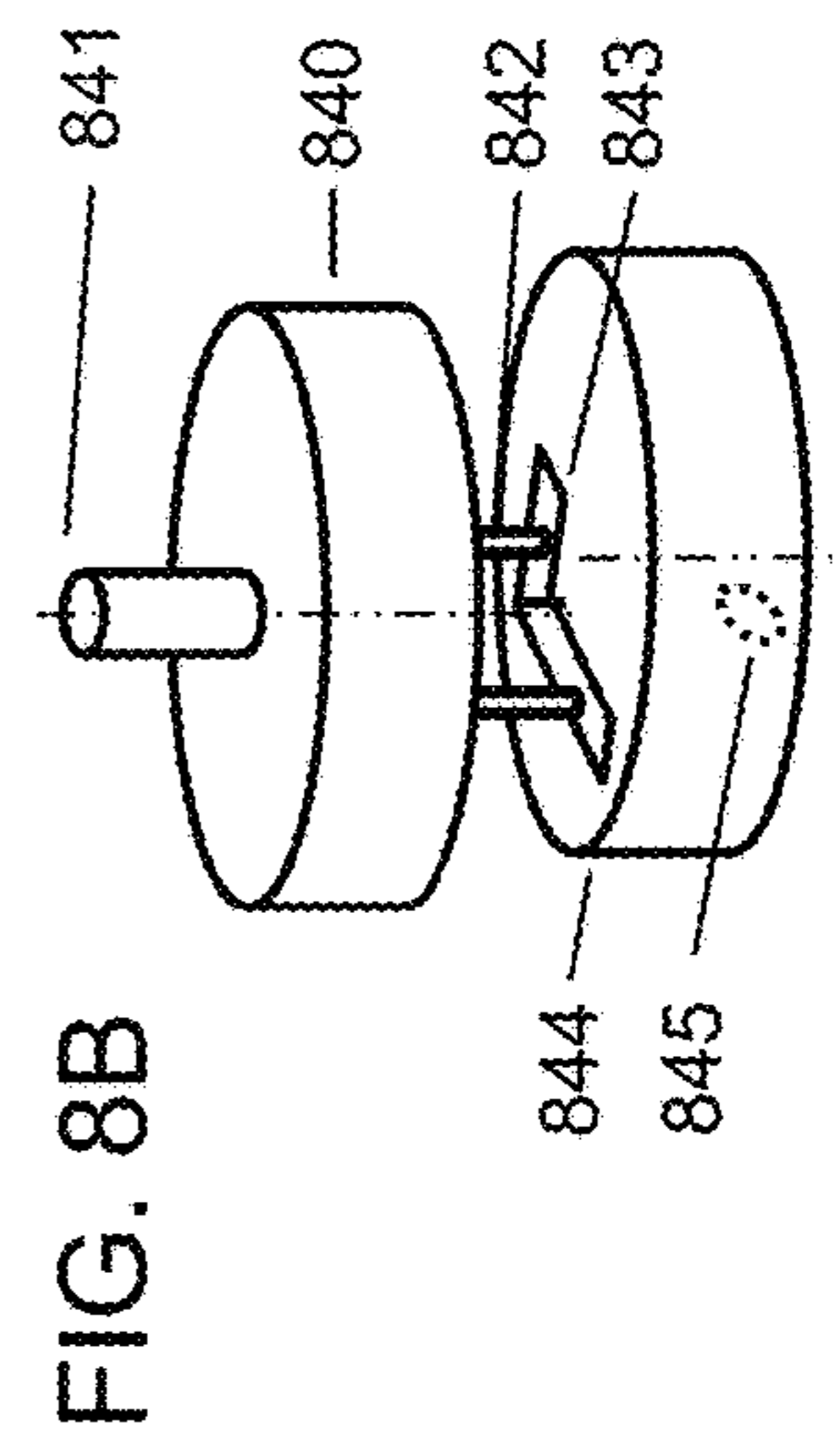
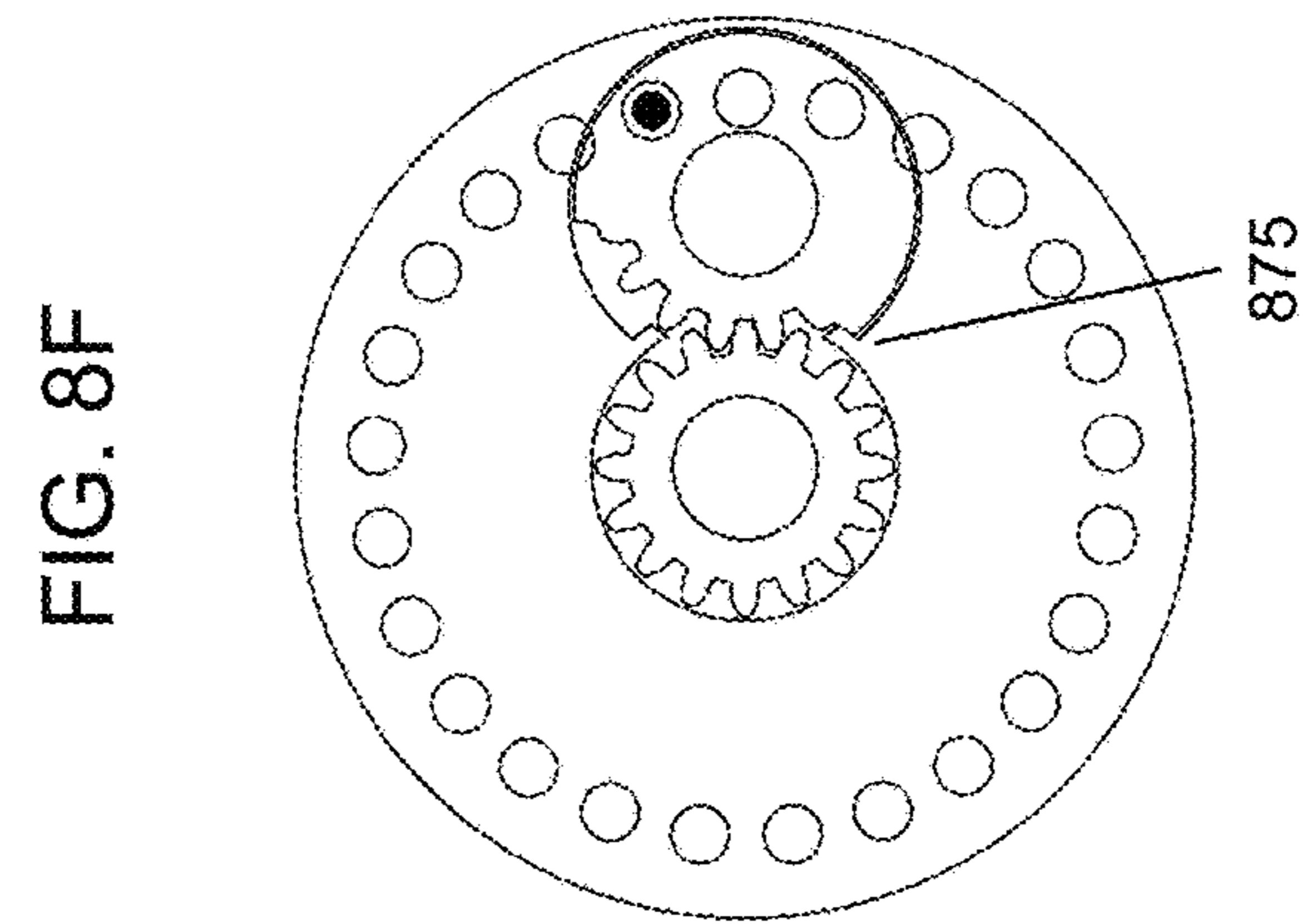
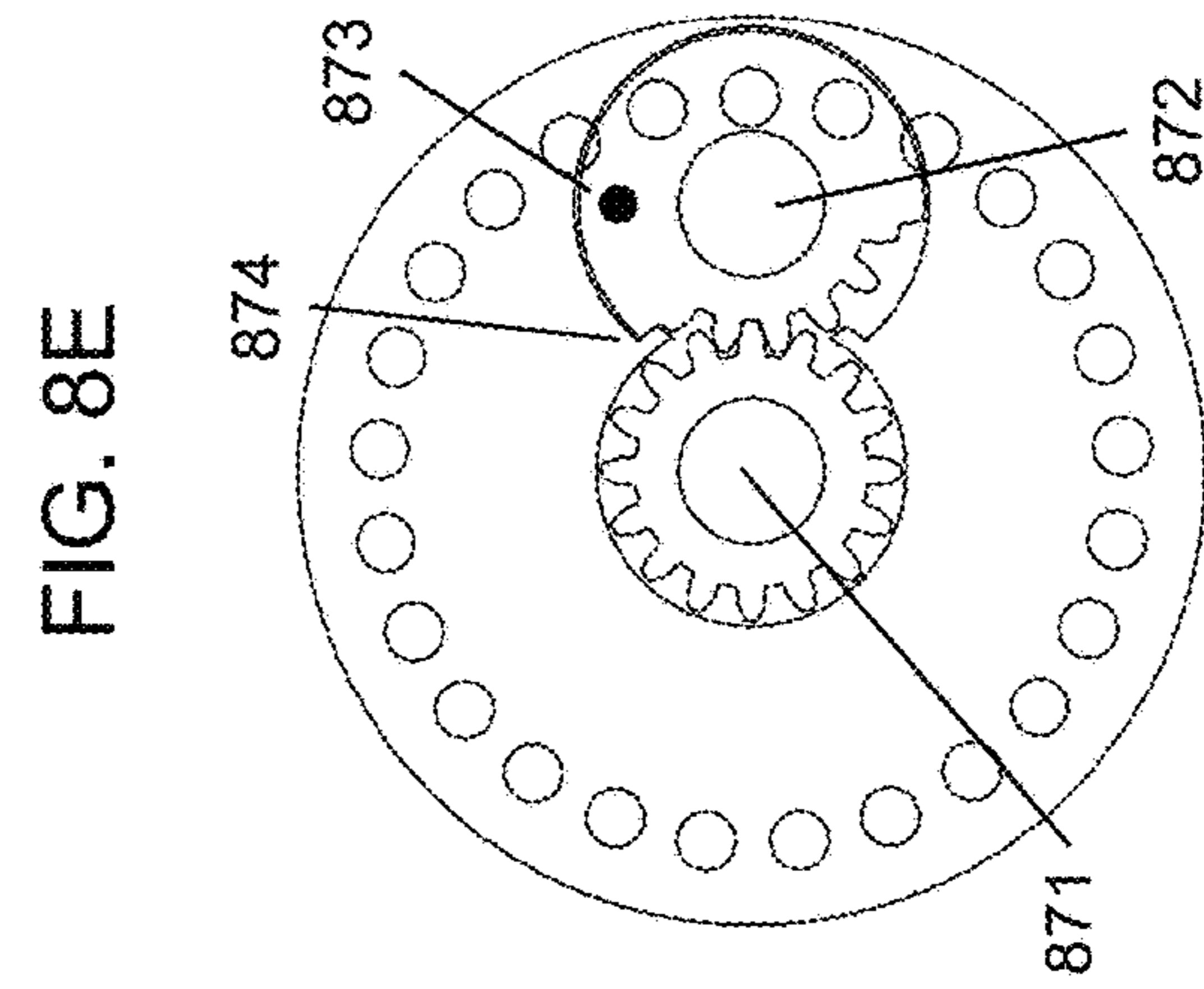
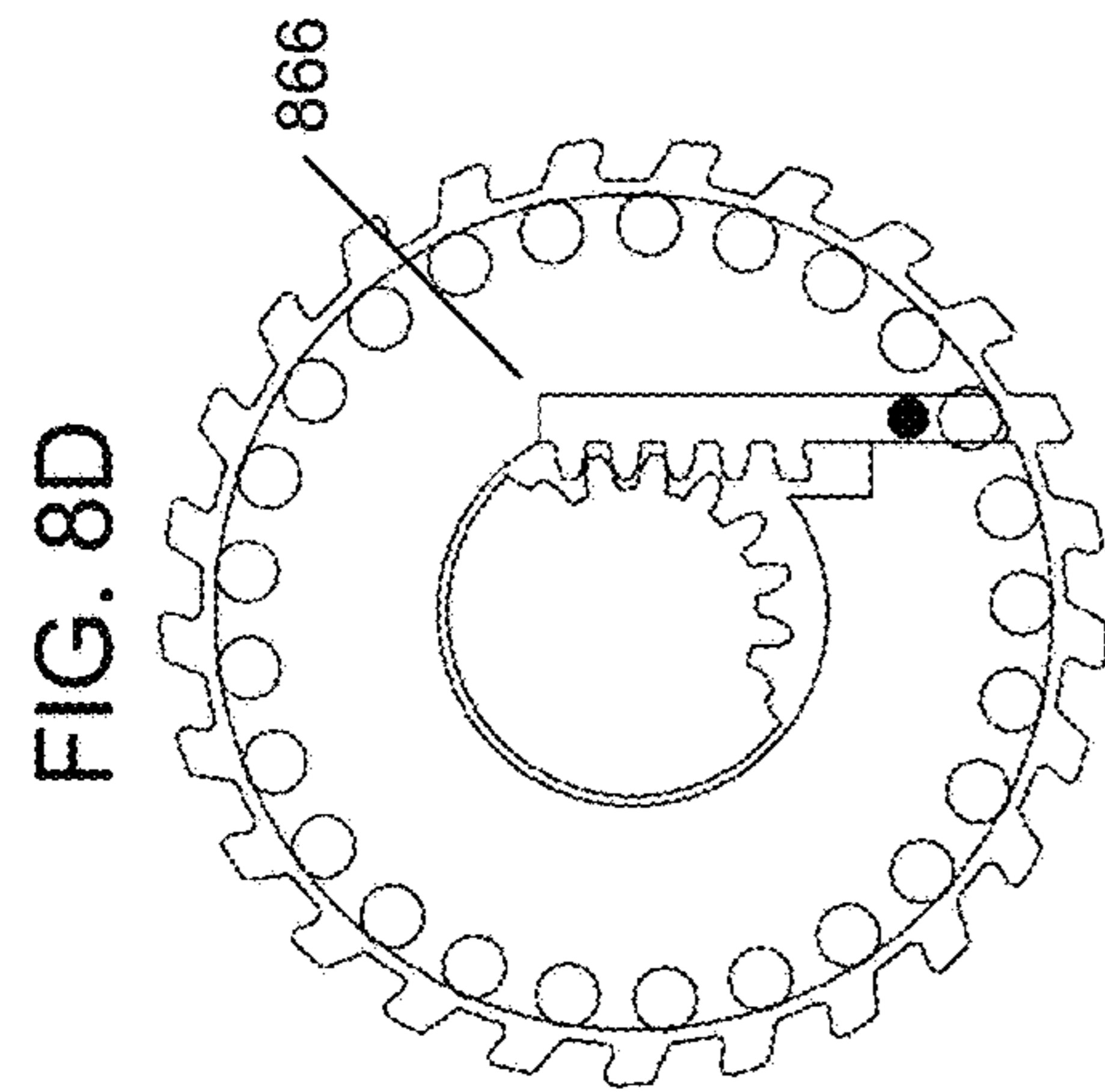
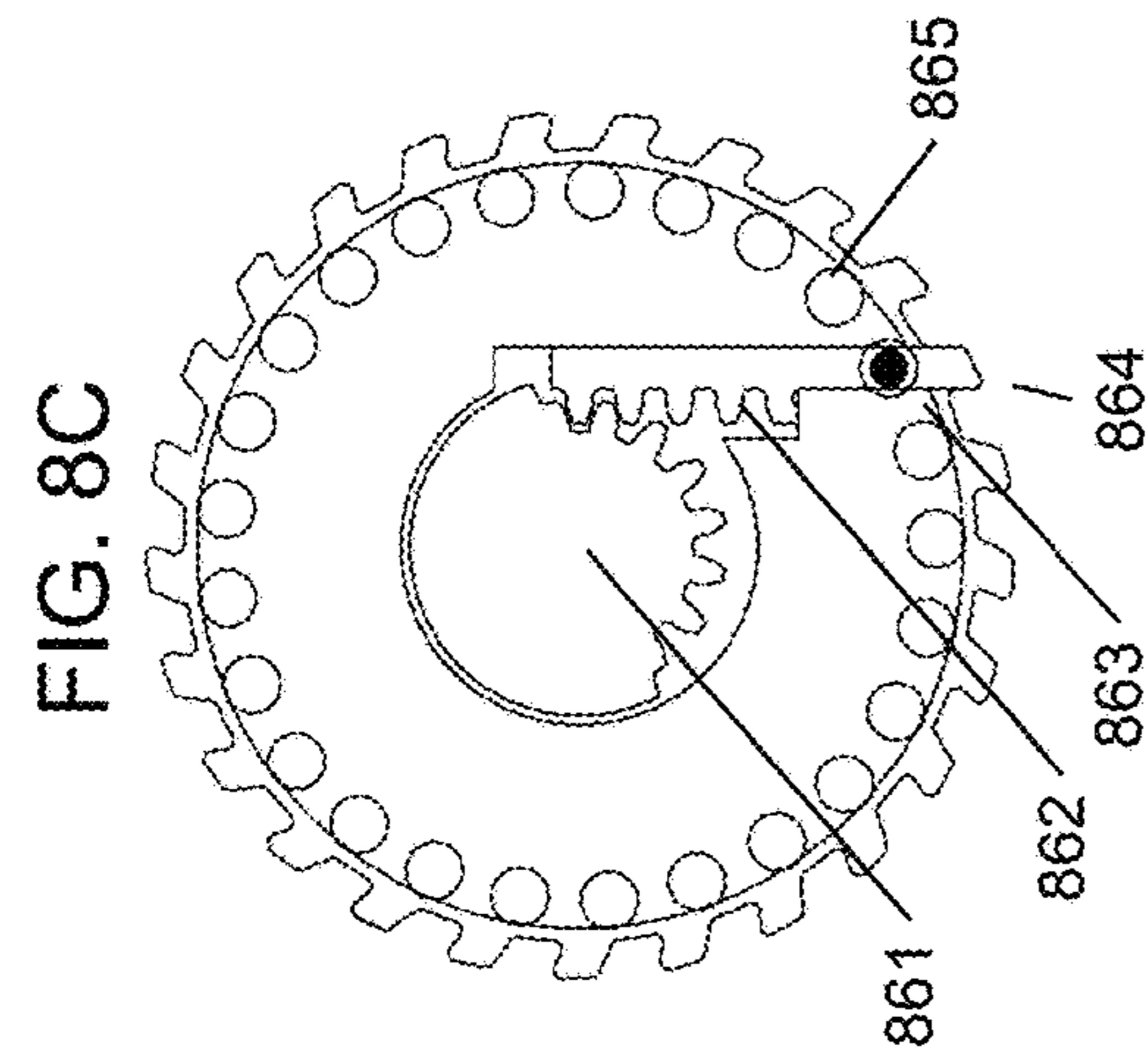
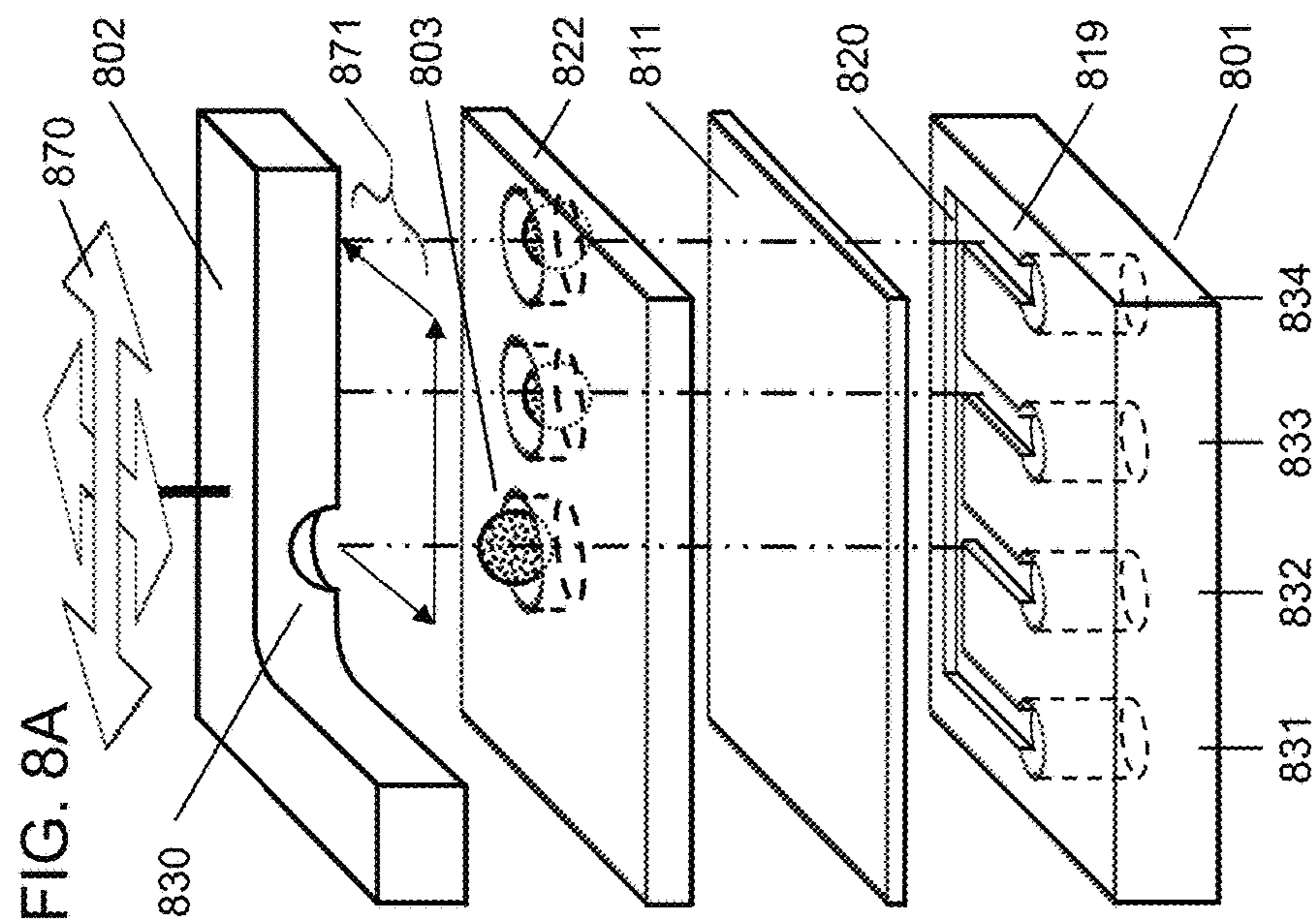


FIG. 8G

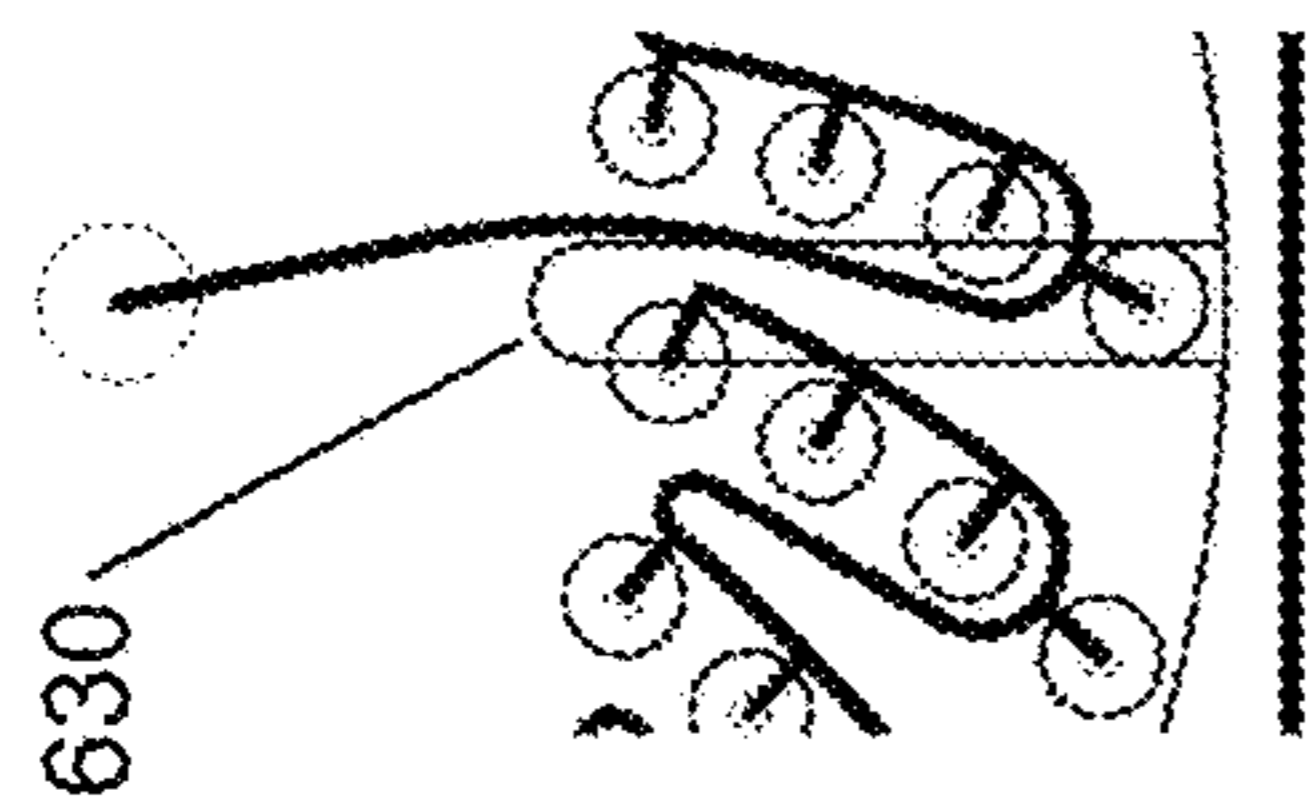


FIG. 8H

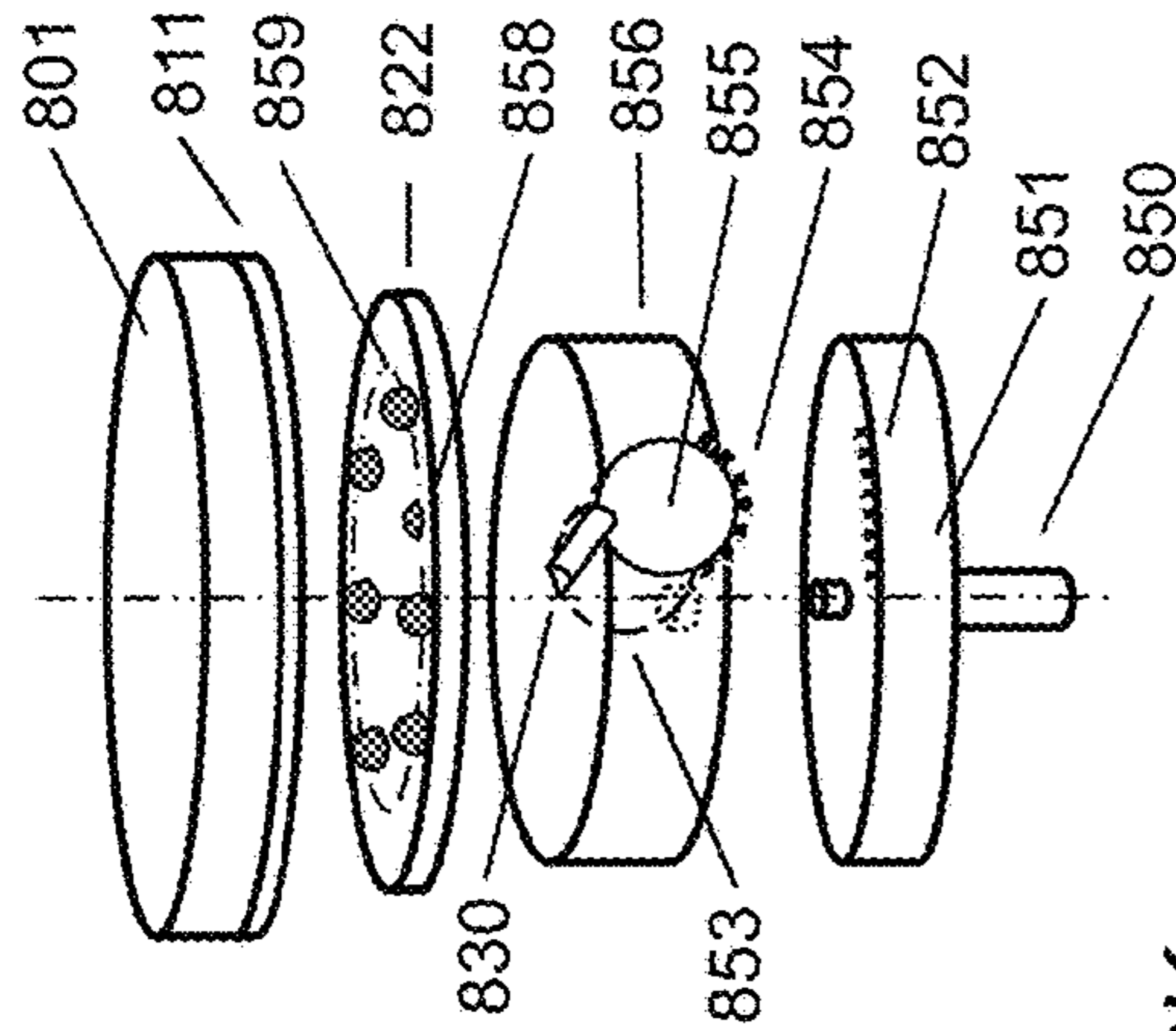


FIG. 8I

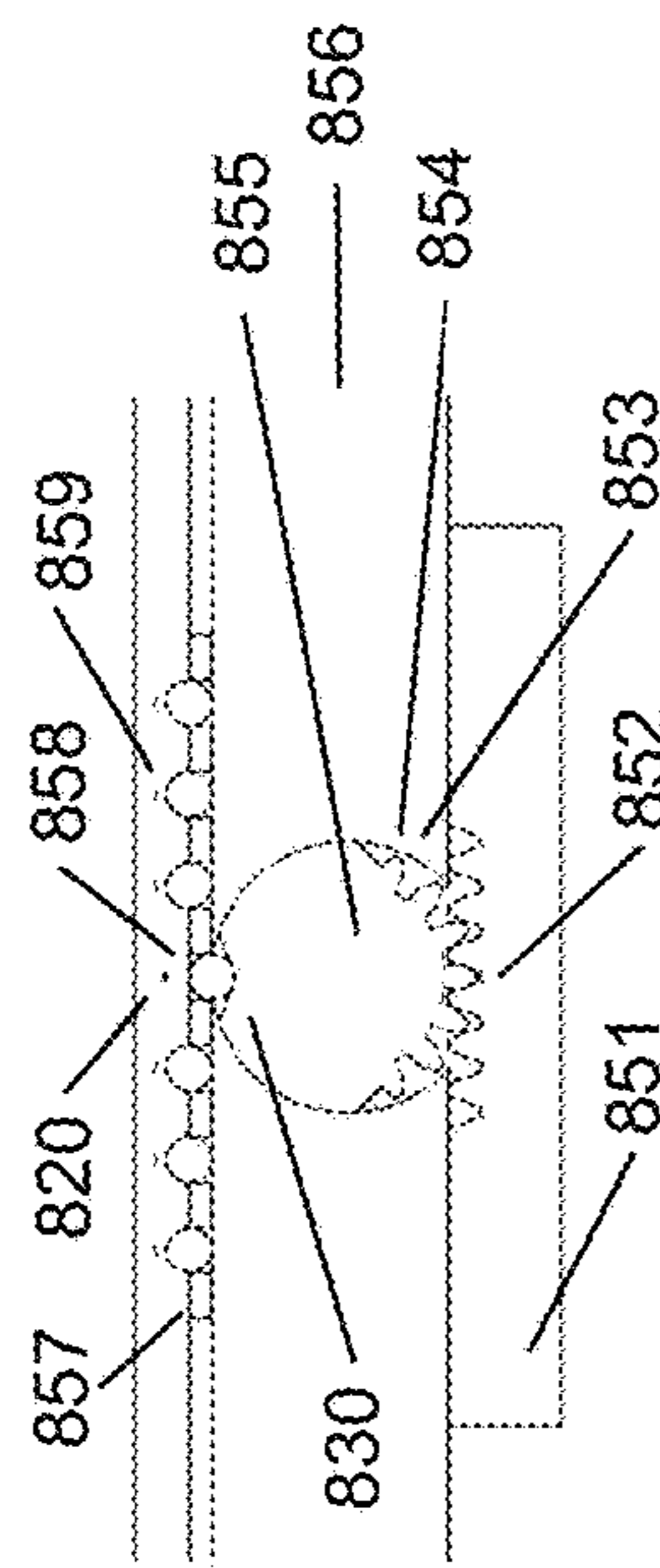


FIG. 8J

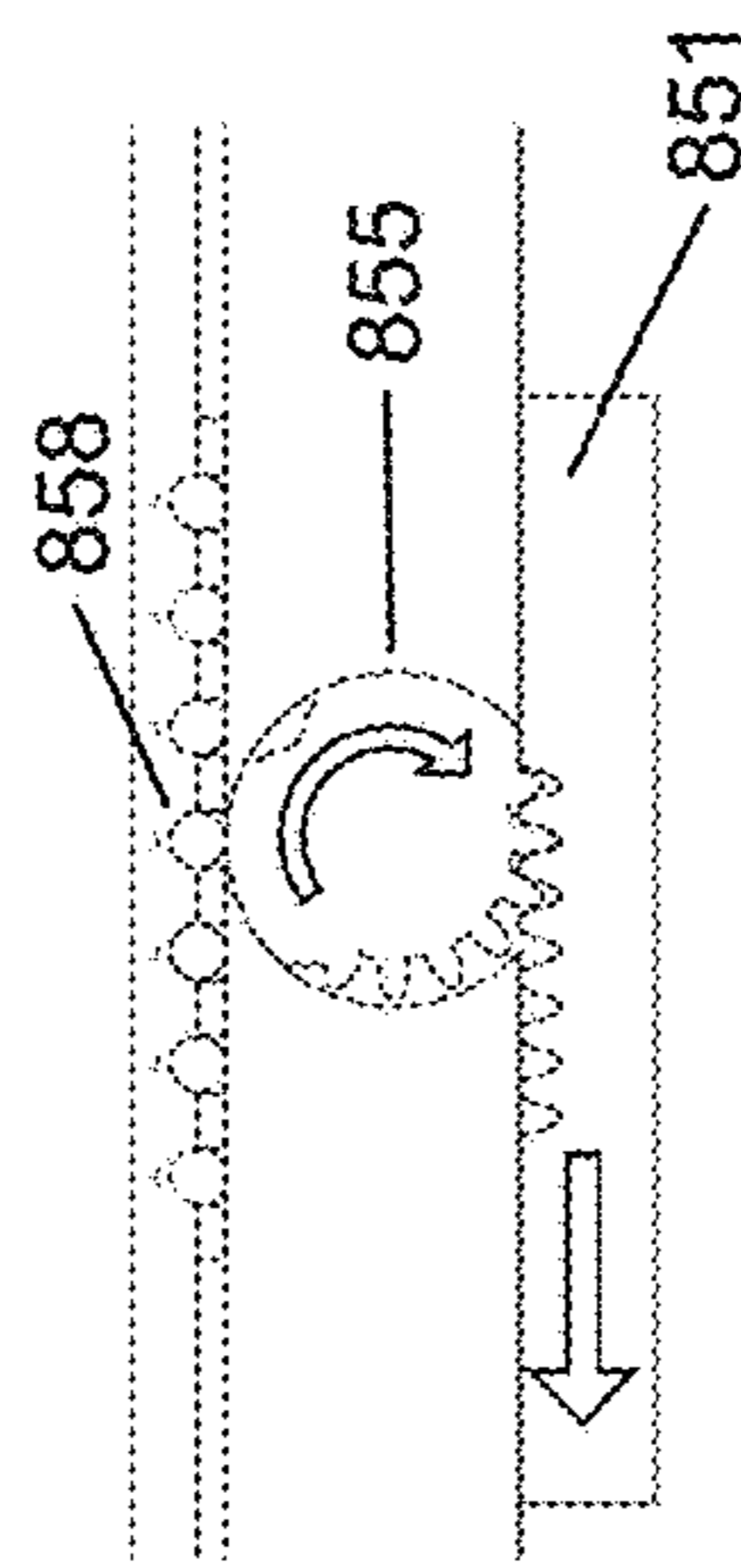


FIG. 8K

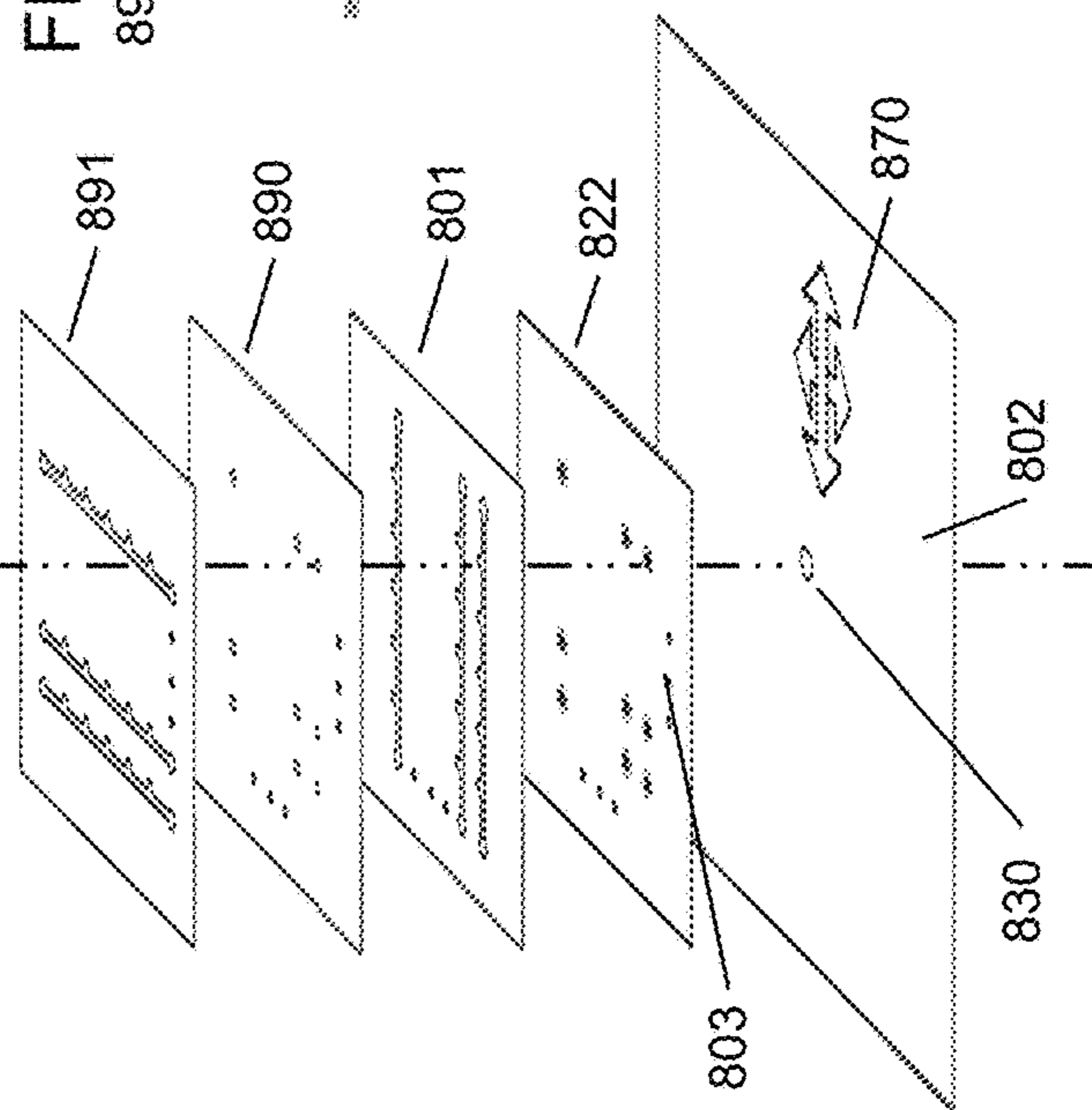


FIG. 8L

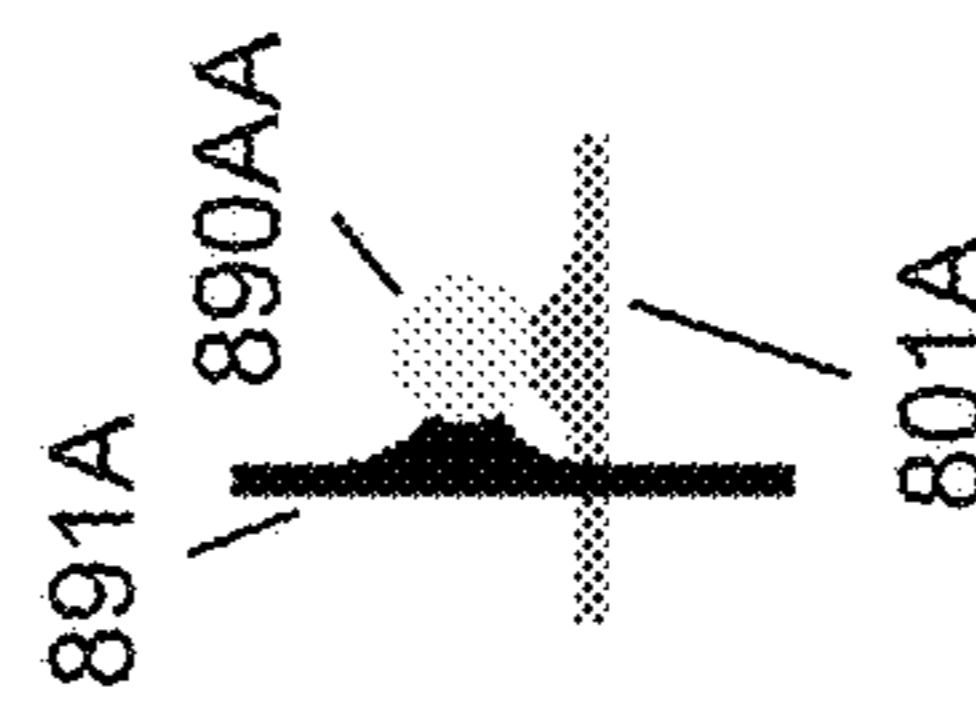


FIG. 8M

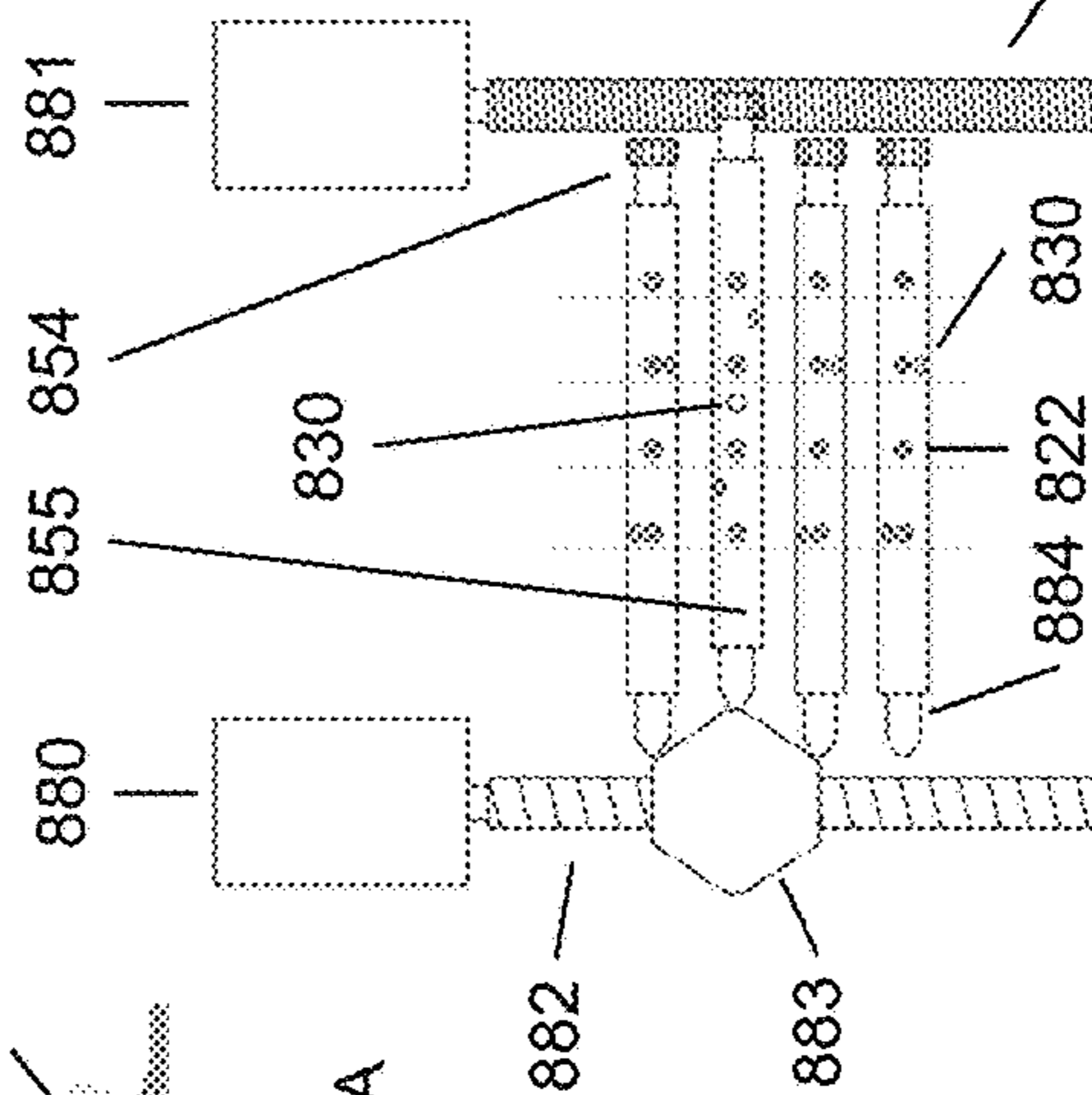


FIG. 8N

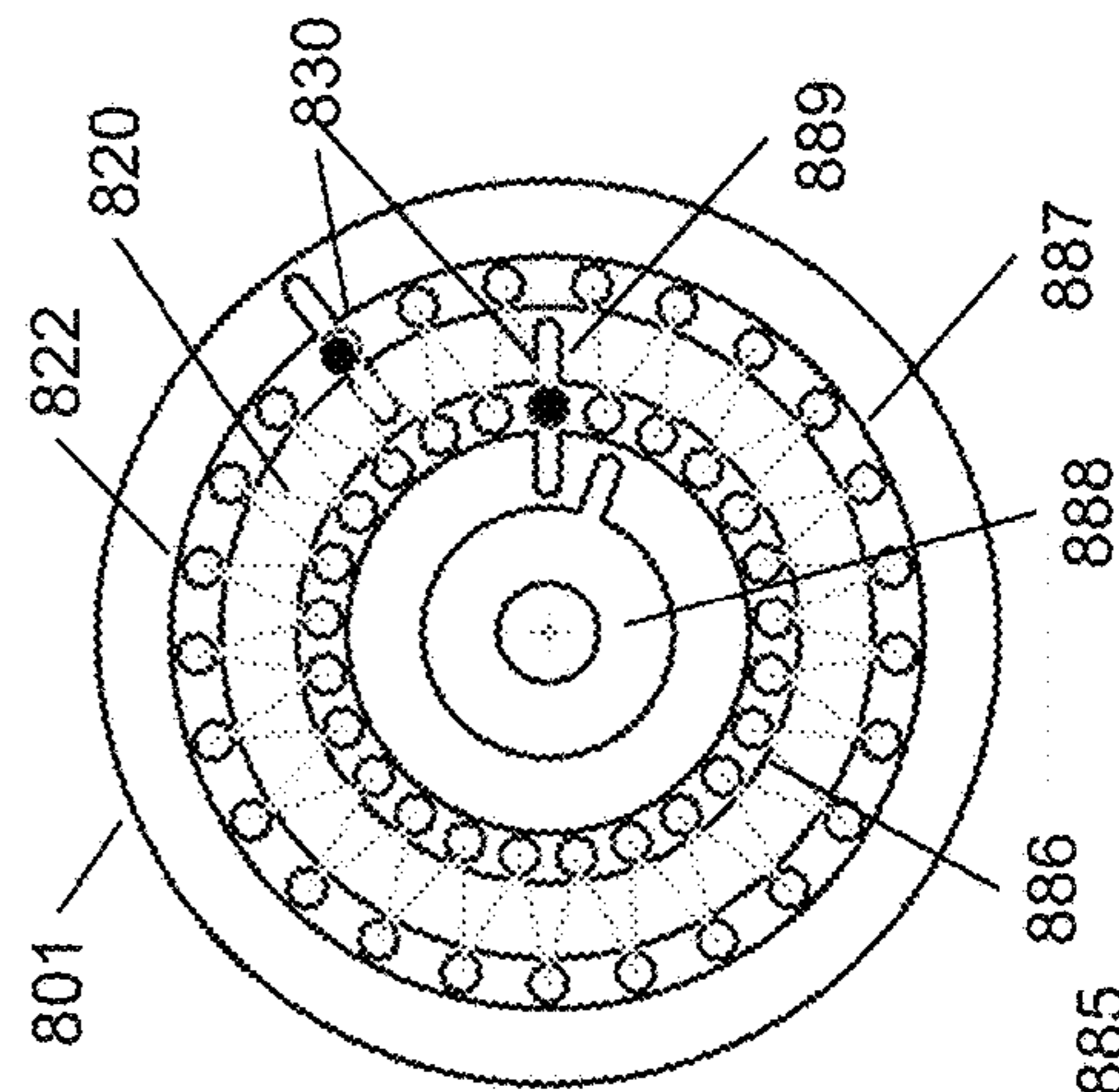


FIG. 9A

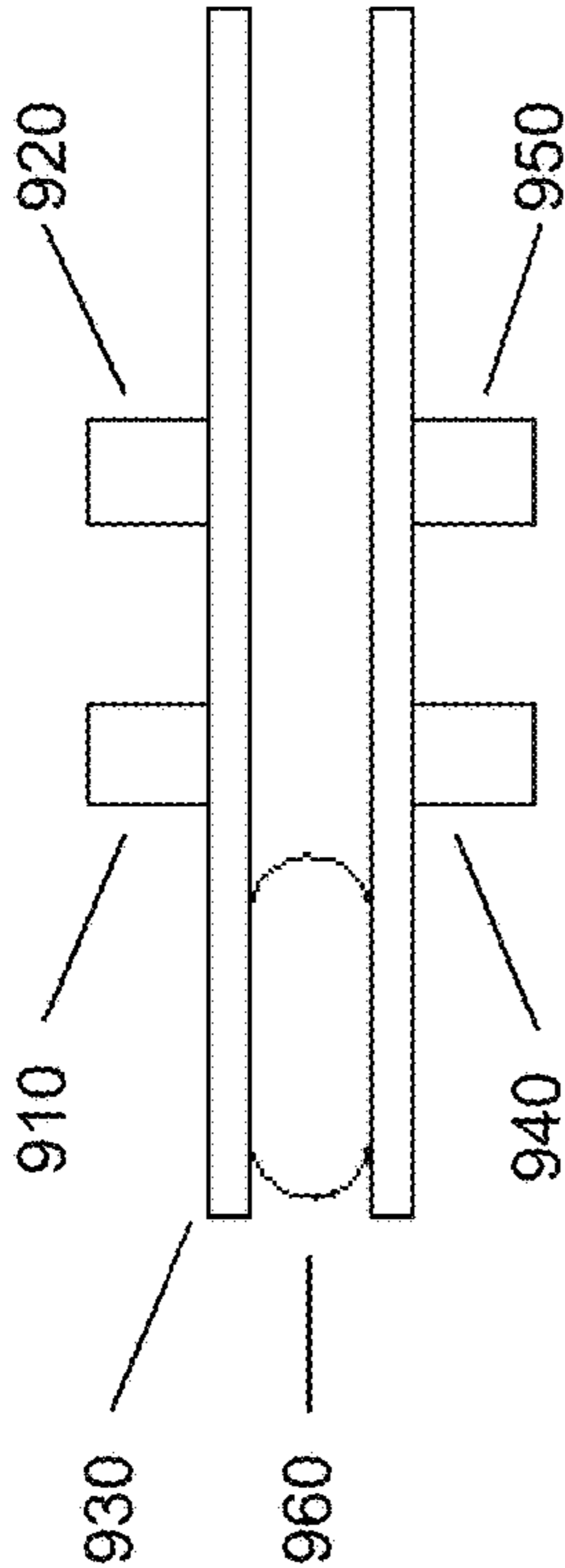


FIG. 9B

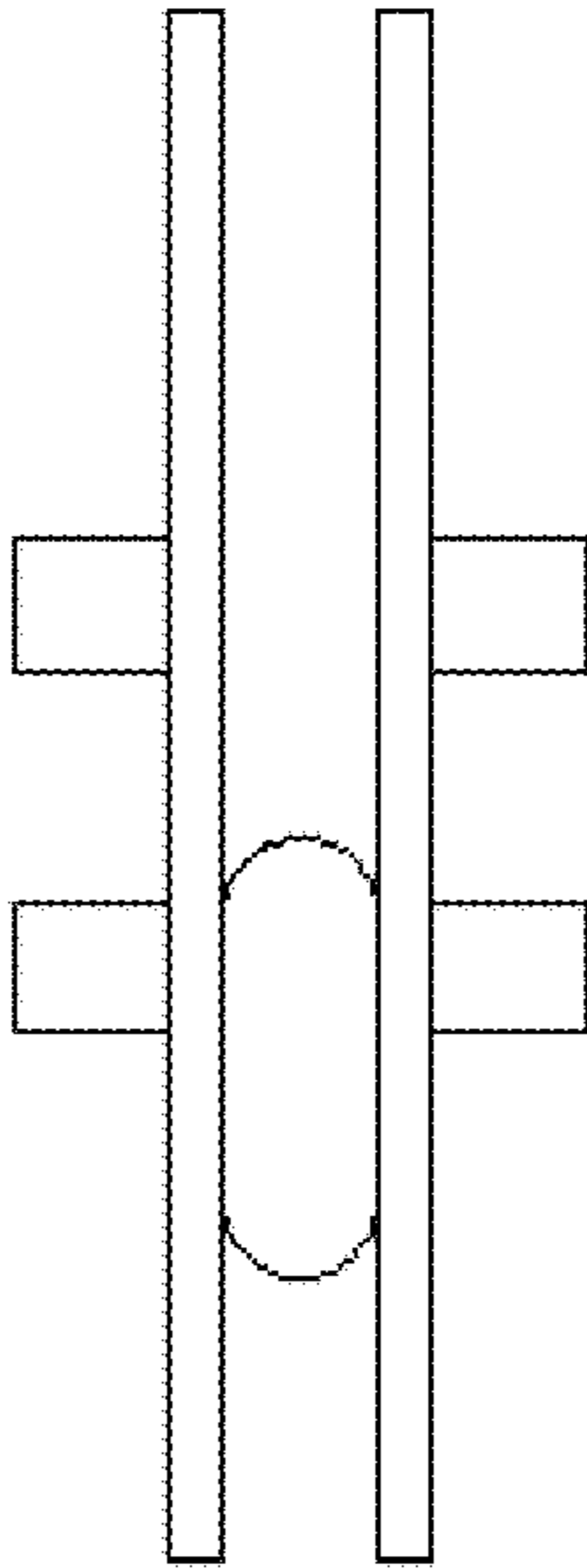


FIG. 9C

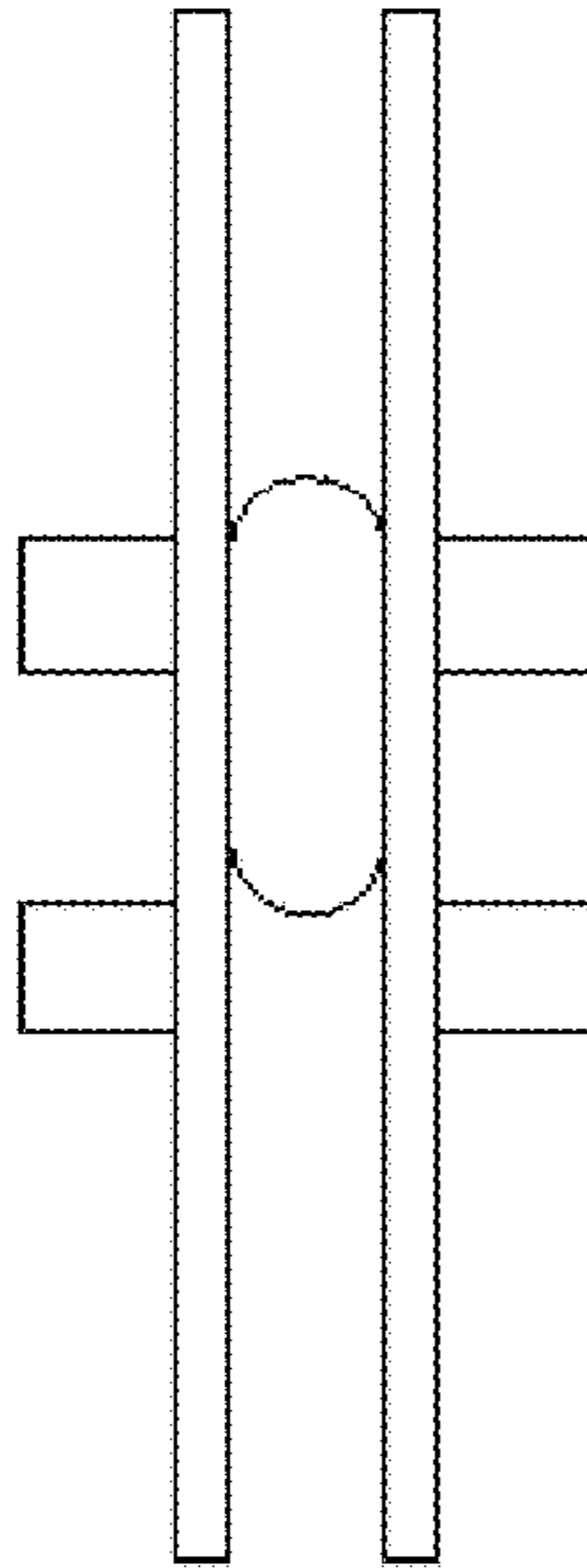


FIG. 9D

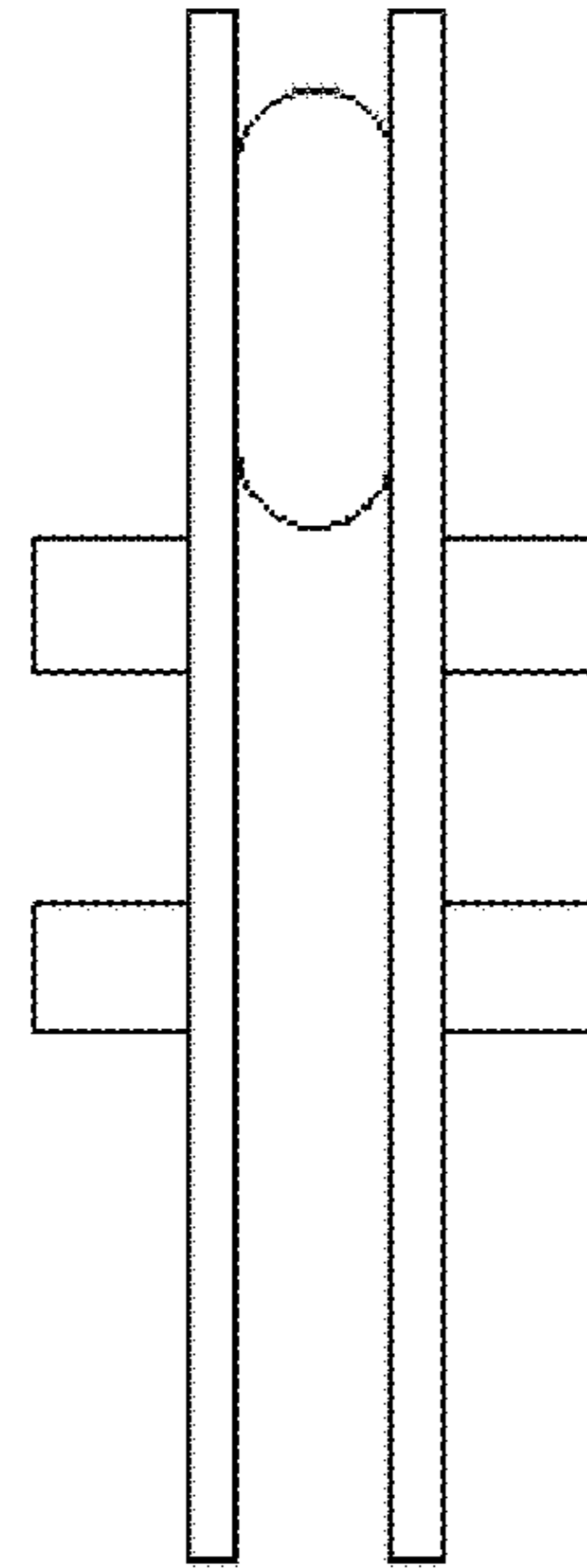
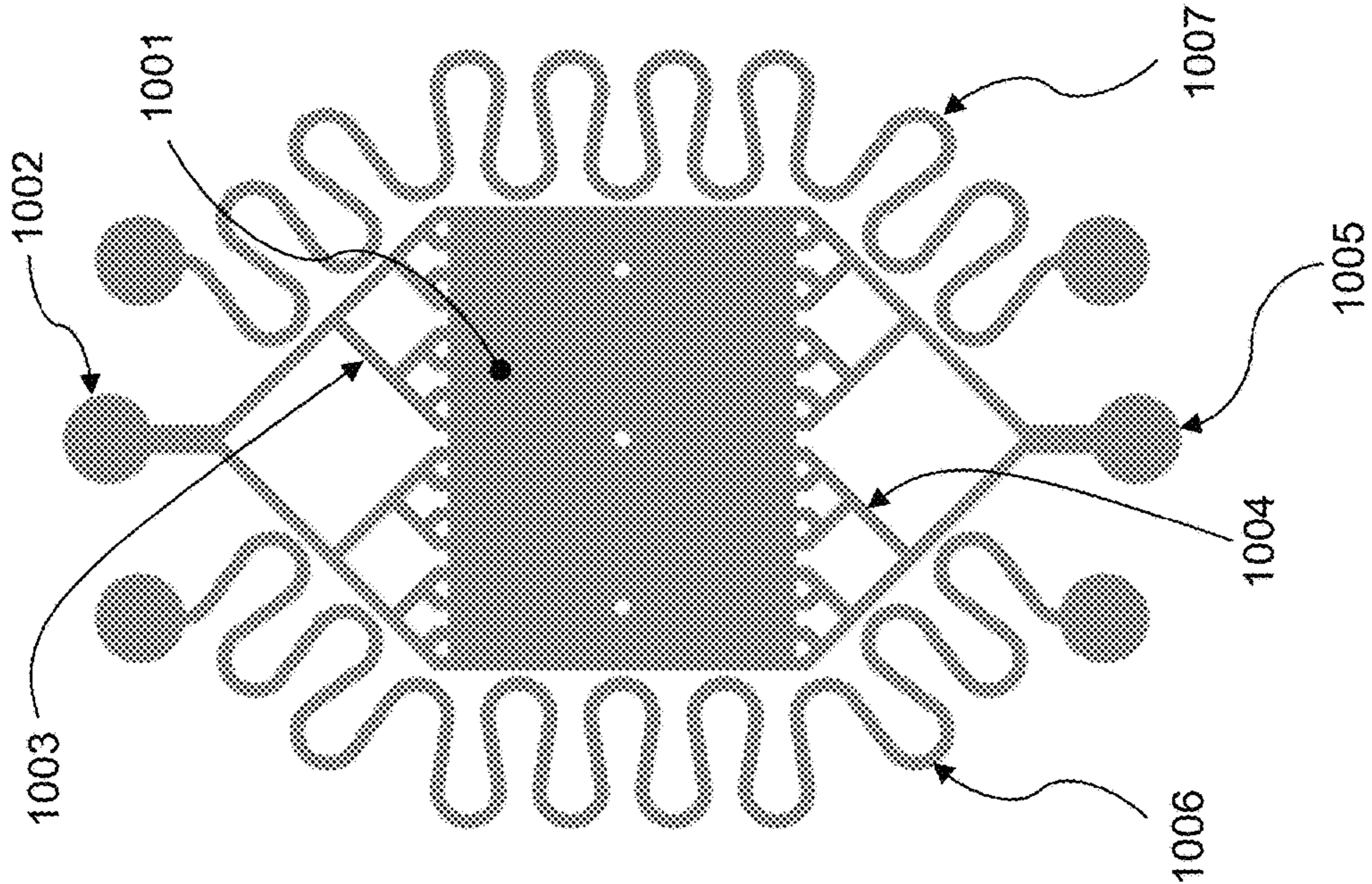


FIG. 10



MICROFLUIDIC SYSTEMS, PUMPS, VALVES, FLUIDIC CHIPS THEREOF, AND APPLICATIONS OF SAME

CROSS-REFERENCE TO RELATED PATENT APPLICATIONS

This application is a continuation application of U.S. patent application Ser. No. 17/623,350, filed Dec. 28, 2021, now allowed, which is a U.S. national phase entry of PCT Patent Application Serial No. PCT/US2020/040061, filed Jun. 29, 2020, which claims priority to and the benefit of U.S. Provisional Patent Application Ser. No. 62/868,303, filed Jun. 28, 2019, and is also a continuation-in-part application of PCT Application Serial Nos. PCT/US2019/047190, PCT/US2019/047307 and PCT/US2019/047324, all filed Aug. 20, 2019. Each of the above-identified applications is incorporated herein by reference in its entirety.

STATEMENT AS TO RIGHTS UNDER FEDERALLY-SPONSORED RESEARCH

This invention was made with government support under Grant Nos. 5UG3TR002097-02, U01CA202229 and HHSN271201700044C awarded by the National Institutes of Health, Grant No. 83573601 awarded by the U.S. Environmental Protection Agency, Grant No. 2017-17081500003 awarded by the Intelligence Advanced Research Projects Activity, and Grant No. CBMXCEL-XL1-2-001 awarded by the Defense Threat Reduction Agency through Subcontract 468746 by Los Alamos National Laboratory (LANL). The government has certain rights in the invention.

FIELD OF THE INVENTION

The invention relates generally to fluidic systems, and more particularly to microfluidic systems, pumps and valves, fluidic chips thereof, and applications of the same.

BACKGROUND INFORMATION

Existing pumps and valves are used in controlling and sensing organs-on-chips. These pumps and valves are implemented in a fluidic cartridge that contains the mechanical, electrical, and microfluidic components necessary for operation thereof. However, further improvement and refinement of the pumps and valves may be required. Therefore, a heretofore unaddressed need exists in the art to address the aforementioned deficiencies and inadequacies.

SUMMARY OF THE INVENTION

One aspect of the present invention relates to a microfluidic system, which is used as a tilted-actuator pump, and includes: a support plate; a fluidic chip disposed on the support plate, wherein the fluidic chip has a fluidic network comprising at least one fluidic channel; an actuator having a plurality of compression structures configured to roll against the fluidic chip to control the fluidic channel to switch locally between an open state and a closed state, wherein each of the compression structures is a roller; and a motor shaft inserted in the actuator to drive the actuator to rotate relative to the fluidic chip; wherein the actuator and the motor shaft are disposed to tilt from an actuator-contact surface of the fluidic chip, such that the actuator rotates in a plane tilted by an angle with respect to the actuator-contact surface of the fluidic chip. In one embodiment, the motor

shaft is perpendicular to the support plate, and the fluidic chip is a wedge-shaped fluidic chip, such that the actuator and the motor shaft are disposed to tilt from the actuator-contact surface of the wedge-shaped fluidic chip. Alternatively, in one embodiment, the motor shaft is tilted and is not perpendicular to the actuator-contact surface of the fluidic chip and the support plate, such that the actuator and the motor shaft are disposed to tilt from the actuator-contact surface of the fluidic chip that has parallel contacting and fluidic surfaces. Alternatively, in one embodiment, the motor shaft is perpendicular to the support plate, and a passive wedge structure is disposed between the fluidic chip and the support plate, such that the fluidic chip is disposed to tilt from the support plate, and the actuator and the motor shaft are disposed to tilt from the actuator-contact surface of the fluidic chip.

A further aspect of the present invention relates to a microfluidic system, which includes: a support plate; a fluidic chip disposed on the support plate, wherein the fluidic chip has a fluidic network comprising at least one fluidic channel; at least one compression structure, configured to compress or decompress the fluidic network within the fluidic chip; an actuator, controlling the compression structure at one or more compression or decompression sites; and a motor shaft inserted in the actuator, configured to rotate the actuator relative to the fluidic chip, wherein the actuator controls the compression structure at the compression or decompression site to compress or decompress the fluidic channel at a particular location when the actuator rotates or otherwise moves.

In one embodiment, the actuator is an actuator assembly including: a ball cup facing the fluidic chip, forming the receiving cavity between the ball cup and the fluidic chip, wherein the at least one compression structure comprises a plurality of balls disposed in the receiving cavity and configured to roll against the fluidic chip; a ball cage disposed between the balls; and a traction disc disposed between the ball cup and the balls, configured to generate a traction force to compress the balls to roll against the fluidic chip.

In one embodiment, the fluidic chip is a spiral pump chip including: a first surface facing and fixed to the support plate; and a circular zone disposed on a second surface facing the actuator assembly, wherein each compression structure of the actuator rolls against the circular zone; wherein each fluidic channel of the spiral pump chip is a spiral fluidic channel having an outer end outside the circular zone and an inner end within the circular zone, and each spiral fluidic channel partially aligns with the circular zone along a vertical direction, such that each compression structure rolls along the circular zone, compressing the portion of each spiral fluidic channel to pump a fluid inside the non-compressed segments of each spiral fluidic channel.

In one embodiment, the fluidic chip is a rotary peristaltic pump chip, each fluidic channel within the rotary peristaltic pump chip has a pumping channel interconnected with an output channel and an output bypass channel, and the at least one compression structure comprises a plurality of balls configured to roll against an outer surface of the pumping channel and to press a fluid in the pumping channel toward the output channel and the output bypass channel.

In one embodiment, the fluidic chip is an analytical valve chip, and the fluidic network within the analytical valve chip includes: a sensor output channel connected to a sensor; a waste output channel connected to a waste reservoir; one or more bioreactor input channels, each being connected to a bioreactor; and a plurality of rinse/calibration input chan-

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nels; wherein the compression structure comprises a plurality of caged balls, and the actuator comprises a sliding actuating surface with actuating recesses that, depending upon actuator position, compress or release the balls against the sensor output channel, the waste output channel, and the rinse/calibration input channels to interconnect the bioreactor input channel and the rinse/calibration input channels with the sensor output channel and the waste output channel, wherein in a calibration mode, at least one of the bioreactor input channels is selected to be interconnected to the waste output channel, allowing an analyte from the corresponding bioreactor to be sent to the waste reservoir through the selected bioreactor input channel and the waste output channel, and the rinse/calibration input channels are successively interconnected to the sensor output channel to perform rinse and provide calibration media to the sensor; and in a measurement mode, one of the bioreactor input channels is selected to be interconnected to the waste output channel, allowing the analyte from the selected bioreactor to be sent to the sensor through the bioreactor input channel and the sensor output channel to perform an analytic measurement of the analyte by the sensor, and the other bioreactor input channels and one or more of the rinse/calibration input channels are interconnected to the waste output channel.

In one embodiment, the fluidic chip is a multi-port valve chip comprising a first port and a plurality of second ports, wherein the fluidic channel of the multi-port valve chip interconnects the first port with all of the second ports, the at least one compression structure comprises a plurality of caged balls and a recess corresponding to the caged balls, each of the caged balls is located corresponding to one of the second ports, and when the actuator rotates, only one of the caged balls is located in the recess to allow a corresponding second port to switch to an open state, and the other of the caged balls are not located in the recess such that the other corresponding second ports remain in a closed state.

In one embodiment, the multi-port valve chip is a random-access valve, and the actuator includes: a first actuator disk connected to the motor shaft, and having a tangential rack; and a second actuator disk having a partial pinion disposed at a circumferential side and mated with the tangential rack of the first actuator disk, wherein the recess is formed on the partial pinion; wherein when the tangential rack reaches and jams at an extreme end of the partial pinion, the first actuator disk drives the second actuator disk to rotate relative to the fluidic chip; and when the tangential rack does not reach the extreme end of the partial pinion, the first actuator disk drives the partial pinion to rotate relative to the second actuator disk.

In one embodiment, the fluidic chip is a direct-access valve chip having two caged-ball locations corresponding to each fluidic channel, the at least one compression structure comprises at least two balls corresponding to the two caged-ball locations, wherein each ball is configured to press the direct-access valve chip to switch a corresponding portion of each fluidic channel to a closed state, and the actuator is a lagging actuator including: an outer actuator, fixed to the motor shaft and having an outer groove corresponding to one of the two caged-ball locations; and an inner actuator, having a limiting pocket and having an inner groove corresponding to the other of the two caged-ball locations. Each of the inner groove and the outer groove, when aligned with the corresponding one of the two caged-ball locations, relieves the corresponding ball to switch the corresponding portion of each fluidic channel to an open (uncompressed) state. A limiting pin is fixed to the outer actuator and inserted in the limiting pocket of the inner

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actuator. The limiting pocket has an arc-length such that, when the lagging actuator rotates along a clockwise direction relative to the direct-access valve chip, the limiting pin reaches a clockwise extreme end of the limiting pocket, and the outer groove and the inner groove are unaligned, allowing at most one of the outer groove and the inner groove to align with the balls corresponding to one of the fluidic channels; and when the lagging actuator rotates along a counterclockwise direction relative to the direct-access valve chip, the limiting pin reaches a counterclockwise extreme end of the limiting pocket, and the outer groove and the inner groove are aligned, allowing both the outer groove and the inner groove to align with the balls corresponding to one of the fluidic channels.

In yet another aspect, a microfluidic system is provided, which is a random-access bistable valve, and includes: a support plate; a fluidic chip disposed on the support plate, wherein the fluidic chip has a common fluidic channel and a plurality of access channels; an elastomeric membrane disposed on the fluidic chip; a plurality of caged balls disposed on the elastomeric membrane, corresponding to and aligned with the access channels, and an actuator disposed on the elastomeric membrane and having a recess, wherein the actuator presses the caged balls against the elastomeric membrane to seal the access channels in a closed state; wherein a relative position of the recess is randomly movable relative to the fluidic chip, and when the recess moves to a position to align with one of the balls, the recess allows the one of the caged balls to release the elastomeric membrane and switch the corresponding access channel to an open state.

In one embodiment, the actuator includes: a central partial pinion connected to the motor shaft; and a rack pawl located in an actuator slot and mated with the central partial pinion, wherein the recess is formed on the rack pawl; wherein when the central partial pinion rotates clockwise, the rack pawl moves and allows the recess to align with one of the caged balls; and when the central partial pinion rotates counterclockwise, the rack pawl moves and retracts the recess, such that the recess does not align with any of the caged balls; and wherein when the central partial pinion rotates counterclockwise to an extreme position, the rack pawl moves to abut against an end of the actuator slot, and the central partial pinion drives the entire actuator to rotate relative to the fluidic chip.

In one embodiment, the actuator includes: a central pinion connected to the motor shaft; and a partial pinion mated with the central pinion, wherein the recess is formed on the partial pinion; wherein when the central pinion rotates, the central pinion drives the partial pinion to rotate relative to the fluidic chip, allowing the recess to move to the position to align with one of the caged balls or to retract and not to align with any of the balls; and wherein when the central pinion rotates to an extreme position of the partial pinion, the central pinion drives the entire actuator to rotate relative to the fluidic chip.

In certain embodiments, the microfluidic system further includes a bubble-tracking flow meter, which includes: two light-transmission detecting devices disposed on two locations of the fluidic channel of the fluidic chip, each of the two light-transmission detecting devices comprising: a light source disposed on a first side of the fluidic channel, configured to emit light; and a light detector disposed on a second, opposite side of the fluidic channel, configured to receive light emitted by the light source; wherein a bubble injected in the fluidic channel is configured to trigger each of two light-transmission detecting devices, such that a flow

rate of the fluidic channel is determined by measuring the time difference between the threshold signals reported by two light-transmission detecting devices.

In certain embodiments, the microfluidic system further includes a gas exchange bioreactor, which includes a chamber located between and in communication with an input port and an output port, where a bioreactor perfusion media is configured to pass through the chamber; and a plurality of gas exchange channels surrounding the chamber, such that gas passing through the gas exchange channels is configured to diffuse through a material between the chamber and each gas exchange channel and to interact with a content of the chamber.

These and other aspects of the invention will become apparent from the following description of the preferred embodiment taken in conjunction with the following drawings, although variations and modifications therein may be affected without departing from the spirit and scope of the novel concepts of the disclosure.

BRIEF DESCRIPTION OF THE DRAWINGS

The accompanying drawings illustrate one or more embodiments of the invention and, together with the written description, serve to explain the principles of the invention. Wherever possible, the same reference numbers are used throughout the drawings to refer to the same or like elements of an embodiment.

FIGS. 1A-1C show a tilted rotor pump according to certain embodiments of the invention, where FIG. 1A shows a wedge-shaped fluidic chip, FIG. 1B shows a tilted actuator, and FIG. 1C shows an additional wedge.

FIGS. 2A and 2B show a rolling ball actuator assembly according to one embodiment of the present invention.

FIGS. 2C and 2D show a rolling ball actuator assembly according to another embodiment of the present invention.

FIGS. 2E and 2F show a microfluidic pump having the rolling ball actuator assembly of FIGS. 2A-2B.

FIGS. 3A-3G show a spiral pump according to certain embodiments of the invention.

FIG. 4 shows a rotary peristaltic pump according to certain embodiments of the invention.

FIGS. 5A-5G show a multi-port, multi-throw analytical valve according to certain embodiments of the invention.

FIGS. 6A-6G show a multi-port valve according to certain embodiments of the invention.

FIGS. 7A-7C show a lagging-actuator direct-access valve according to certain embodiments of the invention.

FIGS. 8A-8N show a random-access bistable valve according to certain embodiments of the invention.

FIGS. 9A-9D show a bubble-tracking flow meter according to certain embodiments of the invention.

FIG. 10 shows a gas exchange bioreactor according to certain embodiments of the invention.

DETAILED DESCRIPTION OF THE INVENTION

The invention will now be described more fully herein-after with reference to the accompanying drawings, in which exemplary embodiments of the invention are shown. The invention may, however, be embodied in many different forms and should not be construed as limited to the embodiments set forth herein. Rather, these embodiments are provided so that this disclosure will be thorough and complete,

and will fully convey the scope of the invention to those skilled in the art. Like reference numerals refer to like elements throughout.

One aspect of the present invention relates to a microfluidic system, which is used as a tilted-rotor or actuator rotary peristaltic pump. FIGS. 1A-1C show a tilted actuator pump according to certain embodiments of the invention. Specifically, FIG. 1A shows a substantially vertical motor shaft **101** inserted into a pump actuator **102** that moves the rollers **103** to compress a wedge-shaped fluidic chip **104** with contacting surface **110** and fluidic surface **120** with a wedge angle θ between them that is mounted upon a support plate **100**, where $\theta \neq 0$. FIG. 1B indicates how the same varying force between the rollers and the contacted surface of the fluidic chip can be accomplished by tilted shaft **106** and the pump actuator **102**, such that the actuator **102** and the rollers therein rotate in a plane that is tilted by angle θ with respect to the fluidic chip **105**. FIG. 1C shows a substantially vertical motor shaft **101**, but with the contacted surface of fluidic chip **105** separated from the support plate **100** by a passive wedge **107** with angle θ . In all cases, the wedges or motor tilt reduces the flow transients associated with abrupt engagement and disengagement of a roller with the underlying channel.

One aspect of the present invention relates to a microfluidic system, which utilizes a rolling ball actuator. FIGS. 2A-2D show a rolling ball actuator assembly according to certain embodiments of the invention, and FIGS. 2E and 2F show a microfluidic pump having the rolling ball actuator assembly. As shown in FIGS. 2A and 2B, the rolling ball actuator assembly **200** includes a sprocket **201**, which functions as a ball cage, to maintain the separation of balls **202**. In certain embodiments, the actuator assembly **200** may include at least one ball **202**, and the sprocket **201** may be necessary when multiple balls **202** are provided. The balls **202** roll against an elastomeric O-ring **203** (see FIG. 2B), which functions as a traction disc that provides the traction force to allow the balls **202** to roll against the fluidic chip **213** (see FIGS. 2E and 2F). Between the balls **202**, the fluidic chip **213** is not compressed so that the fluidic channel can capture the fluid being pumped. The round or square cross-section O-ring **203** is positioned in a recess groove in ball cup **204** in such a way to avoid contact with the rotating sprocket ball cage **201**. The radial position of the balls is determined by a ball cup **204** and the sprocket **201**. A set screw in a threaded hole **205** attaches the actuator assembly **200** to the motor shaft **215** (see FIGS. 2E and 2F). FIGS. 2C and 2D show an actuator assembly according to another embodiment, with an elastomeric washer **207** as a flat elastomeric traction disk that lies flat on the bottom of the ball cup **204** with a spacer/washer **208** above in the center to create a vertical separation between the traction disk **207** and the sprocket **201**. FIG. 2D shows the traction disk **207** being penetrated by a central shoulder **209** that is part of the ball cup **204** that elevates the actuator **201** and prevents it from rubbing against the disk **207**, thereby avoiding damage to the traction washer caused by rubbing against the sprocket. As shown in FIGS. 2E and 2F, a through-plate fluidic chip **213** with pumping channels (not shown) is supported by the fluidic support plate **214**. The motor shaft **215** rotates the actuator assembly **200** in contact with the fluidic chip **213**, thus forming a microfluidic pump.

FIGS. 3A-3G show a spiral pump according to certain embodiments of the invention. Specifically, FIG. 3A shows a through-plate elastomeric fluidic chip as a single-channel spiral peristaltic pump **300**, which may be used as the fluidic chip **213** in FIGS. 2E and 2F. The through-plate elastomeric

fluidic chip **313** has six outer protrusions **301** and a single inner protrusion **331** that align and hold the chip **313** in a support plate (**214** in FIGS. **2E** and **2F**). These protrusions **301** and **331** are optional and are used for convenience here to combine the functions of mechanical positioning and tubing ports and do not affect the operation or performance of the described spiral pump. The microfluidic channel **320** has an outer end **321** to a tubing port within one of the outer protrusions **301**, and an inner end **329** that connects to a tubing port in the inner protrusion **331**. A multiple-ball rolling ball actuator (such as the actuator assembly **200** in FIGS. **2E** and **2F**) compresses a circular zone **340** that crosses a segment of the spiral fluidic channel **320** at point **325**. As the ball actuator continues to move, in this example counterclockwise, the channel **320** is fully collapsed by the compression zone, and the dots **302** represent the sequential positions of one of the many balls in the actuator, as shown at the location "A" to "F" of maximum channel compression at sequential instants of time, as indicated by the six section lines in FIG. **3A** and the sectional views in FIG. **3B**. At location A, the channel **320** is fully compressed, as shown by **362** in FIGS. **3B** and **3C**, and blocks the flow of fluid. The point moves as the actuator rotates. In this example, the pumping of the channel **320** is from the outer end **321** to the inner end **329** (through points A to F), and at the point F, the ball being tracked no longer compresses the channel **320** so that it relaxes to its native dimensions (**367**, FIG. **3C**). As the balls travel along their circular path, the fluid is trapped between the travelling compression zones and moves along the channels, because beneath each ball in the compression zone the cross-sectional area of the channel **320** will be less than the relaxed value given by the native dimensions of the channel **367** (FIG. **3C**). As the balls move out of the compression zone, the trapped fluid will be gradually released towards the channel outlet **329**. If the dots A-F were to represent separate balls rather than a single ball being tracked with time, each of the compression zones A-to-B, B-to-C, C-to-D, D-to-E, and E-to-F acts as a travelling fluidic capacitor that absorbs pressure and volume changes, while the incomplete compression zones between the dots (C, D, E) act as resistors in a series of resistor-capacitor low-pass filters that move along the spiral channel and attenuate severely the fluctuations normally associated with a peristaltic pump. A similar filtering effect occurs to minimize reflected input fluctuations as the channel enters the compression zone between **321** and AA'. The exact spiral shape of the spiral channel **320**, its size relative to the actuator, and the diameter and spacing between the balls in the rolling ball actuator will determine the low-pass filter characteristics of the spiral pump. The gradual restoration of the compressed channel shape depicted in FIGS. **3B** and **3C** as the actuator balls roll away from the channel contributes to the gradual, smooth release of the fluid trapped between the ball compression zones. While in this example the actuator is rotating counterclockwise to pump from the outer end **321** to the inner end **329**, the device may also function in reverse, pumping from **329** to **321** with clockwise actuator rotation. In certain embodiments, the parameters that describe the curvature of the spiral can be adjusted to minimize output pulsations preferably for one direction of motion. A different parameterization could optimize the performance for the opposite direction of rotation.

Given that only a small fraction of the area of the fluidic chip **313** is occupied by the spiral channels and only one outer protrusion **301** contains a tubing port **321**, in certain embodiments, it is possible to add additional channels to the fluidic chip **313**, as shown in FIGS. **3D** (6 channels) and **3E**

(12 channels), with the corresponding 6 and 12 tubing ports respectively on the inner protrusion **331**. Further, given that all the channels in either FIG. **3D** or **3E** will produce identical flow rates, within manufacturing tolerances, half of the channels could be used to deliver fluid to one side of a sealed barrier bioreactor, for example a neurovascular unit (NVU) on a chip, and the other half used to deliver fluid to the other side of the barrier. Thus, the six-channel chip in FIG. **3D** could use a single motor and actuator to perfuse both sides of three two-chamber NVUs. Alternatively, the matched pumping channels could ensure that the same amount of fluid that was delivered to the input of a bioreactor was removed from the other, to minimize pressurized flow across the barrier, in the form of a push-pull pump pair, and the 12-channel pump in FIG. **3E** could do push-pull perfusion of both sides of three NVU bioreactors.

While a constant level of fluid in an open reservoir could be maintained by pumping in the exact amount of fluid as is pumped out, in practice this is difficult to accomplish, as pump properties or local conditions vary over time. The inevitable mismatches could lead to a reservoir being emptied or overfilled. In certain embodiments, the channels in FIGS. **3D** and **3E** may alternate in their cross-sectional area; for example, using two different channel widths and/or depths, the pumping rate of the larger channels would be proportionally larger than the smaller channels, which allows a multichannel spiral pump to maintain a particular level of fluid **381** in multiple open bioreactors **380**, as shown in FIG. **3F**, since the level of fluid in the bioreactor would be set by the height of the withdrawal tube **383** that would be designed to pump fluid faster than the fluid delivered by input tube **382**. Because the withdrawal channel pumps faster than the delivery channel, if the fluid level is higher than the bottom of the withdrawal tube **383**, the level will drop because more fluid is being pumped out. If the fluid level is lower than the bottom of the withdrawal tube **383**, the withdrawal tube **383** will pump air and the fluid level will rise, thereby regulating the fluid level.

FIG. **3G** shows a six-channel spiral pump that has a common central port. In this configuration, a clockwise rotation will deliver equal amounts of fluid to each of the outer ports, serving as a splitter that does not suffer from the inevitable imbalances that can occur with a passive splitter. Rotation in the counterclockwise direction will draw fluid from each of the outer ports and collect it at the inner one, for example to collect at identical rates effluent from multiple bioreactors and deliver it to a common reservoir or analytical instrument. In certain embodiments, not all channels/ports present must be used, which allows an application of this fluidic chip such that, with the actuator rotating counterclockwise, the collective flow rate may be selected by connecting any number of outer ports to supply tubing while blocking or recirculating the unused ports.

In the embodiment as described above, the spiral pump has the protrusions, and the balls are used as compression structures. In certain embodiments, the spiral pump does not require the protrusions. In certain embodiments, the balls may be replaced by rollers or alternative compression structures. Other embodiments of the spiral pump can utilize certain shapes of rollers or rollers in combination with force-distributing ridges rather than balls to provide the periodic moving pressure zones that result in progressively lesser degrees of channel compression in the regions of spiral channel closest to the center of the spiral that is end of the spiral that is typically designated as the fluid output port.

FIG. 4 shows a rotary peristaltic pump according to certain embodiments of the invention, which provides an alternative means to reduce peristaltic pump fluctuations. As shown in FIG. 4, the microfluidic chip 401 has a pumping channel 402, an output channel 404, and an output bypass channel 403 that connects 401 to the bioreactor or collection reservoir (not shown). A rotating rolling actuator 410, shown with a circumferential view, contains multiple balls 411 and a common cage 412. An external force applied to the balls 411 by either the cage 412 or to an upper moving traction disc (see FIGS. 2A-2D) causes the balls 411 and the cage 412 to move rightward, as shown by the arrow. As the balls 411 compress the pumping channel, the balls 411 create compression zones that capture fluid and, as the actuator moves rightward, the trapped fluid does as well. The use of two connection channels 403 and 404 prevent the fluid from being trapped and pressurized as the balls 411 reach the end of the channel 402 and fluid is expelled. The combination of the two connection channels 403 and 404 ensures that the delivery of fluid by the pump is never interrupted, which commonly happens with peristaltic pumps during the roll off transition. A corresponding structure could exist on the input of the pump to avoid transient halting of the input flow or when the pump is operated in the suction mode.

FIGS. 5A-5G show a multi-port, multi-throw analytical valve according to certain embodiments of the invention. Specifically, FIGS. 5A and 5B show the operation and utility of the multi-port, multi-throw analytical valve to control the connection of the output flow of one or more perfused microbioreactors or organs 540 to a metabolic or other sensor 550 or a waste reservoir 551. During the operation of the analytical valve in either a measurement mode (FIG. 5A) or a calibration mode (FIG. 5B), the output flow of the bioreactor(s) is never blocked. As shown in FIG. 5A, in the measurement mode, the output of the organ(s) 540 passes through the sensor 550 by the position of the valve 575, and the common fluidic channels of the valve 570 and the pump 580 are rinsed by having the pump 580 withdraw rinse media from reservoir 590 and direct it towards the waste reservoir 551. Other calibration solutions 570 could be pumped to the waste reservoir 551 as well. Further, as shown in FIG. 5B, in order to calibrate the metabolic sensor 550, which is prone to drift, the valve 570 is switched to the calibration mode by selecting calibration media (CAL 2 shown) from one of several calibration media reservoirs 560 to perform the calibration operation, the calibration media is delivered to the sensor 550 by the pump 580, and the output(s) of the organ(s) 540 is directed towards waste 551 by the action of valve 575. In this design, the organ(s) may be perfused by gravity, pneumatic pressure, or a pump (not shown) such that the organ is always continuously perfused.

FIG. 5C shows a single microfluidic analytical valve 500 that can implement the various modes described in FIGS. 5A and 5B. As shown in FIG. 5C, the analytical valve 500 includes a fluidic chip 501 with protrusions 521 that serve as tubing ports and anchor the fluidic chip 501 to the support plate 514, and microfluidic channels in the fluidic network 520 are sealed within the fluidic chip 501. The actuator 502, with ball-actuating grooves 530 in an actuating surface 533, is driven by a motor shaft 505, and includes actuating elements 503, a ball cage 504, and an off-board pump (not shown). The actuator 502 rotates to change the state of the valve and the caged actuating elements (in this embodiment balls) slide against the actuator. For example, in a first state as shown in FIG. 5D (where an actuator angle $\Theta=0^\circ$), the analytical valve 500 collects an analyte from the bioreactor (not shown) through a bioreactor input channel, and sends it

to a waste reservoir (not shown) through a waste output channel, while also collecting a rinse solution and directing it first through an internal fluidic channel 510, the off-board pump (not shown), through another internal fluidic channel 511, and finally to the sensor (not shown) through a sensor output channel. In a second state as shown in FIG. 5E (where the actuator angle $\Theta=120^\circ$), a calibration solution is selected (e.g., CAL 08) through a corresponding calibration input channel and directed to the sensor through the sensor output channel, while the bioreactor input channel is interconnected to the waste output channel to send the analyte from the bioreactor to waste. In a third state (where the actuator angle $\Theta=252-285^\circ$, not shown), the analyte remains directed from the bioreactor to waste, while all other conduits are closed and idle. In a fourth state as shown in FIG. 5F (where the actuator angle $\Theta=300^\circ$), the bioreactor input channel is switched and interconnected to the sensor output channel to direct the analyte from the bioreactor to the sensor, while all other conduits are idle. In a fifth state as shown in FIG. 5G (where the actuator angle $\Theta=306^\circ$), a rinse solution is directed through a rinse input channel to pass the length of channels 512, 513 and sent to waste, while the analyte remains are collected from the bioreactor and sent to the sensor. In the embodiments as shown in FIGS. 5A-5G, the analytical valve 500 is designed such that fluid being pumped into the fluidic chip 501 from the bioreactor has an outlet at all times (either sent to the sensor, to waste, or to both), as not to cause a dead-end scenario that might rupture the fluidic chip 501 or interrupt perfusion of a sensitive organ chip. In certain embodiments, the number of ports or channels that can be serviced as shown in FIGS. 5C-5G is determined by the available circumference of the through-plate fluidic chip 501 and the underlying tubing-port protrusions 521 that anchor the fluidic chip 501 to the support plate 514, and the minimum spacing between individual channels in the fluidic network 520. As shown in FIG. 5C, a typical valve has 1 inlet/outlet port and 25 outlet/inlet ports, depending upon the chosen flow direction. In certain embodiments, different embodiments of the fluidic network 520 could use some of the 25 ports to service two or more independent bioreactors whose output is either sent to a sensor or waste.

FIGS. 6A-6G show a multi-port valve according to certain embodiments of the invention. Specifically, the multi-port valve 600 is built upon the architecture of the rotary planar valve assembly 500 in FIG. 5C, except with a vastly higher port density. The multi-port valve 600 increases the number of ports by having the tubing port directly beneath each valve actuator, as shown in FIGS. 6A and 6B, where a through-chip fluidic valve unit 600 has a tubing 650 with a bore 651 seated in the tubing port of a circular through-plate fluidic chip 601 with multiple protrusions 621 inserted into fluidic support plate 614. In the open state as shown in FIG. 6A, the ball 603 is seated in the recess 630 in the actuator 602, and the access channel 619 in the fluidic chip is open and connected to tubing bore 651. As shown in FIG. 6B, the actuator 602 is rotated to the left so that the ball 603 is lifted out of the recess 630 to compress, collapse, and seal the access channel 621, switching it to the closed state. The resistance to shear force between the tubing 650 and the protrusion 621, and the insertion of the protrusion 621 into the support plate 614 together support the compressive force delivered by the ball 603 to create a compression zone and seal 660 immediately beneath the tubing port.

FIG. 6C shows a multi-port valve according to one embodiment, where the fluidic chip 601 has 100 valve units 600 with the protrusions 621 all penetrating corresponding

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holes in the support plate **614**. As shown in FIG. **6C**, a central port (i.e., the first port) **680** is connected to a single common channel **620** that is everywhere located outside of the compression zone **660** in FIG. **6B** that supplies (or collects) media from each of the valve units (i.e., the second ports), such that the first port **680** is interconnected with all of the second ports. The design does not require any cross-overs of the fluidic channels, so all fluidic channels are in a single layer. FIG. **6D** shows an enlarged view of the relation between the access channels **619** and the common channel **620**, where the length of each access channel **620** is kept as short as possible to extend beyond the compression zone **660** in FIG. **6B** to minimize the dead volume and fluid retention associated with the uncompressed portion of each sealed channel. FIG. **6D** also shows a radial actuator recess groove **630** that can span the radial distance occupied by the four-deep pattern of valve units **600** that are angled to allow the radial actuator groove **630** to access one valve unit at a time, depending on the angle to which the actuator is rotated. In other embodiments, the valve in FIG. **6D** with M ports could be divided into N identical sections, each with separate input ports **680** and common channels **620**, and an actuator **602** with N recesses, to create an $M \times N$ multiple-port/multiple-throw valve.

FIGS. **6E-6G** show the valve unit according to different embodiments, where the fluid is conveyed to the valve region not vertically by a tube **650** (see FIG. **6A**) but horizontally by a channel **618** that is connected to a vertical via **627** that is in turn connected to access channel **619**. In each of FIGS. **6E-6G**, the left panels show the open state similar to FIG. **6A**, and the right panels show the closed state similar to FIG. **6B**. As shown in FIG. **6E**, the upper fluidic layer **690** with the channel **618** is either rigid or elastomeric, the middle via layer **691** is rigid and supports the compressive force, and the lower layer **692** with channel **619** is elastomeric. The valve in FIG. **6F** has only two fluidic layers **694** and **695** backed by a rigid support plate **693**, and does not have a via layer and hence cannot provide fluidic cross-overs because the vias are created by any intersections of channels on opposing surfaces of the two layers **694** and **695**. As shown in FIG. **6G**, a rigid support layer **696** supports the compressive force delivered to the rigid or elastomeric upper layer **697** without channels, a via layer **698** with a channel to the right, and a lower elastomeric layer **699** with a channel to the left, thus supporting fluidic cross-overs because the channels are in the upper surfaces of elastomeric layers **698** and **699**, and the middle layer **698** also provides the vias. In each embodiment, all layers are bonded to prevent leaks. The high density of ball actuators in FIGS. **6C-6D** can also be used to create a pump, since the use of three balls on a single straight channel operated in a specific sequence creates a pump. In certain embodiments, it is possible to create a rotating pump actuator that can provide this sequence with a properly curved groove.

FIGS. **7A-7C** show a lagging-actuator direct-access valve according to certain embodiments of the invention. Specifically, the rotary valves described above are all serial access valves, with the ports being addressed one after another as the actuator is rotated. Using FIG. **6C** as an example, suppose that the valve port in a first position is currently open, and it is necessary to close the port in the first position and open another port in an eighth position. Thus, the actuator would be rotated from the first position to the eighth position, transiently opening and closing all intermediate ports. As long as the fluidic channels were not pressurized and the actuator was rotated quickly, there would be minimal fluid displaced from channels in the second to seventh

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positions. Accordingly, a lagging-actuator direct-access valve has the ability to go from one valve position to a distant one without having to transiently open and close each intermediate channel. As shown in FIG. **7A**, a valve chip **700** has multiple actuating element (ball) locations **701** operating on each of the input/output fluidic channels **702** connected to a common fluidic channel **703**. Each channel **702** is normally pinched closed by two balls **720** and **721** (see FIG. **7C**). A given input/output channel **702** pinched by at least one ball **720** and **721** is closed. In order to open the given input/output channel **702**, the compressive force applied to both corresponding balls **720** and **721** must be relieved concurrently. In other words, if either or both balls **720** and **721** are not actuated from their normally-closed position, the channel **702** remains closed.

FIG. **7B** shows a lagging-actuator assembly **710**, including an inner (driven) actuator **711** and an outer (driving) actuator **712**, as coaxially aligned on a motor shaft **713**. The outer actuator **712** is locked to the motor shaft **713** by a set screw (not shown) in the screw hole **718**. A limiting pin **714** is affixed to the outer actuator **712**, and its motion is constrained to within the bounds of a limiting pocket **715** on the inner actuator **711**. When the outer actuator **712** is rotated clockwise, the limiting pin **714** is driven to the clockwise extreme end of the limiting pocket **715**, and the reverse is also true. The arc-length of limiting pocket **715** establishes an intended backlash or "lag" between the outer actuator **712** and the inner actuator **711**. As the outer actuator **712** rotates clockwise as viewed from above, the limiting pin **714** contacts clockwise extreme end of limiting pocket **715**, and the outer actuator **712** and the inner actuator **711** begin to rotate as a whole, with an outer groove **717** on the outer actuator **712** and an inner groove **716** on the inner actuator **711** unaligned. With grooves **716** and **717** unaligned, all input/output channels **702** see compression from at least one ball **720** and **721** at all times. Beginning in this state and immediately following reversal in rotational direction of the outer actuator **712**, the inner actuator **711** remains stationary (by friction and/or presence of actuator element **720** within the inner groove **716**) until the limiting pin **714** contacts the other end of the limiting pocket **715**, and the inner actuator **711** and the outer actuator **712** rotate as a whole with the grooves **716** and **717** axially aligned. In this case, with actuator grooves **716**, **717** axially aligned, both pinch points established by the balls **720** and **721** are relieved concurrently, and target channel **702** opens to flow.

FIG. **7C** shows a lagging-actuator assembly **710** as seen by the fluidic chip **700** as well as corresponding cross-sectional views, in multiple steps (from left to right) required for opening target channel **702** to flow. As the grooves **716**, **717** approach a target zone, the inner ball **720** and the outer ball **721** remain pressed into the fluidic chip, thereby blocking flow. When the lagging-actuator assembly **710** rotates from its previous position, no channel has both balls released concurrently. In the second step, by rotating counterclockwise (as seen by the fluidic chip **700**), the outer groove **717** reaches and aligns with the outer ball **721**. In the third step, after further counterclockwise rotation, the outer groove **717** has rotated past alignment with the outer ball **721**, while the inner groove **716** reaches and aligns with the inner ball **720**. In the rightmost and last step, rotation reverses until the outer groove **717** also aligns with the outer ball **721** while the inner (driven) actuator **711** remains stationary. Both balls have now retracted to open the target channel **702**.

In a different application, the actuator assembly **710** may spin along a same direction continuously (rather than moving to a designated channel and stopping) with the grooves

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unaligned, causing the balls **720**, **721** to sequentially relax momentarily. As the pinched channels **702** momentarily relax, the fluid previously displaced by respective balls **720**, **721** returns to fill the void. As the actuator assembly **710** continues to rotate, the balls **720**, **721** once again pinch the channel **702**, and the corresponding fluid is again displaced. The result is a pulsation of fluid through the conduit within and/or connected to the channel **702**, and this pulsation could be used at the end of the conduit to mix or agitate a reservoir of liquid in which it is submerged. Since no channels are relieved of both pinch points concurrently in this application, there is no net flow through channels **702**. In yet another application, it is also possible to provide the sequence required for unidirectional pumping by employing concentric rings that have a small "lag" offset. By making the lag offset operate in both directions, the sequence will be the same on the fluidic no matter which direction the motor is turning. This could be useful when coupling other mechanical components that are direction sensitive and could allow different modes of operation while always pumping fluid in the same direction.

FIGS. **8A-8M** show a random-access bistable valve according to certain embodiments of the invention, which provides random access to a valve that is bistable (each port is either open or closed, independent of whether the actuator is energized or not) and does not require the serial opening and closing of intermediate channels as previously discussed. In certain embodiments, the random-access bistable valve uses an actuator with two spatial degrees of freedom to provide random access to each port. As shown in FIG. **8A**, a rigid or elastomeric fluidic chip **801** has one common channel **820** and three access channels **819**, each with their own tubing ports **831-834** from the bottom. The channels are sealed by an elastomeric membrane **811** that is bonded to the fluidic chip **801**. Three actuator balls **803** are captured by a ball cage **822** and are pressed into the membrane **811** by the actuator **802** with a recess **830**. As shown, the leftmost ball **803** is released and the channel below it is open, whereas the right two balls are compressed into the membrane **811**, thereby sealing those two channels. An X-Y actuator device **870** can move the recess **830** along a trajectory **871** that will allow the recess to open the rightmost valve while leaving the middle valve unchanged. The actuation device **870** in FIG. **8A** may require two independent motors. In another embodiment, the mechanism in FIG. **8B** allows a single motor to change the radial position of an actuating recess depending upon the direction of rotation of the actuator. Specifically, FIG. **8B** shows a two-part actuator having an upper disk **840** and a lower disk **844** coupled by two pins **842** in one or more slots **843**, such that rotation in one direction would place the actuating recess at one distance from the axis of rotation, but rotation in the opposite direction would result in the actuating recess being pushed to a different radius. The upper disk **840** is rotated by a motor drive shaft **841** to rotate the two pins **842**, with one closer to the axis of the disk **840** than the other. The drive pins **842** engage the drive slot **843** in the lower disk **844**. The shape of the drive slot **843** is designed to maximize the difference in the radial distance moved by the actuating recess **845** relative to the axis of the motor shaft **841** and the upper disk **840** when the disk is rotated first in one direction and then in another.

In certain embodiments, the radial control of the actuating recess can also be controlled by miniature gears enclosed within a rotating actuator. For example, as shown in FIGS. **8C** and **8D**, the motor (not shown) rotates a central partial pinion **861**, which in turn drives the rack of a radial pawl **862**. Rotation of central pinion **861** in the clockwise direc-

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tion drives the pawl **862** and the actuating recess **863** outward, until the pawl **862** engages in the stationary slots **864** that define the angular location of the recess **863**. In this case, the recess **863** is directly above one of the 25 available balls **865** in the cage layer above the channels within the valve fluidic chip. When the pawl **862** is rotated counterclockwise (see FIG. **8D**), the pawl **862** is retracted, and the recess **863** is no longer opening the valve at that angular location. Because the pawl **862** jams against the end of the actuator slot **866**, the torque applied by the motor causes the entire actuator assembly to rotate counterclockwise, allowing the pawl **862** and the recess **863** to be moved to another angular location. Reversing the rotation to the clockwise direction drives the pawl outward and engages another stationary slot than the one as shown in FIG. **8C**.

FIGS. **8E** and **8F** show another embodiment, which accomplishes the same radial control by having the actuator recess driven by a pinion gear with limited rotation. When the pinion reaches its stop, the motor torque rotates the entire actuator to the desired position. The gears would be hidden beneath a planar surface that allows the actuator to slide under the balls, with the balls dropping only when they are in the recess **873**. The full central pinion **871** drives a partial pinion **872**. When the central pinion **871** is driven in a clockwise direction, the actuation recess **873** is drawn in until the upper stop **874** is encountered, at which point the entire assembly would rotate clockwise to the desired valve position. As shown in FIG. **8F**, the partial pinion **872** is rotated in the counterclockwise position, the recess **873** is driven out to engage with the desired actuating ball, and the lower stop **875** prevents the recess from being moved further out. Various combinations of clockwise and counterclockwise rotation of the central drive pinion thereby allow any desired valve to be actuated without engaging any intermediate ones.

In other embodiments, the random-access valve with geared detent control can be applied to other valves, such as the 100-port rotary planar valve in FIGS. **6C** and **6D**. FIG. **8G** partially shows a valve of FIG. **6D** with the actuator groove **630**. This valve can be made into a random-access valve if it is possible to remove the groove when it is traversing balls whose opening is not desired. As shown in FIGS. **8H-8J**, the mechanism converts the planar pinion/rack/stop approach of FIGS. **8E** and **8F** into a radial, cylindrical valve actuator that rotates in a similar directional manner, except in a vertical plane to drive a horizontal, radial cylinder that exposes or hides actuator groove **830**. As shown in FIG. **8H**, the lower actuator disk **851** is driven by a motor shaft **850** to rotate teeth of a tangential rack **852**. These teeth engage with teeth of a partial pinion **854** in the actuator cylinder **855** in an upper actuator disk **856**. A stationary ball cage **822** has a ball **858** resting in the actuator groove **830** so that the corresponding valve in the fluidic chip **801** is open (see FIG. **8I**). The adjacent balls **859** are not in the groove **830**, and thus are elevated in the ball cage **822** and compress membrane **811** to seal the corresponding channels controlled by the elevated balls **859**. FIG. **8I** shows how the cylindrical actuator **855** is captured in the radial and horizontal cylindrical hole **853**. As shown in FIG. **8J**, the lower actuator disk has been rotated to the left, causing the cylindrical actuator **855** to rotate clockwise, such that ball **858** is no longer in the recess, and the corresponding channel is closed. In certain embodiments, other mechanical configurations can be used to displace or hide the actuating recess or recesses. In certain embodiments, the valves could be actuated by linear rather than rotational motion of the activating recess or recesses relative to the activation sites.

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In certain embodiments, the valve shown conceptually in FIG. 8A can be generalized into a “crossbar” valve that can connect any channel in one layer with any channel in a second layer. As shown in FIG. 8K, a planar actuator **802** contains an actuating recess **830** that can be moved in two orthogonal directions by an actuating device **870**. The ball cage and the balls **822** are between the actuator and the first fluidic layer **801**. A via layer **890** separates the first fluidic layer **801** from the second fluidic layer **891**. If the spacing between the channels and the balls in the cage is sufficient, the actuator recess can be moved from any location to any other location without actuating any valve between these two positions. This system could readily create a 100×100 ribbon-fluidic crossbar valve formed at the overlapping intersection of two 100-channel ribbon fluidics **801** and **891**. With adequate spacing between the channels in the ribbon fluidics **801** and **891**, it would also be possible to use a diagonal line or other array of multiple actuating recesses **830** in planar actuator **802** to create a two-dimensional Moiré pattern such that there is a unique X-Y location of **802** such that a particular one of the many recesses **830** would align with one of the many via valves created by the array of vias in the via layer **890**. In another embodiment, the use of multiple recesses **830** in actuator **802** could provide particular combinations of open and closed valves in a fluidic network. FIG. 8L shows the details of the protrusions that allow any multi-port via valve to be closed without blocking all downstream channels, including the overlap of the protrusion at the first valve position in the lower channel layer **801** (**801A**) with the protrusion at the first valve position in the upper channel layer **891** (**891A**), and the via that connects the two (**890AA**). Alternatively, a 100×100 crossbar valve could be implemented by having the 100 inputs **621** of the multi-port valve in FIG. 6C serve as the input to the 100×100 crossbar valve, with the output common port **680** being connected to the central input common port **680** of a second multi-port valve, whose 100 outputs **621** thereby address a different set of 100 fluidic lines, and this valve would also require two independent motors to specify the input and the output that would be connected to the common line connecting the two common ports **680**.

In another embodiment, a sliding roller actuator system as shown in FIG. 8M can use the cylindrical actuator concept of FIG. 8H to implement the X-Y control of a crossbar valve without the need to rely on traversing a single or multiple fixed actuator recesses **830** across the area of the valve. As shown in FIG. 8M, a cam motor **880** with a lead screw **882** drives the cam **883** to the position to apply pressure to the end **884** of a horizontally spring-loaded cylindrical actuator **855**. The rightward displacement of the cylindrical actuator **855** engages the pinion **854** on the threads of the horizontal axis control lead screw **885**. Activation of the motor **881** can then control the angular position of the cylindrical actuator **855**, allowing rotation without allowing any of the multiple actuating recesses **830** to engage any one of the via valves **822** in that horizontal row of the via valve array. Once the angular position of **855** has been selected to engage one and only one via valve, the cam **884** is moved away and the cylinder **855** returns to its original position to open the designated via valve. There is independent control of each horizontal valve set, as controlled by a single actuator **855**, and independent control of the vertical set of cylindrical actuators, allowing more than one valve to be open at a time.

In yet another embodiment, a concept of the lagging actuator as discussed above can also be used to create a single-motor, 25×25-port crossbar valve, as shown in FIG. 8N. A valve chip **801** contains two concentric circular arrays

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of 25 via valves **822**, all connected by a long common channel **820** that alternates between the inner and outer arrays, in a continuous series. Inner and outer actuator rings **886** and **887** each contain a single actuating recess **830** (black circle). The central motorized actuator **888** has a single protrusion that can cause the inner ring to rotate either clockwise or counterclockwise by engaging with the actuator protrusions **889** on the central actuator **888** and the rings **886** and **887**. A sequence of sequential clockwise and counterclockwise rotations of the central actuator **888** can cause the two actuator recesses **830** to be positioned over the selected inner and outer via valves. The use of multiple actuating rings could enable the lagging-actuator direct access of FIG. 7.

In each of the valves as described above, the compression structure is shown as a plurality of caged balls that are pressed into or released from a fluidic channel by an actuating surface with recesses. In other embodiments, the same functions could be performed using an actuator that engages either caged cylinders or other shapes, or fixed cantilevers or levers.

FIGS. 9A-9D show a bubble-tracking flow meter according to certain embodiments of the invention. The bubble-tracking flow meter can be realized using the pumps and valves in any of the embodiments and is not limited to those described above. As shown in FIG. 9A, the flow meter includes two light-transmission detecting devices separated by a known fixed distance, formed by light sources **910** and **920** and corresponding light detectors **940** and **950** located on the opposite sides of a fluidic channel or tube **930** to detect the presence or absence of a bubble in the channel or tube. A pump and valve (not shown) inject a bubble **960** that moves at a particular velocity along the channel between the two light-transmission detecting devices (FIGS. 9B-9D), where the leading or trailing edge of the bubble is used to trigger the detector circuitry (not shown) to determine the time it took for the injected bubble to traverse the distance between the detectors. The pump can reverse direction, return the bubble to its starting position, and send it across again at a different flow rate to calibrate the pump, or withdraw the bubble. In another embodiment, ultrasound could be used to detect the bubble.

FIG. 10 shows a bioreactor with gas delivery/exchange capabilities according to certain embodiments of the invention. As shown in FIG. 10, the layout of the bioreactor chamber **1001** is formed and perfused through an input port **1002**, a splitter network **1003**, a collector network **1004**, and an output port **1005**. In this embodiment, two gas exchange channels **1006** and **1007** flank the bioreactor chamber **1001**, the splitter network **1003**, and the collector network **1004**. In this instance the gas exchange channels **1006**, **1007** have a serpentine shape to increase the surface through which gases, fluids containing certain concentrations of gasses, or gasses with certain moisture levels flowing through channels **1006** and **1007** interact with the material from which the construct is made. The gas diffusing through said material will, in turn, interact with the bioreactor contents of the bioreactor chamber **1001**. In this embodiment, a gas concentration gradient may be established by sending different gases, or different concentrations of the same gas, through the two channels **1006** and **1007**. Alternatively, the gas composition in the channels **1006** and **1007** may be identical.

The foregoing description of the exemplary embodiments of the invention has been presented only for the purposes of illustration and description and is not intended to be exhaus-

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tive or to limit the invention to the precise forms disclosed. Many modifications and variations are possible in light of the above teaching.

The embodiments were chosen and described in order to explain the principles of the invention and their practical application so as to enable others skilled in the art to utilize the invention and various embodiments and with various modifications as are suited to the particular use contemplated. Alternative embodiments will become apparent to those skilled in the art to which the invention pertains without departing from its spirit and scope. Accordingly, the scope of the invention is defined by the appended claims rather than the foregoing description and the exemplary embodiments described therein.

What is claimed is:

1. A microfluidic system, being a tilted-actuator pump, and comprising:

a support plate;

a fluidic chip disposed on the support plate, wherein the fluidic chip has a fluidic network comprising at least one fluidic channel;

an actuator having a plurality of compression structures configured to roll against the fluidic chip to control the fluidic channel to switch between an open state and a closed state, wherein each of the compression structures is a roller; and

a motor shaft inserted in the actuator to drive the actuator to rotate relative to the fluidic chip;

wherein the actuator and the motor shaft are disposed to tilt from an actuator-contact surface of the fluidic chip, such that the actuator rotates in a plane tilted by an angle with respect to the actuator-contact surface of the fluidic chip.

2. The microfluidic system of claim 1, wherein: the motor shaft is perpendicular to the support plate, and the fluidic chip is a wedge-shaped fluidic chip, such that the actuator and the motor shaft are disposed to tilt from the actuator-contact surface of the wedge-shaped fluidic chip; or

the motor shaft is tilted and is not perpendicular to the actuator-contact surface of the fluidic chip and the support plate, such that the actuator and the motor shaft are disposed to tilt from the actuator-contact surface of the fluidic chip; or

the motor shaft is perpendicular to the support plate, and a passive wedge structure is disposed between the fluidic chip and the support plate, such that the fluidic chip is disposed to tilt from the support plate, and the actuator and the motor shaft are disposed to tilt from the actuator-contact surface of the fluidic chip.

3. The microfluidic system of claim 1, wherein the fluidic chip is a spiral pump chip comprising:

a first surface facing and fixed to the support plate; and a circular zone disposed on a second surface facing the actuator assembly, wherein each compression structure of the actuator rolls against the circular zone;

wherein each fluidic channel of the spiral pump chip is a spiral fluidic channel having an outer end outside the circular zone and an inner end within the circular zone, and each spiral fluidic channel partially aligns with the circular zone along a vertical direction, such that each compression structure rolls along the circular zone, compressing the portion of each spiral fluidic channel to pump a fluid inside each spiral fluidic channel.

4. The microfluidic system of claim 1, further comprising a bubble-tracking flow meter, comprising:

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two light-transmission detecting devices disposed on two locations of the fluidic channel of the fluidic chip, each of the two light-transmission detecting devices comprising:

a light source disposed on a first side of the fluidic channel, configured to emit light; and

a light detector disposed on a second, opposite side of the fluidic channel, configured to receive light emitted by the light source;

wherein a bubble injected in the fluidic channel is configured to trigger each of two light-transmission detecting devices, such that a flow rate of the fluidic channel is determined by measuring a triggering time difference between the two light-transmission detecting devices.

5. The microfluidic system of claim 1, further comprising a gas exchange bioreactor, comprising:

a chamber located between and in communication with an input port and an output port, wherein a bioreactor perfusion media is configured to pass through the chamber; and

a plurality of gas exchange channels surrounding the chamber, such that gas passing through the gas exchange channels is configured to diffuse through a material between the chamber and each gas exchange channel and to interact with a content of the chamber.

6. A microfluidic system, comprising:

a support plate;

a fluidic chip disposed on the support plate, wherein the fluidic chip has a fluidic network comprising at least one fluidic channel;

at least one compression structure, configured to compress or decompress the fluidic network within the fluidic chip;

an actuator, controlling the compression structure at a compression site; and

a motor shaft inserted in the actuator, configured to rotate the actuator relative to the fluidic chip, wherein the actuator controls the compression structure at the compression site to compress or decompress the fluidic channel at a particular location when the actuator rotates or moves,

wherein the actuator is an actuator assembly comprising:

a ball cup facing the fluidic chip, forming the receiving cavity between the ball cup and the fluidic chip,

wherein the at least one compression structure comprises a plurality of balls disposed in the receiving cavity and configured to roll against the fluidic chip;

a ball cage disposed between the balls; and

a traction disc disposed between the ball cup and the balls, configured to generate a traction force to compress the balls to roll against the fluidic chip.

7. The microfluidic system of claim 6, wherein the fluidic chip is a rotary peristaltic pump chip, each fluidic channel within the rotary peristaltic pump chip has a pumping channel interconnected with an output channel and an output bypass channel, and the at least one compression structure comprises a plurality of balls configured to roll against an outer surface of the pumping channel and to press a fluid in the pumping channel toward the output channel and the output bypass channel.

8. The microfluidic system of claim 6, further comprising a gas exchange bioreactor, comprising:

a chamber located between and in communication with an input port and an output port, wherein a bioreactor perfusion media is configured to pass through the chamber; and

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- a plurality of gas exchange channels surrounding the chamber, such that gas passing through the gas exchange channels is configured to diffuse through a material between the chamber and each gas exchange channel and to interact with a content of the chamber. 5
- 9.** A microfluidic system, comprising:
- a support plate;
 - a fluidic chip disposed on the support plate, wherein the fluidic chip has a fluidic network comprising at least one fluidic channel; 10
 - at least one compression structure, configured to compress or decompress the fluidic network within the fluidic chip;
 - an actuator, controlling the compression structure at a compression site; and 15
 - a motor shaft inserted in the actuator, configured to rotate the actuator relative to the fluidic chip, wherein the actuator controls the compression structure at the compression site to compress or decompress the fluidic channel at a particular location when the actuator 20 rotates or moves,
- wherein the fluidic chip is a spiral pump chip comprising:
- a first surface facing and fixed to the support plate; and
 - a circular zone disposed on a second surface facing the actuator assembly, wherein each compression structure of the actuator rolls against the circular zone; 25
- wherein each fluidic channel of the spiral pump chip is a spiral fluidic channel having an outer end outside the circular zone and an inner end within the circular zone, and each spiral fluidic channel partially aligns 30 with the circular zone along a vertical direction, such that each compression structure rolls along the circular zone, compressing the portion of each spiral fluidic channel to pump a fluid inside each spiral fluidic channel. 35
- 10.** The microfluidic system of claim 9, wherein the actuator is an actuator assembly comprising:
- a ball cup facing the fluidic chip, forming the receiving cavity between the ball cup and the fluidic chip,

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- wherein the at least one compression structure comprises a plurality of balls disposed in the receiving cavity and configured to roll against the fluidic chip;
 - a ball cage disposed between the balls; and
 - a traction disc disposed between the ball cup and the balls, configured to generate a traction force to compress the balls to roll against the fluidic chip.
- 11.** A microfluidic system, comprising:
- a support plate;
 - a fluidic chip disposed on the support plate, wherein the fluidic chip has a fluidic network comprising at least one fluidic channel;
 - at least one compression structure, configured to compress or decompress the fluidic network within the fluidic chip;
 - an actuator, controlling the compression structure at a compression site; a motor shaft inserted in the actuator, configured to rotate the actuator relative to the fluidic chip, wherein the actuator controls the compression structure at the compression site to compress or decompress the fluidic channel at a particular location when the actuator rotates or moves; and
 - a bubble-tracking flow meter, comprising two light-transmission detecting devices disposed on two locations of the fluidic channel of the fluidic chip, each of the two light-transmission detecting devices comprising:
 - a light source disposed on a first side of the fluidic channel, configured to emit light; and
 - a light detector disposed on a second, opposite side of the fluidic channel, configured to receive light emitted by the light source;
- wherein a bubble injected in the fluidic channel is configured to trigger each of two light-transmission detecting devices, such that a flow rate of the fluidic channel is determined by measuring a triggering time difference between the two light-transmission detecting devices.

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